

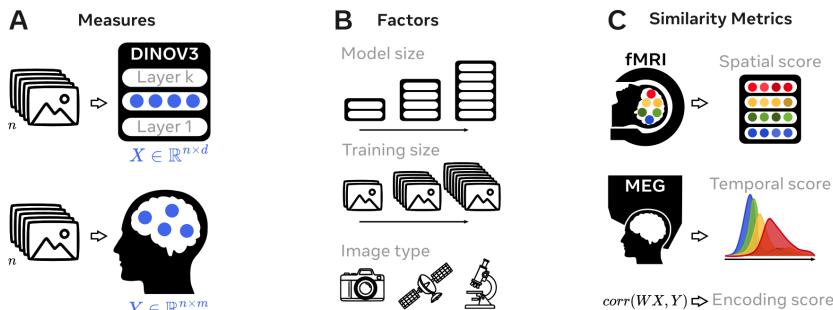
000 001 002 003 004 005 006 007 008 009 010 011 012 013 014 015 016 017 018 019 020 021 022 023 024 025 026 027 028 029 030 031 032 033 034 035 036 037 038 039 040 041 042 043 044 045 046 047 048 049 050 051 052 053 DISENTANGLING THE FACTORS OF CONVERGENCE BETWEEN BRAINS AND DINOV3

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ABSTRACT

Many AI models trained on natural images develop representations that resemble those of the human brain. However, the factors that drive this brain-model similarity remain poorly understood. To disentangle how the model, training and data independently lead a neural network to develop brain-like representations, We trained a family of [self-supervised DINOV3 vision transformers](#) that systematically varied these different factors. We compare their representations of images to those of the human brain recorded with both fMRI and MEG, providing high resolution in both spatial and temporal analyses. We assess the brain-model similarity with three complementary metrics focusing on overall representational similarity, topographical organization, and temporal dynamics. We show that all three factors - model size, training amount, and image type - independently and interactively impact each of these brain similarity metrics. In particular, the largest DINOV3 models trained with the most human-centric images reach the highest brain-similarity. This emergence of brain-like representations in AI models follows a specific chronology during training: models first align with the early representations of the sensory cortices, and only align with the late and prefrontal representations of the brain with considerably more training. Finally, this developmental trajectory is indexed by both structural and functional properties of the human cortex: the representations that are acquired last by the models specifically align with the cortical areas with the largest developmental expansion, thickness, least myelination, and slowest timescales. Overall, these findings disentangle the interplay between architecture and experience in shaping how artificial neural networks come to see the world as humans do, thus offering a promising framework to understand how the human brain comes to represent its visual world.



Method Figure. **A.** We compare the activation of DINOv3, a state-of-the-art self-supervised computer vision model trained on natural images, to the activations of the human brain in response to the same images. **B.** To understand the factors that make DINOv3 more-or-less similar to the brain, we train *from scratch* a variety of models on different image domains (pictures from human-centric cameras, satellite images or biological data), and with a varying amount of data. **C.** We compare each model to both functional Magnetic Resonance Imaging (fMRI, with high spatial resolution) and Magneto-Encephalography (MEG, with high temporal resolution) by computing the overall linear similarity of their representations (encoding score) and the similarity of their hierarchical organization (spatial and temporal scores).

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1 INTRODUCTION

058 **Brain-AI similarity.** Deep learning has transformed computer vision over the past decade. State-
059 of-the-art deepnets now achieve human-level or superior performance across a variety of tasks in-
060 cluding classification (Siméoni et al., 2025; Tschannen et al., 2025), object detection (Redmon et al.,
061 2016), semantic segmentation (Cheng et al., 2022), and medical image analysis (Esteva et al., 2017;
062 Lorenci et al., 2025). Surprisingly, the internal representations of these deep learning models appear
063 to be related to those of the human brain: multiple electrophysiology (Yamins et al., 2014a; Yamins
064 & DiCarlo, 2016; Schrimpf et al., 2018; Zhuang et al., 2021), functional Magnetic Resonance Imaging
065 (Eickenberg et al., 2017; Millet et al., 2023; Doerig et al., 2025; Tang et al., 2023; Nikolaus et al.,
066 2024), magneto-encephalography studies (Cichy et al., 2016; Seeliger et al., 2018; Caucheteux &
067 King, 2022; Banville et al., 2025) have now consistently shown that the activation patterns of these
068 models linearly map onto those of the cortex in response to the same images.

069 **Theoretical importance.** Understanding the principles at the origin of this representational simi-
070 larity between AI models and the human brain is of primary importance, to understand the laws of
071 information processing that may be universally shared across neural networks. Indeed, several lines
072 of research (Hasson et al., 2020; Huh et al., 2024; van Rossem & Saxe, 2024; Cagnotta et al., 2024;
073 Mehrer et al., 2020; Mahner et al., 2025; Simkova et al., 2025) suggest that there exists universal
074 principles that constrain the structure and emergence of representations in neural networks.

075 **Challenge: Unclear causes.** The precise factors responsible for the representational similarity be-
076 tween computer vision models and the human remain currently unclear. This gap of knowledge
077 is partly due to the fact that previous studies primarily focused on pretrained networks that *simul-
078 taneously* vary in training objectives, architectures and data regime (Conwell et al., 2021; Rajesh
079 et al., 2024). How each of these factors independently and interactively leads a model to converge
080 to brain-like representations thus remains unclear.

081 To address this issue, we systematically train a variety of DINOv3 models (Siméoni et al., 2025),
082 while independently varying their size, data type and training quantity. DINOv3 has the advantage
083 of being self supervised, and can thus be trained on different types of naturalistic but non-human
084 centric and non-labelled data such as satellite images (Siméoni et al., 2025) and biological images
085 (Lorenci et al., 2025).

086 Here, we compare a variety of DINOv3 models to the brain responses to images, as recorded with
087 ultra high field (7T) functional MRI and magneto-encephalography (MEG) to get a high spatial
088 and temporal resolution of the cortical representations, respectively. For this, we implement three
089 similarity metrics. First, we use a standard linear mapping metric, often referred to as *encoding score*
090 (Naselaris et al., 2011b), which evaluates the linear correspondence between the representations of
091 two systems. Second, we evaluate, with fMRI, whether this linear mapping follows a similar *spatial*
092 organization, whereby the first and last layers of the model would best match the sensory visual and
093 prefrontal cortices, respectively. Finally we evaluate, with MEG, whether this mapping follows a
094 similar *temporal* organization, whereby the first and last layers of the model best match the early
095 and late MEG responses, respectively.

