LINBRIDGE: A LEARNABLE FRAMEWORK FOR INTER PRETING NONLINEAR NEURAL ENCODING MODELS

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ABSTRACT

Neural encoding of artificial neural networks (ANNs) aligns the computational representations of ANNs with brain responses, providing profound insights into the neural basis underpinning information processing in the human brain. Current neural encoding studies primarily employ linear encoding models for interpretability, despite the prevalence of nonlinear neural responses. This leads to a growing interest in developing nonlinear encoding models that retain interpretability. To address this problem, we propose LinBridge, a learnable and flexible framework based on Jacobian analysis for interpreting nonlinear encoding models. LinBridge posits that the nonlinear mapping between ANN representations and neural responses can be factorized into a linear inherent component that approximates the complex nonlinear relationship, and a mapping bias that captures sample-selective nonlinearity. The Jacobian matrix, which reflects output change rates relative to input, enables the analysis of sample-selective mapping in nonlinear models. LinBridge employs a self-supervised learning strategy to extract both the linear inherent component and nonlinear mapping biases from the Jacobian matrices of the test set, allowing it to adapt effectively to various nonlinear encoding models. We validate the LinBridge framework in the scenario of neural visual encoding, using computational visual representations from CLIP-ViT to predict brain activity recorded via functional magnetic resonance imaging (fMRI). Our experimental results demonstrate that: 1) the linear inherent component extracted by LinBridge accurately reflects the complex mappings of nonlinear neural encoding models; 2) the sample-selective mapping bias elucidates the variability of nonlinearity across different levels of the visual processing hierarchy. This study not only introduces a novel tool for interpreting nonlinear neural encoding models but also provides novel evidence regarding the distribution of hierarchical nonlinearity within the visual cortex.

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1 INTRODUCTION

In recent years, aligning the computational representation of artificial neural networks (ANNs) with 040 brain activity through neural encoding models significantly advances our understanding of the neural 041 basis underlying information processing in the human brain. Previous research primarily employs 042 linear encoding models due to their interpretability (Naselaris et al., 2011a; Yamins & Dicarlo, 043 2016). However, the prevalence of nonlinear neural processes is well recognized (Naselaris et al., 044 2011b; Wang et al., 2023; Tang et al., 2024; Jain & Huth, 2018), which may limit the ability of linear models to fully capture the complex dynamics of brain activity. This limitation not only undermines the predictive performance of linear encoding models but also restricts their capacity to effectively 046 interpret neural activity. 047

With the rapid advancement of deep neural networks, nonlinear encoding models are increasingly
utilized (Zhang et al., 2019; Li et al., 2022; Cui et al., 2020; 2021). These models incorporate activation functions or other nonlinear structures, allowing them to better capture the brain's responses to
complex stimuli and leading to improved predictive performance compared to linear models (Zhang
et al., 2019; Li et al., 2022; Cui et al., 2020; 2021). However, as illustrated in Figure 1, nonlinear
encoding models exhibit sample-specific characteristics, resulting in unstable structures that complicate the interpretation of underlying relationships.



Figure 1: Comparison of linear and nonlinear encoding models. In linear encoding models, the mapping relationship between the feature space and brain activity space is invariant across input samples. On the contrary, nonlinear encoding models exhibit sample-specific characteristics, resulting in an unstable structure that complicates the interpretation of the underlying relationships.

065 In this study, we propose LinBridge, a learnable and flexible framework based on Jacobian analysis 066 for interpreting nonlinear encoding models. The Jacobian matrix, which quantifies the output change 067 rates relative to input, enables the analysis of sample-selective mapping in nonlinear models (Gale & 068 Nikaido, 1965). LinBridge posits that the nonlinear mapping between the computational representa-069 tions and neural responses can be factorized into two components: a linear inherent component that approximates the complex nonlinear dynamics, and a mapping bias that captures sample-selective 071 nonlinearities. However, this factorization presents a dilemma: the sample-selective nonlinearities introduce substantial variability in the Jacobian matrices across different input-output pairs, compli-072 cating the extraction of consistent and interpretable mapping structures within nonlinear encoding 073 models. 074

075 To address this challenge, we propose a self-supervised learning strategy based on contrastive learn-076 ing, which has demonstrated superior capabilities in differentiating shared and distinctive attributes 077 through paired-sample analysis (Oord et al., 2018; Schneider et al., 2023). Within the contrastive learning framework, LinBridge maximizes shared linear component within the Jacobian matrices while minimizing the influence of nonlinear features (nonlinear mapping biases) on those shared 079 components, leading to an effective delineation of the linear inherent component and the nonlinear mapping biases. In addition, this self-supervised learning strategy allows LinBridge to adapt 081 effectively to various nonlinear encoding models. Furthermore, LinBridge incorporates a low-082 dimensional embedding module that facilitates dimensionality reduction while preserving the in-083 trinsic structure of the feature space, providing a more intuitive tool for analyzing the brain's linear 084 and nonlinear responses to external stimuli. The contributions of this work are summarized as fol-085 lows:

- We introduce LinBridge, a flexible framework designed to extract both the linear inherent component and the nonlinear mapping biases from nonlinear encoding models. This framework enables an interpretable analysis of the nonlinear mappings between computational representations and brain responses.
 - The linear inherent component extracted by LinBridge exhibits activation patterns highly consistent with the original nonlinear encoding model, suggesting that the complex mappings in nonlinear neural encoding models can be effectively captured.
 - We apply LinBridge to a neural encoding exploration of vision transformer models and reveal the variability in nonlinearity across different levels of the visual processing hierarchy.
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2 BACKGROUND AND RELATED WORKS

