

Unlocking 2D Promptable Foundation Models for 3D Vessel Segmentation by Automatic Prompt Generation

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Abstract

3D vessel segmentation is a core task in medical image analysis, playing a crucial role in disease diagnosis and surgical planning. While fully supervised 3D segmentation methods rely on costly high-quality annotations, prompt-guided models (e.g., ScribblePrompt) provide a promising alternative with their zero-shot generalization capability for efficient 3D segmentation. Nevertheless, when directly applied to 3D tasks, these 2D methods require slice-wise prompts, disregarding the continuity of 3D structures and leading to low efficiency. To address this issue, we propose an innovative method based on automatic prompt generation, which integrates with pre-trained 2D interactive models to achieve efficient 3D vessel segmentation. By leveraging spatial continuity and contextual information, our method automatically generates prompts across the entire 3D volume from a single user-provided prompt. Experiments conducted on public and in-house vessel datasets demonstrate the effectiveness of the proposed method, showing that it achieves segmentation accuracy comparable to or better than state-of-the-art models, while significantly reducing the interaction cost.

Keywords: Vessel Segmentation, Foundation Models, Automatic Prompting, Topology Preservation.

1. Introduction

Cardiovascular diseases remain the leading cause of death worldwide. According to data from the World Health Organization, approximately 17.9 million people die from cardiovascular diseases each year, accounting for 32% of global deaths (Chen et al., 2020). Accurate vascular morphometry analysis is crucial for early diagnosis, risk assessment, and treatment planning for cardiovascular diseases (Sweeney et al., 2024; Zeng et al., 2024).

Vascular segmentation, as a fundamental technology in medical image analysis, aims to accurately extract vascular structure from medical images, including vessel trajectory, morphology, diameter, and other clinical biomarkers (Liu et al., 2022; Qi et al., 2023). These details are vital for diagnosing vascular conditions such as stenosis or aneurysms and are valuable for surgical planning and intervention guidance (Fu et al., 2023; Yao et al., 2023). However, significant challenges persist due to factors such as the intricate complexity of vascular structures, inherent imaging quality limitations, and various pathological alterations that complicate automated analysis (Acebes et al., 2024; Shi et al., 2024).

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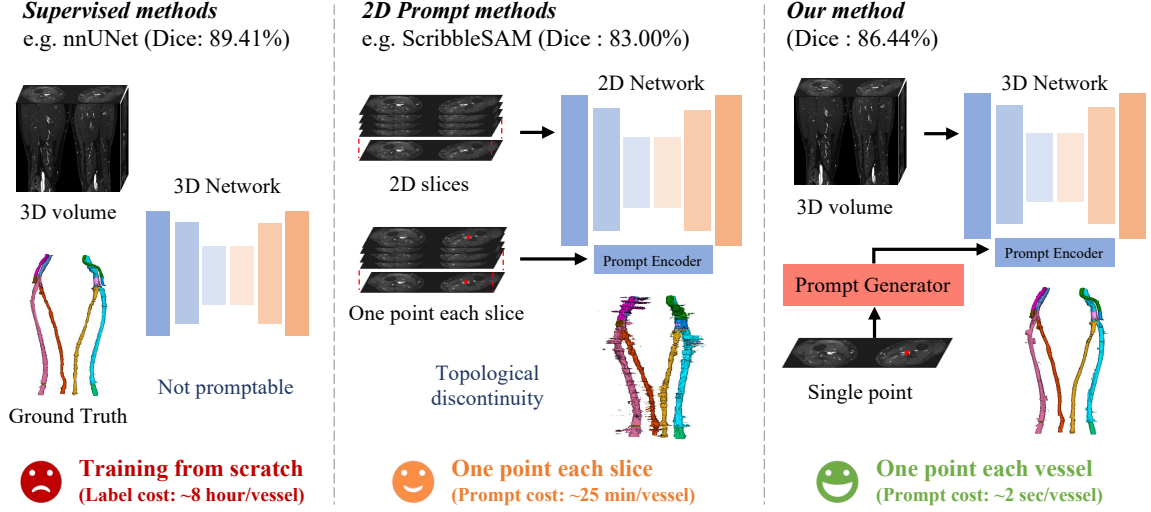