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2 METHOD

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2.1 APPROACH

099 We aim to identify the factors that make modern computer vision models process and represent nat-
100 ural images similarly to the human brain. Following previous work (Kriegeskorte et al., 2008; Di-
101 Carlo et al., 2012; King & Dehaene, 2014), we rely on the definition of "representation" as "linearly
102 readable information". We employ the encoding analysis procedure introduced by Naselaris et al.
103 (2011b) to evaluate the representational similarity between an AI model and brain recordings. This
104 linear model seeks to find whether there exists a linear mapping $W \in \mathbb{R}^{m \times d}$ that reliably predicts
105 m -dimensional brain activity ($Y \in \mathbb{R}^{n \times m}$) given the d -dimensional model activation ($X \in \mathbb{R}^{n \times d}$)
106 in response to n images:

$$107 \arg \min_W \{ \|Y - XW\|_2^2 + \lambda \|W\|_2^2 \}$$

108 with λ the ridge regularization parameter. **We use linear probes to maintain geometries of compared**
 109 **representations.** We use scikit-learn’s RidgeCV (Pedregosa et al., 2011), 10 logarithmically-spaced
 110 regularization λ in between 10^0 and 10^8 , and a 5-split cross-validation.
 111

112 **2.2 METRICS**
 113

114 **Encoding score** Given two representations X and Y , we quantify their overall representational
 115 similarity by computing, for each split separately and then averaged, an *encoding score* with a
 116 Pearson correlation score $R \in [-1, 1]$:

117
$$R = \text{corr}(WX_{\text{test}}, y_{\text{test}})$$

 118

119 We rely on encoding as the basis for our three metrics (encoding, spatial, and temporal scores), rather
 120 than decoding, as decoding metrics cannot be meaningfully compared across models with different
 121 architectures and representational spaces. Following the rationale of (Naselaris et al., 2011a), encoding
 122 provides an interpretable mapping from model features to neural responses, comparable across
 123 **architectures and training regimes.** For clarity, we can either summarize the average R score across
 124 brain dimensions, or plot them all separately to get information about where brain activations are
 125 linearly predictable from the model. In some analysis, we use $\bar{R} = R/\max(R)$, the normalized
 126 encoding score, which peaks at 1.
 127

128 **Spatial score** To assess whether a model organized its processing hierarchy similarly to that of a
 129 brain with a *spatial score*, we proceed in four steps. First, we evaluate an encoding score for each
 130 dimension m of the brain, and from 22 layers $k \in [0, 1]$ of the model, where 0 is the first layer, and
 131 1 is the last layer. Second, we identify the layer that best predicts this brain response: k^* . Third, we
 132 approximate the hierarchical position m^* of each brain region, as its Euclidean distance from V1 in
 133 the standardized MNI space, in mm. Note that this is a coarse approximation, as the actual cortical
 134 hierarchy does not strictly follow such distances, and may be considerably more complex (Felleman
 135 & Van Essen, 1991). Finally, we compute the spatial score as the correlation between m^* and k^* .
 136 For clarity we restrict these analyses to regions of interest.
 137

138 **Temporal score** To evaluate an analogous metrics from MEG recordings, we estimate a *temporal*
 139 *score*: the correlation between the model layers k and T_{\max}^{layer} – the time at which each layer of the
 140 model is maximally predictive of brain activity. To limit noisy estimate, we average on the temporal
 141 window during which $\bar{R}^k \geq 95\%$ where \bar{R}^k is the normalized encoding-score of the layer k .
 142

143 **2.3 MODELS**
 144

145 **Architecture.** DINOv3 is an open-source, state-of-the-art, self supervised learning vision trans-
 146 former model trained on 1.7 billion natural images (Siméoni et al., 2025). We train, from scratch,
 147 a selection of eight variants of this DINOv3 model to ensure a comprehensive evaluation ranging
 148 through architectures, training scale and data types.
 149

150 First, we leverage the DINOv3-7B, trained across $1e^7$ checkpoints. We analyze comparatively DINO
 151 Small, Base, Large and Giant, after training for $5e^6$ training steps on 1.7B images with the same con-
 152 figuration. Additionally, we train and analyze comparatively 3 versions of the DINO Large archi-
 153 tecture: DINO human, DINO Cellular and DINO Satellite. These models were configured similarly
 154 and trained, from scratch, over $5e^6$ steps on 10M images; they only differ in the type of images with
 155 which they were trained.
 156

157 **2.4 DATASETS.**
 158

159 **Images.** DINOv3-7B and DINO human were trained on the same human-centric data. This dataset
 160 was constructed from a large pool of web images, street views and ImageNet (Deng et al., 2009).
 161 These images went through platform-level content moderation to prevent harmful contents, in order
 162 to obtain an data pool of approximately 17 billion images. This data pool was curated following the
 163 procedure of (Siméoni et al., 2025) to obtain a large-scale pre-training dataset of 1.7 billion images.
 164 To compare models trained with different types of images, we re-trained three distinct large DINOv3
 165 with one of three types of natural images – human-centric, cellular and satellite images – matched
 166 in terms of quantity (10M images each).
 167

168 Human-centric images correspond to the dataset used for training the original DINOv3 model. For
 169

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Table 1: Specifications of DINOv3 model variants.

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Model	Parameters	Layers	Batch	Images
DINOv3	7B	40	4096	Human centered 1.7B
DINOv3 Giant	1.1B	32	4096	Human centered 1.7B
DINOv3 Large	300M	24	4096	Human centered 1.7B
DINOv3 Base	86M	12	4096	Human centered 1.7B
DINOv3 Small	21M	12	4096	Human centered 1.7B
DINOv3 Human	300M	24	2048	Human centered 10M
DINOv3 Cellular	300M	24	2048	Cellular 10M
DINOv3 Satellite	300M	24	2048	Satellite 10M

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177 our comparative analyses on human-centric, cellular and satellite images, we randomly selected
 178 from this dataset of 1.7 billion images a subset of 10 million images.

179 Cellular images correspond to the ExtendedCHAMMI dataset, which consists of fluorescent micro-
 180scopic images of cells revealing cellular structures into different channels (e.g. nucleus, mitochondria,
 181 microtubules, etc.) (Lorenci et al., 2025).

182 Satellite images correspond to a random subset of the SAT-493M dataset, which consists of approxi-
 183 mately 500 million images sampled randomly from Maxar RGB ortho-rectified imagery at 0.6 meter
 184 resolution (Siméoni et al., 2025).

185 **Magnetoencephalography (MEG).** We use the THINGS-MEG dataset (Hebart et al., 2023a),
 186 which consists of MEG recordings from four healthy participants viewing 22,500 naturalistic im-
 187 ages, representing a total of 1,800 object concepts (Hebart et al., 2023b). Images were presented
 188 during 1.5 s, while participants maintained fixation. To limit the impact of noise we apply a band-
 189 pass filter between 0.1 and 20 Hz, down-sample the signal at 30 Hz, time-lock the brain responses to
 190 individual words, and epoch the corresponding neural data between -0.5 s and +3 s relative to word
 191 onset using MNE-Python (Gramfort et al., 2013). Finally, we z-score MEG signals across words,
 192 for each MEG channel and each time point independently.

193 *time ROIs.* We study individually three 0.05s-long time ROIs across the processing time of an im-
 194 age, to study the relative impact of each layer in the encoding of the cognitive process at play during
 195 that time. These time windows span .08-.13s, .13-.18s and .5-.55s.

196 T_{\max}^{layer} . To study the dynamics of each layer, we compute T_{\max}^{layer} , the mean of the temporal window
 197 during which $\tilde{R}^{\text{layer}} \geq 95\%$ where \tilde{R}^{layer} is the normalized encoding-score of each layer.