099 100 2.1 LINEAR NEURAL ENCODING MODELS

Due to their simplicity and interpretability, linear neural encoding models are widely applied across various domains to disentangle the neural basis underpinning information processing in the brain, including vision (Yamins et al., 2014; Khaligh-Razavi & Kriegeskorte, 2014; Güçlü & van Gerven, 2015; Eickenberg et al., 2017; Zhuang et al., 2021), audition (Zhou et al., 2023; Li et al., 2023; MILLET et al., 2022; Tuckute et al., 2023; Vaidya et al., 2022), and language (Liu et al., 2023; Caucheteux & King, 2022; Goldstein et al., 2022; Jain & Huth, 2018; Schrimpf et al., 2021; Abdou, 2022). However, the inherent nonlinear dynamics of neural activity limit the predictive power and interpretability of linear models, particularly when addressing more complex cognitive func-

tions. This limitation is especially pronounced in higher-order cortical areas, which often involve complex and dynamic interactions, suggesting that their underlying neural mechanisms may not be adequately captured by linear representations (Naselaris et al., 2011b).

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2.2 NONLINEAR NEURAL ENCODING MODELS

114 Nonlinear encoding models emerge as a solution to the limitations of linear models by incorporat-115 ing nonlinear structures that more effectively capture the complex patterns of brain activity. These 116 approaches demonstrate superior predictive performance compared to linear models (Zhang et al., 117 2019; Li et al., 2022; Cui et al., 2020; 2021). However, the opaque nature of nonlinear encoding 118 models presents significant challenges in understanding the mapping between the computational representations and brain responses. To address this challenge, most existing methods adopt the 119 framework proposed by (Tank et al., 2021), leveraging various time-series prediction models to en-120 hance the interpretability of these learned black-box mappings (Khanna & Tan, 2019; Bussmann 121 et al., 2021; Suryadi et al., 2023). In particular, the Jacobian matrix has been employed to elucidate 122 the local mapping relationships in artificial neural networks (ANNs) (Zhou et al., 2024; Suryadi 123 et al., 2023). Nonetheless, nonlinear models often exhibit sample-specific mappings, leading to 124 substantial variability in the Jacobian matrices across different input-output pairs. This variabil-125 ity complicates the extraction of consistent and interpretable mapping structures within nonlinear 126 encoding models.

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3 Methods

131 3.1 DATASET AND PREPROCESSING

We use the Natural Scenes Dataset (NSD) (Allen et al., 2021) in this study. The NSD dataset 133 contains fMRI data from eight subjects passively viewing 73,000 color natural scene images over 40 134 hours. These images are cropped from the MS-COCO dataset (Lin et al., 2014), with each image 135 displayed for three seconds and repeated three times across 30 to 40 scanning sessions, resulting in a 136 total of 22,000 to 30,000 experimental trials. The fMRI data in the NSD are acquired using a whole-137 brain gradient-echo EPI (echo-planar imaging) sequence at 7T, with a resolution of 1.8 mm and a 138 repetition time of 1.6 seconds. Single-trial beta maps are estimated using a customized general linear 139 model and released alongside the raw fMRI data (Wang et al., 2022; Tang et al., 2024). Similar to 140 previous studies (Wang et al., 2022; Tang et al., 2024), these beta maps are normalized (zero mean 141 and unit variance) within each run and averaged across image repetitions to be used as functional 142 brain activity measures. In our experiments, each image and its corresponding beta map are treated as a single sample. We divide the dataset into training, validation, and testing sets in a ratio of 8:1:1 143 (8000:1000:1000 samples). Notably, subjects 1, 2, 5, and 7 complete the full experimental protocol, 144 and thus, their fMRI data are utilized in our experiments. In the experiments on neural encoding of 145 vision transformer models, we use the pre-trained CLIP-ViT (Radford et al., $2021)^1$ image encoder 146 to derive the computational representation of the visual image stimuli. 147

149 3.2 ENCODING MODEL

The general encoding model can be formulated as follows:

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 $\hat{y} = f(x) \tag{1}$

where x denotes the feature space of external stimuli, \hat{y} is the brain activity space, and $f(\cdot)$ denotes the encoding function. Specifically, the computational representation of visual images spans the feature space, and the normalized beta maps serve as the brain activity space. To validate LinBridge, we construct both linear and nonlinear models in simplified form. Each model consists of two fully connected layers, with the nonlinear model additionally incorporating a ReLU activation function. Further details regarding the encoding models are provided in A.1. The mean squared error (MSE) (Huang et al., 2017) is used as the loss function in the encoding model.

¹https://huggingface.co/openai/clip-vit-base-patch32.

162 3.3 COMPUTATION OF THE JACOBIAN MATRIX

The Jacobian matrix captures the local linear mapping between feature space and neural responses. It reflects the sensitivity of the neural encoder to variations in the input. Upon completion of model training, we fix the parameters of the encoding model and input the test set data to obtain the corresponding predictions. Given the k-th sample $x_k \in \mathbb{R}^d$ in the test set and the prediction of the nonlinear neural encoder $\hat{y}_k = f(x_k) \in \mathbb{R}^p$, the Jacobian matrix JM_k can be calculated by taking the derivative of the model's output with respect to its input as follows:

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$$\mathbf{J}\mathbf{M}_{k} = \left(\frac{\partial \hat{y}_{k}}{\partial x_{k}}\right)^{T} = \begin{bmatrix} \frac{\partial \hat{y}_{k,1}}{\partial x_{k,1}} & \cdots & \frac{\partial \hat{y}_{k,p}}{\partial x_{k,1}} \\ \vdots & \ddots & \vdots \\ \frac{\partial \hat{y}_{k,1}}{\partial x_{k,d}} & \cdots & \frac{\partial \hat{y}_{k,p}}{\partial x_{k,d}} \end{bmatrix} \in \mathbb{R}^{d \times 1 \times p}$$
(2)

We denote the collection of Jacobian matrices of all testing samples as $\mathbf{JM} \in \mathbb{R}^{d \times N \times p}$, where d = 512 is the dimensionality of the representation, N = 1000 is the sample size of the test set, and p is the number of voxels.