Figure 1: Motivation and Performance Overview. Comparison of three paradigms for 3D vessel segmentation. (Left) Fully Supervised Methods (e.g., nnU-Net): Achieve high accuracy but require labor-intensive voxel-wise annotations (~8 hours/vessel). (Middle) Naive 2D Prompt Methods (e.g., ScribbleSAM): Apply slice-by-slice prompting, which is still time-consuming (~25 min/vessel) and often leads to topological discontinuities (broken vessels) due to lack of 3D context. (Right) Our Method: By utilizing a single initialization point, our approach automatically generates prompts via topological continuity learning. We achieve competitive performance comparable to supervised methods but with orders of magnitude faster interaction (~2 sec/vessel), ensuring coherent 3D structures.

Traditional manual segmentation is labor-intensive and prone to inter-observer variability. While deep learning-based methods have automated segmentation in mainstream modalities like coronary CTA (Dai et al., 2024; Geng et al., 2024; Qiu et al., 2023; Xie et al., 2024), their success heavily relies on large-scale, high-quality annotated datasets (Guo et al., 2024). This data dependency becomes a bottleneck for emerging imaging techniques such as Fe-MRA or underrepresented peripheral vessels (Ghodrati et al., 2022). Recently, promptable foundation models, such as the Segment Anything Model (SAM), have emerged as a promising solution to annotation scarcity due to their impressive zero-shot generalization capabilities. However, a critical limitation hinders their application in 3D medical imaging: standard foundation models are inherently 2D. Applying them to 3D volumes typically requires slice-by-slice prompting, which disrupts the 3D spatial continuity of vascular structures and results in prohibitive interaction costs (Magg et al., 2025). This issue is particularly pronounced in complex scenarios like Fe-MRA, where sparse acquisition protocols lead to topological discontinuities (Si et al., 2025), making simple slice-wise propagation unreliable (Si et al., 2024).

To bridge the gap between 2D foundation models and 3D vascular segmentation, we propose an innovative framework that unlocks the potential of SAM through *automatic*

prompt generation. As illustrated in Fig. 1, our approach addresses the inefficiency of slice-wise interaction by leveraging the inherent geometric continuity of vessels. Instead of requiring dense prompts for every slice, our method necessitates only a single initial point. It then employs a topology-aware strategy to automatically propagate prompts across the entire 3D volume, effectively “stitching” 2D predictions into a coherent 3D structure. This strategy integrates two key innovations: (1) an end-to-end segmentation framework with global and local continuity constraints to overcome spatial inconsistencies; and (2) a confidence-aware prompt generation mechanism that exploits vascular topology to refine and extend segmentation cues iteratively. By combining the generalization power of SAM with explicit vascular priors, we reduce the annotation time from hours to seconds while maintaining high topological consistency.

The main contributions are summarized as follows:

- We introduce a novel topology-constrained framework that extends 2D promptable models to 3D vascular segmentation, requiring only a single initialization point to achieve comprehensive volumetric segmentation.
- We develop a topology-driven automatic prompt generation strategy that leverages vascular structural continuity with iterative confidence-aware refinement, significantly reducing interaction costs compared to slice-wise prompting.
- Extensive experiments demonstrate the effectiveness of our method, achieving state-of-the-art performance with 86.44% Dice on a public CTA dataset and 80.20% Dice on an in-house Fe-MRA dataset, showcasing superior generalization across different modalities and vascular complexities.

2. Method

Upon the success of prompt-based learning in medical imaging (Ma et al., 2024), we propose a dimension-hybrid framework that unlocks the potential of 2D foundation models for 3D vascular segmentation. As illustrated in Fig. 2, our method requires only a *single* user-provided point on the first slice to segment the entire 3D volume. The framework consists of two synergistic components: (1) a **Weakly Supervised 3D Network** that extends a 2D SAM-based backbone with local and global geometric constraints to ensure volumetric consistency, and (2) a **Topology-Aware Prompt Generator** that automatically propagates and refines point prompts across slices, eliminating the need for slice-by-slice prompting.

