

Breaking Speed Limits with Simultaneous Ultra-Fast MRI Reconstruction and Tissue Segmentation



Paper #239



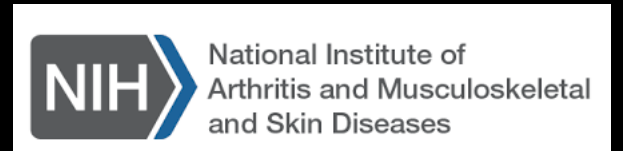
Francesco Calivà, Andrew P. Leynes, Rutwik Shah, Upasana U. Bharadwaj,
Sharmila Majumdar, Peder E. Z. Larson, Valentina Pedoia

Disclosure

I have no financial interests or relationships to disclose with regard to the subject matter of this presentation.

Funding source

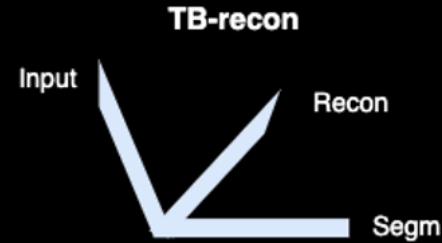
This project was supported by R00AR070902 from the National Institute of Arthritis and Musculoskeletal and Skin Diseases, National Institutes of Health, (NIH-NIAMS).



Deep Learning in Magnetic Resonance Imaging (MRI)

- Long scanning time is the **main** limitation of MRI
- We devised a DL framework for **MRI reconstruction and segmentation** from highly undersampled MRIs
- We bridged image reconstruction and analysis by proposing a **task-based** reconstruction approach

Input: 1.5× AF

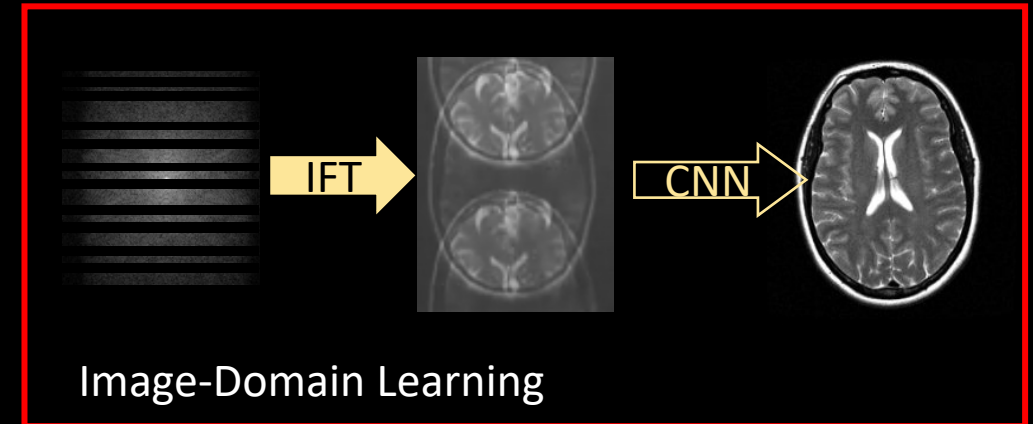


Reconstruction + Segmentation



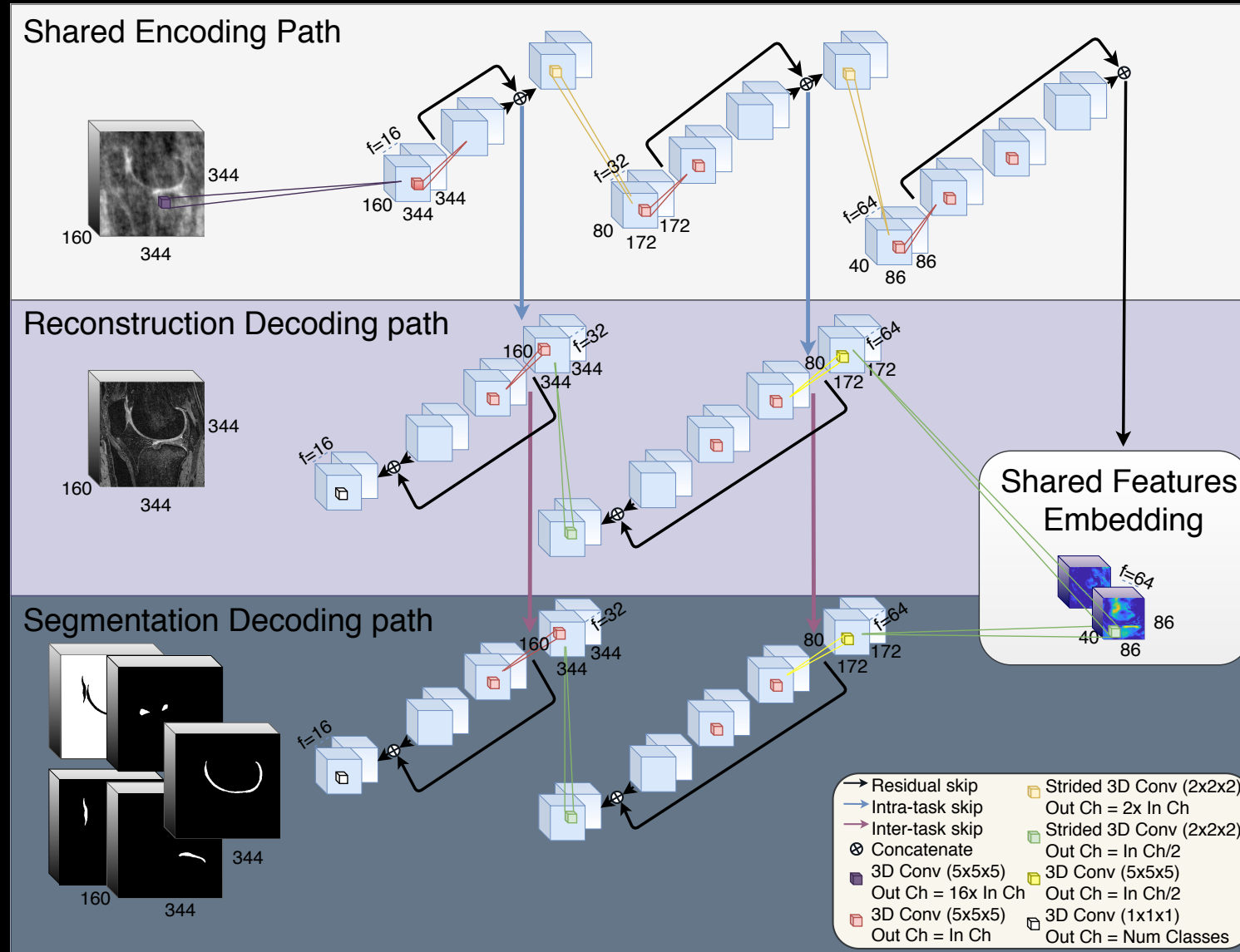
Hypotheses:

- Reconstruction in the image-domain provides higher data **interpretability** over k-space
- Reconstruction and segmentation are similar and related tasks

