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# ManiBCI: Manipulating EEG BCI with Invisible and Robust Backdoor Attack via Frequency Transform

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## Abstract

1 The electroencephalogram (EEG) based brain-computer interface (BCI) has taken  
2 the advantages of the tremendous success of deep learning (DL) models, gaining a  
3 wide range of applications. However, DL models have been shown to be vulnerable  
4 to backdoor attacks. Although there are extensive successful attacks for image,  
5 designing a stealthy and effective attack for EEG is a non-trivial task. While  
6 existing EEG attacks mainly focus on single target class attack, and they either  
7 require engaging the training stage of the target DL models, or fail to maintain  
8 high stealthiness. Addressing these limitations, we exploit a novel backdoor attack  
9 called **ManiBCI**, where the adversary can arbitrarily manipulate which target class  
10 the EEG BCI will misclassify without engaging the training stage. Specifically,  
11 ManiBCI is a three-stages clean label poisoning attacks: **1)** selecting one trigger  
12 for each class; **2)** learning optimal injecting EEG electrodes and frequencies masks  
13 with reinforcement learning for each trigger; **3)** injecting the corresponding trigger's  
14 frequencies into poisoned data for each class by linearly interpolating the spectral  
15 amplitude of both data according to the learned masks. Experiments on three EEG  
16 datasets demonstrate the effectiveness and robustness of ManiBCI. The proposed  
17 ManiBCI also easily bypass existing backdoor defenses. Code will be published  
18 after the anonymous period.

## 19 1 Introduction

20 Deep learning (DL) has greatly boosted the performances of the electroencephalogram (EEG) based  
21 brain-computer interfaces (BCI), which have been widely used in medical diagnosis [1], healthcare  
22 [2], and device control [3, 4]. While DL-based systems are shown to be vulnerable to backdoor  
23 attacks (BA) [5–7], where an adversary embeds a hidden backdoor into a DL models to maliciously  
24 control it's outputs for inference samples containing particular triggers (a.k.a, poisoned samples), the  
25 security of the DL-based EEG BCI has been long neglected.

26 However, compared to image, designing an effect and stealthy BA for EEG is not trivial for three  
27 difficulties, which lead to three questions. **D1:** EEG data has a significantly low signal-to-noise  
28 ratio (SNR) [8], even the accuracies of original EEG tasks are very low [9]. **Q1:** How to develop an  
29 EEG BA with high attack success rate (ASR) while preserving the clean accuracies of original task?  
30 **D2:** Previous studies demonstrated for different EEG tasks, there are some different critical EEG  
31 electrodes and frequencies that strongly related to the performance of EEG BCI [10–14], indicating  
32 that the trigger-injection strategy (*i.e.*, which electrodes and frequencies to inject triggers) inevitably  
33 affect the performance of BA. **Q2:** How to find the optimal strategy for different EEG tasks? **D3:**  
34 Certain classes of EEG have specific morphology that can easily be identified by human expert, *e.g.*,  
35 in epilepsy detection, the amplitudes of the ictal phase EEG are larger than those of the normal state  
36 phase EEG [15]. **Q3:** How to maintain the consistency of the label and the morphology?

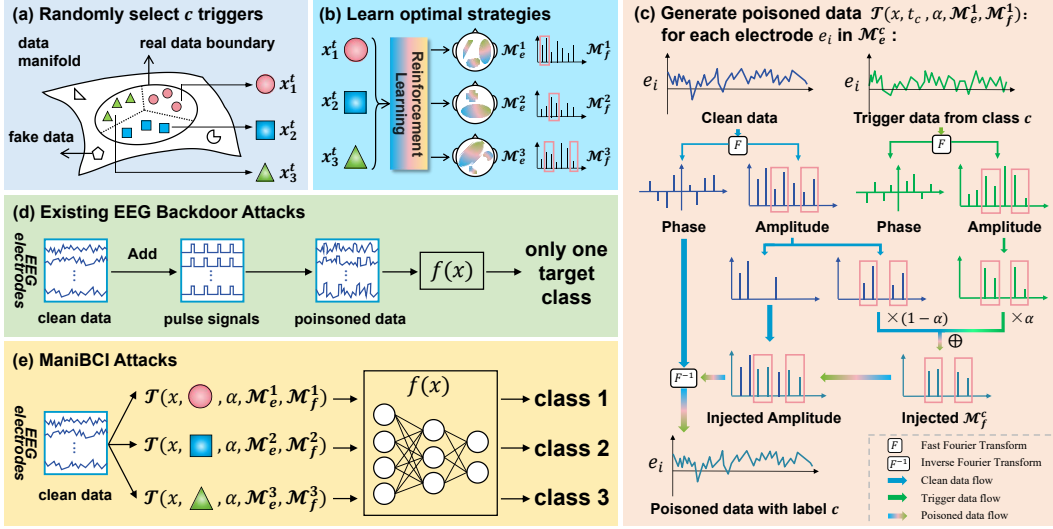


Figure 1: (a)-(c) The framework of ManiBCI: (a) The trigger selection and EEG data distribution from the view of manifold learning. (b) Learning optimal electrodes and frequencies injection strategies. (c) The generation process of ManiBCI. (d) The payloads of the existing backdoor attacks. (e) The payloads of ManiBCI, which can arbitrarily manipulate the output of EEG BCI models.

37 The first BA for EEG modality is demonstrated in Fig 1 (d), where the narrow period pulse (NPP)  
 38 signals are added as the trigger for single target class attack [16, 17]. To generate invisible trigger, the  
 39 adversarial loss is applied to learn a spatial filter as the trigger function [18]. Recently, some BA for  
 40 time series (EEG signal is a kind of time series) adopt generative adversarial net (GAN) to produce  
 41 poisoned data [19, 20]. However, there are rich information in the frequency domain of EEG [21–24].  
 42 No matter these BA are stealthy or not, they all inject unnatural perturbation in the temporal domain,  
 43 which will inevitably bring unnatural frequency into the real EEG frequency domain.

44 In this paper, we propose a novel backdoor attack for **manipulating EEG BCI** called **ManiBCI** to  
 45 address **Q1**, which injects triggers in the frequency domain. Specifically, ManiBCI is a three-stage  
 46 clean label poisoning attack demonstrated in Fig 1 (a-c): **1**): selecting  $c$  triggers from  $c$  classes, as  
 47 these triggers are all real EEG, the frequency of these triggers are all natural. Thus, the poisoned  
 48 data are similar to the real EEG as shown in Fig 2(b). **2**): learning optimal injecting strategies for  
 49 each trigger with reinforcement learning to enhance the performance of EEG BA, addressing **Q2**. **3**):  
 50 injecting each trigger’s frequencies into clean EEG of the same class as the triggers for each class,  
 51 which maintains the consistency of the label and morphology, addressing **Q3**.

52 The main contributions of this paper are summarized below:

- 53 • We propose a novel backdoor attack for EEG BCI called **ManiBCI**, which can attack  
 54 arbitrary class while preserving stealthiness without engaging the training stage.
- 55 • To the best of our knowledge, it is the first work that considers the efficacy of different EEG  
 56 electrodes and frequencies in EEG backdoor attacks with reinforcement learning.
- 57 • Extensive experiments on three EEG BCI datasets demonstrate the effectiveness of ManiBCI  
 58 and the robustness against several common EEG preprocessings and backdoor defenses.

## 59 2 Related Work

### 60 2.1 Backdoor Attacks

61 Backdoor attacks has been deeply investigated in image processing filed [25–27]. BadNets [28] is  
 62 the first BA, where the adversary maliciously control the DL to misclassify the input images contain  
 63 suspicious patches to a target class. Other non-stealthy attacks like blended [5] and sinusoidal strips  
 64 based [29] were studied then. To achieve higher stealthiness, some data poisoning BA were developed,

65 including shifting color spaces [30], warping [31], regularization [32] and frequency-based [33–38].  
 66 Other stealthy attacks [39–41] generate invisible trigger patterns by adversarial loss, which requires  
 67 the control of the model’s training process.

68 Recently, the EEG-based BCIs have shown to be vulnerable to BA  
 69 [16–18]. The NPP signals are added to clean EEG to generate non-  
 70 stealthy poisoned samples in [16, 17], which significantly modifies  
 71 the spectral distribution (as shown in Fig 2 (a)) and results in low  
 72 stealthiness. From the view of data manifold in Fig 1 (a), NPP-  
 73 added EEG are fake data. To generate more stealthy poisoned  
 74 data which stay in the real data boundary. The adversarial loss  
 75 has been applied backdoor EEG BCI [18] and time series [19, 20],  
 76 but these methods require controlling the training process of the backdoor models and can only  
 77 attack a single target class. Meng *et.al.* tried to achieve multi-target attacks with adding different  
 78 types of signals to clean EEG, *i.e.*, NPP, sawtooth, sine, and chirp [16]. However, these signals  
 79 are not stealthy in both the temporal and frequency domain. To attack multi-target class with high  
 80 stealthiness, Marksman backdoor [41] generates invisible sample-specific patterns for each possible  
 81 class, but it needs controlling the training stage. Moreover, generating trigger patterns with a neural  
 82 network for each sample is time-consuming.

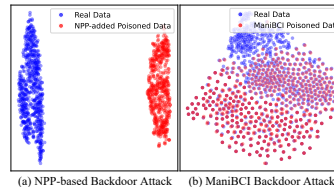


Figure 2: t-SNE visualization.

83 Different from the EEG BA in the temporal domain, we firstly propose to attack in the frequency  
 84 domain. Our attack is more stealthy than NPP-based attack, faster than other trigger generation  
 85 attack, and more practical as requiring no control of the target models. It is worth noting that the  
 86 frequency-based BA for image [33–38] cannot be applied for time series, as they do not consider the  
 87 characteristics of time series and fail to maintain the stealthiness for poisoned time series data.

## 88 2.2 Backdoor Defenses

89 To cope with the security problems of backdoor attacks, several categories of defensive methods have  
 90 been developed. Neural Cleanse [42] is a trigger reconstruction based methods. If the reconstructed  
 91 trigger pattern is significantly small, the model is identified as a backdoor model. Assuming the  
 92 trigger is still effective when a triggered sample is combining with a clean sample, STRIP [43]  
 93 detects the backdoor model by feeding the combined samples into the model to see if the predictions  
 94 are still with low entropy. Spectral Signature [44] detects the backdoor model based on the latent  
 95 representations. Fine-Pruning [45] erases the backdoor by pruning the model.

96 Besides the above defenses designed for backdoor attacks, there are some common EEG pre-  
 97 processing methods, such as bandstop filtering and down-sampling, should be considered when  
 98 designing a practical robust backdoor attack for EEG BCI in the real-world scene.