198 **Functional Magnetic Resonance Imaging (fMRI).** We leverage the Natural Scenes Dataset (Allen
 199 et al., 2022), a 7 tesla fMRI dataset which consists of recordings from eight subjects, each observing
 200 a total of 10 000 natural scenes during 4 seconds each, while performing a continuous recognition
 201 task. We encode the BOLD signal on the fsaverage surface at 5.5 s after image onset. This timestep
 202 corresponds to the peak of decoding of the image from the BOLD signal.

203 *Regions of interest (ROIs).* For clarity, we select a representative set of 15 regions of interest (ROIs)
 204 spanning the anatomy of the cortex, among the regions encoded with an averaged FDR-corrected
 205 t-test $p < 0.01$, among voxels forming the ROI. These ROIs are distributed from posterior-occipital
 206 lobe to prefrontal cortex.

207 To investigate the cortical properties that index representational similarity, we analyze our results in
 208 light of four cortical maps, made available through Neuromaps (Markello et al., 2022):

209 *Cortical expansion* (Hill et al., 2010) reflects the difference of cortical surface area between infants
 210 and adults.

211 *Myelin concentration* is estimated from the T1w/T2w ratio in the HCP S1200 dataset (Van Essen
 212 et al., 2013).

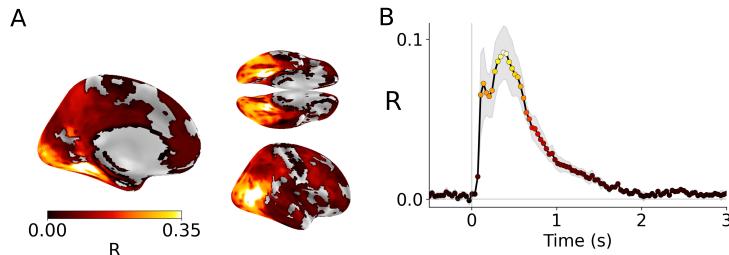
213 *Intrinsic timescales* are derived from mapping electromagnetic networks to hemodynamic network
 214 and indexing the temporal integration window of each region (Shafiei et al., 2021).

215 *Cortical thickness* is estimated by measuring the distance between "white" and "pial" Freesurfer
 216 surfaces (Fischl, 2012) from structural MRI in the Human Connectome Project (Van Essen et al.,
 217 2013).

216 2.5 STATISTICS
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218 *fMRI voxels*. We only plot and analyze voxels thresholded with $p < 0.01$ after a FDR-corrected
219 t-test. *Across subjects*. To evaluate statistical estimates across subjects, we perform a Wilcoxon test
220 using `scipy` (Virtanen et al., 2020). To correct for multiple comparison, we apply a false discovery
221 rate correction, as implemented in MNE-Python (Gramfort et al., 2013).

222 *Half times*. To analyze the speed of convergence of DINO models during training, we estimate the
223 ‘half time’: the training step at which the similarity metric reaches half of its final value.

224 3 RESULTS
225226 3.1 DINOv3-BRAIN SIMILARITY
227

238 **Figure 1: Brain-DINOv3 similarity across space and time. A. Across cortical space.** Similarity
239 between DINOv3 embedding and the fMRI responses to corresponding images as estimated with a
240 Pearson Brain-Score, and FDR-corrected-thresholded at $p < 0.01$ (left: medial view of left hemisphere,
241 top right: bottom view; bottom right: lateral view of right hemisphere). **B. Across time.**
242 Similarity between DINOv3 embedding and MEG responses to the corresponding images. The
243 error bar indicates the standard error of the mean across 4 subjects.

245 **Encoding score.** To verify that DINOv3 generates representations of natural images that are simi-
246 lar to those of the brain, we perform a cross-validated encoding analysis by evaluating the linear
247 mapping between the activations of DINOv3 and of the brain in response to the same images. Func-
248 tional MRI results show that DINOv3 has representations that primarily peak in the visual pathway
249 ($R = .45 \pm .039$ - SEM across subjects), mostly in the lateral-occipitotemporal (MT: $R = .34 \pm .026$)
250 and ventromedial visual cortex (VMV2: $R = .28 \pm .025$), Fig 1A.

251 MEG results show that this similarity rises around 70 ms after image onset ($R = .09 \pm .017$, Fig 1B)
252 and remains significantly above chance level up to 3 seconds after image onset ($p < 1e-3$).
253 These results are consistent with past studies (Eickenberg et al., 2017; Schrimpf et al., 2018; Tang
254 et al., 2025) and additionally show that areas typically discarded from the visual pathways, e.g. pre-
255 frontal regions BA 44, BA 45, IFSa and IFSp, also present activations that are linearly predictable
256 from the AI embedding.

257 **Spatial score.** Does the hierarchy of representations of DINOv3 correspond to the visual hierarchy
258 in the human brain? To address this question, we estimate the “spatial score”. The fMRI results
259 confirm that the lowest layers of DINOv3 tend to best predict the lower-level sensory regions such
260 as V1, whereas the highest layers tend to best predict higher-level regions of the brain, such as the
261 prefrontal cortex (Fig 2A, B). The Pearson correlation between (i) the Euclidean distance between
262 each brain region and V1, and (ii) the best encoding layer is highly significant, $R = 0.38$, $p < 1e^{-6}$
263 (Fig 2B). **Temporal score.** To complement this fMRI “spatial score”, we evaluate an MEG “tempo-
264 ral score”. We identify the layer which best predicts each time ROIs relative to image onset in the
265 MEG. The results show a significant correlation between layers and their T_{\max}^{layer} , hereafter referred
266 to as the temporal score (Fig 2C, D). The temporal score $R = 0.96$, $p < 1e^{-12}$, shows that the early
267 and late layers of DINOv3 consistently align with the earliest and latest MEG responses, respec-
268 tively. **Generalization to multiple architectures.** To test for generalization of Encoding, Spatial
269 and Temporal scores we reproduce these results on a variety of seven vision models including CNNs,
supervised and self-supervised ViTs as well as vision-language contrastive transformers. We find
similar scores for all three metrics, across all these models (Figs. S1,S2,S3,S4,S5)

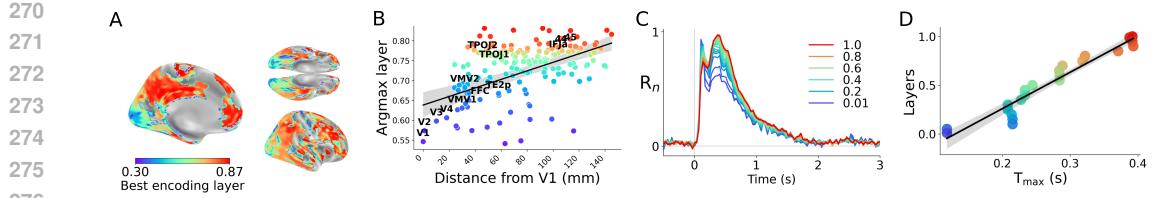


Figure 2: **The representational hierarchy of DINOv3 corresponds to the brain's.** **A.** Voxel-wise best encoding layers of DINOv3, FDR-corrected and thresholded at $p < 0.01$ (left: medial view of left hemisphere, top right: bottom view; bottom right: lateral view of right hemisphere). **B.** Plotting the correlation between the best encoding layer for each region and the euclidean distance of this region from V1, in mm. The Pearson correlation is $r = 0.38$, $p < 1e-6$. Plotted regions are encoded with FDR-corrected thresholding at $p < 0.01$. **C.** Dynamic brain-score across time between each layer of DINOv3 and MEG responses to the corresponding still images. **D.** Plotting the correlation between the layers and their T_{\max}^{layer} , in s. The Pearson correlation is $r = 0.84$, $p < 1e-5$. Plotted regions are encoded with FDR-corrected thresholding at $p < 0.01$.