179 3.4 LINBRIDGE

LinBridge leverages Jacobian matrices (JM) to quantify the complex mapping relationships in nonlinear encoding models. It extracts the linear inherent component ($JM_{inherent}$), which captures consistent, interpretable mapping structure invariant to input samples, and the nonlinear mapping biases (ΔJM) that reflect the unique nonlinear behaviors associated with distinct inputs.

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3.4.1 EXTRACTION OF THE LINEAR INHERENT COMPONENT

Similar to the dimensionality reduction architecture introduced in CEBRA (Schneider et al., 2023)², LinBridge employs a multi-layer convolutional neural network (CNN) to refine the input Jacobian matrices. Specifically, LinBridge progressively compresses the sample dimension of the Jacobian matrix using the CNN, enabling the extraction of the linear inherent component ($JM_{inherent} \in \mathbb{R}^{d \times 1 \times p}$) that captures the linear mapping between the input representations of the nonlinear neural encoding model and the corresponding voxel activations in the brain. This approach provides a more structured interpretation of neural activity.

3.4.2 Nonlinear Mapping Biases ΔJM

196 We directly subtract $JM_{inherent}$ from JM to obtain the nonlinear mapping biases ΔJM . This opera-197 tion ensures that both the linear inherent component and the nonlinear mapping biases retain within 198 the original space of JM. Therefore, the computation of ΔJM follows:

$$\Delta \mathbf{J}\mathbf{M} = \mathbf{J}\mathbf{M} - \mathbf{J}\mathbf{M}_{\text{inherent}} \in \mathbb{R}^{d \times N \times p}$$
(3)

201 3.4.3 LOW-DIMENSIONAL EMBEDDING

LinBridge incorporates a low-dimensional embedding module that linearly reduces the dimensions of $JM_{inherent}$, JM, and ΔJM to a more compact representation. This linear dimensionality reduction effectively preserves the relative spatial distances of $JM_{inherent}$ JM, and ΔJM in the latent space. On the one hand, lower dimensional features increase the effectiveness of contrastive learning, on the other hand, it reduces computational cost. Specifically, we use a fully connected (FC) layer to project each matrix into a low-dimensional space.

$$\mathbf{JM}_{\text{inherent}}^{\text{down}} = FC_{\text{Downsample}}(\mathbf{JM}_{\text{inherent}}) \in \mathbb{R}^{1 \times p}$$
(4)

$$\mathbf{JM}^{\text{down}} = FC_{\text{Downsample}}(\mathbf{JM}) \in \mathbb{R}^{N \times p}$$
(5)

$$\Delta \mathbf{J}\mathbf{M}^{\text{down}} = FC_{\text{Downsample}}(\Delta \mathbf{J}\mathbf{M}) \in \mathbb{R}^{N \times p}$$
(6)

In the equations above, the superscript "down" in $\mathbf{JM}_{inherent}^{down}$, \mathbf{JM}^{down} , and $\Delta \mathbf{JM}^{down}$ indicates the dimensionality-reduced representations. Generally, they are the result of applying FC module to the original $\mathbf{JM}_{inherent}$, \mathbf{JM} , and $\Delta \mathbf{JM}$, reducing them to a more compact, low-dimensional space.

²https://github.com/AdaptiveMotorControlLab/CEBRA.



Figure 2: Nonlinear Encoding Model and the LinBridge Framework. (a) Image representation extraction and the general neural encoding model structure; (b) LinBridge framework, which includes the computation of JM, the extraction of $JM_{inherent}$ based on CNN module, the calculation of ΔJM , and the implementation of a low-dimensional embedding module.

241 3.4.4 LOSS FUNCTION

The low-dimensional embeddings ($\mathbf{JM}_{inherent}^{down}, \mathbf{JM}^{down}$, and $\Delta \mathbf{JM}^{down}$) of these matrices are uti-lized for contrastive learning. Essentially, JM_{inherent} represents the shared linear components of JM in the latent space. The objective of the contrastive learning framework is to maximize the alignment of these components while minimizing the influence of the unique nonlinear characteris-tics represented by ΔJM . Consequently, it seeks to maximize the distinctiveness of $JM_{inherent}$ in relation to ΔJM . To this end, LinBridge employs the InfoNCE loss function (Oord et al., 2018; Schneider et al., 2023)³. Contrastive learning maximizes the similarity between the reference sam-ple and positive samples ($\mathbf{JM}_{inherent}^{down}$ and \mathbf{JM}^{down}), while concurrently minimizing the similarity between the reference sample and negative samples ($\mathbf{JM}_{inherent}^{down}$ and $\Delta \mathbf{JM}^{down}$). Thus, the InfoNCE loss function in this study is formulated as follows:

$$\mathcal{L}_{\text{InfoNCE}} = -\frac{1}{N} \sum_{i=1}^{N} \log \frac{\exp(\text{sim}(\mathbf{J}\mathbf{M}_{\text{inherent}}^{\text{down}}, \mathbf{J}\mathbf{M}_{i}^{\text{down}})/\tau)}{\exp(\text{sim}(\mathbf{J}\mathbf{M}_{\text{inherent}}^{\text{down}}, \mathbf{J}\mathbf{M}_{i}^{\text{down}})/\tau) + \sum_{j=1}^{N} \exp(\text{sim}(\mathbf{J}\mathbf{M}_{\text{inherent}}^{\text{down}}, \Delta \mathbf{J}\mathbf{M}_{j}^{\text{down}})/\tau)}$$
(7)

where $sim(\cdot, \cdot)$ denotes the similarity metric (e.g., cosine similarity), and τ is the temperature parameter. Additionally, we introduce L1-regularization to prevent overfitting of ΔJM :

$$\mathcal{L}_{\text{Reg}} = \lambda \sum |\Delta \mathbf{J} \mathbf{M}| \tag{8}$$

where $\lambda = 0.01$ is the regularization coefficient. The final loss function is as follows:

$$\mathcal{L}_{\text{total}} = \mathcal{L}_{\text{InfoNCE}} + \mathcal{L}_{\text{Reg}} \tag{9}$$

In summary, the structural block diagram is shown in Figure 2. LinBridge utilizes a Jacobian matrixdriven strategy, enabling its application to any neural encoding model.