2.1. Weakly Supervised 3D Network with Geometric Constraints

Conventional volumetric methods (Isensee et al., 2021) often suffer from high computational costs, while naive 2D slice-based approaches neglect the inherent 3D continuity of vascular structures. Our approach bridges this gap by employing a pre-trained 2D SAM encoder to extract robust features from individual slices, while enforcing 3D consistency through a dual-level regularization framework.

Given a 3D volume, we process it as a sequence of 2D slices. For each slice I_i , the network takes the image and an automatically generated prompt p_i (detailed in Sec. 2.2)

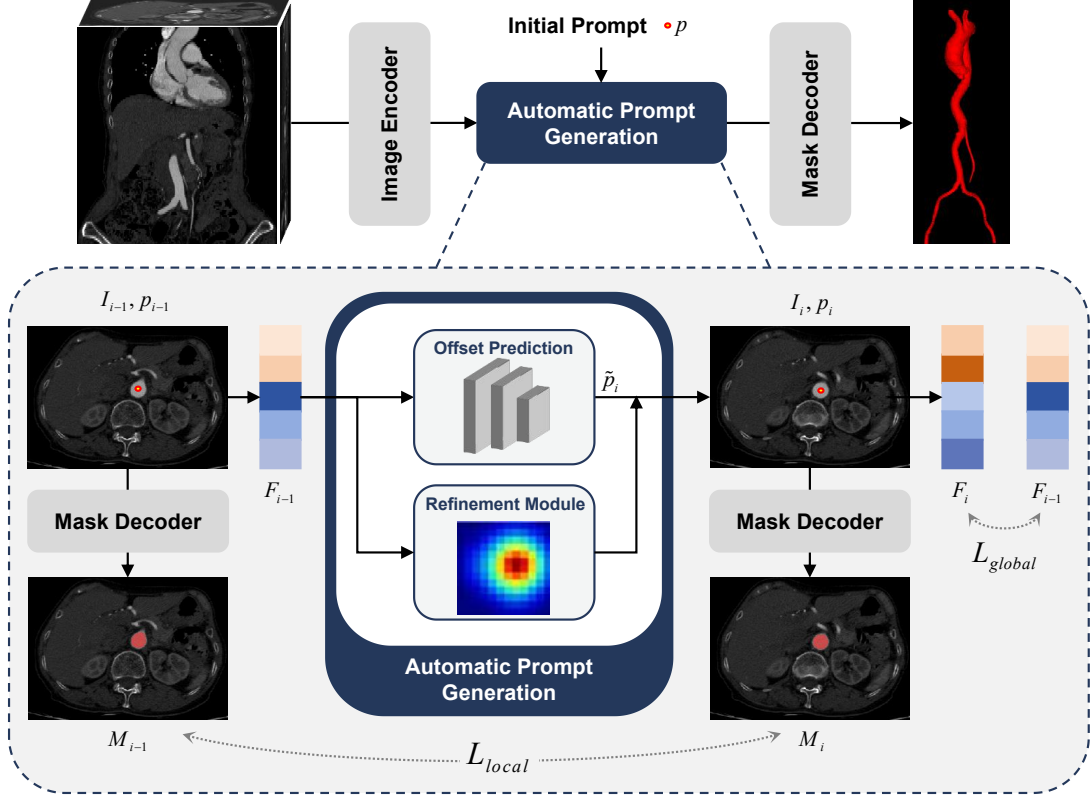


Figure 2: Overview of the proposed framework. (Top) The 3D weakly supervised network processes the volume slice-by-slice, enforcing volumetric consistency via Local Continuity Loss (L_{local}) and Global Consistency Loss (L_{global}). (Bottom) The Automatic Prompt Generation module propagates the prompt from slice $i - 1$ to i . It utilizes an Offset Prediction network and a Refinement Module based on previous features F_{i-1} to accurately locate the vessel center p_i .

to predict a segmentation probability map P_i . To address the topological fragmentation common in 2D-based predictions, we introduce two loss functions:

Local Continuity Loss (L_{local}). Vascular structures exhibit gradual morphological transitions across adjacent slices. To enforce this smoothness, we impose a local continuity constraint that penalizes abrupt changes in the segmentation shape and position. We formulate the inter-slice gradient consistency as:

$$L_{grad} = \sum_i \|\nabla_z P_i - \nabla_z P_{i+1}\|_1 \quad (1)$$

where $\nabla_z P_i = P_i - P_{i-1}$ represents the discrete difference of probability maps along the z -axis (slice dimension). Minimizing the difference between consecutive gradients ($\nabla_z P_i$ and $\nabla_z P_{i+1}$) effectively encourages a constant velocity in shape evolution, resulting in smooth vascular boundaries.

Additionally, to ensure intra-slice spatial smoothness and reduce noise, we incorporate a Total Variation (TV) term. The aggregate local loss is defined as:

$$L_{local} = L_{grad} + \lambda_{TV} \sum_i \|\nabla_{xy} P_i\|_1 \quad (2)$$

where ∇_{xy} denotes the spatial gradient within the 2D slice, and λ_{TV} balances the regularization strength (empirically set to 0.1).

Global Consistency Loss (L_{global}). While local constraints handle immediate transitions, they may fail to prevent semantic drift over long distances. We therefore introduce a global consistency loss operating in the latent feature space. We assume that the deep feature representations of the same vessel should remain semantically consistent across the volume. We maximize the cosine similarity between the feature embeddings F of adjacent slices:

$$L_{global} = \sum_i \left(1 - \frac{F_i \cdot F_{i+1}}{\|F_i\|_2 \|F_{i+1}\|_2} \right) \quad (3)$$

where F_i is the bottleneck feature map extracted by the Prompt Encoder for slice i . This constraint ensures that the network maintains a stable internal representation of the vascular target throughout the 3D volume.

2.2. Topology-Aware Automatic Prompt Generation

Standard prompt-based methods require manual interaction for each slice, which is prohibitive for 3D volumes with hundreds of slices. To automate this, we design a **Point Prompt Generator** (Fig. 2, bottom) that predicts the optimal prompt p_i for the current slice based on the segmentation result of the previous slice. It operates in two steps:

Step 1: Feature-Driven Offset Prediction. Vessels are continuous tubular structures. The center of a vessel in slice i can be inferred from its position in slice $i - 1$ plus a displacement vector. We employ a lightweight Offset Prediction Module that utilizes the deep features F (from the Prompt Encoder) to estimate this transition. The tentative prompt \tilde{p}_i is calculated as:

$$\tilde{p}_i = p_{i-1} + \text{Net}_{\text{offset}}(F_{i-1}) \quad (4)$$

where p_{i-1} is the prompt used in the previous slice. By conditioning the offset on the rich semantic features F_{i-1} , the network learns to anticipate the vessel’s trajectory (e.g., curvature and branching).

Step 2: Confidence-Guided Refinement. Relying solely on offset prediction may lead to accumulated errors over time. To correct this, we refine the prompt using the network’s own confidence map. After obtaining the initial probability map P_i using \tilde{p}_i , we identify the high-confidence region $\arg \max(P_i)$. The final refined prompt p_i is computed as a weighted fusion:

$$p_i = (1 - \lambda) \cdot \tilde{p}_i + \lambda \cdot \arg \max(P_i) \quad (5)$$

where $\lambda \in [0.1, 0.5]$ is an adaptive scalar derived from the peak confidence value of P_i . This refinement step acts as a self-correction mechanism: if the network is confident in its segmentation (high λ), the prompt is pulled towards the actual vessel center; if uncertainty is high, the system relies more on the topological prior \tilde{p}_i . This ensures robust tracking even in complex vascular bifurcations.

3. Experiments

3.1. Dataset and Implementation Details

We evaluate the efficacy and robustness of our proposed method on two distinct vascular datasets: an in-house Fe-MRA dataset and the publicly available SEG.A. 2023 challenge dataset (Radl et al., 2022). The Fe-MRA dataset serves to assess performance under weakly supervised conditions for complex peripheral vessels, while the public dataset is employed to rigorously validate cross-modality generalization and segmentation accuracy on the Aortic Vessel Tree in CTA scans.