## 99 3 Methodology

### 100 3.1 EEG BCI Backdoor Attacks and Threat Model

101 Under the supervised learning setting, a classifier  $f$  is learned using a labeled training set  $\mathcal{S} =$   
 102  $\{(x_1, y_1), \dots, (x_N, y_N)\}$  to map  $f : \mathcal{X} \rightarrow \mathcal{C}$ , where  $x_i \in \mathcal{X}$  and  $y_i \in \mathcal{C}$ . The attacker in single target  
 103 class backdoor attacks aims to learn a classifier  $f$  behaves as follows:

$$104 \quad f(x_i) = y_i, \quad f(T(x_i)) = c_{tar}, \quad c_{tar} \in \mathcal{C}, \quad \forall (x_i, y_i) \in \mathcal{S}, \quad (1)$$

104 where  $T : \mathcal{X} \rightarrow \mathcal{X}$  is the trigger function and  $c_{tar}$  is the target label. For multi-target class backdoor  
 105 attacks, the trigger function has an extra parameter  $c_i$ , which manipulates the behavior of  $f$  flexibly:

$$106 \quad f(x_i) = y_i, \quad f(T(c_i, x_i)) = c_i, \quad \forall c_i \in \mathcal{C}, \forall (x_i, y_i) \in \mathcal{S}. \quad (2)$$

106 We consider a malicious data provider, who generates a small number of poisoned samples (labeled  
 107 with the target class) and injects them into the original dataset. A victim developer collects this  
 108 poisoned dataset and trains his model, which will be infected a backdoor.

109 We use a cross-validation setting to evaluate all BAs, each EEG dataset  $\mathcal{D}$  is divided into three  
 110 parts: training set  $\mathcal{D}_{train}$ , poisoning set  $\mathcal{D}_p$ , and test set  $\mathcal{D}_{test}$ . Specifically, for a dataset contains  $n$   
 111 subjects, we select one subject’s data as  $\mathcal{D}_p$  one by one, and the remaining  $n - 1$  subjects to perform

112 leave-one-subject-out (LOSO) cross-validation, *i.e.*, one of the subjects as  $\mathcal{D}_{test}$ , and the remaining  
 113  $n - 1$  subjects as  $\mathcal{D}_{train}$  (one of the subjects in  $\mathcal{D}_{train}$  is chosen to be validation set). In summary,  
 114 for a dataset contains  $n$  subjects, there are  $n(n - 1)$  runs to validate each EEG BCI backdoor attack  
 115 method. A poisoned subset  $\mathcal{S}_p$  of  $M$  ( $M < N$ ) examples is generated based on  $\mathcal{D}_p$ . Then  $\mathcal{S}_p$  is  
 116 combined with  $\mathcal{D}_{train}$  to acquire  $\mathcal{S} = \{\mathcal{S}_p, \mathcal{D}_{train}\}$ . The poisoning ratio is defined as :  $\rho = M/N$ .

### 117 3.2 Reinforcement Learning for Optimal Trigger-Injection Strategies

118 The learning of the injecting electrodes set  $\mathcal{M}_e^{c_i}$  and frequencies set  $\mathcal{M}_f^{c_i}$  for each selected trigger  
 119 in class  $c_i$  can be formulated as a non-convex optimization problem. Under this optimization  
 120 framework, the strategy generator function will learn the optimal  $\mathcal{M}_e^{c_i}$  and  $\mathcal{M}_f^{c_i}$  for each EEG trigger  
 121 to implement ManiBCI BA on target DL model  $f$ , which is supposed to have a high clean accuracy  
 122 (CA) on the clean data and attack success rate (ASR) on the poisoned data:

$$\min_{\mathcal{M}_e^{c_i}, \mathcal{M}_f^{c_i}} \mathbb{E}_{(x_i, y_i) \sim \mathcal{D}} [\mathcal{L}(f(x_i), y_i) + \lambda \mathcal{L}(f(\mathcal{T}(x_i, x_{c_i}^t, \alpha, \mathcal{M}_e^{c_i}, \mathcal{M}_f^{c_i})), c_i)]. \quad (3)$$

123 However, finding the optimal adaptive injecting strategies for each trigger is not trivial as the searching  
 124 space is too large (*e.g.*, if injecting half of the 62 electrodes, there are  $\binom{62}{31} \approx 4.65 \times 10^{17}$  cases for  
 125 deciding  $\mathcal{M}_e^{c_i}$ ). Reinforcement learning (RL) is an appropriate method for tackling this questions.  
 126 The objective of RL is to find a sampler  $\pi$  to maximize the expect of the reward function:

$$\begin{aligned} \pi^* &= \arg \max_{\pi} \mathbb{E}_{\tau \sim \pi(\tau)} [R(\tau)] = \arg \max_{\pi} \sum_{\tau} [R(\tau) \cdot p_{\pi}(\tau)] \\ &= \arg \max_{\pi} \sum_{\tau} [R(\tau) \cdot \rho_0(s_1) \cdot \prod_{t=1}^{T-1} \pi(a_t | s_t) \cdot \mathcal{P}(s_{t+1} | s_t, a_t)], \end{aligned} \quad (4)$$

127 where  $R(\tau)$  is reward function of a trajectory  $\tau = (s_1, a_1, r_1, \dots, s_T)$ , the  $s_i, a_i, r_i$  means the state,  
 128 action, and reward at time  $i$ . The  $\rho_0$  indicates the sampler of initial state. In our settings, the action  
 129 (strategies) do not affect the state (triggers). Hence, we can simplify Eq 4 by removing the states  $s_i$ :

$$\pi^* = \arg \max_{\pi} \sum_{\tau} [R(\tau) \cdot \prod_{t=1}^{T-1} \pi(a_t)]. \quad (5)$$

130 However, we do not care about the reward of the whole trajectory, we only acquire a single strategy  
 131 for each trigger. Thus, we replace the  $R(\tau)$  with  $R(a_t)$  and select the  $a_t$  whose  $R(a_t)$  is the biggest  
 132 as the optimal strategy. Here, an RL algorithm called policy gradient [46] is adopted to learn an  
 133 agent (*i.e.*, policy network  $\pi_{\theta}^{c_i}$  with parameters  $\theta$ ) to find the optimal strategy for each trigger. After  
 134 removing the state  $s_t$  and replacing  $R(\tau)$ , the gradient estimator is:

$$\hat{g} = \nabla_{\theta} \mathbb{E}_{\tau \sim \pi_{\theta}(\tau)} [R(\tau)] = \sum_{\tau} [R(a_t) \cdot \nabla p_{\pi_{\theta}}(a_t)] = \mathbb{E}_t [R_t(a_t) \cdot \nabla_{\theta} \log \pi_{\theta}], \quad (6)$$

135 where  $a_t$  and  $R_t$  is the action and estimator of the reward function at timestep  $t$ . The expectation  
 136  $\mathbb{E}_t$  indicates the empirical average. Here,  $a_t = \{\mathcal{M}_e^{c_i}, \mathcal{M}_f^{c_i}\}$ . The parameters of  $\pi_{\theta}^{c_i}$  are updated by  
 137  $\theta_{t+1} = \theta_t + \eta \hat{g}$ ,  $\eta$  is the learning rate. We run the RL for T steps and take the best  $a_t$  as the strategy.

138 The CA and ASR are obtained by implementing ManiBCI only on  $\mathcal{S}$ . Specifically, we use a concise  
 139 network as the agent which takes the extracted spatial-temporal features from triggers into account  
 140 to generate better policy. This agent has two output vectors  $v_1 \in \mathbb{R}^E, v_2 \in \mathbb{R}^F$ , where  $E$  and  $F$  is  
 141 the number of EEG electrodes and frequencies. The electrodes and frequencies are in  $\mathcal{M}_e^{c_i}$  and  $\mathcal{M}_f^{c_i}$   
 142 only if the corresponding positions in  $v_1$  and  $v_2$  have Top- $k$  values,  $k$  is  $\gamma E$  for electrodes and  $\beta F$  for  
 143 frequencies, where  $\gamma, \beta \in (0, 1]$  are hyperparameters.

144 Besides the performance of CA and ASR, there are two important concerns: **C1**: Robustness against  
 145 common EEG preprocessig-based defenses; **C2**: Stealthiness against human perceptions. The reason  
 146 why we consider **C1** is that the bandstop filtering is widely used for preprocessing EEG signals. For  
 147 instance, if we inject the triggers into a concentrated frequency band 50-60Hz, it is easy to filter the  
 148 trigger out using a 50Hz low pass filter, resulting in attack failure. Thus, scattering the injection  
 149 positions in various frequency can effectively evade from specific frequency filter defenses. To  
 150 address **C2**, injecting the trigger into higher frequencies is more invisible than lower frequencies [47].  
 151 Taking all into consideration, we define the estimator of the reward function  $R_t$  as follows:

$$R_t(a_t) = R_t(\mathcal{M}_e^{c_i}, \mathcal{M}_f^{c_i}) = \text{CA} + \lambda \text{ASR} + \mu \text{dis}(\mathcal{M}_f^{c_i}) + \nu \min(\mathcal{M}_f^{c_i}), \quad (7)$$

152 where the  $\mathcal{M}_f^{c_i}$  indicates the set of all injecting frequency positions, and  $\text{dis}()$  calculates the minimal  
 153 distance between each pair of positions. Thus,  $\text{dis}(\mathcal{M}_f^{c_i})$  is the discrete (DIS) loss, and  $\min(\mathcal{M}_f^{c_i})$  is  
 154 the high frequency (HF) loss, which can scatter the injection positions in various frequency bands  
 155 and inject as high frequencies as possible. The  $\lambda, \mu, \nu \in \mathbb{R}$  are hyperparameters.

### 156 3.3 Poisoned Data Generation via Frequency Transform

157 After selecting the  $C$  triggers from each class and learning the strategy for each trigger, the poisoned  
 158 data are generated by injecting these triggers into clean data with the corresponding strategies. As  
 159 shown in Fig 1(c), given a clean data  $x_i \in \mathcal{D}_p$  with label  $c_i$ , and a trigger data  $x_{c_i}^t$ , let  $\mathcal{F}^A$  and  $\mathcal{F}^P$  be  
 160 the amplitude and phase components of the fast Fourier transform (FFT) result of a EEG signals, we  
 161 denote the amplitude and phase spectrum of  $x_i$  and  $x_{c_i}^t$  as:

$$\mathcal{A}_{x_i} = \mathcal{F}^A(x_i), \mathcal{A}_{x_{c_i}^t} = \mathcal{F}^A(x_{c_i}^t), \mathcal{P}_{x_i} = \mathcal{F}^P(x_i), \mathcal{P}_{x_{c_i}^t} = \mathcal{F}^P(x_{c_i}^t). \quad (8)$$

162 The new poisoned amplitude spectrum  $\mathcal{A}_{x_i}^P$  is produced by linearly interpolating  $\mathcal{A}_{x_i}$  and  $\mathcal{A}_{x_{c_i}^t}$ . In  
 163 order to achieve this, we produce a binary mask  $\mathcal{M}^{c_i} \in \mathbb{R}^{E \times F} = 1_{(j,k)}, j \in \mathcal{M}_e^{c_i}, k \in \mathcal{M}_f^{c_i}$ , whose  
 164 value is 1 for positions of all corresponding to elements in both electrode and frequency sets and 0  
 165 elsewhere. Denoting  $\alpha \in (0, 1]$  as the linear interpolating ratio, the new poisoned amplitude spectrum  
 166 can be computed as follows, where  $\odot$  indicates Hadamard product:

$$\mathcal{A}_{x_i}^P = [(1 - \alpha)\mathcal{A}_{x_i} + \alpha\mathcal{A}_{x_{c_i}^t}] \odot \mathcal{M}^{c_i} + \mathcal{A}_{x_i} \odot (1 - \mathcal{M}^{c_i}). \quad (9)$$

167 Finally, we adopt the injected poisoned amplitude spectrum  $\mathcal{A}_{x_i}^P$  and the clean phase spectrum  $\mathcal{P}_{x_i}$  to  
 168 get the poisoned data by inverse FFT  $\mathcal{F}^{-1}$ :

$$x_i^p = \mathcal{F}^{-1}(\mathcal{A}_{x_i}^P, \mathcal{P}_{x_i}). \quad (10)$$

169 By generating  $x_i^p$  through this frequency injection approach, we obtain a subset  $\mathcal{S}_p = \{x_1^p, \dots, x_M^p\}$ ,  
 170 which will combine with  $\mathcal{D}_{train}$  to form the whole training dataset  $\mathcal{S}$ . The EEG DL model  $f$  is then  
 171 trained with  $\mathcal{S}$  to obtain the ability of behaving as equation 2.