3.5 EVALUATION METRICS

We use the coefficient of determination (R^2) to evaluate the predictive performance of the neural encoding models on the test set. To assess the statistical significance of the predictions, we follow

³https://github.com/RElbers/info-nce-pytorch.



Figure 3: Comparison of R^2 between linear and nonlinear encoding models, showing predictions significantly above chance levels (P < 0.05, FDR corrected). (a) R^2 in the linear encoding model; (b) R^2 in the nonlinear encoding model; (c) The histograms of R^2 in the whole brain, the primary visual cortex (PVC), the secondary visual cortex (SVC), and the tertiary visual cortex (TVC). Results for other subjects are provided in A.3.

the method described in (Wang et al., 2023), conduct 200 bootstrapped resampling iterations on the test set and calculating FDR-corrected *P*-value thresholds for various performance metrics (Wang et al., 2023; Subramaniam et al., 2024).

4 Results

4.1 PREDICTION OF VISUAL CORTEX WITH NONLINEAR ENCODERS

300 We compare the predictive performance of the linear and nonlinear encoding models. Figure 3 shows the R^2 values for both models for Subject 2 (all results reported in the main text are exempli-301 fied using Subject 2 unless otherwise stated). The results demonstrate that the nonlinear encoding 302 model activates a broader range of brain regions compared to the linear model (24,490 voxels vs. 303 16,084 voxels), particularly in the visual cortex. Figure 3 (c) further illustrates that the nonlinear 304 encoding model achieves significantly higher R^2 values across various visual areas, including the 305 primary visual cortex (PVC: V1), secondary visual cortex (SVC: V2, V3, V4), and tertiary visual 306 cortex (TVC: EBA, PPA, RSC, OPA, FFA-1, FFA-2). Notably, 9.30% of the voxels in the nonlinear 307 encoding model exhibit relatively good predictive performance ($R^2 > 0.05$), in contrast to 6.65% 308 in the linear model. These results suggest that the nonlinear encoding model outperforms the linear 309 one.

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4.2 LINEAR INHERENT COMPONENT: LINEAR INTERPRETATIONS OF NONLINEAR MAPPINGS 313

314 Figure 4 (a) illustrates the stability of the linear inherent component extracted by LinBridge. We 315 calculate the Pearson correlation coefficients between the linear inherent component obtained at various batch sizes (batchsize $\in [16, 32, 64, 128, 256, 512]$) and the linear inherent component 316 obtained at a batch size of 1000, that is, the entire test set. The training strategies are detailed in A.2. 317 This analysis is repeated for 200 times to obtain means and standard deviations. As shown in Figure 318 4 (a), the inherent structure extracted by LinBridge is highly stable across all evaluated batch size, 319 as evidenced by Pearson coefficients approaching 1. This high stability suggests that LinBridge can 320 accurately capture the relationship carried by the encoding model even with small batch sizes. 321

The linear inherent component extracted by LinBridge closely aligns with the activation patterns in the nonlinear encoding model (Figures 3 (b) and 4 (b)). Additionally, we compare the R^2 values of the nonlinear encoding model and the linear inherent component extracted by LinBridge across



Figure 4: Comparison of the linear inherent component extracted by LinBridge to the brain activation predicted by the nonlinear encoding model. (a) The stability of the extracted linear inherent component across different batch sizes. (b) Activation patterns of the linear inherent component extracted by LinBridge. (c) Comparison of the distribution of R^2 values between the linear inherent component extracted by LinBridge and the original nonlinear encoding models in the whole brain, PVC, SVC and TVC. Results for other subjects can be found in A.4.

the whole brain, PVC, SVC, and TVC (Figure 4 (c)). The R^2 values in the two conditions exhibit high correlations, with Pearson correlation coefficients of 0.9972, 0.9949, 0.9937, and 0.9984 at the whole brain level, and in PVC, SVC, and TVC, respectively. The linear inherent component achieves comparable or even superior performance in specific brain regions. All these results demonstrate that the linear inherent component extracted by LinBridge can accurately capture the complex relationship represented by the nonlinear encoding model.

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4.3 NONLINEAR ENCODING IN VISUAL CORTEX

The variations of ΔJM regarding to various samples are valuable to characterize the nonlinearity of voxel-wise encoding model, and hence the visual cortex.

361 However, the high dimension of ΔJM complicates the quantification of its variations among sam-362 ples. In this context, the low-dimensional embedding ΔJM^{down} derived from LinBridge provides 363 a novel perspective for depicting the nonlinearity of the visual cortex. To this end, we incorporate 364 linear fitting (Allen et al., 2021; Cohen, 1997; Hlinka et al., 2011) to assess how ΔJM varies with 365 different samples. Specifically, for each selected voxel, we first generate a sample index array and then extract the corresponding response values from ΔJM^{down} . We subsequently calculate the coef-366 367 ficients of a first-degree polynomial through polynomial fitting, with these coefficients representing the linear response weights of the voxel across different categories. It is hypothesized that a voxel 368 responses to external stimuli linearly if the corresponding ΔJM^{down} is invariant to different sam-369 ples (i.e., the absolute value of the first derivative approaches 0). Conversely, the voxel is deemed 370 nonlinear. Thus, we employ the absolute value of the first derivative (AFD) as a metric to evaluate 371 the nonlinearity of a voxel. 372

We first perform dimensionality reduction for the Clip-Vit features of all the 73,000 stimulus images
using t-SNE (Van der Maaten & Hinton, 2008). We then reorder the image samples in descending
order according to their 1D-representation resulting from t-SNE. Figures 14-16 in A.5 show the
sorted image samples, demonstrating an obvious transition from "simple" to "complex", as well as
that the samples with similar semantics cluster together. This distribution pattern remains consistent
across subjects.

