Learning convex regularizers satisfying the variational source condition for inverse problems



1. BACKGROUND ON INVERSE PROBLEM

- Reconstruct image $x^* \in \mathbb{X}$ from noisy observation (data) $y^{\delta} = Ax^* + \text{noise} \in \mathbb{Y}.$
- $A : \mathbb{X} \to \mathbb{Y}$ is the forward operator.
- ▶ $\|\text{noise}\| \leq \delta$
- Inverse problems are ill-posed, i.e., A is either non-ir poorly conditioned.
- Variational regularization:

$$x_{\lambda} \in \operatorname*{arg\,min}_{x \in \mathbb{X}} \frac{1}{2} \|y^{\delta} - Ax\|_{2}^{2} + \lambda \psi_{\theta}(x)$$

► $\{\psi_{\theta}\}_{\theta \in \Theta}$ is a convex regularizer.

• ψ_{θ} -minimizing solution:

$$x^{\dagger} \in \mathop{\arg\min}_{x \in \mathbb{X}} \psi_{\theta}(x)$$
 subject to $Ax = y^{0}$

- Variational source condition: is satisfied if there ex $w^{\dagger} \in \mathbb{Y}$ such that $A^* w^{\dagger} \in \partial \psi_{\theta}(x^{\dagger})$.
- Bregman distance: $D_{\psi_{\theta}}(x_1, x_2) := \left\{ \psi_{\theta}(x_1) - \psi_{\theta}(x_2) - \langle u, x_1 - x_2 \rangle \middle| u \in \partial \psi_{\theta}(x_2) \right\}$
- **Convergence rate** [1]: If the source condition holds, each minimizer x_{λ} of (1), there exists $d \in D_{\psi_{\theta}}(x_{\lambda}, x^{\dagger})$

$$d \leqslant \lambda rac{\|w^{\dagger}\|^2}{2} + rac{\delta^2}{2\,\lambda}.$$

Therefore, choosing $\lambda \propto \delta$ leads to an $O(\delta)$ converge the variational reconstruction x_{λ} to x^{\dagger} .

2. PARAMETRIZING THE REGULARIZEF



- ψ_{θ} is constructed recursively by taking non-negative convex functions (starting from affine), and then appl (point-wise) monotonically-increasing convex activati
- The filter weights in the orange layers need to be ≥ 0 , whereas the blue layers can have any real-valued filters.
- The activation functions are taken to be leaky-ReLU with negative slope 0.2 (convex and monotone).

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IS	3. LEARNING THE REGUL
lata)	• Main idea: If A is invertible, source cond solution x of (1), the following holds: $\ell = (x; \Theta) = \prod (A^*)^{-1} \nabla d \log C$
nvertible or	 The smaller the quantity l_{sc}(x; θ) is, the r as a variational solution. Encourages the ground-truth images to the so variational problem.
(1)	 For non-invertible A, replace the inverse pseudo-inverse. Training loss:
(2)	$L(\theta) = \frac{1}{n} \sum_{i=1}^{n} \psi_{\theta}(x_i) - \frac{1}{n} \sum_{i=1}^{n} \psi_{\theta}(z_i) + \lambda_{g}$
xists some $_{\theta}(x_2)$	 x_i: ensemble of clean images z_i = A[†]y_i^δ: ensemble of noisy images L_{gp}: soft gradient penalty to enforce 1-Lipschitz Can solve the variational problem with th sub-gradient or Bregman iterations [4].
, then for such that	4. NUMERICAL EXAMPLES: D
(3) ence rate of	true noisy ACR-SC (GD
2	true noisy ACR-SC (GD
XN) [2, 3].	
$z_{L+1} \qquad \qquad$	true noisy ACR-SC (GD)
sums of olying a tion.	 λ_{sc} = 2.0, λ_{gp} = 10.0 The average PSNR and SSIM over 100 r images: noisy: 13.93 ± 0.13 dB, 0.51 ± 0.08 ACR-SC (GD): 22.72 ± 0.64, 0.77 ± 0.04 ACR-SC (Bregman): 20.29 ± 0.88, 0.86 ± 0.03

gradient-descent. Bregman iterations perform better in terms of recovering the contrast while yielding effective denoising.

ULARIZER

ondition dictates that for any

$||\psi_{\theta}(x)|| < \infty$

e more suitable x would be

solution of the resulting

se with the Moore-Penrose

$$\lambda_{gp}L_{gp}(\theta) + \lambda_{sc}L_{sc}(\theta)$$
 (4)

hitz bound on
$$\psi_{\theta}$$

the learned regularizer via

DENOISING



0 randomly chosen test

• Took $\lambda = 25$ for the Bregman technique and $\lambda = 5$ for vanilla

5. CT RECONSTRUCTION EXPERIMENTS

• Experiments on Mayo-clinic low-dose CT data (2016):

- Extracted 2D slices of size 512×512 from 3D scans.

- 4. No. of learnable parameters in ψ_{θ} : 590928.
- optimizer with η , β_1 , $\beta_2 = 10^{-5}$, 0.90, 0.99.





(a) ground-truth

(b) FBP: 21.19, 0.22



(e) LPD: 35.76, 0.92



(f) AR: 33.52, 0.86

• ACR-SC is only marginally inferior to ACR, while it still total-variation (TV).

- regularizer satisfying the source condition.
- Unsupervised learning, no paired data needed.
- variational problem.
- Theoretical grounding for Bregman iterations.
- drop in reconstruction quality.

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AMBRIDGE IMAGE ANALYSIS

2. Trained on 9 patients (2250 slices), evaluated on one (128 slices).

3. Parallel-beam projection, 200 angles, 400 lines/angle, Gaussian noise with $\sigma_e = 2.0$ (25 dB of signal-to-noise ratio in the data space).

5. $\lambda_{sc} = 2.0$ and $\lambda_{gp} = 5.0$, trained for 10 epochs, batch-size was four. Adam







(g) ACR: 31.24, 0.86 outperforms classical model-based methods such as

6. SUMMARY

• Developed a novel training loss for learning a data-driven convex

• Possible to derive convergence rate estimates for the resulting

• Enforcing the source condition does not lead to any significant

REFERENCES

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(d) U-net: 34.42, 0.90



(h) ACR-SC: 30.93, 0.85