## 172 4 Experiments

### 173 4.1 Datasets, Baselines, and Experimental Setup

174 **Emotion Recognition (ER) Dataset** SEED [12] is a discrete EEG emotion dataset studying three  
 175 types of emotions: happy, neutral, and sad. SEED collected EEG from 15 subjects.

176 **Motor Imagery (MI) Dataset** BCIC-IV-2a [48] dataset recorded EEG from 9 subjects while they  
 177 were instructed to imagine four types of movements: left hand, right hand, feet, and tongue.

178 **Epilepsy Detection (ED) Dataset** CHB-MIT [49] is an epilepsy dataset required from 23 patients.  
 179 We cropped and resampled the CHB-MIT dataset to build an ED dataset with four types of EEG:  
 180 ictal, preictal, postictal, and interictal phase EEG.

181 **Non-stealthy Baselines** As mentioned in previous sections, to the best of our knowledge, ManiBCI  
 182 is the first work that studies multi-trigger and multi-target class (MT) backdoor in EEG BCI. For  
 183 comparison, we design several baseline approaches which can be divided into two main groups:  
 184 non-stealthy and stealthy. Non-stealthy attacks contains **PatchMT** and **PulseMT**. For a benign EEG  
 185 segment  $x \in \mathbb{R}^{E \times T}$ . PatchMT is a multi-trigger and MT extension of BadNets [28] where we fill the  
 186 first  $\beta T$  timepoints of a EEG segments with a constant number, *e.g.*,  $\{0.1, 0.3, 0.5\}$  for three-class  
 187 task. PulseMT is a multi-trigger and MT extension of NPP-based backdoor attacks [16] where we  
 188 use NPP signals with different amplitudes, *e.g.*,  $\{-0.8, -0.3, 0.3, 0.8\}$  for different target classes.

189 **Stealthy Baselines** Previous works generate stealthy poisoned samples by controlling the training  
 190 stage and can only attack single target class [18–20]. As they control the training of target model,  
 191 it is unfair to directly compare their methods with ManiBCI. There is no stealthy MT BA for EEG.  
 192 Thus, we design two MT stealthy attacks baselines: **CompMT** and **AdverMT**. CompMT generates  
 193 poisoned samples for different target classes by compressing the amplitude of EEG with different

Table 1: The clean accuracy and attack success rate for each target class with 40% poisoning rate. The best results are in **bold** and the second best are underlined.

Dataset	Emotion Recognition					Motor Imagery						Epilepsy Detection						
	Method	Clean	ASR	0	1	2	Clean	ASR	0	1	2	3	Clean	ASR	0	1	2	3
EEGnet	No Attack	0.477	0.333	-	-	-	0.327	0.250	-	-	-	-	0.508	0.250	-	-	-	-
	PatchMT	<u>0.492</u>	0.382	0.577	0.232	0.337	<u>0.283</u>	0.824	0.866	0.880	0.787	0.762	<u>0.460</u>	0.549	0.532	0.430	0.388	0.845
	PulseMT	0.463	<u>0.778</u>	<b>0.844</b>	0.509	<b>0.981</b>	0.270	0.825	0.947	0.656	0.758	0.938	0.439	<u>0.810</u>	<u>0.853</u>	<u>0.745</u>	<u>0.729</u>	0.913
	CompMT	0.443	0.385	0.099	0.377	0.678	0.269	<u>0.865</u>	0.530	<u>0.997</u>	<u>0.983</u>	<u>0.948</u>	0.437	<u>0.547</u>	0.261	0.280	0.714	<u>0.933</u>
	AdverMT	0.457	0.334	0.276	0.330	0.396	0.257	0.243	0.316	0.192	0.230	0.235	0.413	0.250	0.326	0.264	0.200	0.210
	ManiBCI	<b>0.535</b>	<b>0.857</b>	<u>0.831</u>	<b>0.791</b>	<u>0.949</u>	<b>0.323</b>	<b>1.000</b>	<b>0.999</b>	<b>1.000</b>	<b>1.000</b>	<b>0.999</b>	<b>0.477</b>	<b>0.944</b>	<b>0.930</b>	<b>0.954</b>	<b>0.921</b>	<b>0.970</b>
DeepCNN	No Attack	0.497	0.333	-	-	-	0.301	0.250	-	-	-	-	0.443	0.250	-	-	-	-
	PatchMT	<u>0.481</u>	0.342	0.248	0.323	0.453	0.276	0.704	0.638	0.977	0.774	0.425	0.431	<u>0.729</u>	0.416	<b>0.890</b>	0.719	0.892
	PulseMT	0.450	<u>0.596</u>	<b>0.815</b>	0.334	<u>0.638</u>	0.261	0.829	<u>0.764</u>	0.968	0.819	0.765	0.405	<b>0.885</b>	<b>0.872</b>	<u>0.862</u>	<b>0.861</b>	<b>0.943</b>
	CompMT	0.461	0.427	0.473	<u>0.473</u>	0.336	<u>0.286</u>	<u>0.887</u>	0.638	<u>0.982</u>	<u>0.946</u>	<u>0.980</u>	<u>0.446</u>	0.538	0.196	0.466	0.571	<u>0.918</u>
	AdverMT	0.367	0.388	0.298	0.453	0.412	0.245	0.247	0.320	0.221	0.196	0.240	0.396	0.275	0.354	0.218	0.227	0.301
	ManiBCI	<b>0.534</b>	<b>0.832</b>	<u>0.732</u>	<b>0.865</b>	<b>0.901</b>	<b>0.315</b>	<b>1.000</b>	<b>1.000</b>	<b>1.000</b>	<b>1.000</b>	<b>0.999</b>	<b>0.469</b>	<u>0.828</u>	<u>0.725</u>	0.839	<u>0.845</u>	0.904
LSTM	No Attack	0.506	0.333	-	-	-	0.264	0.250	-	-	-	-	0.462	0.250	-	-	-	-
	PatchMT	0.509	0.368	0.311	0.392	0.401	0.261	0.429	0.395	0.296	0.386	0.639	0.450	0.513	0.500	0.437	0.417	0.700
	PulseMT	0.511	<u>0.824</u>	<u>0.883</u>	0.645	<u>0.943</u>	<b>0.265</b>	0.533	0.787	0.327	0.282	0.737	<u>0.451</u>	<u>0.804</u>	<b>0.845</b>	<u>0.769</u>	0.709	<u>0.895</u>
	CompMT	0.484	0.490	0.272	0.269	0.929	0.260	0.548	0.219	0.511	<u>0.523</u>	0.940	<b>0.455</b>	0.435	0.194	0.217	0.490	0.840
	AdverMT	0.367	0.415	0.472	0.453	0.321	0.239	0.271	0.308	0.215	<u>0.247</u>	0.312	0.432	0.268	0.367	0.232	0.198	0.275
	ManiBCI	<b>0.519</b>	<b>0.954</b>	<b>0.998</b>	<b>0.868</b>	<b>0.996</b>	<u>0.264</u>	<b>0.966</b>	<b>0.987</b>	<b>0.988</b>	<b>0.901</b>	<b>0.986</b>	0.444	<b>0.865</b>	<u>0.795</u>	<b>0.833</b>	<b>0.857</b>	<b>0.975</b>

194 ratios, *e.g.*,  $\{-0.1, 0, 0.1\}$  for three-class task. AdverseMT is a multi-trigger and MT extension of  
 195 adversarial filtering based attacks [18], where we using a local model trained only on  $\mathcal{S}_p$  to generate  
 196 different spatial filters  $\mathbf{W}_i^*$  for different target classes, then we apply these spatial filters to generate  
 197 poisoned samples. More details are written in Appendix D.

198 **Experimental Setup** We demonstrate the effectiveness of the proposed ManiBCI backdoor through  
 199 comprehensive experiments on the above three EEG datasets, more details of each dataset and  
 200 preprocessings are illustrated in Appendix C. We follow the poisoning attack setting as the previous  
 201 works [16] and consider three EEG DL models for classifier  $f$ : EEGNet [50], DeepCNN [51], and  
 202 LSTM [52, 53]. For all methods, we train the classifiers using the Adam optimizer with learning rate  
 203 of 0.001. The batch size is 32 and the number of epochs is 100. For all datasets and baselines, the  
 204 interpolating ratio  $\alpha = 0.8$ , the electrode poisoning ratio  $\beta = 0.1$ , the electrode poisoning ratio  $\gamma =$   
 205  $0.5$ . For the reinforcement learning of ManiBCI, we train  $\pi_\xi$  using the Adam optimizer with learning  
 206 rate of 0.01. The hyperparameters in advantage function is set to  $\lambda = 2$ ,  $\mu = 0.3$ , and  $\nu = 0.005$ .  
 207 More details of the experimental setup can be found in the supplementary material.

## 208 4.2 Effectiveness of ManiBCI

209 This section presents the attack success rates of ManiBCI and baselines. To evaluate the performance  
 210 in the multi-trigger multi-payload scenario, for each test sample  $(x, y) \in \mathcal{D}_{test}$ , we enumerate all  
 211 possible target labels  $c_i \in \mathcal{C}$  including the true label  $y$  and inject the trigger to activate the backdoor.  
 212 The attack is successful only when the backdoor classifier  $f$  correctly predicts  $c_i$  for each poisoned  
 213 input  $x$  with a target label  $c_i$ .

### 214 4.2.1 Attack Performance

215 The clean-data accuracy (Clean) and ASR (Attack) for each class of all attack methods on three EEG  
 216 tasks with three EEG DL models are presented in Table 1. The AdverMT, designed for single-target  
 217 attack, fails to attacks multiple target classes. Our ManiBCI significantly outperforms baselines at  
 218 almost all cases ( $p < 0.05$ ) except attacking DeepCNN on the ED dataset, having ASRs above 0.8 on  
 219 three datasets and even achieving an ASR of 1.000 on the MI dataset. These results demonstrate that  
 220 our ManiBCI is effective across different EEG tasks and EEG models. PulseMT achieves the second  
 221 best on ER and ED dataset, CompMT achieves the second best on the MI dataset.

### 222 4.2.2 Performance of the Reinforcement Learning: Policy Gradient

223 Displaying in Table 2, the performance of the policy gradient was compared with other common  
 224 optimization algorithms, including genetic algorithm (GA) [54] and random selection (The search  
 225 space is too large for performing grid search as explained in Section 3.2). It can be observed that the

226 policy gradient outperforms GA while only spending 16% training time of GA. We plot the learning  
 227 curve of RL in Appendix F.3, which demonstrates that RL learns well strategies within 50 epochs, i.e.,  
 228 only trains 50 backdoor models and saves lots of time. The random algorithm can achieve a not bad  
 229 results, proving that our methods can be applied without RL if some performance drop is acceptable.