Fe-MRA Dataset. Our study utilized retrospectively collected FE-MRA data from 50 patients acquired between 2023 and 2024. All scans were performed on Siemens scanners with magnetic field strengths of either 3.0 Tesla or 1.5 Tesla. The acquisitions exhibit isotropic in-plane resolution of approximately 0.8 mm in the X-Y dimensions, with a slice thickness of approximately 1.0 mm in the Z dimension. To establish a reliable ground truth, each volumetric scan was independently annotated by two board-certified radiologists with over 5 years of experience in vascular imaging, with the final reference standards determined through a consensus review process.

SEG.A. Dataset. To rigorously evaluate generalization, we further validate our method on the SEG.A. benchmark from the MICCAI 2023 Challenge. This dataset comprises 56 CTA scans of the Aortic Vessel Tree aggregated from three distinct centers, introducing significant anatomical and scanner variability. The data exhibits high heterogeneity in resolution, with voxel spacing ranging from $0.44 \times 0.44 \times 0.50\text{ mm}$ to $1.37 \times 1.37 \times 5.00\text{ mm}$. Notably, the dataset includes large-scale volumes exceeding 1,000 slices along the Z-axis, providing a challenging testbed for processing extensive 3D vascular structures.

Implementation Details. To demonstrate the versatility of our framework, we integrated it with two distinct point-prompted architectures: a SAM-based model and a UNet-based model, both adopted from ScribblePrompt (Wong et al., 2024). This selection highlights our method’s ability to extend arbitrary point-prompted backbones for vascular applications without architectural constraints. All models were implemented in PyTorch and trained on a single NVIDIA RTX 4090 GPU (24GB). Training spanned 200 epochs using the AdamW optimizer (learning rate: 1×10^{-4} , weight decay: 1×10^{-5}) and a cosine annealing scheduler with a 10-epoch warm-up.

Evaluation Metrics. We employ a comprehensive set of metrics to assess both geometric accuracy and topological fidelity. Standard segmentation performance is measured using the Dice Similarity Coefficient (DSC) and the 95% Hausdorff Distance (HD95). Given the tubular nature of vascular structures, we specifically include cLDice (Shit et al., 2021) to evaluate centerline connectivity and Betti Error to quantify topological consistency (e.g., broken vessels or false loops), ensuring clinical reliability.

3.2. Experimental Results

To comprehensively evaluate the clinical viability and technical superiority of our point-prompted vascular segmentation framework, we conducted a multi-dimensional comparison against two distinct methodological paradigms. The first category represents the **fully supervised upper bounds**, including the classic UNet (Ronneberger et al., 2015) and

Table 1: Quantitative comparison on the public SEG.A. segmentation task. Supervised methods serve as the upper bound. Best results among point-prompted methods are highlighted in **bold**.

| Type | Method | Dice (% \uparrow) | clDice (% \uparrow) | HD95 (mm \downarrow) | β_0 error (\downarrow) |
|--------------|----------------|----------------------|------------------------|----------------------------|----------------------------------|
| Supervised | UNet | 82.08 | 92.56 | 18.26 | 0.14 |
| | nnUNet | 89.41 | 96.29 | 9.37 | 0.09 |
| Point Prompt | SAMed-2D | 81.21 | 79.23 | 49.41 | 155.33 |
| | MIDeepSeg | 80.91 | 71.56 | 38.08 | 116.28 |
| | ScribblePrompt | 83.00 | 85.65 | 26.42 | 3.26 |
| | Ours | 86.44 | 89.83 | 19.46 | 1.88 |

the self-configuring nnUNet (Isensee et al., 2021), which require labor-intensive pixel-level annotations. The second category comprises **state-of-the-art weakly supervised and interactive methods**, specifically SAMed-2D (Cheng et al., 2023), MIDeepSeg (Luo et al., 2021), and ScribblePrompt (Wong et al., 2024). Our analysis focuses not only on volumetric overlap (Dice) but places particular emphasis on topological fidelity (clDice, β_0 error), which is critical for downstream vascular analysis such as centerline extraction and hemodynamic simulation.