Figure 5 (a) illustrates ΔJM^{down} in the test samples for two voxels, in which the *x*-axis is the sorted image index according to their 1-D t-SNE representation in descending order. The left and right panels correspond to the voxels with the highest and lowest AFD values, respectively. In the left panel, the low-dimensional embedding of ΔJM^{down} varies sharply with the sorted image samples, and the high AFD value indicates strong nonlinearity. Conversely, in the right panel, the low-dimensional embedding of ΔJM^{down} is invariant to image samples, evidencing strong linearity of the voxel.

Figure 5 (b) shows the histograms of AFDs in PVC, SVC, and TVC. The number of voxels with relatively higher AFDs increases significantly from PVC to TVC. This observation may suggest a progressive nonlinearity within the hierarchy of visual cortex. Our findings closely align with previous research. For example, the primary visual cortex predominantly processes relatively simple visual features (Wang et al., 2023; Glasser et al., 2016; Huff et al., 2018), and consequently exhibits lower nonlinear encoding. In contrast, the middle and higher visual cortices manage more complex visual scenes (Wang et al., 2023; Glasser et al., 2016), such as spatial relationships and object recognition, exhibiting stronger nonlinear components in their neural activity.

Figure 5 (c) visualizes the nonlinearity measured by AFDs for significantly activated voxels across
 the whole brain. The PVC and SVC display more linear characteristics, whereas the TVC exhibits
 remarkable nonlinearity, further reinforcing the notion of hierarchical distribution of nonlinearity in
 the visual cortex. The probability density distribution of the AFDs in Figure 5 (d) indicates that the
 TVC demonstrates a higher probability of higher AFDs.

Further analysis reveals that, beyond the visual cortex, other brain regions associated with higher cognitive processing also exhibit nonlinearity (Figure 5 (c)), For instance, the temporoparietaloccipital junction (TPOJ) and prefrontal areas. The TPOJ, recognized as a key region for multimodal information integration (Wang et al., 2023; Glasser et al., 2016), exemplifies the complexity of nonlinear processing and hierarchical information transmission in the brain. In parallel, the nonlinearity of the prefrontal cortex suggests that during higher cognitive tasks, such as decision-making and reasoning, the brain appears to rely on complex nonlinear mechanisms.



Figure 5: Distribution of nonlinear visual encoding in the brain. (a) The left and right images
show voxel fitting results for the highest and lowest evaluation metrics, respectively; (b) Histogram
comparison of evaluation metrics for significantly activated voxels in PVC, SVC, and TVC; (c)
Visualization of evaluation metrics for significantly activated voxels across the whole brain; (d)
Comparison of probability density functions for evaluation metrics of significantly activated voxels
in PVC, SVC, and TVC. Results for other subjects can be found in A.6.

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432 5 CONCLUSIONS, LIMITATIONS, AND PROSPECTS

In this study, we introduce LinBridge, a novel framework aimed at interpreting nonlinear neural encoding models through Jacobian analysis. We hypothesize that the intricate nonlinear mappings between ANN representations and neural responses can be decomposed into a linear inherent component and a sample-selective mapping bias. LinBridge effectively bridges the interpretability and nonlinearity divide, advancing our understanding of neural encoding and serving as a valuable tool for future investigations into complex neural computations across various brain regions.

440 The present study acknowledges several limitations. First, we validate LinBridge by using a simple 441 nonlinear encoding model. In the future, it is interesting to conduct further validation studies using 442 more advanced nonlinear encoding models. Second, while the Jacobian matrix elucidates the map-443 ping relationships between samples and corresponding outputs, its computation remains resource-444 intensive when applied to large datasets. Given that pre-trained encoding models inherently contain gradient information, the incorporation of low-rank matrix decomposition for efficient computation 445 of mapping relationships between samples represents a promising avenue for future work. Third, al-446 though our study focuses on the visual cortex, it is interesting to apply LinBridge to neural encoding 447 models in other modalities such as acoustic, linguistic, and multimodal information. 448