Table 2: Clean and attack performance with with different trigger search optimization algorithms, the poisoning rate is set to 10%. The target model is EEGNet.

Method \ Dataset	Emotion			Motor Imagery			Epilepsy		
	Clean	Attack	Time ↓	Clean	Attack	Time ↓	Clean	Attack	Time ↓
Random	0.520	0.771	-	0.291	0.857	-	0.501	0.721	-
Genetic Algorithm	0.516	0.826	15.2h	0.302	1.000	10.0h	0.492	0.862	30.5h
Policy Gradient	0.535	0.857	2.5h	0.323	1.000	1.8h	0.477	0.944	5.2h

### 230 4.2.3 Performance of Learned Mask Strategies on Other Target Models

231 We demonstrate that the injecting strategies learned on a EEG classifier  $f$  can be used to attack  
 232 other EEG classifiers  $\hat{f}$ . In other words, Marksman can still be effective when the adversary has no  
 233 knowledge of the target models  $\hat{f}$ . To perform the experiments, we use the strategy learned with a  
 234 classifier  $f$ , then generate poisoned samples to attack another classifier  $\hat{f}$  whose network is different  
 235 from  $f$ . Table 3 shows the performance difference, it can be observed that the difference is relatively  
 236 small in most of the cases, demonstrating the transferability of the injecting strategy learned with  
 237 reinforcement learning.

Table 3: Clean and attack performance on other models. Red values represent the decreasing performance in attacks with  $f$  is the same as  $\hat{f}$ . Blue values mean increments or unchanged.

Models	$f$ : EEGNet				$f$ : DeepCNN				$f$ : LSTM			
	$\hat{f}$ : DeepCNN		$\hat{f}$ : LSTM		$\hat{f}$ : EEGNet		$\hat{f}$ : LSTM		$\hat{f}$ : EEGNet		$\hat{f}$ : DeepCNN	
	Clean	Attack	Clean	Attack	Clean	Attack	Clean	Attack	Clean	Attack	Clean	Attack
Emotion	0.458	0.781	0.485	0.938	0.516	0.813	0.490	0.936	0.516	0.863	0.497	0.779
	0.026	0.051	0.034	0.016	0.019	0.044	0.029	0.018	0.019	0.006	0.037	0.053
Motor	0.316	1.000	0.265	0.946	0.309	1.000	0.264	0.972	0.306	1.000	0.306	1.000
	0.001	0.000	0.001	0.020	0.014	0.000	0.000	0.006	0.017	0.000	0.009	0.000
Epilepsy	0.442	0.759	0.469	0.806	0.448	0.943	0.445	0.813	0.448	0.926	0.427	0.850
	0.027	0.069	0.025	0.059	0.029	0.001	0.001	0.052	0.029	0.018	0.042	0.022

### 238 4.2.4 Attack Performance with Different Hyperparameters

239 We investigate the influences of three different hyperparameters: poisoning rate  $\rho$ , frequency injection  
 240 rate  $\beta$ , and electrode injection rate  $\gamma$ . The performance of attacking EEGNet on the ED dataset are  
 241 displayed in Fig 3. It can be seen that the ASRs are positively correlated with poisoning rate. Note  
 242 that it is non-trivial for multi-target class attack, thus the ASR is not high compared to the single class  
 243 attack. ManiBCI outperforms other attacks in all cases and is robust to the change of  $\beta$  and  $\gamma$ .

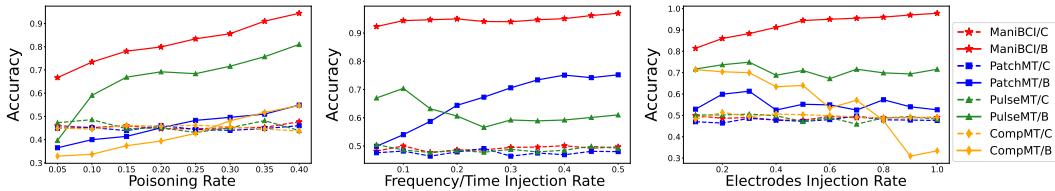


Figure 3: Clean (/C) and attack (/B) performance with different poisoning or injection rates.

244 **4.3 Robustness of ManiBCI**

245 In this section, we evaluate the robustness of our ManiBCI against different EEG preprocessing  
 246 method and various representative backdoor defenses.

247 **4.3.1 Robustness against EEG Preprocessing Methods**

248 To develop an EEG BCI, it is very common to preprocess the raw EEG signals, *e.g.*, 1) band-stop  
 249 filtering and 2) down-sampling. An EEG backdoor attack is impractical in real scenarios if it is no  
 250 longer effective when the target model is trained with the preprocessed poisoned EEG. Hence, we  
 251 must take the robustness against preprocessing methods into account, which is widely ignored in  
 252 the image backdoor attack field. The performance of each method facing different preprocessing  
 253 methods are presented in Table 4. It can be observed that our ManiBCI is robust in all cases. However,  
 254 when removing the DIS loss, the performance of ManiBCI decreases a lot after EEG preprocessing,  
 255 especially facing the 30 Hz high-stop filtering preprocessing due to the HF loss that encourages the  
 256 policy network learns to injecting high frequency.

Table 4: Clean and attack performance on three datasets after different EEG preprocessing methods. The target model is EEGNet. M w.o. DIS means removing the DIS loss in ManiBCI.

	Preprocessing Method	No defense		20 Hz low		30 Hz high		25% down		Average ASR
		Clean	Attack	Clean	Attack	Clean	Attack	Clean	Attack	
ER	ManiBCI	0.535	0.857	0.512	0.829	0.463	0.892	0.518	0.908	0.876
	w/o DIS	0.506	0.859	0.492	0.816	0.466	0.333	0.498	0.807	0.652
MI	ManiBCI	0.323	1.000	0.285	1.000	0.329	1.000	0.321	1.000	1.000
	w/o DIS	0.298	1.000	0.264	1.000	0.322	0.250	0.284	0.990	0.746
ED	ManiBCI	0.497	0.944	0.492	0.914	0.494	0.856	0.516	0.818	0.920
	w/o DIS	0.515	0.250	0.477	0.864	0.508	0.250	0.510	0.249	0.454

257 **4.3.2 Robustness against Neural Cleanse: Trigger Inversion**

258 Neural Cleanse (NC) [42] calculate a metric called Anomaly  
 259 Index by reconstructing trigger pattern for each possible label.  
 260 The Anomaly Index is positively correlated with the size of the  
 261 reconstruction trigger. A model with Anomaly Index > 2 is  
 262 considered to be backdoor-injected. We display the Anomaly  
 263 Indexes of the clean models and the backdoor-injected model  
 264 by ManiBCI in Fig 4. It can be seen that ManiBCI can easily  
 265 bypass NC. The reconstructed trigger patterns on three datasets  
 266 are presented in Appendix F.1.

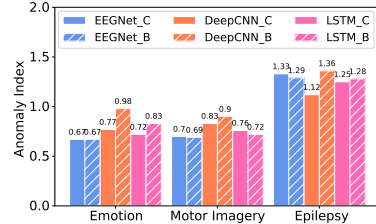


Figure 4: Anomaly Index of three models on three datasets.

267 **4.3.3 Robustness against STRIP: Input Perturbation**

268 We evaluate the robustness of ManiBCI against STRIP [43], which perturbs the input EEG and  
 269 calculates the entropy of the predictions of these perturbed EEG data. Based on the assumption that  
 270 the trigger is still effective after perturbation, the entropy of backdoor input tends to be lower than  
 271 that of the clean one. The results are plotted in Fig 5, it can be seen that the entropy distributions of  
 272 the backdoor and clean samples are similar.

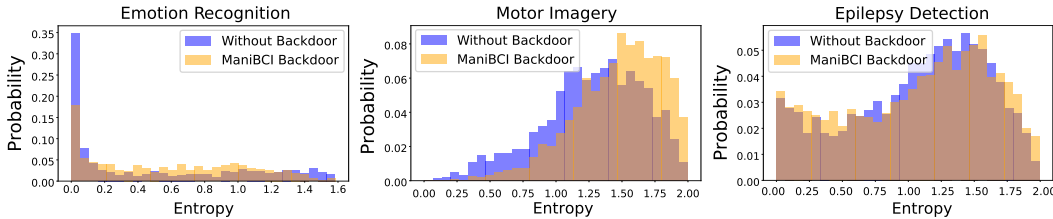


Figure 5: Performance against STRIP on three datasets, the target model is EEGNet.



273 **4.3.4 Robustness against Spectral Signature: Latent Space Correlation**

274 Spectral Signature [44] detects the backdoor samples by statistical analysis of clean data and backdoor  
 275 data in the latent space. Following the same experimental settings in [44], we randomly select 5,000  
 276 clean samples and 500 ManiBCI backdoor samples and plot the histograms of the correlation scores  
 277 in Fig 6. There is no clear separation between these two sets of samples, showing the stealthiness of  
 278 ManiBCI backdoor samples in the latent space.

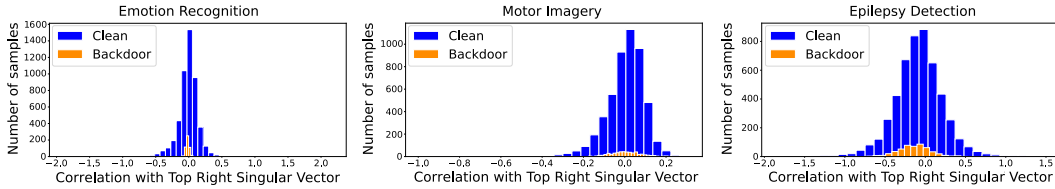


Figure 6: Performance with Top Right against Spectral Signature on three datasets, the target model is EEGNet.

279 **4.3.5 Robustness against Fine-Pruning**

280 We evaluate the robustness of Marksman against Fine-Pruning  
 281 [45], a model analysis based defense which finds a classifier’s  
 282 low-activated neurons given a small clean dataset. Then it  
 283 gradually prunes these low-activated neurons to mitigate the  
 284 backdoor without affecting the CA. We can observe from Fig  
 285 7 that the ASR drops considerably small when pruning ratio  
 286 is less than 0.7, suggesting that the Fine-Pruning is ineffective  
 287 against ManiBCI.

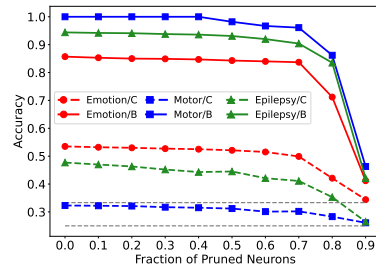


Figure 7: Performances of EEG-Net against Fine-Pruning on three datasets.

288 **4.4 Visualization of Backdoor Attack Samples**

289 To evade from human perception (C2 in Section 3.2), we design to obtain injecting strategies with  
 290 HF loss. It can be seen from the bottom row of Fig 8 that ManiBCI (with HF loss) generates stealthy  
 291 poisoned EEG, which is almost the same as the clean EEG, demonstrating the **High Stealthiness**.  
 292 The poisoned EEG will be conspicuous compared to the clean EEG if remove the HF loss.