3.2 WHAT FACTORS LEAD DINOv3 TO BECOME BRAIN-LIKE?

Impact of training. To clarify the emergence of brain-like processes in DINOv3, we evaluate the encoding score, spatial score and temporal score at each selected training step of DINOv3, and summarize their developmental speed with a ‘half time’: i.e. the training step where half of the final score is reached. First, before training the encoding score reaches $R=.03 \pm 2e^{-4}$, after training it ultimately converges to $R=.09 \pm 5e^{-4}$ (Fig 3). These R-scores are averaged across voxels – the best voxel peaking at $R=.45 \pm .038$. The half time of the encoding score occurs around 2% of the training, around $2e^5$ training steps (i.e. 800 million images). Second, the temporal score emerges faster than the encoding-score: with a half time around 0.7% of the training, and a convergence at $R=0.96$ ($p < 1e^{-12}$). Finally, the spatial score reaches its half time later, at 4% of the training, and converges to $R=0.4$ ($p < 1e^{-6}$). We reproduce the spatial score using the value of each ROI along the sensory-to-transmodal gradient map from (Margulies et al., 2016) instead of the euclidean distance of this ROI from V1, see Supplementary Figure S6. We obtain a similar increase across training from -0.32 to 0.13 (1st to last checkpoint).

Generalization to multiple architectures. Across seven vision models with diverse architectures – CNNs, supervised ViTs, vision-language contrastive transformers, etc.), trained models consistently show higher encoding, spatial, and temporal scores than untrained models. Additionally, trained models tend to show convergent encoding, spatial, and temporal scores, whereas scores from untrained models vary more widely – likely reflecting differences in their inductive biases. These additional analyses are reported in S1,S2,S3,S4,S5, comparing trained and untrained versions of all models.

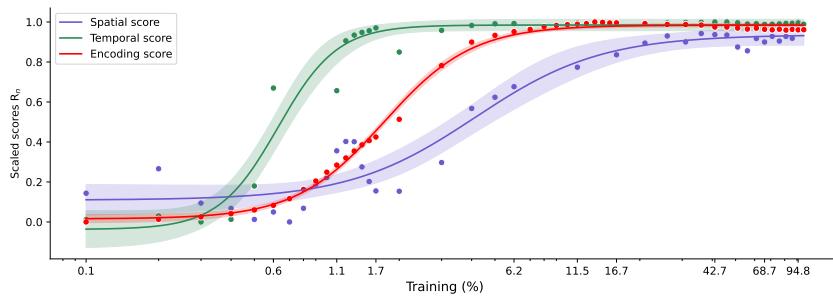


Figure 3: **Evolution of scaled temporal, encoding and spatial scores as a function of DINOv3’s training.** The Evolution of these unscaled metrics is presented in Supplementary Fig. S7.

Are these developmental trajectories identical across temporal and brain regions of interest? To address this issue, we evaluate the same analyses on specific regions or temporal windows of interest. Functional MRI results show that low-level visual regions (e.g. V1, V2) are marked by lower half times of the last layer than high-level prefrontal cortices (e.g. IFSp, IFSa), Fig 4A,C,E. The correlation between half time and anatomical location (coarsely defined as the Euclidean distance to V1) is $R=0.91$, $p < 1e^{-5}$. Similarly for MEG, earlier windows (e.g. <200 ms) are marked by lower half

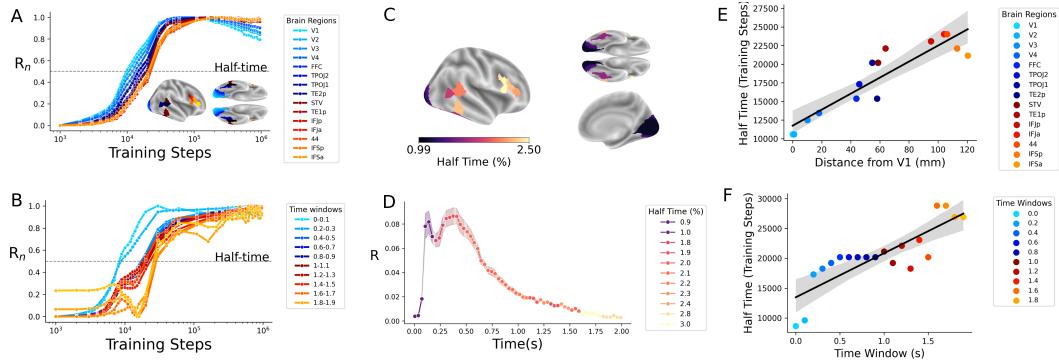


Figure 4: Emergence of brain-like representations. **A.** Normalized brain encoding scores of layer 1 as a function of training for each brain ROI. The dashed line indicates the 50% of the maximum encoding score for each region. **B.** Same as A for MEG time regions of interest (tROIs). **C.** Half time for each brain ROI. **D.** Half time for each time ROI. **E.** Correlation between half time of encoding score across training, and distance of each ROI from V1. **F.** Correlation between half time of encoding score across training, and time position of the encoded cognitive process (tROI).

times than late time windows (e.g. $>1,500$ ms), Fig 4B,D,F. The correlation between half time and temporal peak is $R=0.84$, $p < 1e^{-5}$.

Overall, these results show that the brain responses of the sensory and prefrontal cortices contain representations of images that are acquired early and late in the training of DINOv3, respectively.

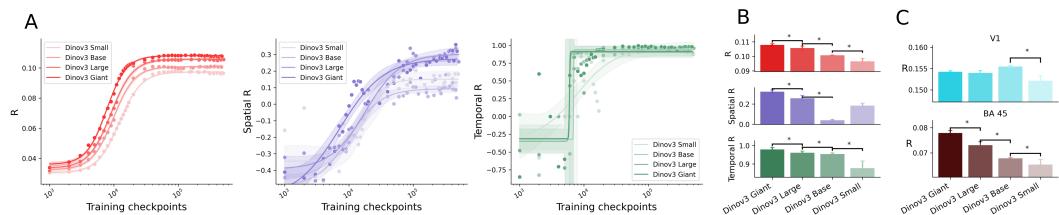


Figure 5: Impact of model size. For inter-model comparisons, significance to $p < 1e^{-3}$ are represented by asterisks *. **A.** Encoding (reds), spatial (purples), and temporal scores (greens) as a function of training and model size. Logarithmic fits of scores across training. **B.** Scores on the final $k=4e^5$ training step. **C.** Encoding scores for V1 and Brodmann area 45 at the end of training.