450 REFERENCES

449

451

452

453

473

474

475

- Mostafa Abdou. Connecting neural response measurements & computational models of language: a non-comprehensive guide. *arXiv preprint arXiv:2203.05300*, 2022.
- Emily J. Allen, Ghislain St-Yves, Yihan Wu, Jesse L. Breedlove, Jacob S. Prince, Logan T Dowdle,
 Matthias Nau, Bradley Caron, Franco Pestilli, Ian Charest, J. Benjamin Hutchinson, Thomas
 Naselaris, and Kendrick Norris Kay. A massive 7t fmri dataset to bridge cognitive neuroscience
 and artificial intelligence. *Nature Neuroscience*, 25:116 126, 2021.
- Bart Bussmann, Jannes Nys, and Steven Latré. Neural additive vector autoregression models for causal discovery in time series. In *Discovery Science: 24th International Conference, DS 2021, Halifax, NS, Canada, October 11–13, 2021, Proceedings 24*, pp. 446–460. Springer, 2021.
- Charlotte Caucheteux and Jean-Rémi King. Brains and algorithms partially converge in natural language processing. *Communications biology*, 5(1):134, 2022.
- Mark S Cohen. Parametric analysis of fmri data using linear systems methods. *Neuroimage*, 6(2): 93–103, 1997.
- Yibo Cui, Chi Zhang, Kai Qiao, Linyuan Wang, Bin Yan, and Li Tong. Study on representation invariances of cnns and human visual information processing based on data augmentation. *Brain Sciences*, 10(9):602, 2020.
- Yibo Cui, Kai Qiao, Chi Zhang, Linyuan Wang, Bin Yan, and Li Tong. Gabornet visual encoding: A lightweight region-based visual encoding model with good expressiveness and biological
 interpretability. *Frontiers in Neuroscience*, 15:614182, 2021.
 - Michael Eickenberg, Alexandre Gramfort, Gal Varoquaux, and Bertrand Thirion. Seeing it all: Convolutional network layers map the function of the human visual system. *NeuroImage*, 152: 184–194, 2017. doi: https://doi.org/10.1016/j.neuroimage.2016.10.001.
- 477 David Gale and Hukukane Nikaido. The jacobian matrix and global univalence of mappings. *Mathematische Annalen*, 159(2):81–93, 1965.
- Matthew F Glasser, Timothy S Coalson, Emma C Robinson, Carl D Hacker, John Harwell, Essa Yacoub, Kamil Ugurbil, Jesper Andersson, Christian F Beckmann, Mark Jenkinson, et al. A multi-modal parcellation of human cerebral cortex. *Nature*, 536(7615):171–178, 2016.
- Ariel Goldstein, Zaid Zada, Eliav Buchnik, Mariano Schain, Amy Price, Bobbi Aubrey, Samuel A
 Nastase, Amir Feder, Dotan Emanuel, Alon Cohen, et al. Shared computational principles for
 language processing in humans and deep language models. *Nature neuroscience*, 25(3):369–380, 2022.

400					
486	Umut Güclü and Marcel A. J. van Gerven. Deep neural networks reveal a gradient in the complexity				
487	of neural representations across the ventral stream 35(27):10005–10014, 2015, doi: 10.1523/				
488	INFUROSCI 5023-14 2015				
489	JNEOKOSCI.3023-14.2013.				
/00	Jaroslav Hlinka, Milan Paluš, Martin Veimelka, Dante Mantini, and Maurizio Corbetta, Functional				
490	connectivity in resting-state fmri: is linear correlation sufficient? <i>Neuroimage</i> , 54(3):2218–2225.				
491					
492	2011.				
493	Heng Huang, Xintao Hu, Yu Zhao, Milad Makkie, Oinglin Dong, Shijie Zhao, Lei Guo, and Tian-				
494	ming Liu. Modeling task fmri data via deep convolutional autoencoder. IEEE transactions on				
495	medical imaging 37(7):1551-1561 2017				
106	meanear magning, 57(1):1551, 2517.				
490	Trevor Huff, Navid Mahabadi, and Prasanna Tadi. Neuroanatomy, visual cortex. 2018.				
497					
498	Shailee Jain and Alexander Huth. Incorporating context into language encoding models for fmri. <i>Advances in neural information processing systems</i> , 31, 2018.				
499					
500					
501	Seyed-Mahdi Khaligh-Razavi and Nikolaus Kriegeskorte. Deep supervised, but not unsupervised,				
502	models may explain it cortical representation. PLOS Computational Biology, 10(11):1–29,				
502	2014. doi: 10.1371/journal.pcbi.1003915.				
503					
504	Saurabh Khanna and Vincent YF Tan. Economy statistical recurrent units for inferring nonlinear				
505	granger causality. arXiv preprint arXiv:1911.09879, 2019.				
506	Linguis Li Dangan Chan Chi Zhang Linguan Wang Din Yan and Li Tang. An improved ashere t				
507	Jingwei Li, Fanpai Chen, Chi Zhang, Linyuan wang, Bin Tan, and Li Tong. An improved gabornet				
508	visual encoding model with nonlinear mapping and data augmentation. In 2022 / In International				
500	Conference on Computational Intelligence and Applications (ICCIA), pp. 180–184. IEEE, 2022.				
509	Yuanning Li, K. Gonala Anumanchinalli, Abdalrahman Mohamad, Paili Chan, H. Laural Carnay				
510	Tuaning El, R. Oopara Anumancipani, Abdenaminan Monanicu, Tem Chen, H. Laurer Cancy,				
511	Junieng Lu, Jinsong wu, and F. Edward Chang. Dissecting neural computations in the numan				
512	auditory pathway using deep neural networks for speech. <i>Nature Neuroscience</i> , 26:2213–2225,				
513	2023. doi: 10.1038/s41593-023-01468-4.				
514	Tsung Vi Lin Michael Maire Serge Belongie James Have Pietro Perona Deva Pamanan Piotr				
515	Dollár and C Laurance Zitaick Microsoft coord Common objects in contast. In Computer				
510	Using ECC 2014. 12th European Conference Zurich Switzerland Sentext. In Computer				
010	VISION-ECCV 2014. 15th European Conference, Zurich, Switzerland, September 0-12, 2014,				
517	Proceedings, Part v 15, pp. 140–155. Springer, 2014.				
518	Xu Liu Mengyue Zhou Gaosheng Shi Yu Du Lin Zhao Zihao Wu David Liu Tianming Liu				
519	and Xintao Hu. Coupling artificial neurons in bert and biological neurons in the human brain.				
520	Proceedings of the AAAI Conference on Artificial Intelligence volume 27 pp 2222 2006 2022				
521	Troceedings of the AAA Conference on Artificial Methogence, volume 57, pp. 8886–8890, 2025.				
522	Juliette MILLET, Charlotte Caucheteux, Pierre Orhan, Yves Boubenec, Alexandre Gramfort, Ewan				
502	Dunbar, Christophe Pallier, and Jean-Remi King. Toward a realistic model of speech processing				
523	in the brain with self-supervised learning. In S. Koveio, S. Mohamed, A. Agarwal, D. Belgrave				
524	K Cho and A Oh (eds.) Advances in Neural Information Processing Systems volume 35 pp				
525	33428-33443 Curran Associates Inc. 2022				
526	55720 55775. Cultaii Associaus, ilic., 2022.				
527	Thomas Naselaris, Kendrick N. Kay, Shinji Nishimoto, and Jack L. Gallant. Encoding and decoding				
528	in fmri. Neurolmage, 56(2):400–410, 2011a.				
520					
520	Thomas Naselaris, Kendrick N Kay, Shinji Nishimoto, and Jack L Gallant. Encoding and decoding				
530	in fmri. <i>Neuroimage</i> , 56(2):400–410, 2011b.				
531					
532	Aaron van den Oord, Yazhe Li, and Oriol Vinyals. Representation learning with contrastive predic-				
533	tive coding. arXiv preprint arXiv:1807.03748, 2018.				
534					
535	Alec Radford, Jong Wook Kim, Chris Hallacy, Aditya Ramesh, Gabriel Goh, Sandhini Agarwal,				
536	Girish Sastry, Amanda Askell, Pamela Mishkin, Jack Clark, et al. Learning transferable visual				
500	models from natural language supervision. In International conference on machine learning, pp.				
00/	8748–8763. PMLR, 2021.				
538					