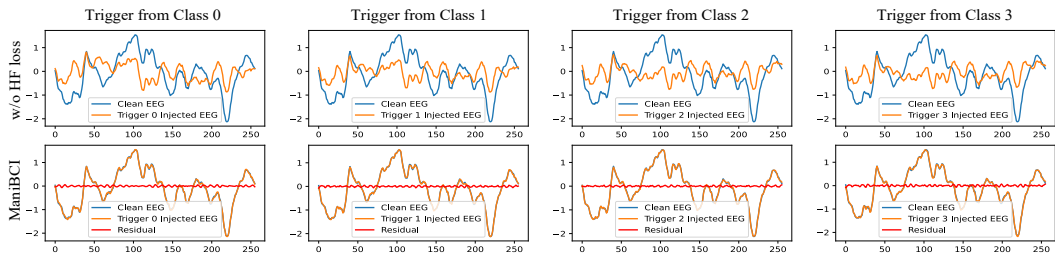


Figure 8: The Clean EEG (Blue), Trigger-injected EEG (Orange) and the Residual (Red) of the ED dataset. The x-axis is the timepoints, the y-axis is the normalized amplitude. Top row: w.o. HF loss; Bottom row: with HF loss. Each column indicates each possible class.

293 **5 Conclusion**

294 In this paper, we proposed ManiBCI, a novel EEG backdoor for manipulating EEG BCI, where the  
 295 adversary can arbitrarily control the output for any input samples. To the best of our knowledge,  
 296 ManiBCI is the first method that considers which EEG electrodes and frequencies to be injected by  
 297 adopting a reinforcement learning called policy gradient to learn the adaptive injecting strategies  
 298 for different EEG triggers and tasks. We specially design the reward function in RL to enhance the  
 299 robustness and stealthiness of ManiBCI. The perturbation of the trigger on clean EEG is almost  
 300 invisible. Our experimental results over three common EEG datasets demonstrate the effectiveness  
 301 of ManiBCI and the stealthiness against the existing representative defenses. This work calls for  
 302 defensive studies to counter ManiBCI for EEG modality.

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## 440 Appendix

### 441 A Limitations

442 Our ManiBCI is a backdoor attack in the frequency domain, which requires to transform the EEG  
443 signals into frequency domain through fast Fourier transform (FFT) and return to temporal domain  
444 through inverse FFT (iFFT). The operation of FFT and iFFT in the trigger injection function are a  
445 little more time-consuming compared to other backdoor attack directly in the temporal domain, like  
446 PatchMT [28] and PulseMT [16]. Future effort will be devoted into the faster implementation of FFT  
447 and iFFT, for example, taking the advantage of modern GPUs.

448 It is a little more time-consuming for the reinforcement learning to acquire the optimal strategies for  
449 each trigger. However, we can obtain a general injecting strategy for each EEG BCI tasks, which can  
450 achieve a relatively good performance without reinforcement learning, as we can see from Table 3  
451 that random injection strategy has an acceptable performance.

### 452 B Broader Impacts

453 With the rapid development of techniques, EEG BCIs gain a wide range of applications from health  
454 care to human-computer interaction. Some companies like Neuralink adopt the EEG BCI to assist  
455 paralytic patients helping themselves in daily lives. However, if the EEG BCI is backdoor attacked  
456 by ManiBCI, which allows the attacker to arbitrarily control BCI’s outputs, the BCI users may fall  
457 into tremendous fatal troubles. For instance, one paralytic patient controls his/her wheelchair by  
458 EEG BCI, the attacker can manipulate the wheelchair to run down a steep staircase. For an epileptic  
459 patient, the attacker can let all the output be Normal State, even when the patient is experiencing  
460 an epileptic seizure. This paper reveals the severe danger faced by EEG BCIs, demonstrating the  
461 possibility that someone can maliciously manipulate the outputs of EEG BCIs with arbitrary target  
462 class.

463 ManiBCI can also be used for positive purposes, like protecting intellectual property of EEG dataset  
464 and EEG models with watermarking. As our ManiBCI has a very small impact of the clean accuracy,  
465 and the poisoning approach is clean label poisoning, ManiBCI is a fantastic method for watermarking  
466 EEG dataset and models.

467 For a company that provides EEG dataset, it can select different EEG triggers for different customs  
468 to generate poisoned data and inject into the dataset provided to customs who buy the dataset. As a  
469 result, the company have the information of which trigger is corresponding to which customs, e.g.,  
470 trigger  $x$  is in the dataset provided to custom  $X$ , trigger  $y$  is in the dataset provided to custom  $Y$ . If an  
471 EEG model from a company which didn’t buy dataset is detected having this watermark (backdoor)  
472 with trigger  $x$ , the company knows that the custom  $X$  leaked the dataset. Similarly, if an EEG model  
473 is detected having this watermark (backdoor) with trigger  $y$ , the company knows that the custom  $Y$   
474 leaked the dataset.

### 475 C Datasets and Preprocessing

476 In this section, we introduce the three datasets used in our experiments, and explain the preprocessing.  
477 Table 5 presents some basic information of these datasets.

Table 5: Basic information of the three datasets

Dataset	Emotion	Motor Imagery	Epilepsy
Class Numbers	3	4	4
Subjects	15	9	23
Electrodes	62	22	23
Sampling Rate	200 Hz	250 Hz	256 Hz

## 478 C.1 Emotion Recognition (ER)

479 The SJTU Emotion EEG Dataset (SEED) was incorporated as the representative dataset of emotion  
480 recognition tasks [12]. It consists of EEG recordings from 15 subjects watching 15 emotional video  
481 clips with three repeated session each on different days. Each video clip is supposed to evoke one  
482 of the three target emotions: positive, neutral, and negative. The EEG signals were acquired by  
483 the 62-channel electrode cap at a sampling rate of 1000 Hz. We performed below preprocessing  
484 procedures for the 62-channel EEG signals: 1) Down-sampling from 1000 Hz to 200 Hz, 2) Band-pass  
485 filtering at 0.3-50 Hz, 3) Segmenting EEG signals into 1-second (200 timepoints), obtaining 3394  
486 EEG segments in each session for each subject.

## 487 C.2 Motor Imagery (MI)

488 We employ the BCIC-IV-2a as a representative dataset of MI classification tasks [48]. It contains  
489 EEG recordings in a four-class motor-imagery task from nine subjects with two repeated session each  
490 on different days. During the task, the subjects were instructed to imagine four types of movements  
491 (*i.e.*, right hand, left hand, feet, and tongue) for four seconds. Each session consists of a total of  
492 288 trials with 72 trials for each type of the motor imagery. The EEG signals were recorded by 22  
493 Ag/AgCl EEG electrodes in a sampling rate of 250 Hz. We segment the 22-channel EEG signals into  
494 1-second segments, resulting in totally 1152 EEG data for each subject.

## 495 C.3 Epilepsy Detection (ED)

496 The CHB-MIT, one of the largest and most used public datasets for epilepsy, is adopted as a  
497 representative dataset of ED tasks [49]. It recorded 877.39 hours of multi-channel EEG in a sampling  
498 rate of 256 Hz from 23 pediatric patients with intractable seizures. However, as the montages (*i.e.*,  
499 the number and the places of electrodes) of EEG signals vary significantly among different subjects’  
500 recordings, we select to use only the EEG recordings with the same 23 channels (see Appendix A)  
501 and discard other channels or the recordings don’t have all these 23 channels. Due to the purpose is to  
502 test whether the backdoor attack works on the ED task, not to study the epilepsy EEG classification,  
503 we segment part of the CHB-MIT dataset to form a four-class ED dataset (*i.e.*, the preictal, ictal,  
504 postictal, and interictal phases). Specifically, for a ictal phase EEG recording of  $t_i$  seconds from  
505  $[s_i, e_i]$  timepoints, we segment the  $[s_i - t_i, e_i]$  EEG as the preictal phase, the  $[e_i, e_i + t_i]$  EEG as the  
506 postictal phase, and another  $t_i$  seconds EEG recordings as the interictal phase which satisfying there  
507 is no ictal phase within half an hour before or after. Then we segment the 23-channel EEG signals  
508 into 1-second segments, consequently, there are 41336 segments left in total from all subjects, 10334  
509 for each phase. As the imbalanced amount of data across different subjects, we separate these 41336  
510 segments into 10 groups and treat the ten groups as 10 subjects.

## 511 D Implementation Details

### 512 D.1 Experiment Computing Resources

513 We use two servers for conducting our experiments. A server with one Nvidia Tesla V100 GPU is  
514 used for running reinforcement learning, the CUDA version is 12.3. Another server with four Nvidia  
515 RTX 3090 GPUs is used for running the backdoor attacks, the CUDA version is 11.4.

### 516 D.2 Details of Baseline Methods

517 In our ManiBCI backdoor attacks, for an EEG segment  $x_i \in \mathbb{R}^{E \times T}$ , we modify the  $\beta F$  frequency-  
518 points and  $\gamma E$  electrodes of a EEG segments with a constant number.

519 There are four baseline methods in our study for multi-target backdoor attacks, two of them are  
520 non-stealthy attacks (**PatchMT** and **PulseMT**) and two are stealthy attacks (**CompressMT** and  
521 **AdverseMT**). In order to achieve a fair comparison, we modify only first  $\gamma E$  electrodes for all  
522 baseline attack methods. For the non-stealthy attacks, which are all on the temporal domains, we  
523 modify  $\beta T$  timepoints of EEG signals. For the stealthy attacks, there is no constraint of the numbers  
524 of the modify timepoints as these attacks achieve stealthiness in another way.

525 For each baseline method, we try our best to find out the best performance, as demonstrated below.  
 526 We promise that we did not maliciously lower the performances of the baseline methods.

### 527 **D.2.1 PatchMT**

528 PatchMT is a multi-trigger and MT extension of BadNets [28] where we fill the first  $\beta T$  timepoints  
 529 and  $\gamma E$  electrodes of a EEG segments with a constant number. Specifically, for an EEG segment  
 530  $x_i \in \mathbb{R}^{E \times T}$ , we set the first  $\gamma E$  electrodes and the first  $\beta T$  timepoints of the EEG segment to a  
 531 constant number. We normalize the EEG segment  $x_i \in \mathbb{R}^{E \times T}$  to let  $\mathbf{x}_i$ 's mean is 0 and std is 1.  
 532 Then set the first  $\gamma E$  electrodes and the first  $\beta T$  timepoints of  $\mathbf{x}_i$  to a different constant number for  
 533 different class. The constant number for each class of  $\{0, 1, 2, 3\}$  for four classes, and  $\{-0.1, 0.0, 1.0\}$   
 534 for three classes. Finally, denormalize  $\mathbf{x}_i$  to original signal  $x_i$ 's scale to generate  $x_i^p$ .

535 Although we try our best to find the best performance of PatchMT, and BadNets [28] is really efficient  
 536 in image backdoor attacks, PatchMT cannot have satisfactory results in EEG BCI attack.

