

Longitudinal Modeling of Stroke using Stochastic Distances and NODDI Diffusion Model

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Synopsis

Limited prior work has explored longitudinal modeling of human brain stroke using advanced diffusion techniques. We aim to address this gap by analyzing longitudinal stroke data from diffusion spectrum imaging for modeling and predicting clinical markers of stroke recovery. Our proposed data analysis method uses a mixed-effect model which exploits stochastic distances from these images for improved regression model statistics and handling of imbalanced, inconsistent longitudinal data. We also demonstrate that this aids in differentiating between population-level and patient-level effects and the corresponding key contributing predictors at each of these levels.

Introduction

Diffusion MRI has been a widely used to study brain stroke. While most studies use DTI¹, recent studies have focused on advanced diffusion techniques (e.g. DKI², NODDI³ which incorporate sophisticated biophysical modeling and have shown improvements over DTI in post-stroke analysis and recovery predictions⁴. However, most of these use a single timepoint in the acute phase (< 1 month of stroke)⁴. Very few studies analyze both acute and chronic stages^{5,6,7} and use a group-wise comparison strategy which doesn't fully exploit the repeated-measure design. In contrast, we present our analysis on Diffusion Spectrum Imaging (DSI) data acquired longitudinally for each stroke subject to model clinical markers of stroke recovery. We hope to characterize immediate as well as long-term post-stroke biophysical changes leading to an improved understanding of stroke recovery and subsequent therapy choices.

Our planned timings for MRI acquisitions are ~2 weeks, 1 month and 3 months. However, despite an initially well-thought study design, often practical limitations arise due to patient unavailability. For example, Fig. 1 (left) shows that longitudinal MRI scans for most patients do not align with these planned timings, including several missing scans. This makes a group-wise analysis inaccurate due to large intra-group variability. We propose using a mixed-effect model which can successfully handle imbalanced and missing timepoints and benefits from a joint estimation of the overall population trend as well as patient-specific trends. However, instead of conventional mixed-effect modeling, we show that whenever possible, using stochastic 'distances' inside these models leads to improved model statistics (Fig.1 (right)). Prior work has shown that stochastic 'distance' measures can be used to quantify the dissimilarity between two image regions-of-interest (ROI). They are more powerful in their ability to capture ROI differences than the traditional approach of using the 'mean diffusion value' as the ROI summary^{8,9,10,11}.

Method

Longitudinal DSI data is acquired from 12 stroke subjects: 5 with 3 timepoints, 7 with 2 timepoints (Fig.1, 3T scanner, NODDI model based on DSI, 203 directions, max b=4000). Corresponding clinical scores (Fugl-Meyer) indicating recovery are also acquired. We use the ODI diffusion values (Orientation dispersion index from the NODDI model³) from the motor tract as they are an important biomarker of post-stroke recovery¹². The mixed-effect regression model uses the following: longitudinal clinical scores (response variable), subject ID (grouping variable), number of 'days' since stroke to capture the DSI scan timings (predictor variable 1), inter-hemispheric difference in the ODI values from the motor ROI (predictor variable 2). The inter-hemispheric ODI differences are captured in one of two ways. 1) 'ODI-Mean-Diff: ROI represented via mean ODI value, with difference as {Mean ODI (Ipsilateral) - Mean ODI (Contralateral)}. 2) ODI-Distribution-Diff (ROI represented using the entire histogram of ODI values, with difference as the Earth Mover Distance between Ipsilateral and Contralateral ODI histograms^{11,10}. After systematically exploring various model choices and variable combinations using likelihood-ratio tests, we summarize the findings from the top three models in Fig. 2 (based on statistical significance of fixed and random regression coefficients and model comparison tests, low standard errors, tight lower-upper bounds). For each model choice, the fixed effect is the overall population-level trend and the random effect is the patient-level deviation from the fixed effect. Both fixed and random effects may include intercept, any of the predictor variables and their combinations.

Results

Longitudinal ODI values are an important predictor at the population-level (along with the intercept) (Models 1,2,3 in Fig. 2, Fig. 3). This matches prior work where diffusion imaging can help with clinical recovery prediction^{1,4}. Individual variability in ODI values is also important to subject-specific trends (Models 1,3). Additionally, due to subject-specific scan timing inconsistencies, 'days' is also a critical predictor for the random-effects (Models 2,3). Results also demonstrate that any model using 'ODI-Mean-Diff' distances, fails to find a statistically significant, population-level ODI trend. Even though the intercept is significant, it does not inform about the value of any of the predictor variables. In contrast, when we use 'ODI-Distribution-Diff' distances, all models find statistically significant, population ODI trend. Note that a lower-upper bound for the random effect which doesn't include zero, indicates a significant subject-specific deviation from the population's fixed effect. Since all models have these bounds outside zero, this points to the importance of mixed-effects modeling which can differentiate the underlying subject-specific effects from the overarching fixed-effects while also identifying the corresponding key contributing predictors for each of these effects.

