
Exploring Simulators for Particle Picking in Cryo-Electron Tomography

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Abstract

To understand how proteins function, we need to know the conformations that they adopt and with what they interact in their native cellular environment. Cryo-electron tomography (cryo-ET) offers a powerful tool by enabling *in situ* imaging of proteins. But high noise levels and the need for expertise in particle identification limit its scalability. In this study, we present a machine learning framework for automated recognition and localization of particles in cryo-ET data. We treat particle picking as an object recognition task and employ a U-Net-based architecture for multi-class segmentation. To overcome the scarcity of annotated data, we train our model on synthetic tomograms generated by a simulator that incorporates empirical noise from publicly available cryo-ET datasets. Our results show that training on a mixed dataset containing both synthetic and empirical backgrounds provides the most effective particle-picking performance, enhancing the model’s robustness to different background types. Furthermore, we demonstrate that training exclusively on simulated particles enables the model to reliably distinguish particles from background in real tomograms, highlighting the potential of simulation-based training strategies in cryo-ET.

1 Introduction

Biomolecules function within cells forming complexes with other biomolecules in different environments characterized by different physio-chemical conditions. To understand their roles, it is essential to identify their spatial localization, structural arrangements, and binding partners *in situ*. Cryo-electron tomography (cryo-ET) images thin slices of frozen biological specimens, offering detailed tomograms and revealing diverse cellular architectures.

Cryo-ET involves the extraction of one or more thin layers of a vitrified specimen that is then imaged by an electron microscope. The sample is tilted within the microscope to obtain multiple 2D projections at different angles. The obtained *tilt-series* of images is then used to reconstruct the tomogram (i.e., 3D volume). This process comes with inherent limitations. To limit radiation damage, only a minimal electron dose can be utilized during imaging, resulting in a low signal-to-noise ratio (SNR). In addition, both the structured background and the lamella thickness reduce particle

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contrast. Thicker lamellae broaden the spread of the electron beam, while the background exhibits scattering strengths comparable to those of the particles. Furthermore, hardware limitations inherent to electron microscopes impede complete angular sampling, leading to the *missing wedge* effect. The missing projections introduce anisotropic resolution that distorts the fidelity of the particles' structural features. Lastly, the crowded and heterogeneous nature of cellular environments further obscures individual macromolecules. As a result, the dense and noisy backgrounds in cryo-ET tomograms present significant challenges for particle localization and segmentation, which are crucial for analyzing macromolecular structures within the cell [1].

Recent advancements in deep learning, particularly U-Net and CNN models, have shown promise for particle picking in cryo-ET by training on highly curated particle datasets [2, 3, 4]. Few-shot learning addresses some of the challenges of costly tomogram annotation [4, 5] but still requires a set of partial annotations for training. On the other hand, training with simulated data alleviates manual annotation burdens and allows the representation of complex biological structures. Simulation-based inference has been successful in extracting mechanistic information from complex experimental data in areas ranging from astrophysics to neuroscience [6] and single-particle cryo-EM [7]. However, developing realistic simulators for *in situ* environments and for the cryo-ET imaging process remains challenging [8, 9, 10]. In this work, we aim to develop a tool that utilizes simulation-based training to identify and locate macromolecules *in situ*, with particular focus on exploring various background models in cryo-ET data simulations.

2 Methods

Simulator We simulate small cubic volume crops, e.g., 32 voxels per edge at a magnification of 5-15 Å per voxel edge (Table 1), instead of a full tomogram, to improve memory handling and facilitate parallelization during training, testing, and inference. The simulation pipeline consists of four steps (Fig. 1A). First, we (i) sample the particle types that will populate the volume crop, assuming that each particle adopts a single known structure (i.e., the template). Each volume crop may contain from zero to an arbitrary number of particles. Then, we (ii) rotate and shift the particles, and simulate the volume with the appropriate voxel size. We then (iii) add the noise rescaled according to a given SNR and (iv) remove the missing wedge. Fig. 1B shows an example simulated volume. To provide our model with a diverse and comprehensive training set, we train it using simulations with a broad range of voxel sizes, rotations, shifts, SNRs, crowding per crop, and missing wedge angles (Table 1). Directly simulating the reconstructed volume crops enables us to bypass the simulation of aberration corrections and tilt-series alignment, making the simulator computationally more efficient. To explore the performance of different noise background simulators, we test three noise models: i) pure Gaussian white noise (synthetic), ii) empirical background taken from experimental tomograms (Table 1), and iii) a mixed simulator that simulates batches of volumes, with half containing synthetic noise and the other half containing an empirical background. For the empirical background crops, we rescale the voxel size accordingly. The experimental noise tomograms were obtained from *in vitro* samples and hippocampal tissue, and the samples differed between the training and testing sets.