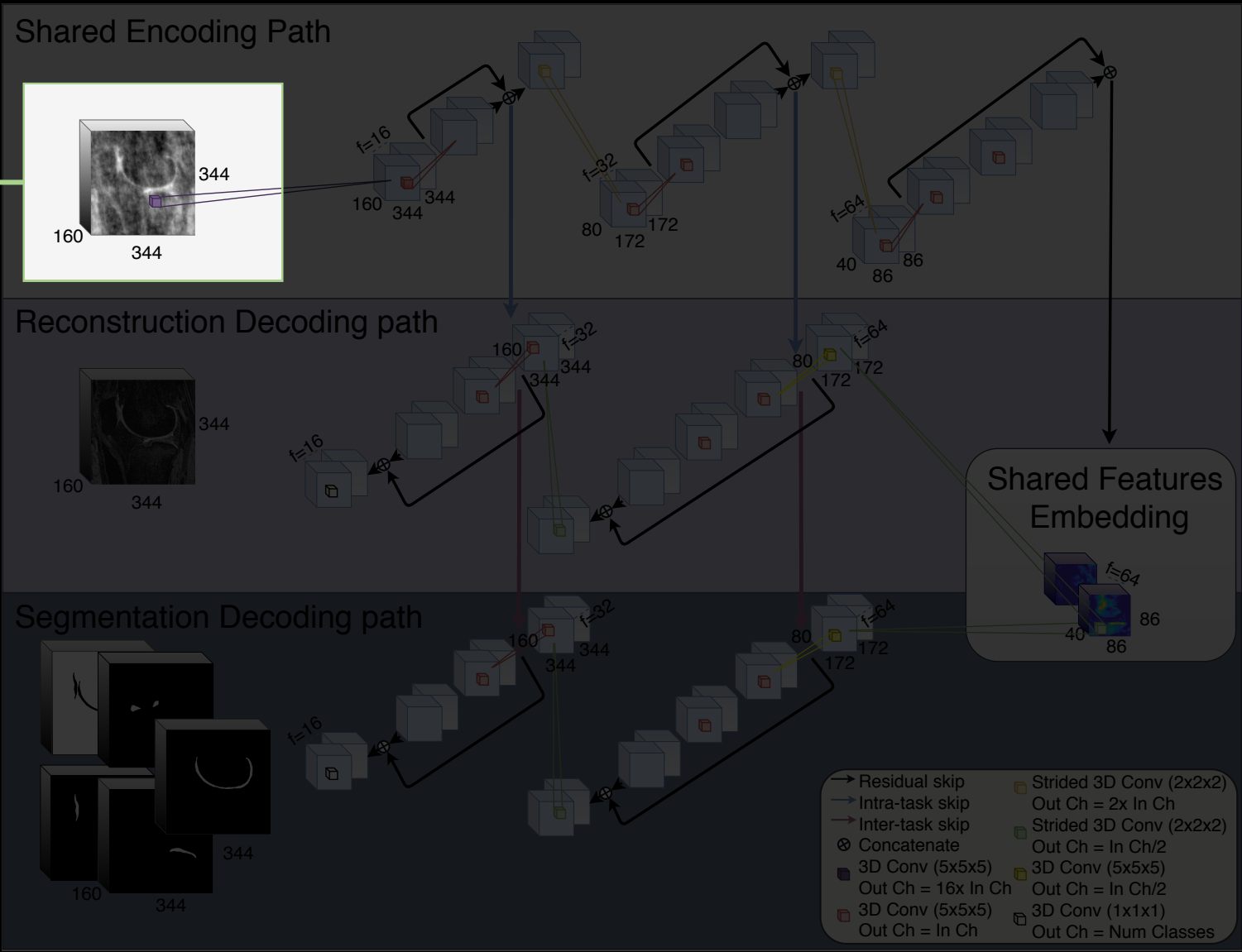


Simultaneous segmentation and image reconstruction

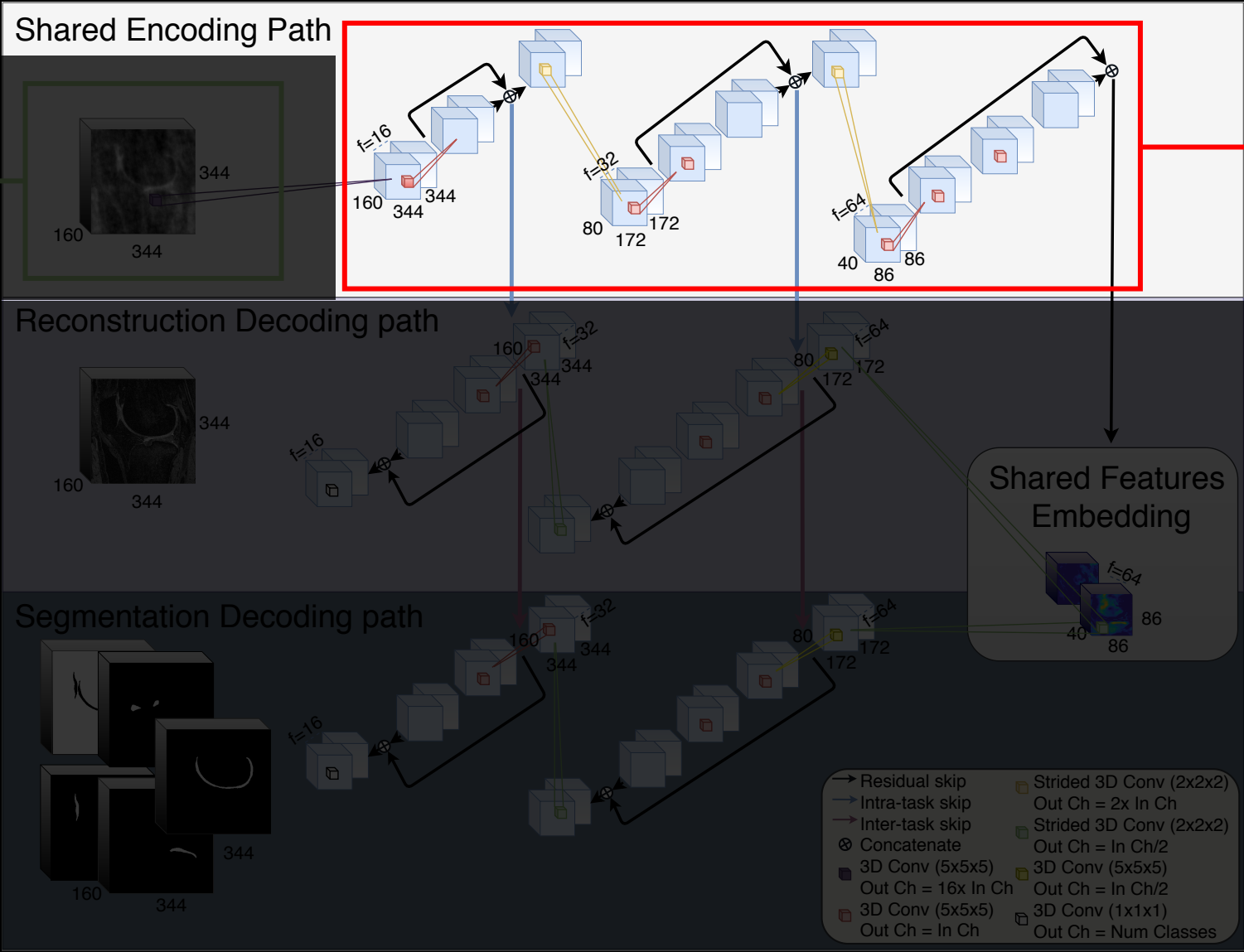
Proposed approach: Task-based image reconstruction: TB-recon