Performance on Public SEG.A. Dataset. Table 1 details the quantitative performance on the SEG.A. dataset. Our method demonstrates a commanding lead among weakly supervised approaches, effectively bridging the gap towards fully supervised baselines. We achieve a Dice score of **86.44%**, surpassing the closest competitor, ScribblePrompt, by **3.44%**. Notably, this performance is highly competitive with the fully supervised nnUNet (89.41%), suggesting that our point-prompted strategy can recover the majority of vascular structures with significantly reduced annotation costs. The HD95 metric, which is sensitive to outliers, is reduced to **19.46 mm** in our method. This indicates that our approach effectively suppresses false positives in the background, a common issue in SAM-based adaptations where the model struggles with low-contrast medical boundaries. Most critically, our method excels in preserving vascular connectivity. We outperform ScribblePrompt by **4.18%** in clDice and reduce the Betti number error (β_0) from 3.26 to **1.88**. This low topological error rate implies that our segmentation masks contain significantly fewer fracture points, ensuring a continuous vascular tree structure that is essential for clinical diagnosis.

Robustness on In-house Fe-MRA Dataset. The Fe-MRA dataset represents a significantly more challenging scenario characterized by intricate peripheral vessels and variable contrast-to-noise ratios. As shown in Table 2, this domain shift exposes the fragility of existing methods. Methods like SAMed-2D and MIDeepSeg exhibit a drastic performance drop (Dice $< 72\%$). These models, primarily trained on natural images or standard medical datasets, lack the specific inductive bias required to track thin, branching vessels, leading to fragmented outputs (high β_0 error > 172). In contrast, our framework maintains high robustness with a Dice score of **80.20%**. More importantly, we achieve a clDice of **88.13%**, which is comparable to the performance on the simpler SEG.A. dataset. This demonstrates that our slice-to-slice propagation mechanism effectively utilizes the 3D coherence of blood

