

# ENHANCING FOREGROUND BOUNDARIES FOR MEDICAL IMAGE SEGMENTATION

Dong Yang\*, Holger Roth, Xiaosong Wang, Ziyue Xu, Andriy Myronenko, Daguang Xu

\* [dongy@nvidia.com](mailto:dongy@nvidia.com)





# MEDICAL IMAGE SEGMENTATION

## Motivation

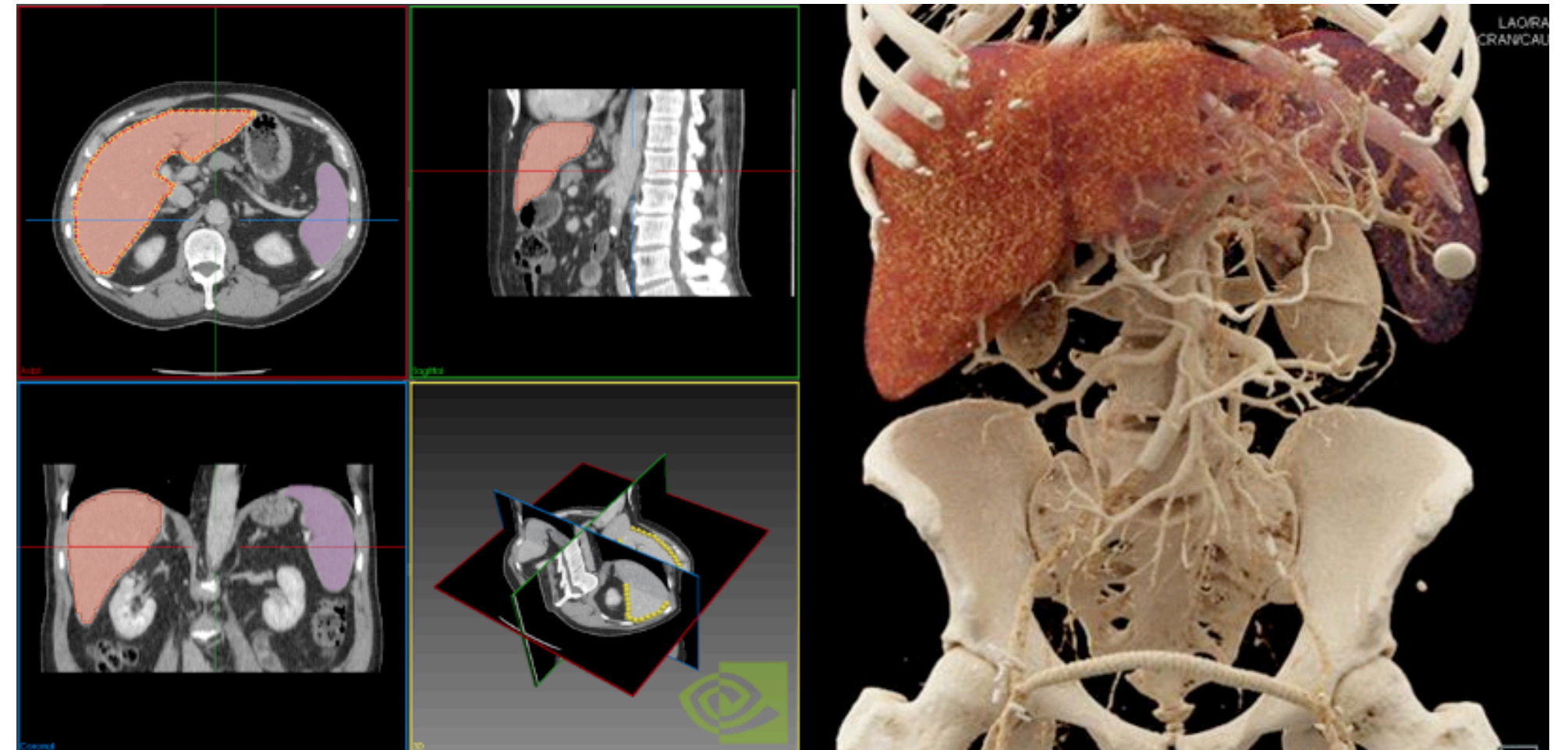
- What?
  - **Pixel-wise classification** in 2D / 3D / 4D medical images
  - Gaining high-level understanding from high-dimensional medical images
- Why?
  - Potentially helpful for disease diagnosis, treatment planning, and surgery planning
- How?
  - **Deep learning (deep neural networks)** with large-scale labeled datasets

# CASE STUDY

## 3D Medical Image Segmentation

Given 3D volumes (e.g. CT, MRI) as input, extracting 3D anatomical structures of organs or tumors

- Challenge - fine-grained details (boundaries)
  - Caused by fuzzy imaging quality, motion blurring, etc.