Input:
zero-filled MRI

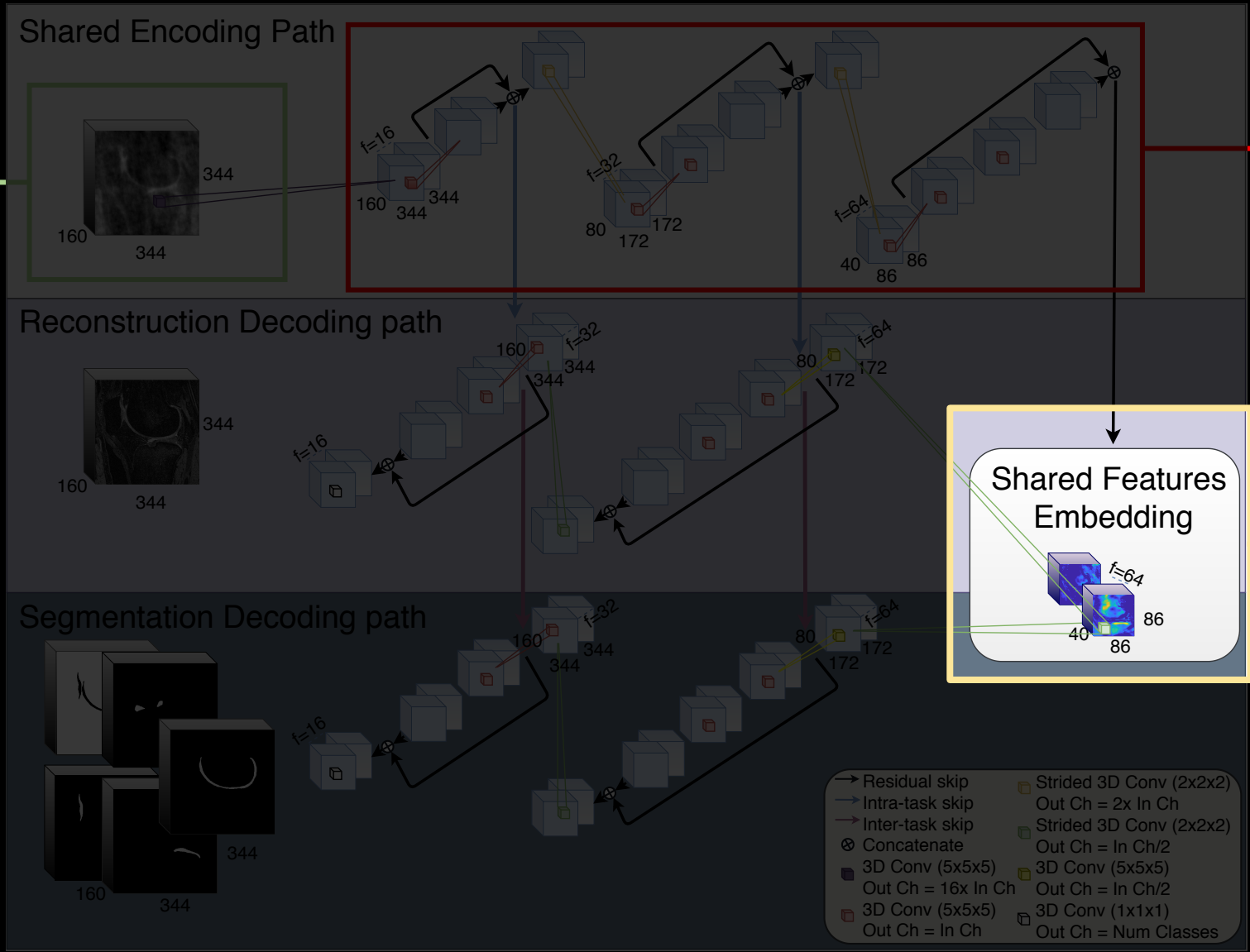


Input:
zero-filled MRI



shared encoder

Input:
zero-filled MRI

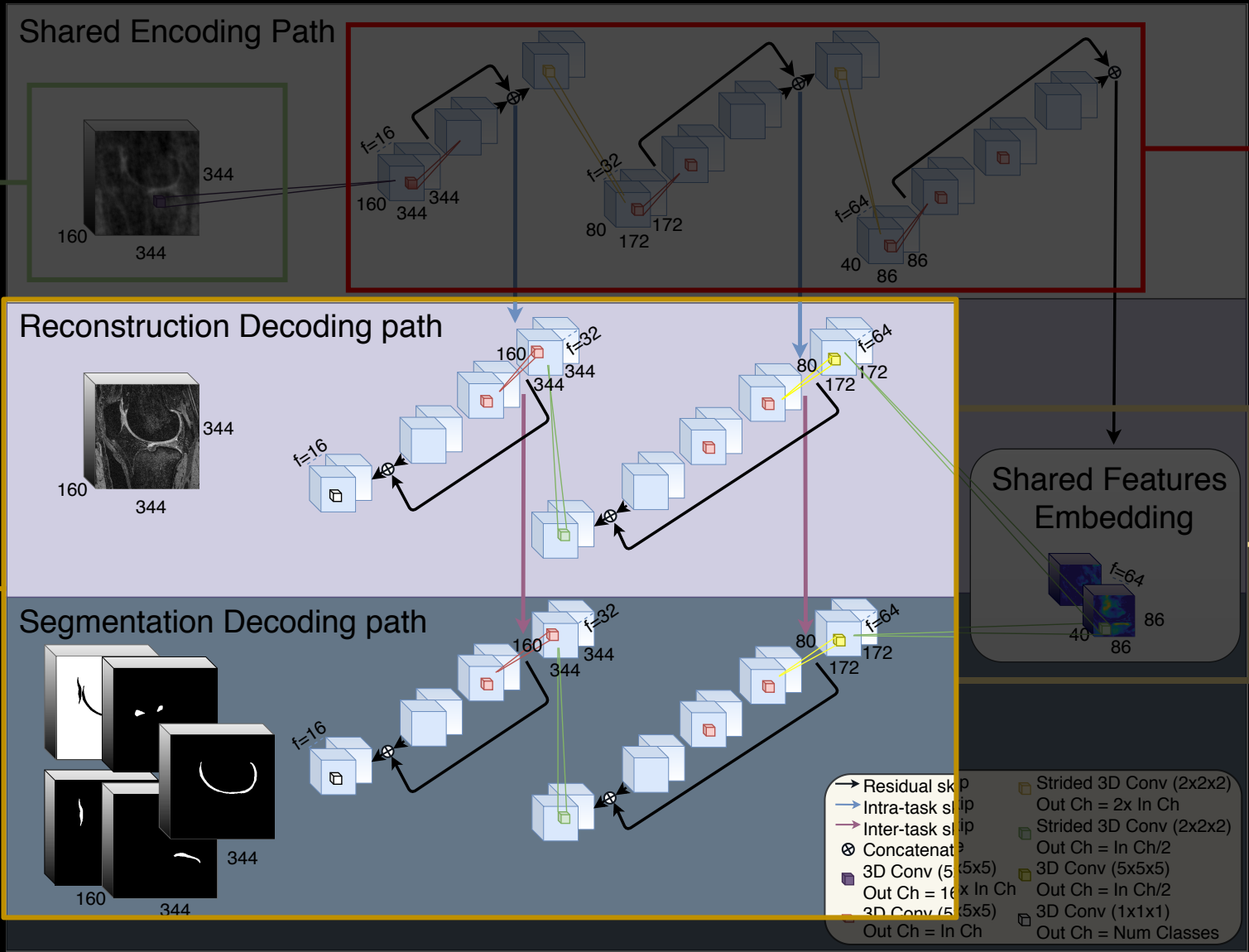


shared encoder

Common
Feature
Embedding

Input:
zero-filled MRI

2 decoders