### 537 **D.2.2 PulseMT**

538 For PulseMT, we met the same questions as the PatchMT: how to identify the amplitude of each NPP  
 539 signal for each class? If the numbers are too large then normal EEG signals, it will be unfair. If the  
 540 numbers are too small, the efficacy of PulseMT is too negative.

541 We normalize the EEG segment  $x_i \in \mathbb{R}^{E \times T}$  to let  $\mathbf{x}_i$ 's mean is 0 and std is 1. The constant amplitude  
 542 for each class of  $\{-0.8, -0.3, 0.3, 0.8\}$ . Finally, denormalize  $\mathbf{x}_i$  to original signal  $x_i$ 's scale to  
 543 generate  $x_i^p$ .

### 544 **D.2.3 CompressMT**

545 Compressing the amplitude of EEG signals in the temporal domain will not change the morphology  
 546 and the frequency distribution of EEG signals, thus obtaining stealthiness. For three-class Emotion  
 547 datasets, the compress rate is  $\{0.8, 0.6, 0.4\}$ . For four-class Motor Imagery and Epilepsy datasets, the  
 548 compress rate is  $\{0.8, 0.6, 0.4, 0.2\}$ .

### 549 **D.2.4 AdverseMT**

550 AdverseMT is another stealthy EEG backdoor attacks, which is the multi-trigger and multi-target  
 551 extension of adversarial spatial filter attacks [18], in which, for EEG segment  $x_i \in \mathbb{R}^{E \times T}$ , it learns  
 552 an Spatial Filter  $\mathbf{W} \in \mathbb{R}^{E \times E}$  by the adversarial loss to let the model  $f$  misclassify  $x_i$ :

$$\min_{\mathbf{W}} \mathbb{E}_{(x_i, y_i) \sim \mathcal{D}} [-\mathcal{L}_{CE}(\mathbf{W}x_i, y_i) + \alpha \mathcal{L}_{MSE}(\mathbf{W}x_i, x_i)], \quad (11)$$

553 However, the original version of [18] requires the access to all training dataset  $\mathcal{D}$  and the control of  
 554 the training process of the model  $f$ . We modify the AdverseMT to only access to the training dataset  
 555  $\mathcal{D}_{train}$ . Note that the adversarial loss dose not have the special design for multi-target backdoor  
 556 attacks, we only run the process  $c$  times for obtaining  $c$  spatial filters for different classes. So the  
 557 poisoned subset are  $\mathcal{S}_p = \{(\mathbf{W}_0(x), 0), (\mathbf{W}_1(x), 1), (\mathbf{W}_2(x), 2), (\mathbf{W}_3(x), 3)\}$ .

## 558 **D.3 Reinforcement Learning Policy Network Architecture**

559 Here, we design a concise but effective convolutional neural networks as the our policy network,  
 560 which is defined as belows:

Table 6: The Architecture of Policy Network

Layer	In	Out	Kernel	Stride
Conv2d	1	32	(1, 3)	(1, 1)
BatchNorm2d				
ELU				
AvgPool2d				
Conv2d	32	64	(1, 3)	(1, 1)
BatchNorm2d				
ELU				
AvgPool2d				
AdaptiveAvgPool2d	64	256		(1, 1)
Flatten				
Linear				

## 561 E Attack Performance of ManiBCI

### 562 E.1 Different Poisoning Rates

563 We present the performance of each backdoor attacks’ performance under different poisoning rates in  
 564 Table 7. We can see that our ManiBCI outperforms other baseline at all poisoning rates, demonstrating  
 565 the superiority of ManiBCI. Note that the performance of ManiBCI on the MI dataset is significantly  
 566 robust to low poisoning rates, i.e., ASR of 1.000 when  $\rho = 0.05$ .

### 567 E.2 Hyperparameter Analysis: Frequency and Electrodes Injection Ratio

568 We present the performance of each backdoor attacks performance under different rates in Table 8  
 569 and Table 9. It can be observed with the increment of  $\beta$  and  $\gamma$ , the attack performance increases.  
 570 Because the trigger is bigger in clean EEG data.

### 571 E.3 Hyperparameter Analysis in Reinforcement Learning

572 We applied the following reward function to acquire the optimal mask strategies for each triggers:

$$Q_t = CA + \lambda ASR + \mu \text{dis}(\mathcal{M}_f^{c_i}) + \nu \min(\mathcal{M}_f^{c_i}), \quad (12)$$

573 where the first part means the clean accuracy, the second part means the attack success rate, the third  
 574 part is aiming to scatter the injection positions in various frequency bands, and the fourth part is  
 575 aiming to inject as high frequencies in EEG signals as possible. Here, we give a simple example to  
 576 demonstrate the reward function. For an 10 timepoints long EEG segment  $x_i, \tilde{x}_i = \mathcal{F}(x_i)$ . If the  
 577  $\mathcal{M}_f^{c_i} = \{2, 3, 5, 7, 9\}$ , because the minimal distance between each pair in  $\mathcal{M}_f^{c_i}$  is  $|2 - 3| = 1$ , thus  
 578  $\text{dis}(\mathcal{M}_f^{c_i}) = 1$ . The  $\min(\mathcal{M}_f^{c_i})$  means the lowest position in  $\mathcal{M}_f^{c_i}$ , thus  $\min(\mathcal{M}_f^{c_i}) = 2$ .

579 The analysis of the  $\lambda$  are presented in Table 10. When  $\lambda$  increase, the Attack performance increases  
 580 while the Clean performance declines slightly.

Table 10: Clean (/C) and attack (/B) performance with ASR’s hyperparameter  $\lambda, \mu = 0.3, \nu = 0.005$ 

	Dataset	Emotion		Motor Imagery		Epilepsy	
		Clean	Attack	Clean	Attack	Clean	Attack
0.5	ManiBCI	0.542±0.03	0.847±0.04	0.327±0.02	1.000±0.01	0.500±0.04	0.922±0.04
1.0	ManiBCI	0.537±0.02	0.855±0.03	0.325±0.02	1.000±0.01	0.482±0.03	0.935±0.05
2	ManiBCI	0.535±0.03	0.857±0.02	0.323±0.02	1.000±0.01	0.477±0.04	0.944±0.02



Table 7: Clean (/C) and attack (/B) performance with different poisoning rates for ManiBCI and other baseline methods. The target model is EEGNet for all cases.

$\rho$	Dataset Method	Emotion		Motor Imagery		Epilepsy	
		Clean	Attack	Clean	Attack	Clean	Attack
0.05	PatchMT	0.390	0.333	0.281	0.791	0.449	0.365
	PulseMT	0.488	0.337	0.275	0.788	0.473	0.397
	ComprsMT	0.448	0.313	0.269	0.754	0.449	0.329
	ManiBCI	0.491	0.566	0.321	1.000	0.460	0.667
0.10	PatchMT	0.443	0.334	0.279	0.785	0.452	0.400
	PulseMT	0.445	0.394	0.281	0.796	0.486	0.591
	ComprsMT	0.509	0.323	0.270	0.778	0.446	0.337
	ManiBCI	0.541	0.718	0.320	1.000	0.452	0.734
0.15	PatchMT	0.455	0.335	0.285	0.805	0.439	0.414
	PulseMT	0.438	0.514	0.280	0.787	0.447	0.669
	ComprsMT	0.488	0.332	0.275	0.792	0.461	0.374
	ManiBCI	0.528	0.805	0.322	1.000	0.460	0.781
0.20	PatchMT	0.481	0.334	0.277	0.816	0.461	0.451
	PulseMT	0.447	0.555	0.285	0.810	0.451	0.692
	ComprsMT	0.470	0.347	0.270	0.795	0.458	0.394
	ManiBCI	0.538	0.773	0.321	1.000	0.447	0.799
0.25	PatchMT	0.487	0.335	0.281	0.820	0.444	0.483
	PulseMT	0.466	0.701	0.275	0.815	0.431	0.684
	ComprsMT	0.493	0.335	0.269	0.800	0.462	0.427
	ManiBCI	0.551	0.836	0.325	1.000	0.447	0.834
0.30	PatchMT	0.459	0.343	0.280	0.809	0.440	0.496
	PulseMT	0.486	0.810	0.272	0.816	0.451	0.716
	ComprsMT	0.499	0.331	0.269	0.825	0.455	0.481
	ManiBCI	0.526	0.829	0.320	1.000	0.451	0.756
0.35	PatchMT	0.437	0.341	0.285	0.805	0.448	0.510
	PulseMT	0.437	0.767	0.275	0.837	0.482	0.757
	ComprsMT	0.473	0.347	0.265	0.851	0.446	0.517
	ManiBCI	0.489	0.763	0.321	1.000	0.453	0.910
0.40	PatchMT	0.490	0.345	0.283	0.824	0.460	0.549
	PulseMT	0.454	0.771	0.270	0.825	0.439	0.443
	ComprsMT	0.464	0.361	0.269	0.865	0.437	0.450
	ManiBCI	0.528	0.849	0.323	1.000	0.477	0.944

Table 8: Clean (/C) and attack (/B) performance with frequency injection rate  $\beta, \gamma = 0.5$

$\beta$	Dataset	Emotion		Motor Imagery		Epilepsy	
		Clean	Attack	Clean	Attack	Clean	Attack
0.05	PatchMT	0.411	0.334	0.272	0.801	0.476	0.499
	PulseMT	0.464	0.752	0.265	0.800	0.505	0.670
	ManiBCI	0.522	0.744	0.319	0.999	0.482	0.923
0.10	PatchMT	0.431	0.363	0.283	0.824	0.482	0.540
	PulseMT	0.460	0.795	0.270	0.825	0.486	0.704
	ManiBCI	0.522	0.813	0.323	1.000	0.500	0.944
0.15	PatchMT	0.413	0.371	0.275	0.821	0.464	0.587
	PulseMT	0.449	0.701	0.271	0.821	0.477	0.632
	ManiBCI	0.532	0.848	0.322	0.998	0.477	0.947
0.20	PatchMT	0.390	0.377	0.271	0.829	0.479	0.644
	PulseMT	0.434	0.769	0.270	0.819	0.484	0.606
	ManiBCI	0.529	0.882	0.325	0.999	0.486	0.950
0.25	PatchMT	0.406	0.385	0.267	0.835	0.491	0.673
	PulseMT	0.491	0.705	0.275	0.832	0.478	0.566
	ManiBCI	0.519	0.865	0.328	0.999	0.486	0.941
0.30	PatchMT	0.417	0.382	0.269	0.831	0.464	0.706
	PulseMT	0.425	0.708	0.273	0.844	0.488	0.592
	ManiBCI	0.521	0.862	0.330	0.999	0.495	0.940
0.35	PatchMT	0.435	0.373	0.270	0.841	0.475	0.734
	PulseMT	0.423	0.621	0.276	0.839	0.479	0.589
	ManiBCI	0.527	0.850	0.332	0.998	0.496	0.947
0.40	PatchMT	0.438	0.378	0.271	0.843	0.469	0.751
	PulseMT	0.481	0.624	0.272	0.845	0.485	0.592
	ManiBCI	0.521	0.893	0.330	0.999	0.501	0.951
0.45	PatchMT	0.460	0.385	0.266	0.844	0.481	0.742
	PulseMT	0.429	0.633	0.277	0.856	0.499	0.601
	ManiBCI	0.519	0.877	0.325	0.999	0.492	0.962
0.50	PatchMT	0.423	0.386	0.263	0.840	0.480	0.752
	PulseMT	0.459	0.514	0.273	0.851	0.492	0.610
	ManiBCI	0.528	0.893	0.329	1.000	0.497	0.970