539 Steffen Schneider, Jin Hwa Lee, and Mackenzie Weygandt Mathis. Learnable latent embeddings for joint behavioural and neural analysis. *Nature*, 617(7960):360–368, 2023.

540	Martin Schrimpf, Idan Asher Blank, Greta Tuckute, Carina Kauf, Eghbal A Hosseini, Nancy Kan-
541	wisher, Joshua B Tenenbaum, and Evelina Fedorenko. The neural architecture of language: In-
542	tegrative modeling converges on predictive processing. Proceedings of the National Academy of
543	<i>Sciences</i> , 118(45):e2105646118, 2021.
544	Vighnesh Subramaniam, Colin Conwell, Christopher Wang, Gabriel Kreiman, Boris Katz, Ignacio
545	Cases and Andrei Barbu Revealing vision-language integration in the brain with multimodal
546	networks. arXiv preprint arXiv:2406.14481, 2024.
547	
548 549	Suryadi Suryadi, Lock Yue Chew, and Yew-Soon Ong. Granger causality using jacobian in neural
550	networks. Chaos: An interasciplinary Journal of Nonlinear Science, 35(2), 2025.
551	Jerry Tang, Meng Du, Vy Vo, Vasudev Lal, and Alexander Huth. Brain encoding models based on
552	multimodal transformers can transfer across language and vision. Advances in Neural Information
553	Processing Systems, 36, 2024.
554	Alay Tank Jan Covart Nicholas Ecti Ali Shqiqiq and Emily B Ecy. Naural granger causality IEEE
555 556	Transactions on Pattern Analysis and Machine Intelligence, 44(8):4267–4279, 2021.
557	Greta Tuckute, Jenelle Feather, Dana Boebinger, and Josh H. McDermott, Many but not all deep
558	neural network audio models capture brain responses and exhibit correspondence between model
559	stages and brain regions. <i>PLOS Biology</i> , 21(12):1–70, 12 2023. doi: 10.1371/journal.pbio.
560	3002366.
561	
562	Aditya R Vaidya, Shailee Jain, and Alexander Huth. Self-supervised models of audio effectively
563	explain human cortical responses to speech. In Kamalika Chaudhuri, Stefanie Jegelka, Le Song,
564	farance on Machine Learning, volume 162 of Proceedings of Machine Learning Research, pp
565	21927_21944 PMI R 17_23 Jul 2022
566	21)27-21)77. 1 WILK, 17-25 Jul 2022.
567	Laurens Van der Maaten and Geoffrey Hinton. Visualizing data using t-sne. Journal of machine
568	learning research, 9(11), 2008.
569	Asia V Wang Kandrich Kan Themas Nasalaria Michael I Tam and I sile Wahles. Incomposed
570	ing natural language into vision models improves prediction and understanding of higher visual
571	cortex. <i>bioRxiv</i> , 2022. doi: 10.1101/2022.09.27.508760.
572	Aria Y Wang, Kendrick Kay, Thomas Naselaris, Michael J Tarr, and Leila Wehbe. Better models of
575	human high-level visual cortex emerge from natural language supervision with a large and diverse
575	dataset. Nature Machine Intelligence, 5(12):1415–1426, 2023.
576	
577	Daniel L. K. Yamins, Ha Hong, Charles F. Cadieu, Ethan A. Solomon, Darren Seibert, and James J.
578	cortex. <i>Proceedings of the National Academy of Sciences</i> , 111(23):8619–8624, 2014.
579	Della Valanda Distanti di tata
580 581	sensory cortex. <i>Nature neuroscience</i> , 19(3):356–365, 2016.
582	
583	Chi Zhang, Kai Qiao, Linyuan Wang, Li Tong, Guoen Hu, Ru-Yuan Zhang, and Bin Yan. A visual
584	by functional magnetic recompany imaging. <i>Journal of neuroscience methods</i> , 225:108218, 2010
585	by functional magnetic resonance imaging. Journal of neuroscience memous, 525.108518, 2019.
586	Zijun Zhang. Improved adam optimizer for deep neural networks. In 2018 IEEE/ACM 26th inter-
587	national symposium on quality of service (IWQoS), pp. 1–2. Ieee, 2018.
588	Manguna Zhou, Yu Liu, David Liu, Zihao Wu, Zhangliang Liu, Liu Zhao, Dailang Zhu, Lui Cu
589	Junwei Han, Tianming Liu, et al. Fine grained artificial neurons in audio transformers for dison
590	tangling neural auditory encoding. In Findings of the Association for Computational Linguistics
591	ACL 2023, pp. 7943–7956, 2023.
592	· · · · · · · · · · · · · · · · · · ·
593	Wanqi Zhou, Shuanghao Bai, Shujian Yu, Qibin Zhao, and Badong Chen. Jacobian regularizer- based neural granger causality. <i>arXiv preprint arXiv:2405.08779</i> , 2024.