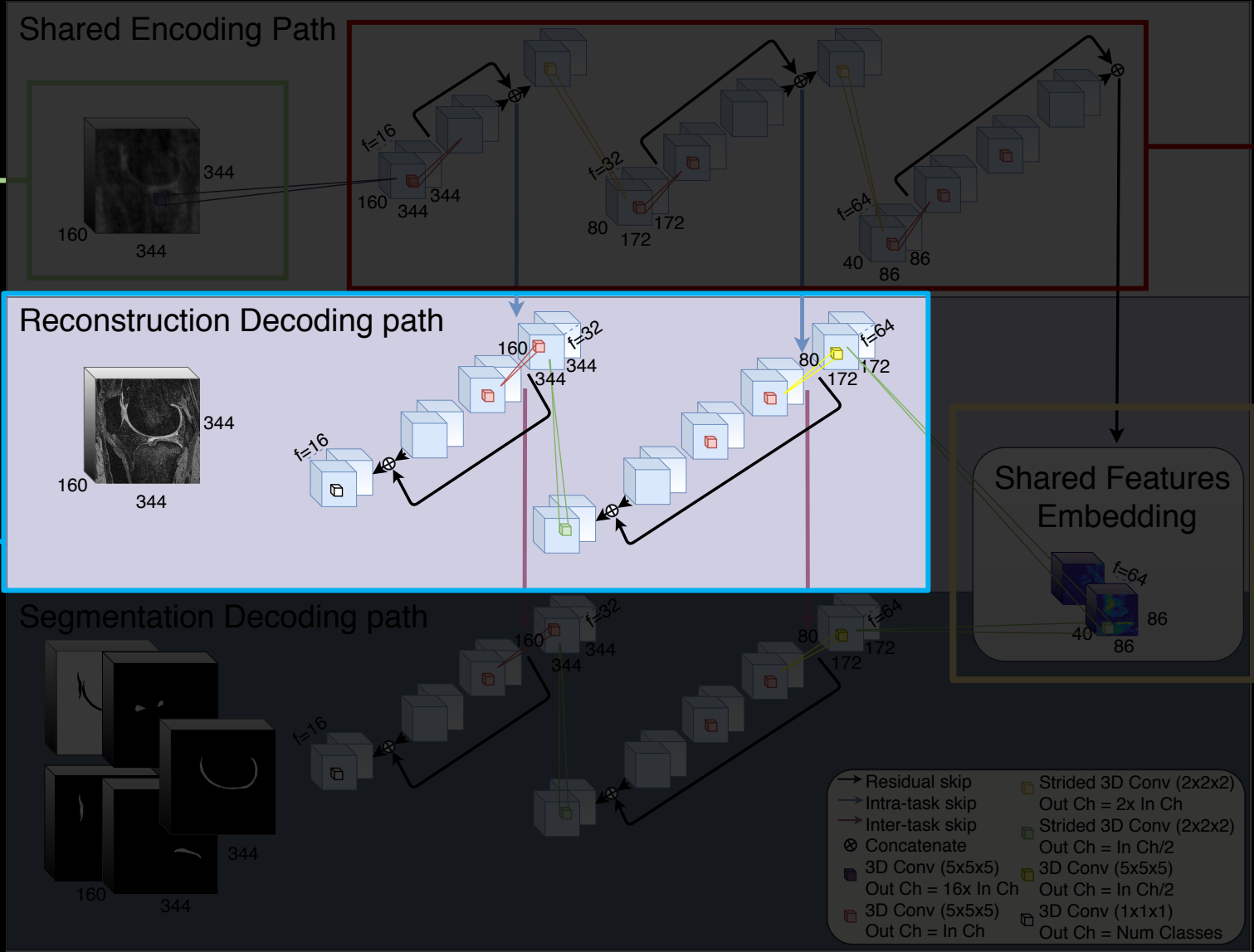


shared encoder

Common
Feature
Embedding

Input:
zero-filled MRI

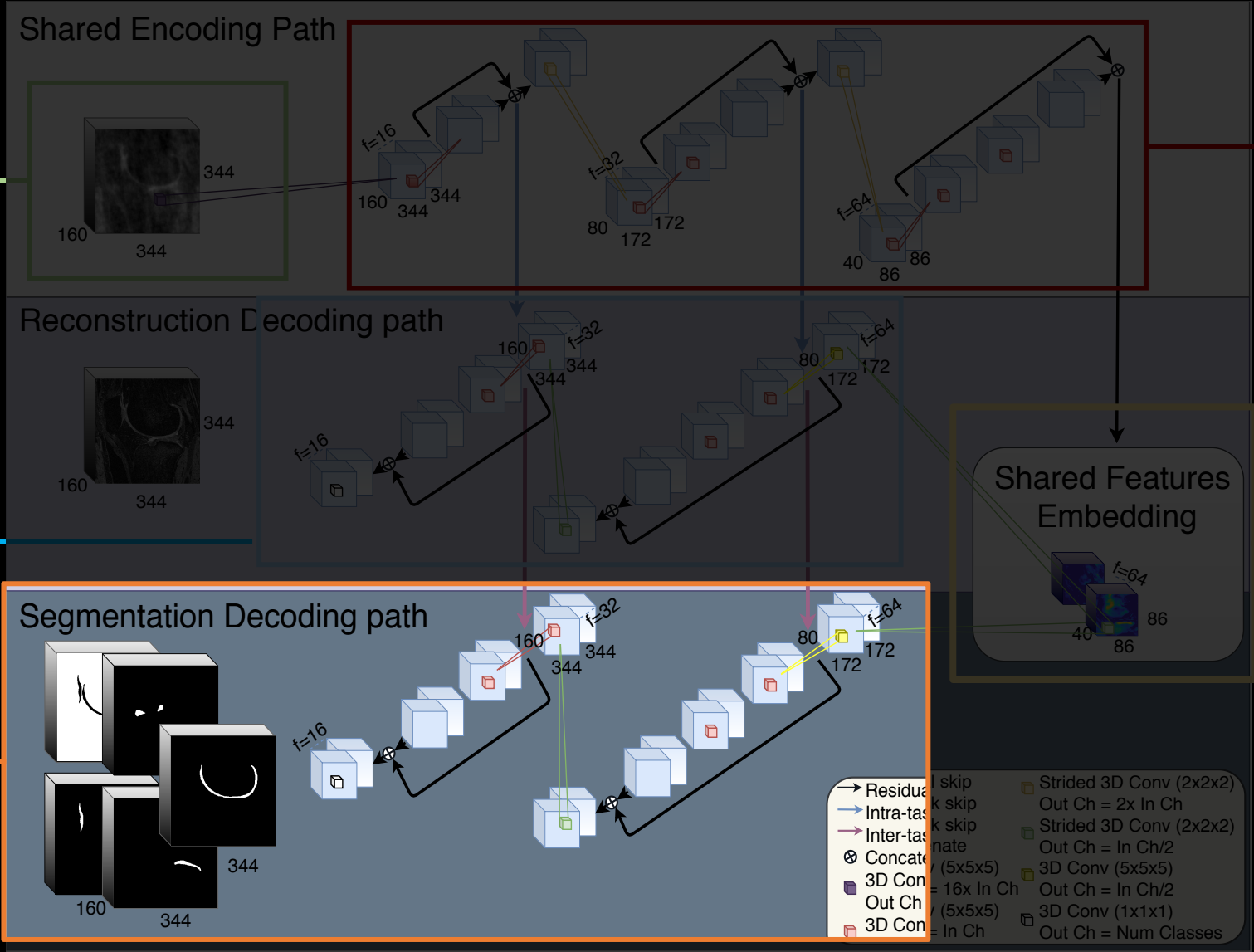
reconstruction
decoder



Input:
zero-filled MRI

reconstruction
decoder

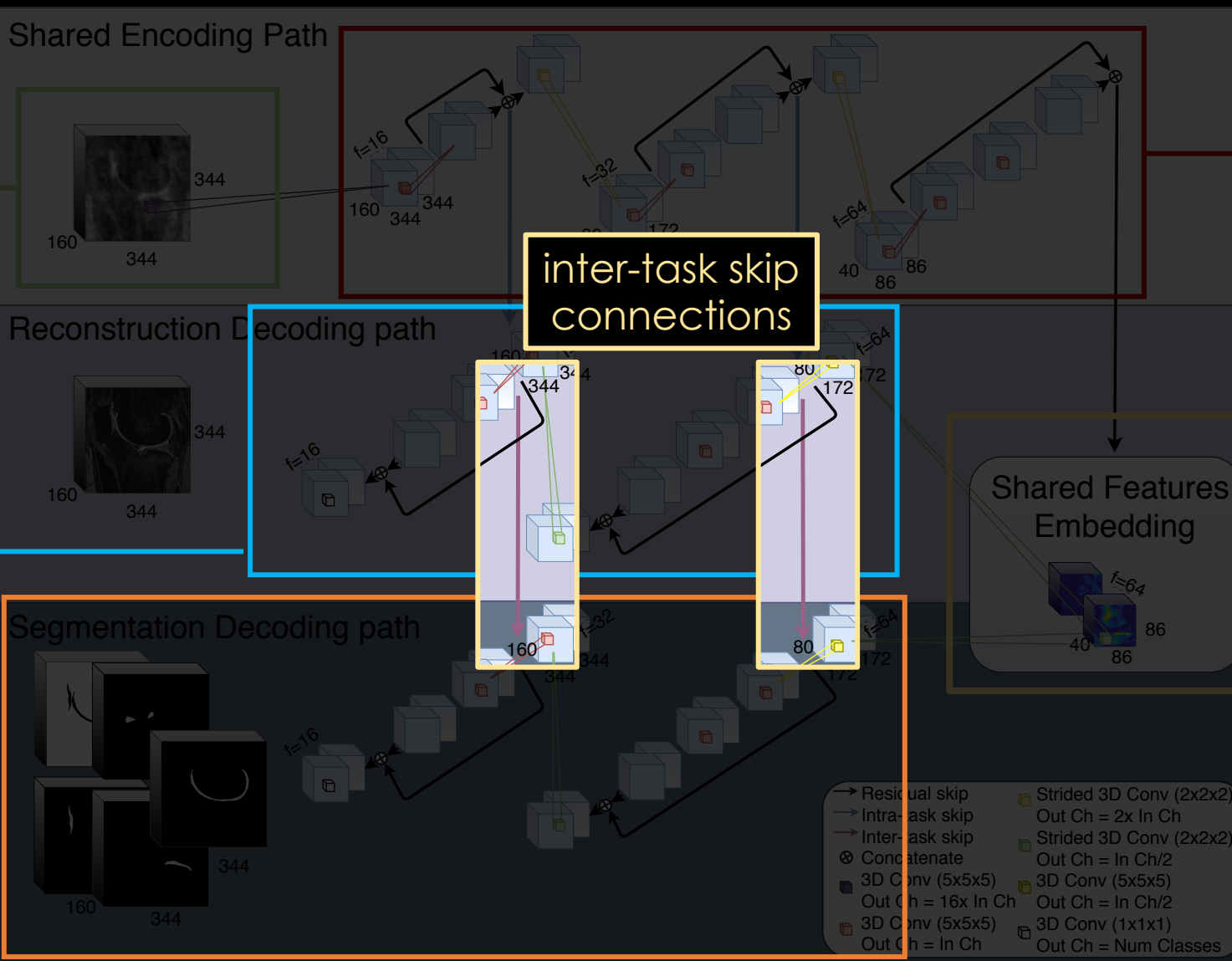
segmentation