Impact of model size. How does model size impact convergence? DINO models of larger scale appear to converge quicker and encode higher-level ROIs more accurately. Model size consistently leads to bigger encoding scores at the end of training ($R_{\text{Giant}} = 0.107 > R_{\text{Large}} = 0.105 > R_{\text{Base}} = 0.101 > R_{\text{Small}} = 0.096$ with $p < 1e^{-3}$). Similar, although noisier phenomena can be observed for spatial scores and temporal scores ($p < 1e^{-3}$), Fig 5A, B. Does model size impact encoding scores similarly across ROIs? Applying the same analysis for each ROI separately shows that model size primarily increases encoding of higher-level cortices like BA45 and IFS as compared to visual cortices like V1, V2. All models present this size-dependent increased encoding significantly in higher-ROIs, only the smallest ones in V1, V2 ($p < 1e^{-3}$) (Fig 5C, see Fig S10 for all studied ROIs).

Impact of image type. To assess how image types influence the development of brain-like representations in a model, we train, from scratch, three distinct DINO models, each using one of three

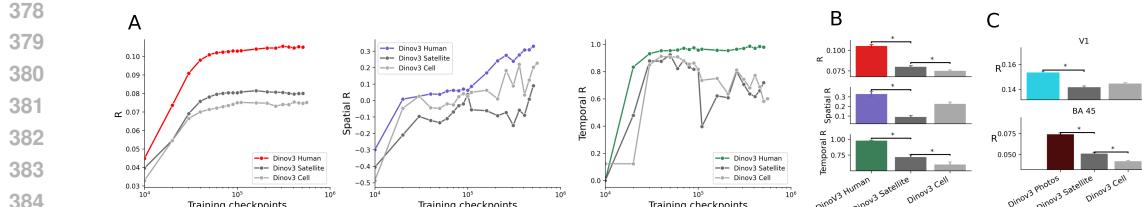


Figure 6: **Impact of image type.** For inter-model comparisons, significance to $p < 1e^{-3}$ are represented by asterisks *. **A.** Encoding (reds), spatial (purples), and temporal scores (greens) as a function of training and image type. **B.** Scores on the final $k=4e^5$ training step. **C.** Encoding scores for V1 and Brodmann area 45 at the end of training.

natural images datasets: satellite images, cell images and classic (human-centric) images. We focus on a single DINOv3 architecture (Dino Large), with a fixed training length and training data quantity (10M images) and data type as the only varying factor. Training improves encoding scores, spatial scores and temporal scores for all image types (Fig 6A), suggesting that these models learn visual features that are universal across these different types of natural images. However, these brain-similarity metrics are lower for satellite and cell images than for human centric images, for encoding, spatial and temporal scores (Fig 6A, B). Interestingly, this difference is observed across all studied regions of interest: e.g. both V1 ($p < 1e^{-3}$) and BA45 ($p < 1e^{-3}$) are better encoded by a model trained with human centric photos than other models (Fig 6C), see S11 for results on all studied ROIs. At the end of training, DINO human reaches a significantly higher performance regarding encoding, temporal and spatial scores ($p < 1e^{-3}$), Fig 6B. These results might unravel from the fact that human centric images reflect visual input that humans are exposed to, whereas satellite images and cell images are images that human brains have not been trained to process.

3.3 LINK TO CORTICAL PROPERTIES

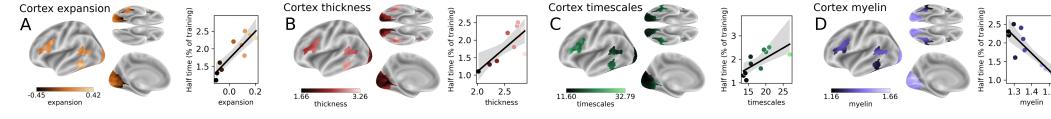


Figure 7: **Relation between shared representations and cortical properties.** **A.** Left. Cortical expansion index, as estimated from the difference between adults and infants' brains, for each ROI (Hill et al., 2010). Right. Correlation between cortical expansion and half time. Each dot is an ROI. **B.** Same as A for cortical thickness, as estimated from (Van Essen et al., 2013). **C.** Same as A for cortical time scales, as estimated from MEG source reconstruction in (Shafiei et al., 2021). **D.** Same as A for myelin concentration, as estimated from (Van Essen et al., 2013).

Is the development of brain-like representations predicted by functional, structural and developmental properties of the cortex? To explore this issue, we evaluate the correlation between the representational half time of encoding and four properties of the cortex.

Cortical expansion. First, we focus on the developmental expansion of cortical regions. Using an atlas comparing infant and adult cortical structures (Hill et al., 2010), we found a strong positive correlation ($R=0.88$, $p < 1e^{-3}$) between half time and cortical expansion (Fig 7A). This indicates that cortical areas marked by greater developmental growth are also those whose representations emerge later in the AI model.

Cortical thickness. Second, we assess the correspondence with cortical thickness, utilizing HCP S12000 estimates. Our results show a significant correlation ($R=0.77$, $p < 1e^{-2}$), suggesting that cortical areas with larger cortical sheets exhibit longer half times (Fig 7B).

Cortical dynamics. Third, the areas with the slowest intrinsic dynamics, as estimated from a source-reconstruction of MEG activity, are also those that tend to have the longest half times ($R=0.71$, $p = .022$). This result directly echoes our MEG results (Fig 2), whereby deeper layers of DINOv3 tend to be associated with slower brain responses (Fig 7C).

Cortical myelin. Finally, this dynamic property appears linked to myelin concentration (Van Essen

432 et al., 2013). Myelin, which facilitates faster neuronal transmission, demonstrated a strong negative
 433 correlation with half time ($R=-0.85$, $p\text{-val} = 1e^{-3}$). This implies that higher myelin concentration is
 434 associated with shorter half times (Fig 7D).

435 In summary, these findings demonstrate a strong predictive relationship between the speed at which
 436 brain-like representations emerge in AI models and various structural and functional characteristics
 437 of the cortex, across development and once developed.