Architecture State-of-the-art computer vision techniques for life science applications utilize U-Nets to perform multiclass segmentation of images and volumes [2, 4, 5, 11]. We build on this methodological framework to carry out particle picking in tomograms. We set up a dynamic U-Net with a number of pooling and upsampling layers, depending on the chosen crops' edge size (Fig. 1C). In addition, we implemented a deep supervision scheme on the U-Net latent representation by training a classifier head. This particle classifier comprises a 3-layer multilayer perceptron (MLP) and serves as a projector head in the context of object recognition tasks. These choices aim to improve the model's generalization performance by enhancing the learning of meaningful latent representations, and are not used for inference [12].

Training Training relies on supervision from the U-Net for multiclass semantic segmentation and from the MLP projector head for particle classification. We trained it exclusively on data simulated on the fly. We trained a model for each of the three different background simulators. For the mixed simulator case, we used a curriculum training (CT) schedule: we started with synthetic noise for the first third of training, then switched to the mixed simulator. To improve the model's classification performance in distinguishing between particles and background, we force our model to identify an additional 'background' class along with the other classes, such that the number of class channels

becomes $N_{\text{classes}} = N_{\text{templates}} + 1$ [13].

The U-Net produces pixel-level logits for each class. Thus, to supervise its output, we utilize the ground-truth (GT) segmentation maps generated along with the simulated data. Each particle is segmented as a sphere centered on the particle with a fixed radius. These are compared pixel-wise with the predicted segmentation maps using a multiclass focal loss; we refer to Appendix 3.1 for further details.

To supervise the particle classification head, we designed a loss function that accounts for the permutation invariance of particle entries within each crop, since multiple particles in the same crop may belong to the same class. The classification head returns the logits for each class channel, particle-wise, which we supervise using a cross-entropy loss; we refer to Appendix 3.1 for further details. To enforce permutation invariance, we use an implementation of a variant of the Jonker-Volgenant algorithm with no initialization [14] to match the target and predicted particle label strings prior to evaluating the cross-entropy loss.

We use the AdamW optimizer [15] with a learning rate of 3×10^{-4} and a weight decay of 1×10^{-5} . We train each model for 650,000 iterations and use a relative weight between the losses of 1.0. We use a batch size of 64. The ablation studies in Appendix Table 2 support our architectural choices.

Testing To evaluate the model’s predictions, we chose the F1 score [16], which provides a measure of the model’s inference performance, accounting for both its precision and recall (Appendix 3.2). To evaluate the F1 score on segmentation predictions, we first filter the segmentation maps to keep only voxels with class probabilities above 0.6. We then post-process these maps using the connected-components-3d algorithm [17] to extract centroids of segmented objects (Fig. 2A, B). Connected components with voxel counts below 0.01 or above the 0.8 percentiles are excluded to avoid spurious centroid predictions arising either from the background class (higher end), or from single- or few-voxel connected components (lower end). We apply this procedure to both the GT segmentation maps and the predictions, then compare the centroids for each class per crop, allowing a tolerance of 5-voxel distance in each direction.

Training and Testing data Following the cryo-ET segmentation Kaggle challenge [18], we chose a similar task to test the background simulators. The tomograms for the empirical background model and the templates used during training and testing are found in Table 1. Note that training and testing empirical backgrounds differ.

Results

The model can pick particles in synthetic tomogram crops. We start by visually inspecting the segmentation maps predicted by the model when using different background training strategies. We find that the model can correctly identify the particles when evaluated on test volumes using the same type of background as used for training, namely, either Gaussian noise or empirical background (Fig. 2A, B, respectively). Notably, the empirical background samples used for testing were never seen by the model during training, suggesting that these models can learn to discern the particles from the background irrespective of the tomogram used.

The U-Net bottleneck’s latent space shows separation between the classes. Next, we examined the model’s performance in representation learning. We applied dimensionality reduction to the U-Net bottleneck latent space, which has a dimensionality of 512. The latent space principal component analysis (PCA) is partially structured with the background class being well-differentiated from the others and the VLP class and the β -galactosidase class diverging in opposite directions (blue and pink, respectively, in Fig. 2C top). Moreover, particle classification appears not to be strongly affected by differences in SNR values: values in the experimental range do not necessarily translate into class mixing (Fig. 2C, bottom).