decoder



Input:
zero-filled MRI

reconstruction
decoder

segmentation
decoder
output: softmax
activation



shared encoder

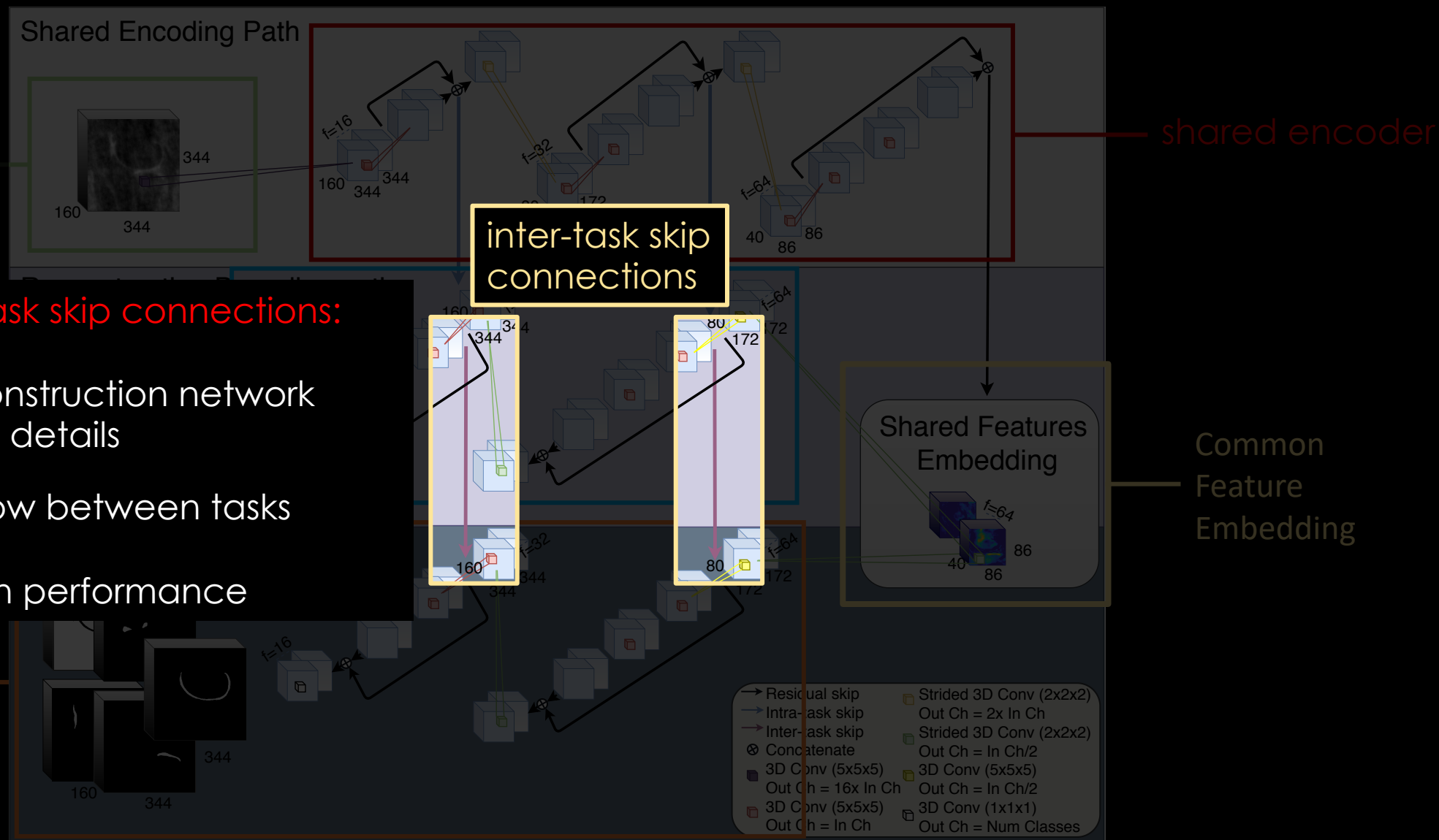
Common
Feature
Embedding

input:
zero-filled MRI

Advantages of inter-task skip connections:

- Features in the reconstruction network better describe fine details
- Facilitate feature flow between tasks
- Better segmentation performance

decoder
output: softmax
activation



End-to-end network training

- Undersampled zero-filled MRI denoising and tissue segmentation
- A multi-task loss is minimized

$$\begin{aligned}\mathcal{L}_{TB-recon} &= \mathcal{L}_{recon} + \alpha \cdot \mathcal{L}_{segm} \\ \mathcal{L}_{recon} &= 1 - SSIM(\hat{y}_{recon}, y_{recon}) + \beta \cdot MAE(\hat{y}_{recon}, y_{recon}) \\ \mathcal{L}_{segm} &= 1 - DICE(\hat{y}_{segm}, y_{segm}) + \gamma \cdot NLL(\hat{y}_{segm}, y_{segm})\end{aligned}$$

with α , β and γ empirically set to 1, 6.67^[2] and 0.01 respectively

- Monitored metric: Dice Similarity Coefficient (DSC)

^[1] Milletari, F., et al. "V-net: Fully convolutional neural networks for volumetric medical image segmentation." Fourth International Conference on 3DV. IEEE, 2016.

^[2] Zhao, H., Gallo, O., Frosio, I., & Kautz, J. (2016). Loss functions for image restoration with neural networks. *IEEE Transactions on computational imaging*, 3(1), 47-57.

Network trained end-to-end

- The network is trained for 500k iterations
- 20 epochs early-stopping
- 5% dropout rate^[3]
- Adam optimizer^[4] (learning rate = 1E-5)
- NVIDIA V100 32GB GPU
- Python 3.6.5 and Tensorflow 1.12

^[3] Srivastava, N., Hinton, G., Krizhevsky, A., Sutskever, I., & Salakhutdinov, R. (2014). Dropout: a simple way to prevent neural networks from overfitting. The journal of machine learning research, 15(1), 1929-1958.

^[4] Kingma, D. P., & Ba, J. (2014). Adam: A method for stochastic optimization. arXiv preprint arXiv:1412.6980.

Imaging data

- 174 knees from 87 participants to the Osteoarthritis Initiative study (OAI)^[5]
- 3D sagittal double-echo steady-state (DESS) MRI scans
- Acquisition parameters:
 - 3.0T Siemens Trio at two time points.
 - TR 16.2ms
 - TE 4.7ms
 - FOV 14cm
 - Readout bandwidth 185kHz
 - Matrix size 384x384x160
 - Resolution 0.364x0.364x0.7mm

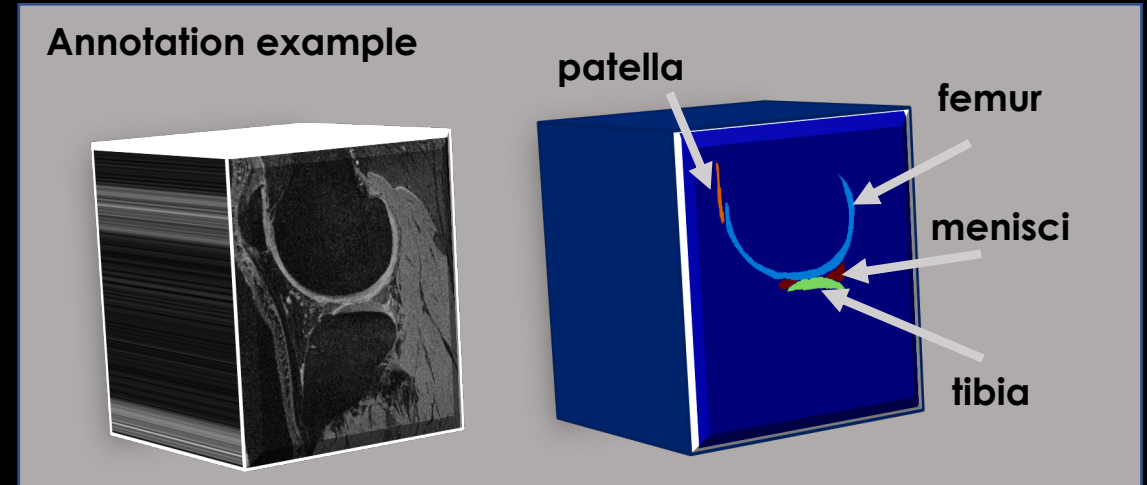


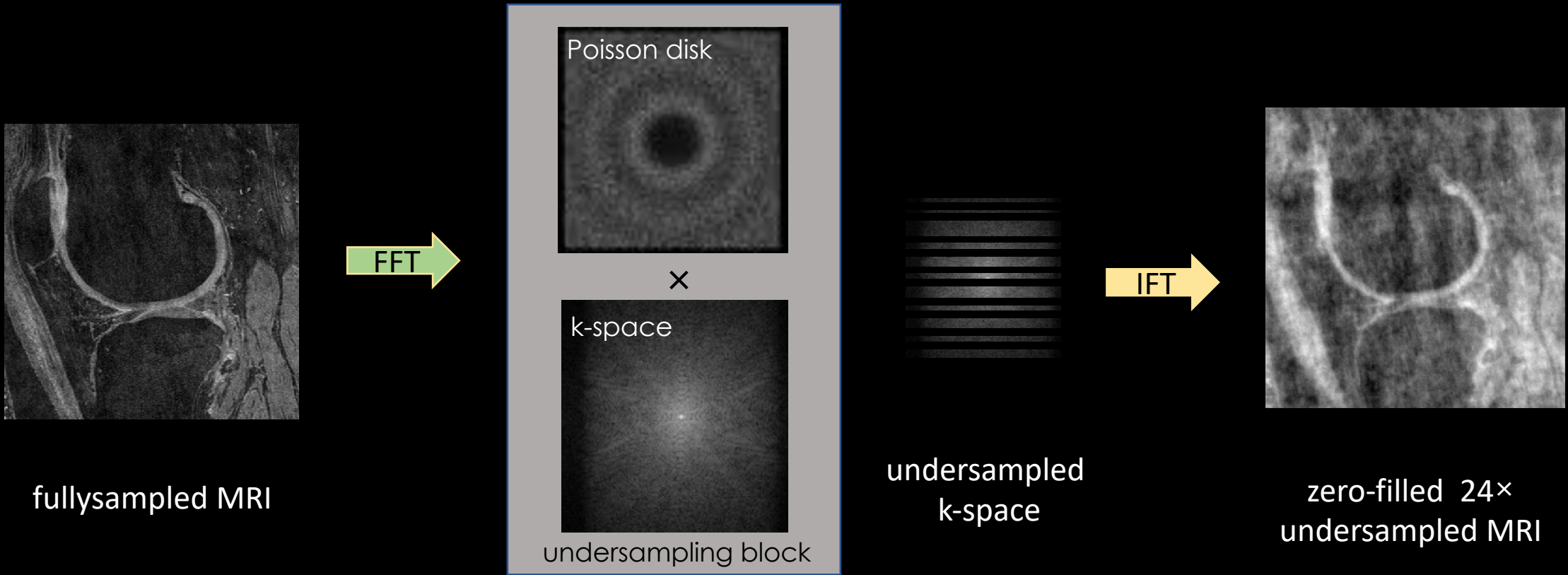
Table 1 Population attributes distribution in training validation and test splits. Race is reported in non-White/White or Caucasian/Black or African American/Asian order; sex in male/female order.

| | Training | Validation | Test |
|--------------------------|------------|------------|------------|
| Age | 59.37±9.09 | 58.57±9.51 | 70.86±7.40 |
| BMI [kg/m ²] | 30.49±4.21 | 33.30±6.01 | 31.23±3.90 |
| Race | 1/47/11/0 | 0/8/6/0 | 1/13/0/0 |
| Sex | 28/31 | 8/6 | 9/5 |

^[5] Peterfy, C. G., Schneider, E., & Nevitt, M. (2008). The osteoarthritis initiative: report on the design rationale for the magnetic resonance imaging protocol for the knee. *Osteoarthritis and cartilage*, 16(12), 1433-1441.