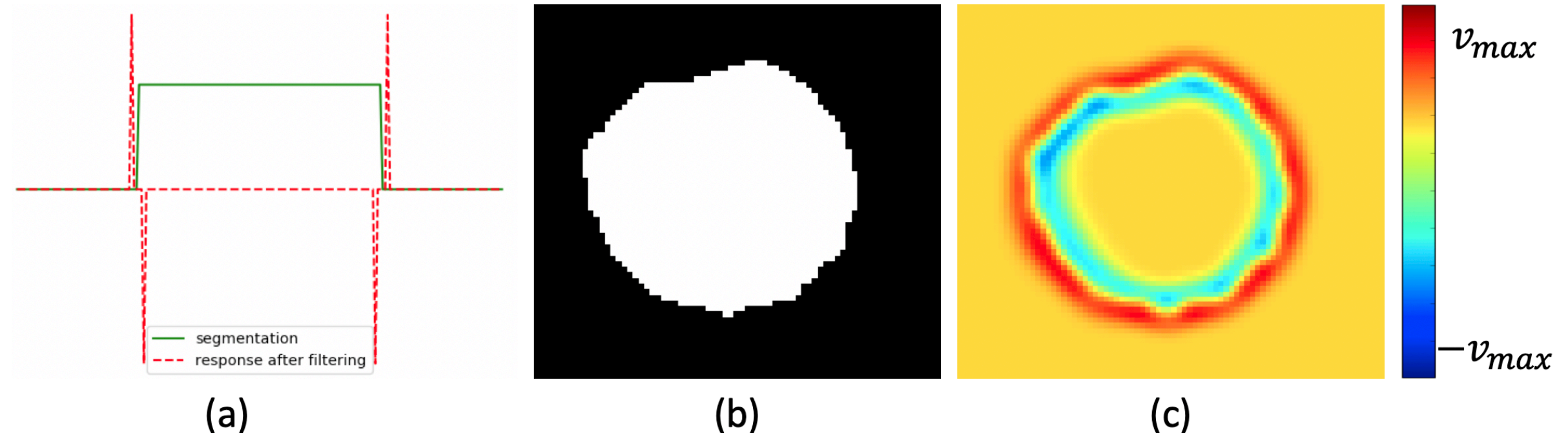
# METHODOLOGY

## A Novel Boundary Regularization in Optimization

a) Laplacian filtering on 1D cross-section of binary mask (red curve indicates filtered response)  $\mathcal{L}(x, y, z) = \frac{\partial^2 S}{\partial x^2} + \frac{\partial^2 S}{\partial y^2} + \frac{\partial^2 S}{\partial z^2}$

b) Ground truth label (binary mask)

c) Filtered result of ground truth label



Advantage

Laplacian filtering can be fully implemented as non-trainable convolutional operations

# METHODOLOGY

## A Novel Boundary Regularization in Optimization

### Optimization objectives

- 1) Distance between prediction and ground truth label - focusing on global structure
- 2) Distance between filtered prediction and filtered ground truth label - focusing on boundary details

$$l_{\text{overall}} = \lambda_1 \cdot l_{\text{dice}} + \lambda_2 \cdot l_{\text{BE}}$$

$$l_{\text{BE}} = \|\mathcal{L}(\mathcal{F}(X)) - \mathcal{L}(Y)\|_2 = \left\| \frac{\partial^2 (\mathcal{F}(X) - Y)}{\partial x^2} + \frac{\partial^2 (\mathcal{F}(X) - Y)}{\partial y^2} + \frac{\partial^2 (\mathcal{F}(X) - Y)}{\partial z^2} \right\|_2$$

# EXPERIMENTS

## Datasets and Performance

Datasets - [Medical Segmentation Decathlon](#) (MSD)

Task 01 - brain tumor segmentation in 3D MRI

Task 09 - spleen (body) segmentation in 3D CT

Baseline model - 3D SegResNet ([Myronenko, 2018](#))

Table 1: Validation Dice comparison with baseline approaches and proposed approach.

Method	Task01	Task09
U-Net ( <a href="#">Ronneberger et al., 2015</a> )	0.72	0.94
AH-Net ( <a href="#">Liu et al., 2018</a> )	0.81	0.95
SegResNet ( <a href="#">Myronenko, 2018</a> )	0.83	0.95
( <a href="#">Myronenko, 2018</a> )+Boundary Loss ( <a href="#">Kervadec et al., 2018</a> )	<b>0.85</b>	0.94
( <a href="#">Myronenko, 2018</a> )+Focal Loss ( <a href="#">Zhu et al., 2019</a> )	0.85	0.95
( <a href="#">Myronenko, 2018</a> )+Proposed BE Loss	<b>0.85</b>	<b>0.96</b>

# EXPERIMENTS

## Visual Comparison of Spleen Segmentation

- Green contour is ground truth label
- Blue contour is the result applying ([Myronenko, 2018](#))
- Yellow contour is from the proposed work





# CONCLUSIONS

## Discussion and Findings

- Boundary enhancement enhanced overall quality of segmentation;
- Enhancement helps for segmentation of both structural and non-structural anatomy (e.g. organ, tumor);
- Boundary regularization in objective is light-weight with minimal increase of computing resource.





THANK YOU!  
QUESTIONS?