Training with mixed background makes the model’s performance robust to background types. We evaluated the particle-picking performance of our models trained on different background types (synthetic, real, and mixed; Fig. 1D, and Figs. 3, ??A, B). The model trained with a synthetic background performs satisfactorily only when evaluated on particles in a Gaussian background. Similarly, the model trained using the empirical background scored satisfactorily only when evaluated on particles in empirical background samples. This suggests that training only on one type of

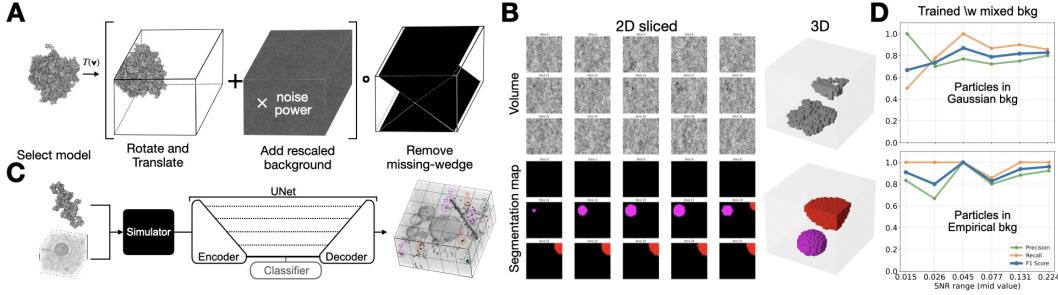


Figure 1: (A) The simulator pipeline. From left to right, we select the particle structures to populate the volumes, apply rotation and translation to each, rescale the background according to the SNR, and remove the missing wedge in Fourier space. (B) An example of a simulated volume with Gaussian background noise and its ground truth (GT) segmentation map (left), shown as 2D slices along the imaging axis. 3D representations of the volume (background not shown) and its GT segmentation (right). Red indicates a ribosome and magenta β -galactosidase. (C) The model’s architecture. We input templates (maps or PDBs) and experimental or Gaussian background crops into the simulator (left), which combines them and passes them to the UNet (center), which finally outputs the segmentation maps of the tomogram crops (right). (D) Model performance when training with mixed background simulators. The line plots show F1 score, precision, and recall at different SNR levels (Appendix 3.2). We report the range mid-value.

background does not allow the model to generalize across background types. Conversely, when trained using the simulator with mixed backgrounds, the model achieved an excellent performance in both tasks with an F1 score up to 1.0, demonstrating generalization across different backgrounds.

Training on synthetic data is sufficient to distinguish particles from background in real tomograms. To assess whether the simulator can reproduce cryo-ET-like data for training, we passed experimental crops through our best-performing model (trained with mixed backgrounds) and projected their latent embedding onto the PCA space spanned by the embedded simulated crops. We observed that the embeddings overlap (Fig. 5A, B), thereby substantiating our hypothesis. Next, we investigated the representation learning performance of our best model on real tomogram crops. To do this, we performed a PCA directly on the embeddings of the empirical crops. Our observations revealed that, in the latent space, crops with no particle (only background) are positioned separately from those that contain particles (Fig. 5C). This indicates that training the model solely on simulated data enables discrimination between crops containing particles and background-only crops in real tomograms. However, when we visualized the predicted segmentations, we noticed that the model struggles to accurately segment the crop (Fig. 5D).

Conclusions and Discussion

In this study, we sought to identify optimal training strategies for background simulators in cryo-ET. Using a U-Net-based architecture, we show that a mixed background simulator is key to achieving robustness, compelling the model to distinguish particles from diverse backgrounds rather than memorizing background-specific features. While this strategy enabled distinguishing particles-containing from background-only crops in real tomograms, the model still struggles with classification. Misclassification of real particles cannot be attributed to low SNR, as the model performs well in equally noisy simulations (Fig. 5C, D, 2C). Moreover, the overlap between the simulated and experimental latent embeddings indicates that the simulator captures most experimental conditions (Fig. 5A, B). Thus, we believe the main pitfall lies in the templates. Although templates seem a straightforward choice for particle picking, they poorly represent molecular heterogeneity [19]. Using a single template for a particle creates bias in our training dataset. Also, the simulator does not account for particle distortions caused by tilt-series misalignment or aberration corrections, which could affect performance. In conclusion, while challenges related to particle distortions and heterogeneity remain, this work highlights the importance of mixed background simulators for advancing particle-picking annotation in cryo-ET.