597 pnas.2014196118. 598 599 600	073/
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A APPENDIX

A.1 NONLINEAR ENCODER AND LINEAR ENCODER



Figure 6: Structural comparison between nonlinear and linear encoding models.

To investigate the relationship between visual feature representations and brain responses, two ANN encoding models are constructed: a linear encoding model (Linear encoder) and a nonlinear encoding model (Nonlinear encoder).

Nonlinear Encoding Model

 $\hat{y}^{nonlinear} = W_2 \sigma (W_1 x + b_1) + b_2 \tag{10}$

(11)

where x denotes the input representations, and W_1, b_1 and W_2, b_2 are the weights and biases of the first and second layers, respectively. σ denotes the ReLU activation function, which introduces nonlinearity to enhance the model's expressiveness.

Linear Encoding Model

This model omits the ReLU activation function, allowing only linear transformations and serving to investigate the performance of linear encoding. In this study, the bias terms b_1 and b_2 are both set to False. Their structural comparison is illustrated in Figure 6. Meanwhile, the detailed code implementations of their models are presented in Algorithms 1 and 2, respectively.

 $\hat{y}^{linear} = W_2(W_1x + b_1) + b_2$

Training Strategy

The training process of the encoding model utilizes the Adam optimizer (Zhang, 2018) for parameter optimization. To prevent overfitting, early stopping is employed, ceasing training if the validation loss fails to improve over 8 consecutive epochs. Additionally, the model parameters that demonstrate the optimal performance on the validation set are recorded and preserved.

691	
692	Algorithm 1 Nonlinear encoding model
693	class NonLinear_ANN_encoder(nn.Module):
694	def init(self, input_dim=512, out_dim=p, hidden_dim=2048):
695	<pre>super(NonLinear_ANN_encoder, self)init()</pre>
696	self.encoder = nn.Sequential(
697	nn.Linear(input_dim, hidden_dim, bias=False),
698	nn.ReLU(),
699	nn.Linear(hidden_dim, output_dim, bias=False)
700	def forward(self, x):
701	return self.encoder(x)

Algo	orithm 2 Linear encoding model	
cl	ass Linear_ANN_encoder(nn.Module):	
	definit(self, input_dim=512, out_dim=p, hidden_dim=2	2048):
	<pre>super(Linear_ANN_encoder, self)init()</pre>	
	self.encoder = nn.Sequential(
	nn.Linear(input_dim, hidden_dim, bias=False),	
	nn.Linear(hidden_dim, output_dim, bias=False)	
de	ef forward(self, x):	
	return self.encoder(x)	
A.2	TRAINING STRATEGIES OF LINBRIDGE UNDER DIFFE	RENT BATCHSIZES
Here	e we demonstrate how LinBridge is trained with different l	batchsizes. Specifically, we provide
the c	code implementations are presented in Algorithms 3. The or	de demonstrates hour LinPridge is
troin	and with different batchesizes, ranging from 16 to large 512 k	batchsizes
tram	ed with different batchsizes, fanging from 10 to large 512 t	batchsizes.
Algo	prithm 3 Training strategies of LinBridge under different b	atchsizes
	A = torch load(project dir)	► Load Jacobian matrix data
ba	a = [16, 32, 64, 128, 256, 512]	\triangleright Set of batchsizes
fo	\mathbf{r} batchsize in batchsize set do	
10	dataset = TensorDataset(JM)	
	dataloader = DataLoader(dataset, batch_size=batchsize, s	huffle=True. drop_last=True)
	info_nce_loss = InfoNCE(negative_mode='unpaired')	
	optimizer = optim.AdamW(['params': LinBridge_model.	.parameters()], lr=1e-3)
	for epoch in 128 do	· · · ·
	for JM_batch in dataloader do	
	optimizer.zero_grad()	
	JM_inherent, delta_JM, JM_inherent_down, JM_do	own, delta_JM_down
	= LinBridge_model(JM_batch)	
	loss = (info_nce_loss(JM_inherent_down.repeat(JM	M_batch.shape[1], 1),
	JM_down, delta_JM_down)	
	+ 0.01 * torch.sum(torch.abs(delta_JM)))	
	loss.backward()	
	optimizer.step()	
	ellu loi and for	
er	end for	



Comparison of \mathbb{R}^2 between Linear and Nonlinear Encoding Models in A.3 OTHER SUBJECTS

Figure 8: Comparison of R^2 between linear and nonlinear encoding models in Subject 1.



Figure 10: Comparison of the linear inherent component extracted by LinBridge with the brain activation of the nonlinear encoding model in Subject 1.



Figure 11: Comparison of the linear inherent component extracted by LinBridge with the brain activation of the nonlinear encoding model in Subject 5.



Figure 12: Comparison of the linear inherent component extracted by LinBridge with the brain activation of the nonlinear encoding model in Subject 7.



A.5 DISPLAY OF TEST IMAGES AFTER PROGRESSIVE SORTING

Figure 13: The images of the test set for Subject 2 after progressive sorting. Each image corresponds sequentially from top to bottom and left to right to the positions 1-1000 in the "Sorted Sample Order" of Figure 5 (a). From this, it can be observed that there is a certain pattern present in the progressively sorted test images.

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1024	rigure 14. Display of test mages for subject I after	progr	CSSIVE	sorting	•	
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A.6 DISTRIBUTION OF NONLINEAR ENCODING IN THE BRAIN IN OTHER SUBJECTS