438

439 4 DISCUSSION

440

441 **Main findings.** Understanding why artificial neural networks develop representations that resem-
 442 ble those in the human brain remains a fundamental challenge to neuroscience and AI (Huh et al.,
 443 2024; Hasson et al., 2020; Shen et al., 2025; Caucheteux & King, 2022). While recent studies have
 444 documented brain–model similarities across a wide range of architectures and training paradigms
 445 (Wang et al., 2023; Conwell et al., 2022), the exact factors that cause this convergence and their
 446 interactions remain unclear. Here, we independently manipulate three factors – model size (from
 447 DINOv3 small to giant), training length (from 0 to $1e^7$ steps on several training sets of 10M and
 448 of 1.7B images) and image type (human-centric, satellite images and biological images) to test how
 449 each of them contributes to the emergence of brain-like representations of natural images. Our find-
 450 ings demonstrate that these three factors all independently and interactively impact the extent to
 451 which a self supervised model converges to brain-like visual processing. **Results show that size,**
 452 **training duration, and data type each shape the emergence of brain-like representations but also**
 453 **brain-like hierarchies, measured through spatial and temporal scores.** Representations, temporal and
 454 spatial hierarchies all emerge – though at different pace across training. When comparing untrained
 455 and trained versions of seven diversified vision models, we find that the vast majority of them consis-
 456 tently develop qualitatively similar encoding, spatial and temporal scores as DINOv3. Our analyses
 457 complement prior work examining only convergence between multiple models (Huh et al., 2024),
 458 demonstrating that this convergence also extends onto human neural representations. Finally, we find
 459 that the emergence of brain-like properties during training follows the developmental maturation of
 460 the human cortex from birth through early adulthood. Although these developmental trajectories
 461 have not been tested in other models, the convergence of encoding, spatial, and temporal scores
 462 for eight diversified vision models may suggest that these additional results regarding DINOv3 are
 463 generalizable to other models. Future research will allow to test this hypothesis.

464

Nativism and empiricism. In particular, the model–brain similarity increases consistently with
 465 larger DINOv3 architectures, longer training, and more ecologically valid data. These results are
 466 consistent with an increasing set of studies showing linearly aligned representations of natural im-
 467 ages (Yamins et al., 2014b; Kriegeskorte, 2015; Schrimpf et al., 2018; Tang et al., 2025; Thobani
 468 et al., 2025), with a hierarchy that maps the functional organization of the visual cortices (Eicken-
 469 berg et al., 2017; La Tour et al., 2022), and dynamics that reflect the ordering of the model’s layers
 470 (Seeliger et al., 2018; Cichy et al., 2016). In addition to its factorial disentanglement, our study
 provides additional contributions.

471

First, this model–brain alignment is not confined to the visual pathways (Eickenberg et al., 2017;
 472 Schrimpf et al., 2018; Tang et al., 2025) but extends into high-level – multi-modal – regions of
 473 the cortex, including the prefrontal cortex (although see e.g. Solomon et al. (2024) for a low-
 474 dimensional set of image features identified in the prefrontal lobe).

475

Second, our independent manipulation of model size, training duration, and data type further show
 476 how these factors *interact* with one another: the largest architectures best align with brain activity
 477 as (1) they get trained and (2) on ecologically-relevant naturalistic images.

478

Third, even non-human-centric datasets (satellite images, biological images) support partial con-
 479 vergence in early visual areas, implying that low-level statistics shared across environments are
 480 sufficient to bootstrap early representations. **Our findings indicate that models trained on human-**
 481 **centric images still tend to develop representations that more closely resemble those of the human**
 482 **visual system.** However, it remains unclear whether this advantage reflects low-level image statis-
 483 **tics (e.g., natural color and texture distributions) or higher-level semantic properties typical of hu-**
 484 **man experience.** Additionally, it remains unclear whether this higher alignment for human-centric
 485 dataset is driven by a distribution of images more similar to the one in the training data of DINOv3.
 Distinguishing between these factors will require future research, for example by evaluating brain

486 responses from participants watching controlled non-human centric images. Overall, these results
 487 suggest that while the architecture supplies a potential, the data remain critical in making these
 488 systems learn representations that are similar to the brain. This interaction between architectures,
 489 training and data provides an empirical framework to the long-standing debates in cognitive science
 490 on nativism versus empiricism, – showing how ‘innate’ and ‘experiential’ interact with one another
 491 in the development of cognition.

492 **Towards a model of the visual cortex ontogeny.** This model-brain alignment follows a surprisingly
 493 steady developmental trajectory. Early in training, the models rapidly acquire representations
 494 that align with the fast and low-level visual responses of the sensory cortices. In contrast, the emergence
 495 of slow and high-level representations – particularly those aligning with the prefrontal cortex
 496 – appears to require both far more training data.

497 This developmental trajectory echoes the biological development of the human cortex: the brain
 498 areas with which the AI models align last during their training are precisely those with the greatest
 499 cortical thickness, slower intrinsic timescales, prolonged maturation, and lower levels of myelination
 500 – i.e. the areas of the associative cortices that are known to slowly develop throughout the first two
 501 decades of life (Dehaene, 2021). This result suggests that the sequential acquisition of representations
 502 in artificial neural networks may spontaneously model some of the developmental trajectories
 503 of brain functions. In doing so, they may ultimately provide a new computational framework to
 504 understand the staged maturation of visual processing in biological systems (Vogelsang et al., 2024;
 505 Zaadnoordijk et al., 2022; Long et al., 2024).

506 **Open questions.** Several results were not anticipated. First, the temporal score, encoding score and
 507 spatial score do not appear to emerge simultaneously – hence leading to the novel question of why
 508 these metrics follow this specific order. The factors that lead the temporal score to emerge are not
 509 entirely clear. However, the temporal score rises before the encoding score 3, suggesting that the
 510 encoding score alone does not solely explain the temporal score. Second, the spatial and temporal
 511 scores are initially negative (respectively significantly, $p = 0.05$, and non-significantly, $p > 0.05$) at
 512 the beginning of model training. This means that the deepest layers of a random DINOv3 tend to best
 513 predict fast and low-level brain responses at the very early (but not late) stages of training. Finally,
 514 the half times of these three metrics are reached in between 1% and 4% – i.e. only $n=1.6B$ images –
 515 of DINOv3 training quantity. This suggests that while low-level brain-like representations are very
 516 quickly learnable, the high-level representations of the brain require a very large amount of data to
 be fully acquired.

517 **Limitations.** While this study offers a controlled analysis of brain–model convergence, several
 518 limitations warrant consideration. First, our findings are based exclusively on a single family of
 519 self-supervised vision models (DINOv3), which are hierarchical by design. It thus remains an open
 520 question whether similar spatial, temporal and encoding scores would emerge with other architectures
 521 and training objectives (Conwell et al., 2021). Second, fMRI and MEG offer limited resolution
 522 and thus provide coarse population-level brain activity and may overlook fine-grained neural mechanisms.
 523 Third, our analyses focus solely on the adult brain, leaving open the question of how these
 524 alignments emerge across development. Understanding when these correspondences arise will require
 525 data from infants, children, or longitudinal cohorts (Evanson et al., 2025). Additionally, we
 526 analyze two datasets where participants watched images most often passively: future work should
 527 assess how different tasks modulate the alignment between DINOv3 and the prefrontal cortex. Future
 528 research should also extend this systematic exploration to additional factors driving brain-like
 529 convergence, as well as to the interactive effects between all of them. Finally, while we quantify
 530 the similarity between representations from models and the brain, the exact nature and semantic
 531 structure of these neuronal representations continues to be a subject of intense ongoing research
 532 (Gifford et al., 2025; Graumann et al., 2022). Closing this interpretability gap certainly remains a
 major challenge to both neuroscience and AI.