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3 Appendix

3.1 Losses: Focal and Cross-entropy Loss

Focal loss:

$$FL = \sum_c \sum_v \alpha_c (1 - p_{v,c})^\gamma \log p_{v,c}, \quad (1)$$

where $p_{v,c}$ is the predicted probability per voxel v and class c . With this choice, we reweight each class by its frequency of appearance (α_c), which is dynamically computed from the GT segmentation maps at each training step. The hyperparameter γ controls the model's focus area. A smaller γ will force the model to focus on areas that are harder to classify, while a larger γ will push the model to focus on higher-confidence areas.

Cross-entropy loss:

$$CE = -\mathbb{E}_P(\log Q), \quad (2)$$

where P is the target distribution and Q is the prediction distribution, both parametrised as an N_{classes} -dimensional simplex.

3.2 Metrics: Precision, Recall and F1 Score

The precision is defined as the fraction of true positives (TP) over all the predicted samples predicted as positive:

$$\text{Precision} = \frac{TP}{TP + FP},$$

where FP is the number of false positives. The recall is defined as the fraction of true positives over all the target positive samples

$$\text{Recall} = \frac{TP}{TP + FN}.$$

The F1 score is defined as

$$F1 = 2 \frac{\text{Precision} \cdot \text{Recall}}{\text{Precision} + \text{Recall}} = \frac{TP}{TP + 0.5(FP + FN)}.$$

3.3 The Model can Classify and Identify Particles in the Simulated Tomogram Crops

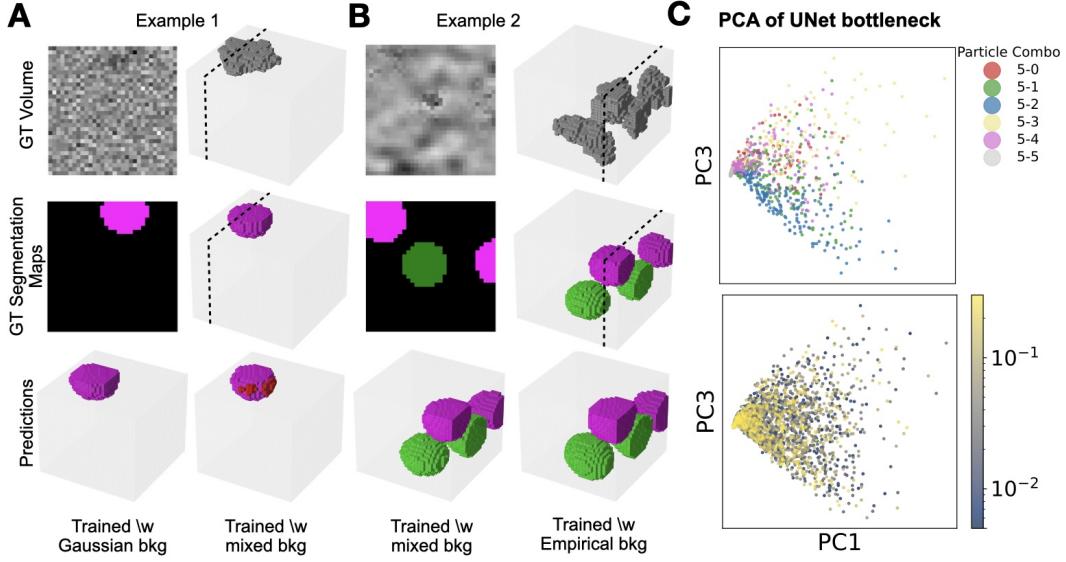


Figure 2: The model classifies and identifies particles in the simulated tomogram crops with Gaussian noise (A) and empirical background (B). Examples of the GT volumes and segmentation are compared to the predictions; the 2D slices are indicated by dashed lines on the 3D volumes. The bottom row shows the predictions when training with a Gaussian background (bkg) or with the mixed bkg. (C) PCA of the UNet bottleneck latent space, evaluated on Gaussian bkg volumes, coloured according to the particle classes (top) and SNR values (bottom) for the model trained with Gaussian bkg.