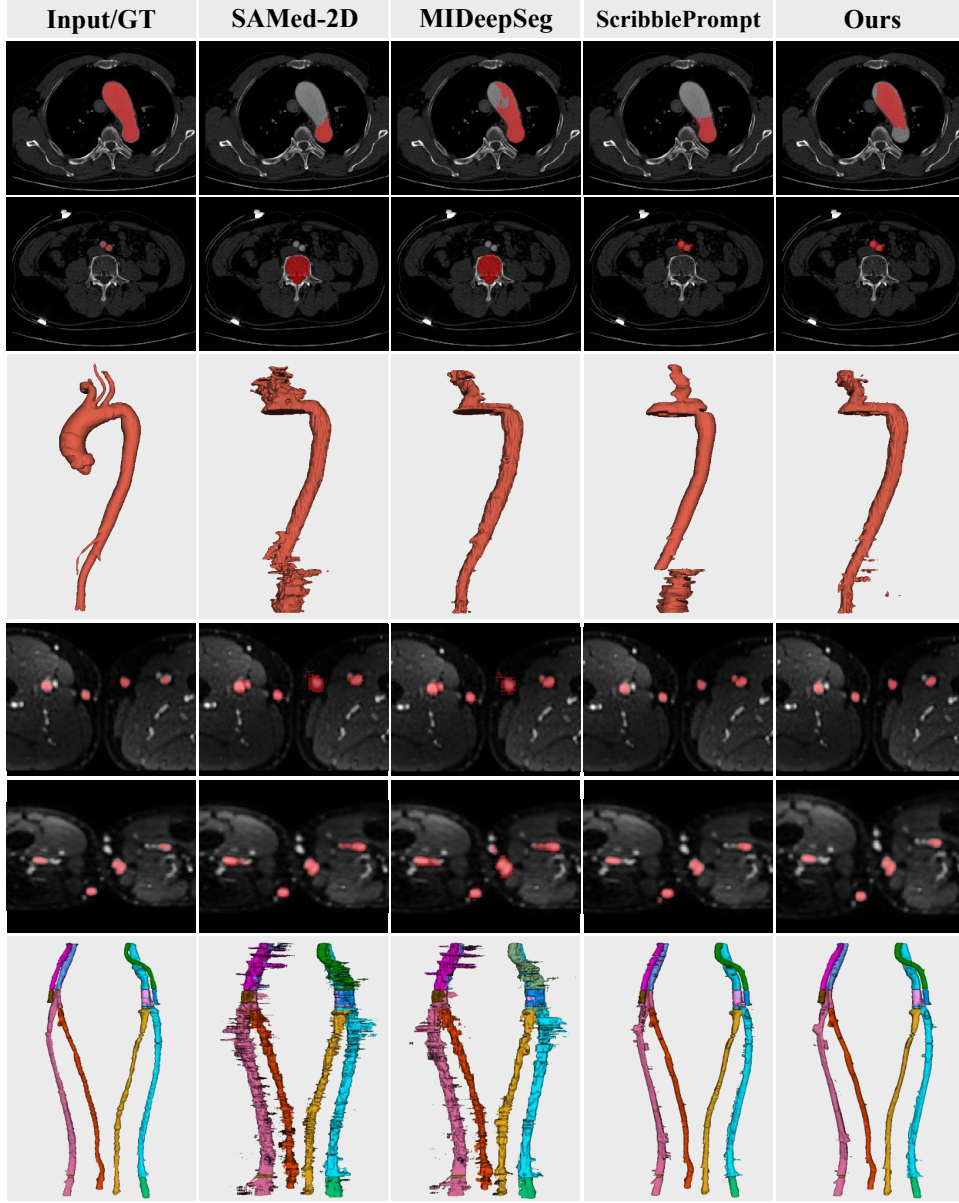


Figure 3: Qualitative comparison of vascular segmentation on SEG.A. (top 3 rows) and Fe-MRA (bottom 3 rows). Topological breaks or false positives are observed in baseline methods, whereas our method effectively corrects them.

vessels, allowing the model to “trace” vessels even when the local contrast is weak. The β_0 error of our method (**40.25**) is substantially lower than ScribblePrompt (67.46). This reduction confirms that our approach is less prone to “breaking” thin vessel segments, a frequent artifact in slice-wise 2D segmentation methods that ignore inter-slice consistency.

Table 2: Quantitative comparison on the challenging in-house Fe-MRA dataset. Note the significant improvement in topological metrics (clDice and β_0 error) achieved by our method.

| Method | Dice (% \uparrow) | clDice (% \uparrow) | HD95 (mm \downarrow) | β_0 error (\downarrow) |
|----------------|----------------------|------------------------|-------------------------|----------------------------------|
| SAMed-2D | 69.57 | 61.65 | 38.69 | 207.6 |
| MIDeepSeg | 72.99 | 67.17 | 38.71 | 172.3 |
| ScribblePrompt | 77.25 | 86.21 | 19.92 | 67.46 |
| Ours | 80.20 | 88.13 | 11.18 | 40.25 |

Qualitative Analysis. Fig. 3 provides a visual comparison that corroborates our quantitative findings. In the SEG.A. dataset (top 3 rows), baseline methods often struggle with boundary definition. For instance, SAMed-2D tends to under-segment the vessel walls, while ScribblePrompt occasionally leaks into adjacent tissues. The disparity is even more pronounced in the Fe-MRA dataset (bottom 3 rows). As indicated by the red arrows, competing methods produce discontinuous “dotted” patterns for distal vessels, severing the vascular tree. Our method, leveraging the propagated point prompts, successfully reconstructs the complete vascular geometry. The 3D renderings clearly show that our result is the only one that maintains the structural integrity of the entire vascular network without significant topological breaks.

3.3. Ablation Study

To investigate the individual contributions of the proposed components to the overall segmentation performance and topological consistency, we conducted a comprehensive ablation study on the SEG.A. dataset. We established a baseline model using the pre-trained SAM-based 2D network with slice-by-slice manual prompting (simulated by using the ground truth center of the previous slice without any learnable offset or refinement). As shown in Table 3, we progressively incorporated the Local Continuity Loss (\mathcal{L}_{local}), Global Consistency Loss (\mathcal{L}_{global}), Offset Prediction, and Confidence-Guided Refinement.