Retrospective undersampling

- Variable-density Poisson disk undersampling mask^[6]
- 5 acceleration factors (AF) 2x, 4x, 6x, 12x, 24x
- Retrospective undersampling performed using the SigPy software^[7]

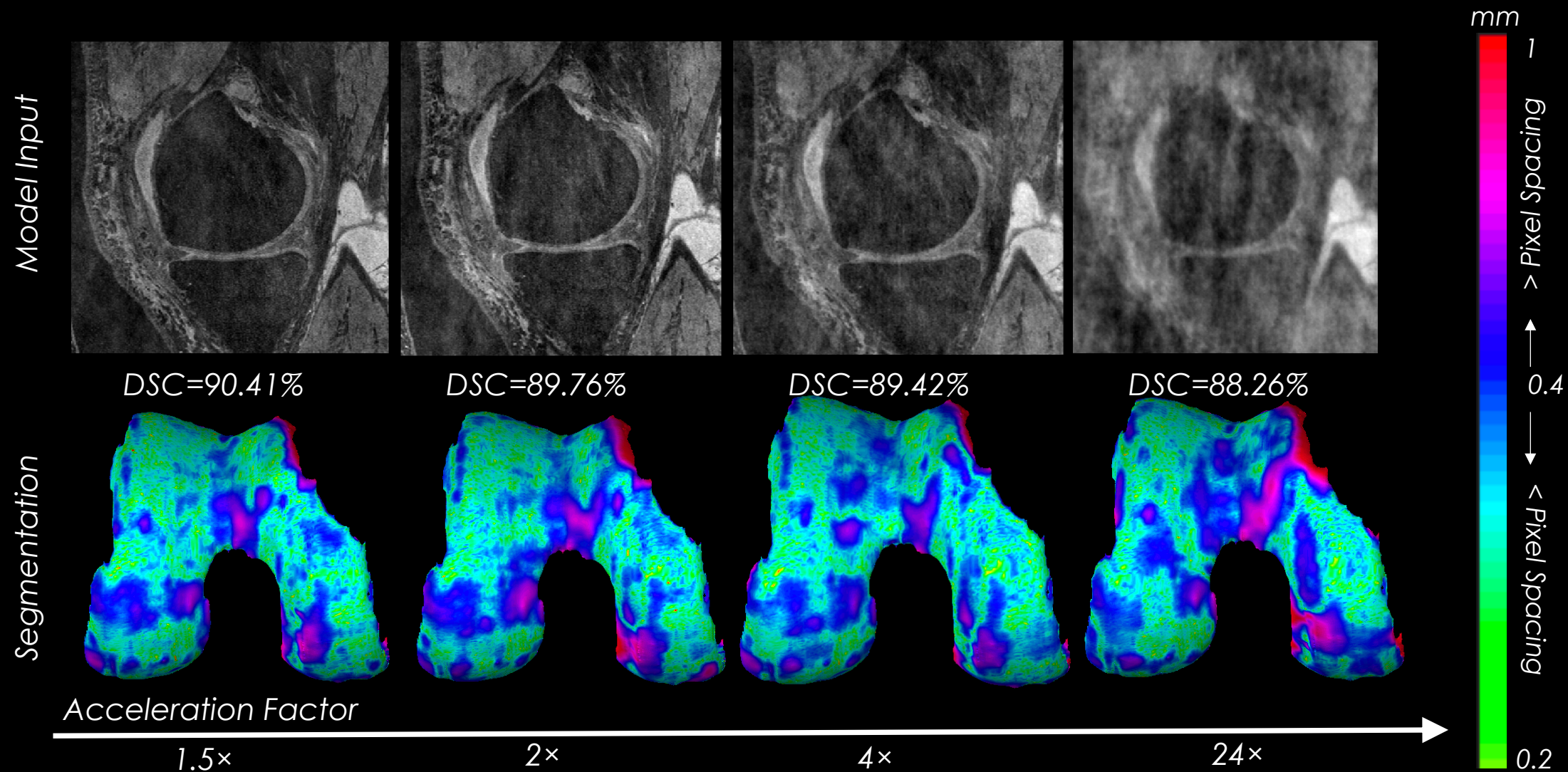


^[6] Bridson, R.. "Fast Poisson disk sampling in arbitrary dimensions." SIGGRAPH sketches. 2007.

^[7] <http://indexsmart.mirasmart.com/ISMRM2019/PDFfiles/4819.html>

Results – TB-recon's femoral cartilage segmentation

Point by Point distance between automatic and manual segmentation



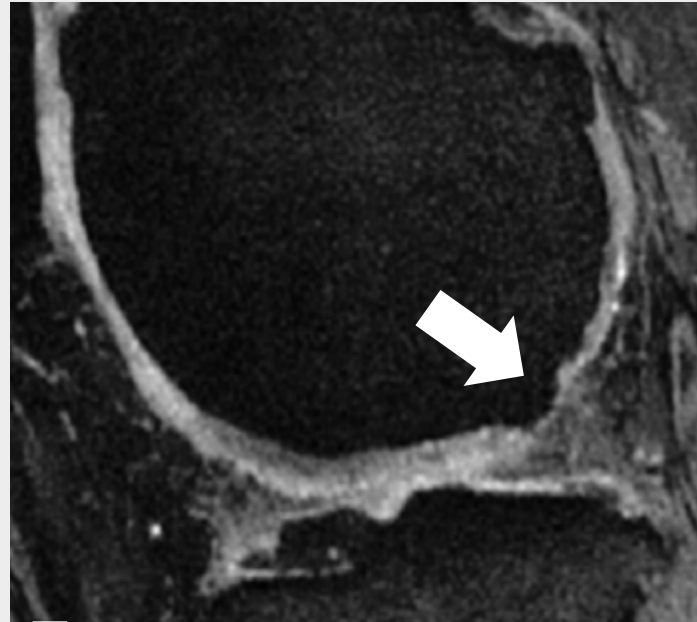
Results – TB-recon Reconstruction

Bone marrow edema visible in a sagittal DESS (A), is well observed at 6× (B) and 12× (B) AFs reconstructed MRIs