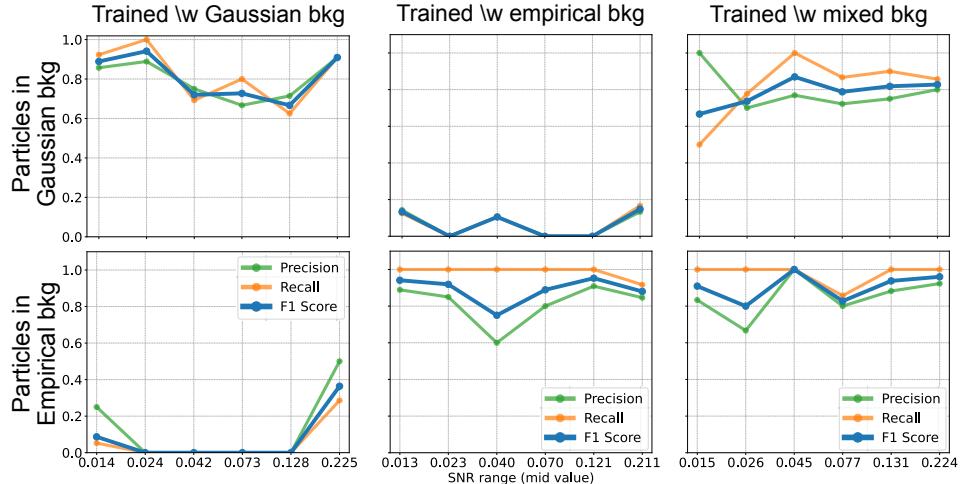


Figure 3: Comparison of model performance between training with synthetic, empirical, and mixed background simulators. The line plots show F1 score, precision, and recall at different SNR levels (Appendix 3.2). We report the range mid-value.

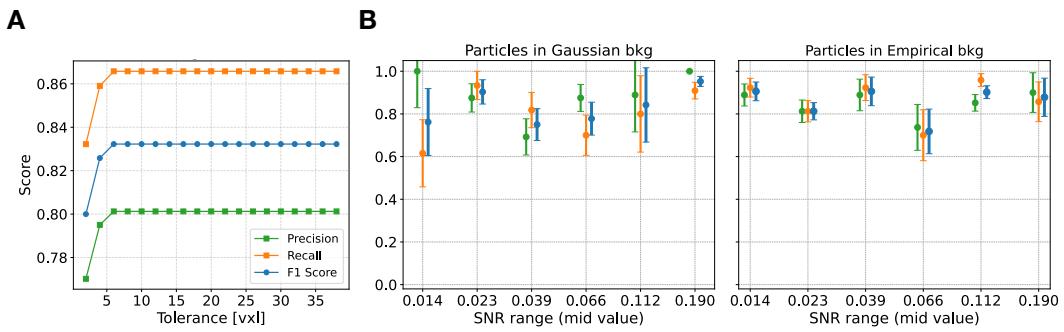


Figure 4: Statistical analysis of the model trained with mixed backgrounds. **(A)** Metrics of the models depending on the allowed distance (in voxels) between the predicted centroids and the ground truth. **(B)** average model metrics across different SNR intervals. The error bars correspond to the standard deviation of the mean.