Table 9: Clean (/C) and attack (/B) performance with electrodes injection rate  $\gamma$ ,  $\beta = 0.1$ 

$\gamma$	Dataset	Emotion		Motor Imagery		Epilepsy	
	Method	Clean	Attack	Clean	Attack	Clean	Attack
0.10	PatchMT	0.431	0.334	0.268	0.795	0.470	0.529
	PulseMT	0.425	0.498	0.269	0.802	0.502	0.717
	ComprsMT	0.407	0.349	0.271	0.805	0.482	0.656
	ManiBCI	0.489	0.485	0.235	0.367	0.499	0.814
0.20	PatchMT	0.473	0.335	0.271	0.805	0.464	0.599
	PulseMT	0.469	0.707	0.270	0.816	0.502	0.737
	ComprsMT	0.465	0.363	0.268	0.812	0.514	0.704
	ManiBCI	0.481	0.709	0.235	0.367	0.486	0.860
0.30	PatchMT	0.423	0.343	0.272	0.803	0.486	0.613
	PulseMT	0.488	0.767	0.273	0.814	0.506	0.749
	ComprsMT	0.451	0.398	0.271	0.811	0.494	0.700
	ManiBCI	0.500	0.743	0.235	0.367	0.490	0.883
0.40	PatchMT	0.453	0.343	0.270	0.812	0.478	0.525
	PulseMT	0.467	0.786	0.271	0.816	0.498	0.688
	ComprsMT	0.443	0.361	0.270	0.820	0.506	0.634
	ManiBCI	0.491	0.767	0.235	0.367	0.478	0.912
0.50	PatchMT	0.431	0.363	0.270	0.813	0.472	0.552
	PulseMT	0.460	0.795	0.269	0.819	0.471	0.710
	ComprsMT	0.430	0.366	0.269	0.821	0.503	0.640
	ManiBCI	0.522	0.813	0.235	0.367	0.477	0.944
0.60	PatchMT	0.452	0.377	0.267	0.819	0.480	0.549
	PulseMT	0.460	0.808	0.269	0.823	0.490	0.672
	ComprsMT	0.459	0.368	0.271	0.826	0.499	0.534
	ManiBCI	0.488	0.828	0.235	0.367	0.495	0.950
0.70	PatchMT	0.443	0.368	0.272	0.812	0.497	0.525
	PulseMT	0.437	0.809	0.270	0.821	0.459	0.716
	ComprsMT	0.456	0.366	0.273	0.835	0.492	0.571
	ManiBCI	0.527	0.853	0.235	0.367	0.489	0.955
0.80	PatchMT	0.461	0.383	0.268	0.821	0.479	0.573
	PulseMT	0.456	0.771	0.267	0.829	0.488	0.699
	ComprsMT	0.431	0.383	0.270	0.833	0.488	0.475
	ManiBCI	0.539	0.865	0.235	0.367	0.489	0.960
0.90	PatchMT	0.439	0.400	0.271	0.817	0.478	0.540
	PulseMT	0.461	0.811	0.269	0.823	0.494	0.694
	ComprsMT	0.459	0.389	0.274	0.836	0.490	0.309
	ManiBCI	0.520	0.824	0.235	0.367	0.489	0.970
1.00	PatchMT	0.430	0.370	0.267	0.823	0.476	0.526
	PulseMT	0.456	0.794	0.271	0.829	0.482	0.716
	ComprsMT	0.453	0.376	0.269	0.830	0.490	0.334
	ManiBCI	0.532	0.846	0.235	0.367	0.491	0.978

581 **F More Visualization Results**

582 In this section, we plot the reconstructed triggers and masks on three datasets in Section F.1, then  
 583 plot more visualizations of backdoor samples in Section ??, and plot the learning curve of our  
 584 reinforcement learning in Section F.3.

585 **F.1 Neural Cleanse: Reconstruction Trigger Patterns**

586 Here, we present more visualization in Figure 9, Figure 10, and Figure 11 of the reconstructed trigger  
 587 patterns and mask patterns for each possible label on three dataset (*i.e.*, the CHB-MIT dataset, the  
 588 BCIC-IV-2a dataset and the SEED dataset) the target model is EEGnet. It can be observed that the  
 589 reconstructed trigger patterns and mask patterns of the clean models and ManiBCI backdoor-injected  
 590 models are very similar to each other. Thus, our ManiBCI backdoor attack can easily bypass the  
 591 defense of Neural Cleanse.

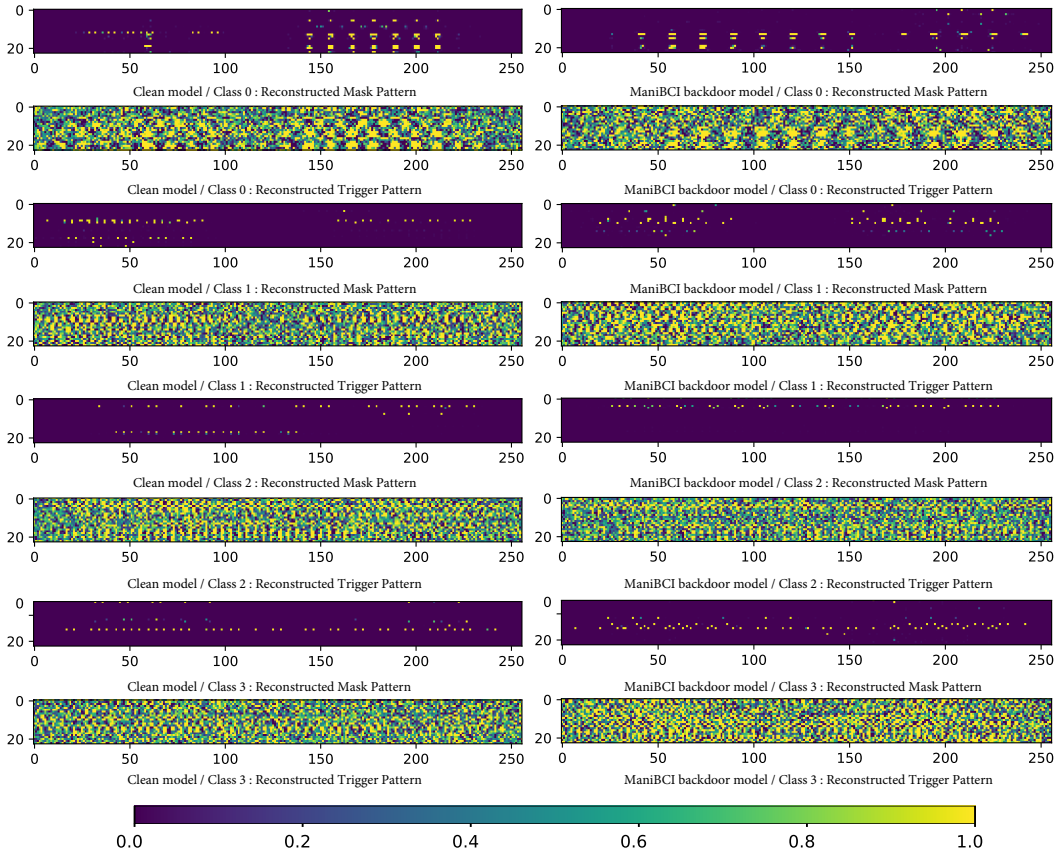


Figure 9: The reconstructed trigger patterns and mask patterns for each possible class in the CHB-MIT dataset. The results in the left column are reconstructed based on the clean model, the results in the right column are reconstructed based on the backdoor model. The EEG segments in the CHB-MIT dataset have 23 electrodes and 256 timepoints.

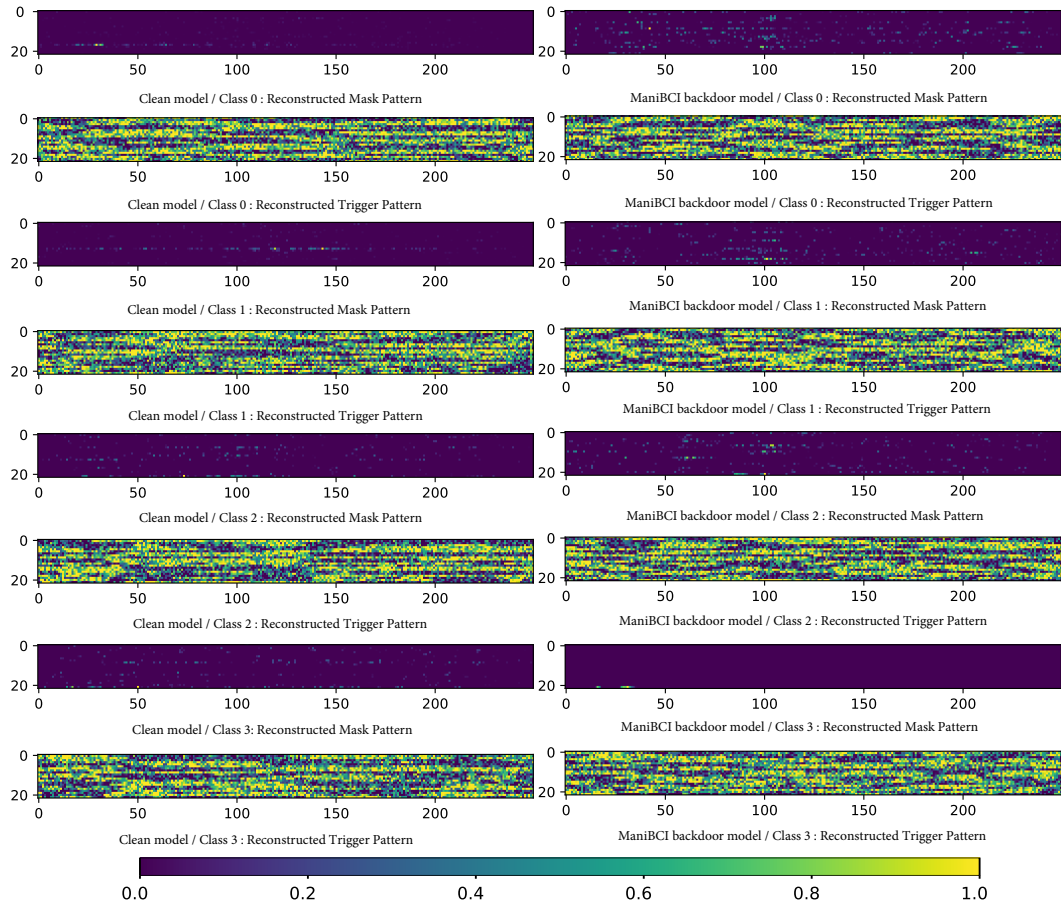


Figure 10: The reconstructed trigger patterns and mask patterns for each possible class in the MI dataset. The results in the left column are reconstructed based on the clean model, the results in the right column are reconstructed based on the backdoor model. The EEG segments in the MI dataset have 22 electrodes and 250 timepoints.