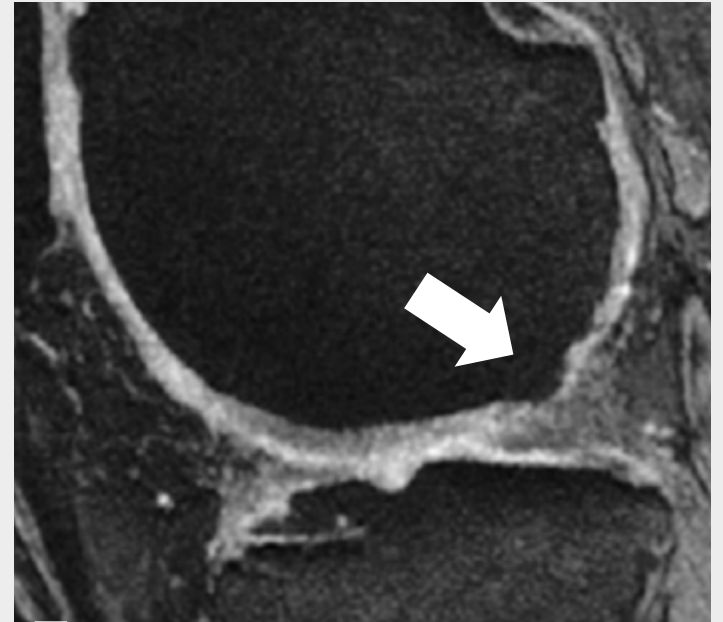
DESS



AF=6×



AF=12×



Results – Ablation study

Investigated importance of:

- MRI reconstruction
- Inter-task skip connections

| Femur - DSC | 4× | 6× | 24× |
|-----------------|-------------------|-------------------|-------------------|
| <i>TB-recon</i> | 87.33±1.93 | 87.58±1.79 | 85.63±2.56 |

| Tibia - DSC | 4× | 6× | 24× |
|-----------------|-------------------|-------------------|-------------------|
| <i>TB-recon</i> | 85.12±3.85 | 86.18±3.59 | 85.84±3.51 |

| Patella - DSC | 4× | 6× | 24× |
|-----------------|-------------------|-------------------|-------------------|
| <i>TB-recon</i> | 82.10±6.83 | 81.76±7.82 | 77.65±7.96 |

| Menisci - DSC | 4× | 6× | 24× |
|-----------------|-------------------|-------------------|-------------------|
| <i>TB-recon</i> | 84.91±2.79 | 83.78±3.06 | 82.28±2.64 |

Results – Ablation study

No MRI reconstruction

| Femur - DSC | 4× | 6× | 24× |
|--------------------|-------------------|-------------------|-------------------|
| <i>TB-recon</i> | 87.33±1.93 | 87.58±1.79 | 85.63±2.56 |
| <i>zero-filled</i> | 82.27±2.75 | 81.79±2.73 | 16.27±0.91 |

| Tibia - DSC | 4× | 6× | 24× |
|--------------------|-------------------|-------------------|-------------------|
| <i>TB-recon</i> | 85.12±3.85 | 86.18±3.59 | 85.84±3.51 |
| <i>zero-filled</i> | 83.32±4.53 | 81.26±5.20 | 29.75±1.80 |

| Patella - DSC | 4× | 6× | 24× |
|--------------------|-------------------|-------------------|-------------------|
| <i>TB-recon</i> | 82.10±6.83 | 81.76±7.82 | 77.65±7.96 |
| <i>zero-filled</i> | 78.10±7.17 | 77.37±6.47 | 70.88±10.59 |

| Menisci - DSC | 4× | 6× | 24× |
|--------------------|-------------------|-------------------|-------------------|
| <i>TB-recon</i> | 84.91±2.79 | 83.78±3.06 | 82.28±2.64 |
| <i>zero-filled</i> | 81.87±2.99 | 81.61±3.15 | 16.69±0.93 |

bold = significant
outperformance

Results – Ablation study

No MRI reconstruction

| Femur - DSC | 4× | 6× | 24× |
|--------------------|-------------------|-------------------|-------------------|
| <i>TB-recon</i> | 87.33±1.93 | 87.58±1.79 | 85.63±2.56 |
| <i>zero-filled</i> | 82.27±2.75 | 81.79±2.73 | 16.27±0.91 |
| <i>naïve</i> | 84.97±2.69 | 82.94±2.99 | 83.71±2.82 |

| Tibia - DSC | 4× | 6× | 24× |
|--------------------|-------------------|-------------------|-------------------|
| <i>TB-recon</i> | 85.12±3.85 | 86.18±3.59 | 85.84±3.51 |
| <i>zero-filled</i> | 83.32±4.53 | 81.26±5.20 | 29.75±1.80 |
| <i>naïve</i> | 84.09±3.86 | 83.26±4.20 | 56.15±2.38 |

| Patella - DSC | 4× | 6× | 24× |
|--------------------|-------------------|-------------------|-------------------|
| <i>TB-recon</i> | 82.10±6.83 | 81.76±7.82 | 77.65±7.96 |
| <i>zero-filled</i> | 78.10±7.17 | 77.37±6.47 | 70.88±10.59 |
| <i>naïve</i> | 53.74±4.36 | 77.62±7.61 | 32.45±2.24 |

| Menisci - DSC | 4× | 6× | 24× |
|--------------------|-------------------|-------------------|-------------------|
| <i>TB-recon</i> | 84.91±2.79 | 83.78±3.06 | 82.28±2.64 |
| <i>zero-filled</i> | 81.87±2.99 | 81.61±3.15 | 16.69±0.93 |
| <i>naïve</i> | 82.35±2.69 | 81.47±3.31 | 54.59±2.24 |

No inter-task skip connections

bold = significant outperformance

| Femur - DSC | 4× | 6× | 24× |
|--------------------|-------------------|-------------------|-------------------|
| <i>TB-recon</i> | 87.33±1.93 | 87.58±1.79 | 85.63±2.56 |
| <i>zero-filled</i> | 82.27±2.75 | 81.79±2.73 | 16.27±0.91 |

For more details on our work, including additional experiments
please refer to our paper #239

Caliva, F., Leynes, A., Shah, R., Bharadwaj, U. U., Majumdar, S., Larson, P., & Padoia, V. (2020, January). Breaking Speed Limits with Simultaneous Ultra-Fast MRI Reconstruction and Tissue Segmentation. In Medical Imaging with Deep Learning

No MRI recon

task skip
ctions

| | | | |
|--------------------|-------------------|-------------------|-------------------|
| <i>TB-recon</i> | 84.91±2.19 | 85.18±3.00 | 82.28±2.04 |
| <i>zero-filled</i> | 81.87±2.99 | 81.61±3.15 | 16.69±0.93 |
| <i>naïve</i> | 82.35±2.69 | 81.47±3.31 | 54.59±2.24 |

bold = significant
outperformance

Contributions

- **TB-recon** for task-based MRI reconstruction
- Segmentation at **ultra-high acceleration factors** is possible
- The proposed **shared encoder** + **inter-task** skip connections facilitate segmentation

Broader impact

Task-based reconstruction can break speed limits, which have hampered the application of magnetic resonance imaging

Potential applications:

- disease and abnormality identification
- organ volume estimation
- lesion size and counting (e.g. multiple sclerosis and micro-bleeds)

**We hope this paper further stimulates
research community's interest on task-based fast MRI**

Acknowledgements

Valentina Padoia's Lab

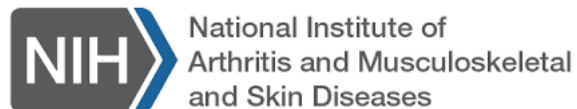
Rutwik Shah
Kaiyang (Victor) Cheng
Alejandro Morales Martinez
Adam Noworolski

Sharmila Majumdar's Lab

Upasana Upadhyay Bharadwaj
Claudia Iriondo

Funding source

This project was supported by R00AR070902 (VP), R61AR073552 (SM/VP) from the National Institute of Arthritis and Musculoskeletal and Skin Diseases, National Institutes of Health, (NIH-NIAMS).



Peder E. Z. Larson's Lab

Andrew P. Leynes
Xucheng Zhu



Francesco.Caliva@ucsf.edu



@FraCaliva



Paper #239