3.4 Training on Synthetic Particles is Sufficient to Distinguish Particles from Background in Real Tomograms

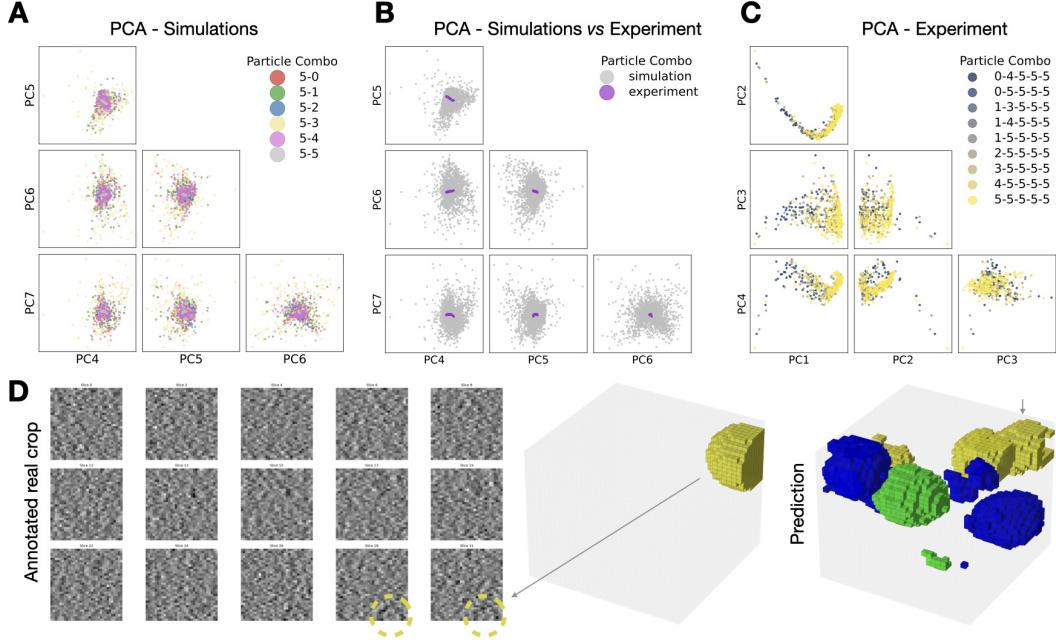


Figure 5: The model’s latent representation distinguishes pure background from particles in real tomograms. (A) PC4 to 7 of the UNet bottleneck latent space representation (original dimensionality 512) of mixed backgrounds tomograms. (B) PC4 to PC7 plots showing the reduced representation of the latent space of simulated and empirical data. After passing the empirical data through the model, we projected them onto the same PCA space as the simulated data. (C) First four PCs of the UNet bottleneck latent-space representation of real tomogram crops. The datapoints are coloured according to the combination of class objects in the crops. Note that class 5 is the background class. (D) Example of a real tomogram crop (left and center) and its predicted segmentation map (right).

3.5 Input Configuration Parameters of the Simulator used during Training and Testing

The tomograms used can be found on the Cryo-ET Data Portal at <https://cryoetdataportal.czscience.com/browse-data/datasets> [20]. The maps used as templates can be found on EMPIAR at <https://www.ebi.ac.uk/empiar>. With an edge length of 32 voxels, the U-Net has a

Table 1: Simulator configuration parameters

Parameter	Value
Batch size	64
Crop edge	32 (vxl)
Obj per crop	5
SNR	[0.0005-0.3]
Shift	[0-20] (vxl)
Voxel size	[5.0-15.0] (Å)
Sphere radius	12 (vxl)
Tomograms used as bkg (Train)	TS_103_5.mrc TS_102_2.mrc TS_100_3.mrc TS_73_6.mrc TS_5_4.mrc 24nov01d_Position_38.mrc 24nov01d_Position_42.mrc 24nov01d_Position_43.mrc TS_6_6.mrc emd_3883.map (Ribosome, class 0, red) emd_24181.map (Thyroglobulin, class 1, green) emd_41917.map (VLP, class 2, blue) emd_41923.map (Apo ferritin, class 3, yellow) emd_0153.map (β -galactosidase, class 4, magenta)
Tomograms used as bkg (Test)	
Templates	

depth of 5 layers, comprising 5 pooling layers (for downsampling) and 5 transposed convolutional layers (for upsampling). Each up- or down-sampling operation is followed by a double convolution. Before the first downsampling layer, we perform a double convolution. Each convolution includes a 3D batch normalization operation followed by a ReLU activation. Each run used 1 A100 Nvidia GPU, 4 CPUs per node, and 16 GB of memory per CPU.

3.6 Ablation Studies

We conducted ablation studies to evaluate the projector head’s impact on centroid prediction accuracy. Additionally, we examined the impact of using spheres with a fixed radius for each class, rather than a different radius for each class, when creating the GT segmentation maps for segmentation supervision. We performed ablation studies based on our most effective training strategy, which used a mixed background simulator. For testing on real backgrounds, we used different tomograms than those used during training. We report the average precision, recall, and F1 score, with a tolerance of 5 voxels for centroid comparison.

Table 2: Ablation studies. The "Loss weight" field indicates the relative weight applied to the projector loss. P, R and F1 stand for Precision, Recall and F1 score, respectively

Ablation	Loss weight	Gaussian bkg			Empirical bkg		
		P	R	F1	P	R	F1
Same sized spheres	1.0	0.7	0.8	0.8	0.8	0.9	0.9
Same sized spheres	0.1	0.7	0.7	0.8	0.7	0.7	0.8
Same sized spheres	0.0	0.7	0.8	0.9	0.7	0.8	0.8
Different sized spheres	1.0	0.5	0.5	0.5	0.4	0.6	0.5

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