A likelihood ratio test to compare the 'ODI-Mean-Diff' models with 'ODI-Distribution-Diff' (last column, Fig. 2) further highlights that stochastic-distances provide better model fits than mean-distances. Overall, Model 3 using 'ODI-Distribution-Diff', gives the best results, with Model 2 with 'ODI-Distribution-Diff', being a close second.

Conclusion

We demonstrate the value of longitudinal modeling for stroke using advanced diffusion techniques. The results are promising and must be validated further on larger datasets. By using data efficiently and jointly across subjects (versus individual patient modeling or dummy variables per subject), a mixed-effect longitudinal model scales better to larger datasets and naturally accounts for correlation in repeated scans. Stochastic 'distance' measures when plugged into classic mixed-effect settings, create an easy but powerful method to exploit subtle, nuanced differences hidden within image ROIs.

Acknowledgements

We are grateful to Dr. Jennifer Majersik, Dr. Lorie Richards, Kinga Aitken, and Dr. Ganesh Adluru of the University of Utah for assisting with the stroke dataset used for this study.

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Figures

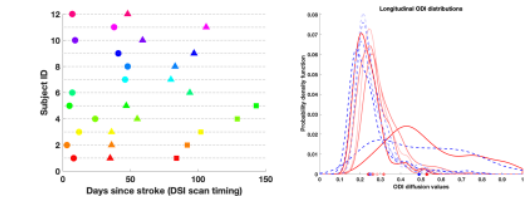


Fig. 1: Left: Longitudinal DSI (Diffusion spectrum imaging) scans acquired for 12 stroke subjects (each subject with different color). The plot shows the scan timings (and highlights missing scans and timing inconsistencies). First scan per subject (circles), second scan (triangle), third scan (square). Right: ODI probability distributions (motor region) for one subject. Red: Ipsilateral, Blue: Contralateral. Dark to lighter colors indicate first to third timepoint. 'Plus' markers show the corresponding mean ODI values for each distribution.

	ODI-Distribution-Diff (uses Earth Mover's distance between ODI diffusion histograms from ROIs)				ODI-Mean-Diff (uses classic difference of mean ODI values in ROIs)				Distribution vs. Mean (Likelihood ratio test to compare model fits)
Models	Fixed effects		Random Effects		Fixed effects		Random Effects		
		Coefficient estimate (Standard Error)	P-value for coefficient	Std. Dev of PDF of random effect (Lower, Upper bounds)		Coefficient estimate (Standard Error)	P-value for coefficient	Std. Dev of PDF of random effect (Lower, Upper bounds)	
#1	Intercept	50.8 (5.0)	1e-10 **	Intercept (0.003, 31.8)	Intercept	45.3 (4.7)	3e-10 **	Intercept (1.15, 35.5)	0.02 (0.01, 0.04)
	ODI	-2.9 (1.2)	0.03 *	ODI (0.5, 4.6)	ODI	181.2 (115.1)	0.13	ODI	
#2	Intercept	47.5 (5.6)	4e-9 **	Intercept (1.5, 28.8)	Intercept	43.1 (5.2)	7e-9 **	Intercept (2.9, 23.9)	0.03 (0.02, 0.04)
	ODI	-2.7 (0.4)	0.01 *	Days (0.03, 0.4)	ODI	174 (101.5)	0.09	Days (0.01, 0.8)	
#3	Intercept	49.7 (5.1)	2e-10 **	Days (0.02, 0.5)	Intercept	45.3 (4.4)	9e-11 **	Days (0.004, 1.4)	0.02 (0.01, 0.03)
	ODI	-3.1 (1.2)	0.01 *	ODI (0.4, 4.3)	ODI	211.9 (114.9)	0.08	ODI	

Fig. 2: Table summarizing the top three longitudinal mixed-effect models among all explored variable combination choices.

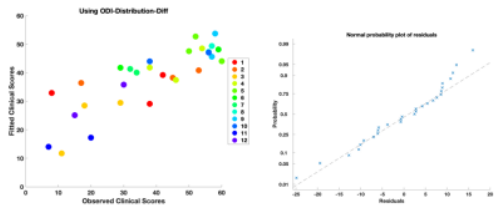


Fig 3: Left: Observed clinical scores versus fitted clinical scores (mixed-effect fit: Fig. 2, Model 3 using ODI-Distribution-Diff distances). Colors indicate grouping by Subject ID. Right: The corresponding residuals plotted against a normal-distribution probability plot showing that residuals mostly follow a 0-mean gaussian, as expected from a well-fitted linear model.