Effectiveness of Geometric Constraints. The baseline model, which treats 3D segmentation as independent 2D tasks, achieved a Dice score of 81.21%. Introducing the Local Continuity Loss (\mathcal{L}_{local}) significantly improved the boundary smoothness between slices, yielding a 1.84% increase in Dice and reducing the HD95 by over 10mm. This confirms that penalizing inter-slice gradient inconsistencies effectively mitigates the “stacking artifacts” common in 2D-to-3D adaptation. Furthermore, the addition of the Global Consistency Loss (\mathcal{L}_{global}) provided a substantial boost in topological fidelity, increasing clDice from 82.05% to 85.12%. By enforcing feature-level similarity across the volume, \mathcal{L}_{global} prevents semantic drift in slices with low contrast or noise, ensuring the model maintains a stable representation of the vessel throughout the scan.

Impact of Automatic Prompt Generation Strategies. A critical innovation of our framework is the replacement of manual prompts with an automated mechanism. We first evaluated the Offset Prediction module (Eq. 4), which predicts the vessel center displacement based on previous features. This mechanism alone achieved a Dice of 85.33%,

Table 3: Ablation study on the SEG.A. dataset. We progressively add components to the Baseline (Naive Slice-wise SAM). \mathcal{L}_{local} : Local Continuity Loss; \mathcal{L}_{global} : Global Consistency Loss; *Offset*: Feature-Driven Offset Prediction; *Refine*: Confidence-Guided Refinement.

| Baseline | \mathcal{L}_{local} | \mathcal{L}_{global} | Offset | Refine | Dice (% \uparrow) | clDice (% \uparrow) | HD95 (mm \downarrow) | β_0 error (\downarrow) |
|----------|-----------------------|------------------------|--------|--------|----------------------|------------------------|-------------------------|----------------------------------|
| ✓ | | | | | 81.21 | 79.23 | 49.41 | 155.33 |
| ✓ | ✓ | | | | 83.05 | 82.05 | 38.12 | 89.45 |
| ✓ | ✓ | ✓ | | | 84.19 | 85.12 | 25.60 | 24.18 |
| ✓ | ✓ | ✓ | ✓ | | 85.33 | 88.51 | 21.05 | 8.62 |
| ✓ | ✓ | ✓ | ✓ | ✓ | 86.44 | 89.83 | 19.46 | 1.88 |

demonstrating that the network can effectively learn the trajectory of vascular structures. However, relying solely on offset prediction led to accumulated errors in tortuous vessel segments, as indicated by a suboptimal β_0 error. Finally, incorporating the Confidence-Guided Refinement (Eq. 5) resulted in the best performance across all metrics. This module acts as a self-correction mechanism; by pulling the prompt towards high-confidence regions, it recovered 1.32% in clDice and reduced the topological error (β_0) to 1.88. This result highlights the necessity of combining historical trajectory priors (offset) with current observational evidence (confidence map) for robust 3D tracking.

4. Conclusion

In this paper, we presented a novel framework that adapts the Segment Anything Model for 3D volumetric vessel segmentation. By integrating a geometric continuity constraint and a global consistency mechanism, we effectively resolved the slice-to-slice inconsistency problem inherent in 2D-to-3D adaptation. Moreover, our proposed learnable offset prediction and confidence-guided refinement modules eliminate the need for manual interaction, enabling fully automated and robust vessel tracking. Extensive experiments demonstrate that our method outperforms existing state-of-the-art approaches in both segmentation accuracy and topological fidelity. We believe this work provides a scalable and effective solution for leveraging 2D foundation models in 3D medical image analysis.

Limitations and Future Work. Although the refinement module reduces error propagation, the slice-by-slice processing within our model remains inherently susceptible to it. Meanwhile, the slice-by-slice processing also prevents the method from recovering vessel segmentation that turn back into earlier slices. Additionally, handling complex bifurcations where a single vessel splits into multiple branches remains a challenge for the current single-point prompting mechanism. Future work will focus on integrating a multi-hypothesis tracking approach to handle bifurcations more effectively and exploring bi-directional propagation to further reduce error accumulation.

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