533 **Conclusion.** Beyond the characterization of the spontaneous convergence between AI models and
 534 brains, these findings chart a path toward using AI models as tools to investigate the organizing
 535 principles of biological vision in the human brain. By showing how machines can come to see like
 536 us, our findings provide cues as to how the human brain may come to see the world.

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540 **A REPRODUCIBILITY STATEMENT**
541542 The paper is based on an open-source MEG dataset (Hebart et al., 2023a) and an open-source fMRI
543 dataset (Allen et al., 2022), as well as several open-source vision models (versions of DINOv3
544 (Siméoni et al., 2025)). These models and datasets are cited in the Introduction and the Methods
545 sections. Regarding the comparative trainings, the satellite and human-centric datasets are currently
546 proprietary, whereas the cellular dataset is a collection of open-source datasets (Lorenci et al.,
547 2025). Linear decoding code is available at:548 <https://mne.tools/stable/generated/mne.decoding.SlidingEstimator.html>.
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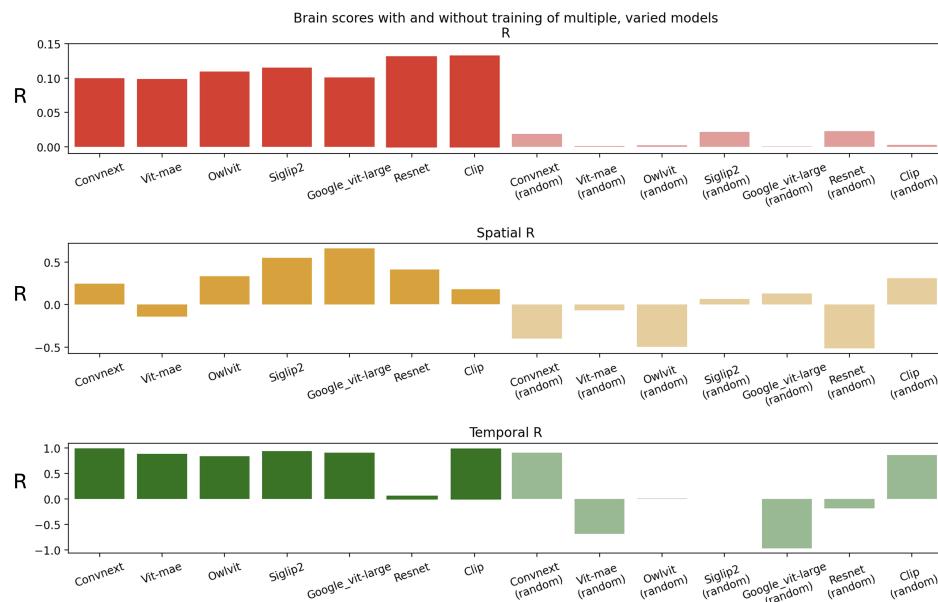
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864 **B APPENDIX**

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Figure S1: **Encoding, spatial and temporal scores reproduced for a range of seven vision models** with varying architectures and training objectives - including CNNs (ResNet-50, ConvNeXt-Large), a self-supervised ViT with different objective than DINOv3 (ViT-MAE, masked image reconstruction), a supervised ViT (ViT-L/16), and vision–language contrastive transformers (CLIP, SigLIP2, OWL-ViT).

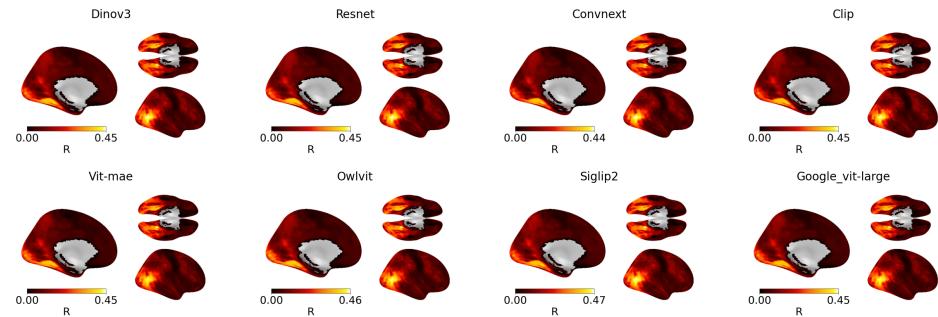
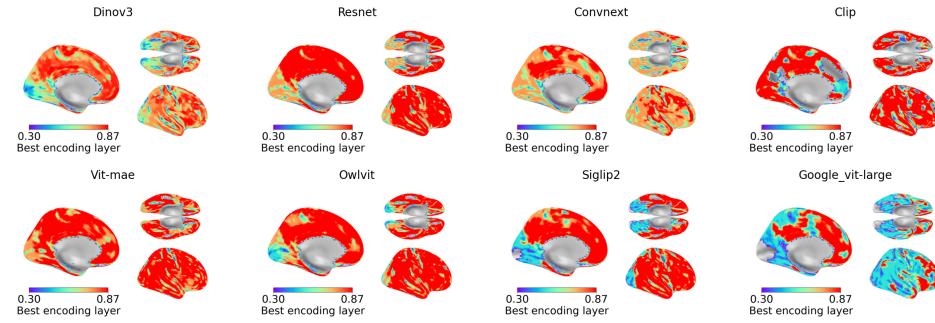
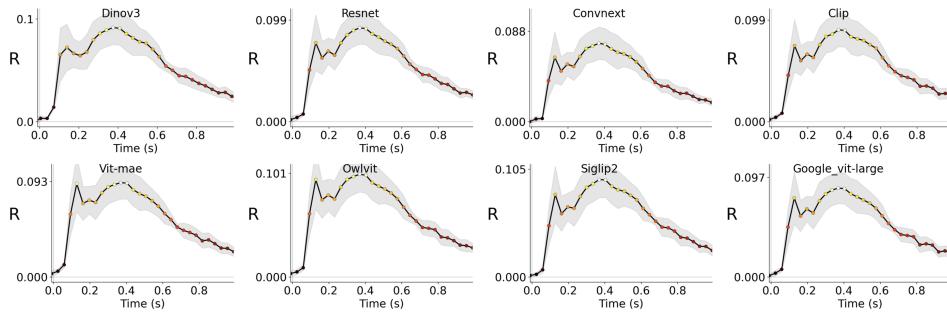
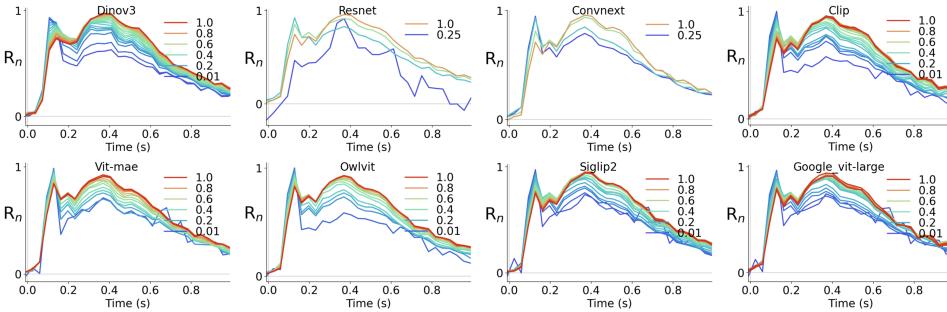


Figure S2: **Encoding scores across cortex, reproduced for a range of seven vision models** with varying architectures and training objectives – including CNNs (ResNet-50, ConvNeXt-Large), a self-supervised ViT with different objective than DINOv3 (ViT-MAE, masked image reconstruction), a supervised ViT (ViT-L/16), and vision–language contrastive transformers (CLIP, SigLIP2, OWL-ViT).