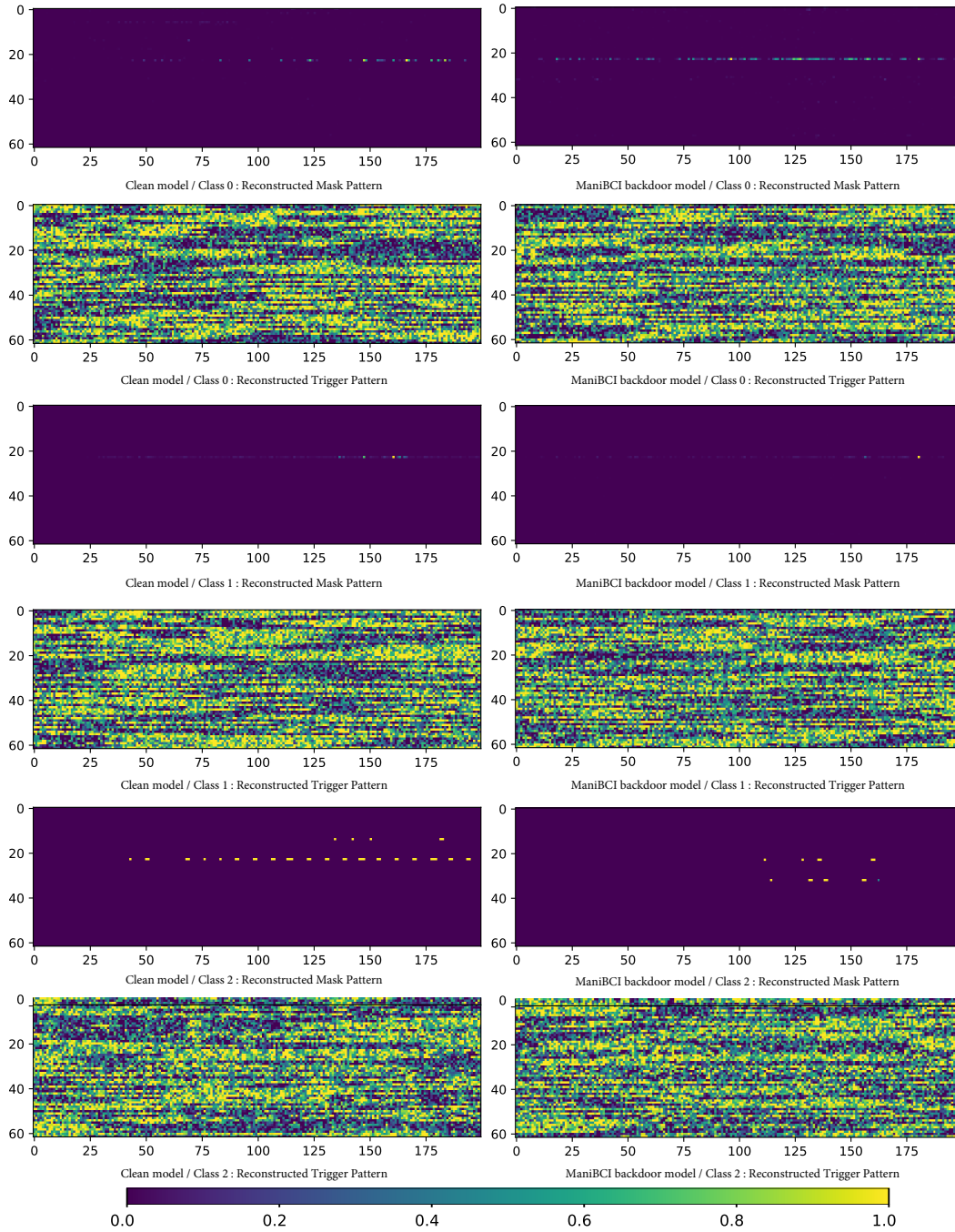


Figure 11: The reconstructed trigger patterns and mask patterns for each possible class in the ER dataset (i.e., SEED dataset). The results in the left column are reconstructed based on the clean model, the results in the right column are reconstructed based on the backdoor model. The EEG segments in the SEED dataset have 62 electrodes and 200 timepoints.

592 **F.2 Visualization of Backdoor Attack Samples**

593 We present more visualization of the backdoor attack samples generated by our ManiBCI on ER  
 594 dataset and MI dataset in Fig 12 and 13. The x-axis is the timepoints, the y-axis is the normalized  
 595 amplitude. Top row: w.o. HF loss; Bottom row: with HF loss. Each column indicates each possible  
 596 class.

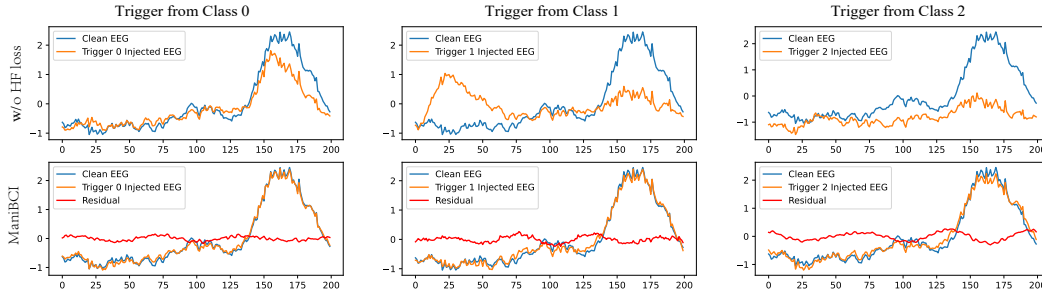


Figure 12: The Clean EEG (Blue), Trigger-injected EEG (Orange) and the Residual (Red) of the ER dataset.

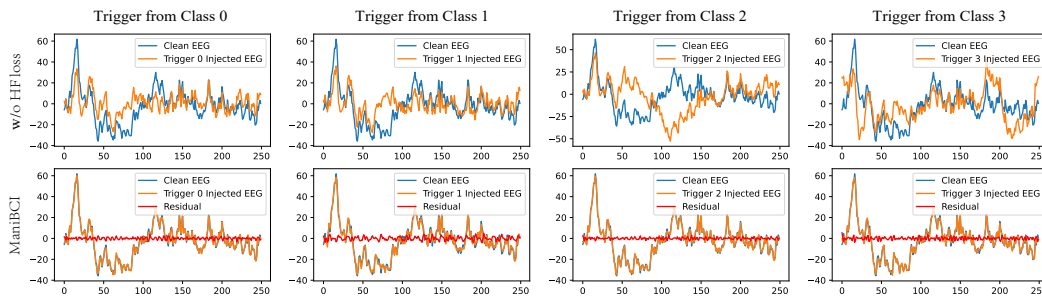


Figure 13: The Clean EEG (Blue), Trigger-injected EEG (Orange) and the Residual (Red) of the MI dataset.

597 **F.3 Visualization of Learning Curves of Reinforcement Learning**

598 We present the visualization of the learning curves of the reinforcement learning of three dataset in  
 599 Fig 14. We can see the effectiveness of our reinforcement, which converged within 50 epochs on the  
 600 ER dataset, that is, only trained 50 backdoor models with different injection strategies. Our RL is  
 601 more effective on the MI dataset and ED dataset, which finds a good strategy within less 10 epochs.  
 602 Our RL is robust when learning strategies for different triggers as demonstrated in Fig 14(c) and (d),  
 603 where the learning curves are quite similar when RL is performing on different triggers.

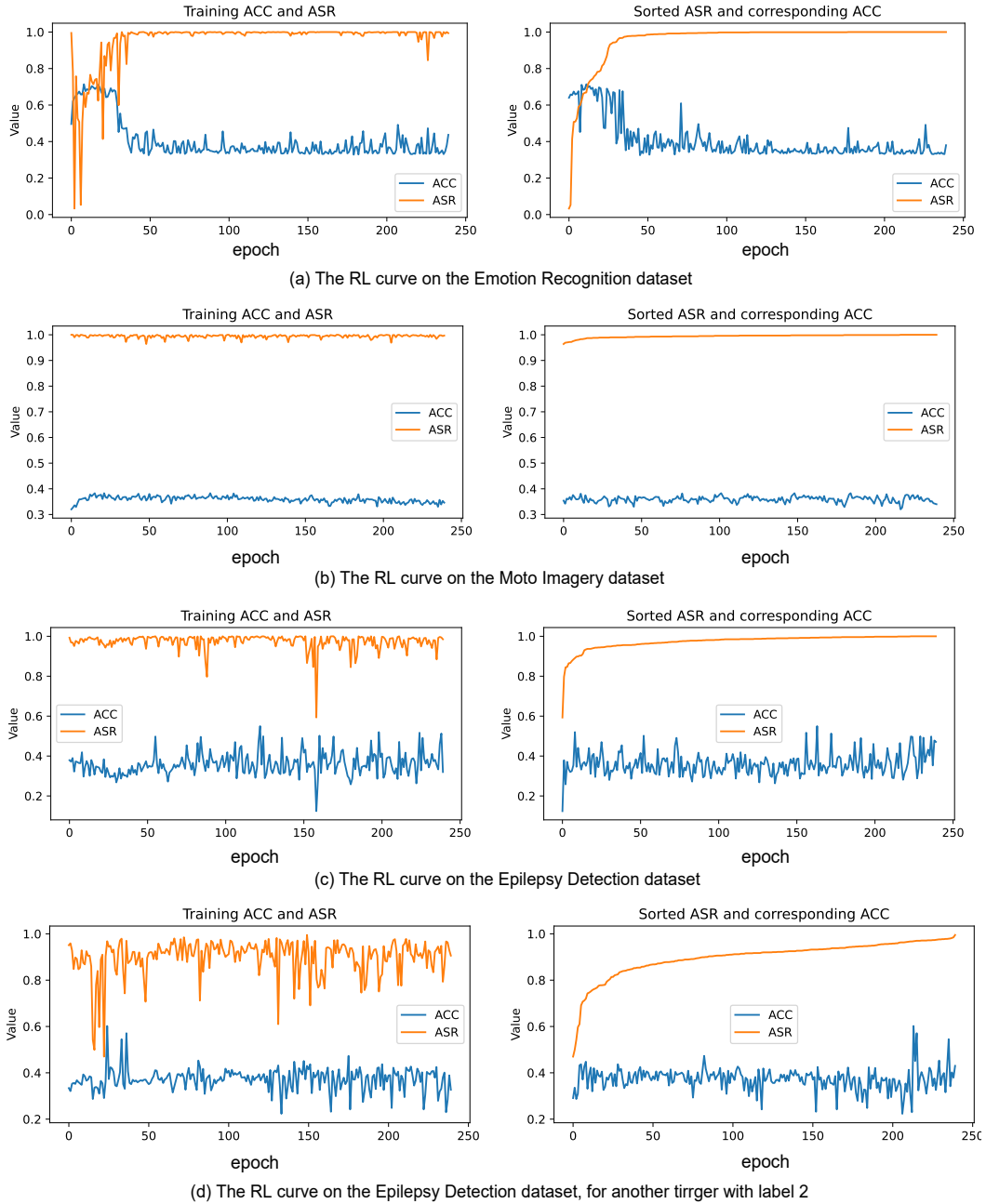


Figure 14: The learning curves of RL on three datasets. The right column is the curve we sort the (ACC,ASR) according to the ASR. The backdoor models are all EEGNet.



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