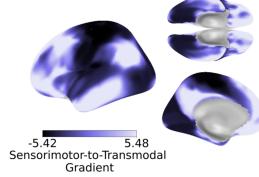
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Figure S3: **Maximally encoding layers across cortex, reproduced for a range of seven vision models** with varying architectures and training objectives – including CNNs (ResNet-50, ConvNeXt-Large), a self-supervised ViT with different objective than DINOv3 (ViT-MAE, masked image reconstruction), a supervised ViT (ViT-L/16), and vision–language contrastive transformers (CLIP, SigLIP2, OWL-ViT).938
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Figure S4: **Encoding scores along time, reproduced for a range of seven vision models** with varying architectures and training objectives – including CNNs (ResNet-50, ConvNeXt-Large), a self-supervised ViT with different objective than DINOv3 (ViT-MAE, masked image reconstruction), a supervised ViT (ViT-L/16), and vision–language contrastive transformers (CLIP, SigLIP2, OWL-ViT).956
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Figure S5: **Encoding scores for each layer along time, reproduced for a range of seven vision models** with varying architectures and training objectives - including CNNs (ResNet-50, ConvNeXt-Large), a self-supervised ViT with different objective than DINOv3 (ViT-MAE, masked image reconstruction), a supervised ViT (ViT-L/16), and vision–language contrastive transformers (CLIP, SigLIP2, OWL-ViT).

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Alternative spatial score computed along
cortex connectivity,
along ROIs



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Figure S6: **Alternative spatial score along the sensory-to-transmodal gradient.** Partial reproduction of the spatial scores results obtained on DINOv3 using the value of each ROI along the sensory-to-transmodal gradient map (Margulies et al., 2016) instead of the euclidean distance of this ROI from V1. We obtain a similar increase across training from -0.32 to 0.13 (1st to last checkpoint).

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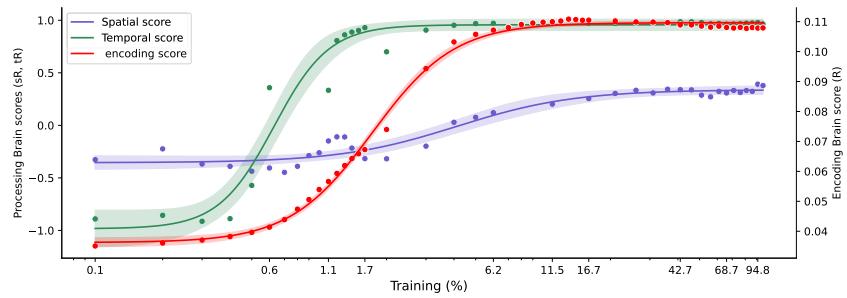


Figure S7: **Evolution of temporal, encoding and spatial scores as a function of DINOv3’s training.**

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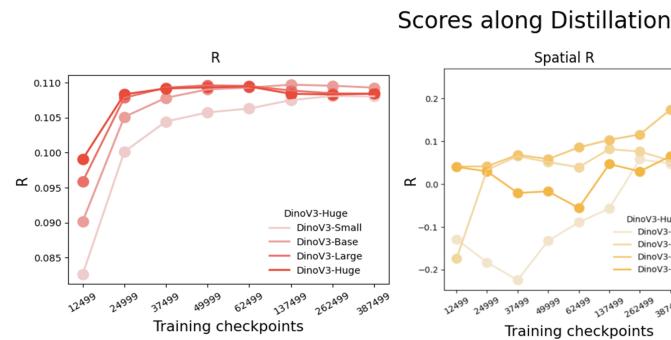
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Figure S8: **Impact of model size along distillation for DINOv3-Small, Base, Large and Huge.** Encoding (reds), spatial (yellow), and temporal scores (greens) as a function of training and model size.



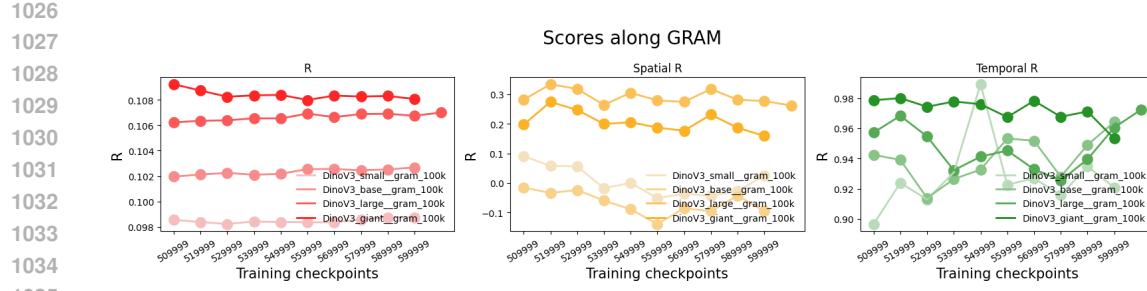


Figure S9: **Impact of model size along GRAM anchoring for DINOv3-Small, Base, Large and Huge.** Encoding (reds), spatial (yellow), and temporal scores (greens) as a function of GRAM anchoring and model size, for models trained from scratch.

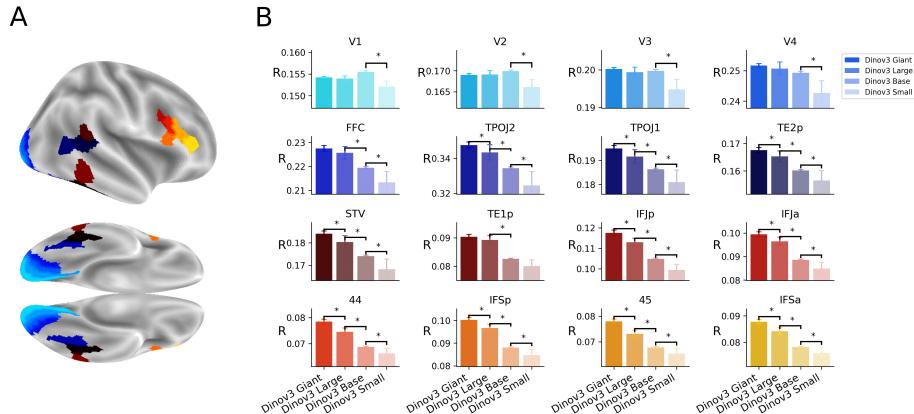


Figure S10: **Impact of model size for multiple ROIs.** For inter-model comparisons, significance to $p < 1e^{-3}$ are represented by asterisks *. **A.** Brain ROIs. **B.** Encoding scores for each ROI at the end of training.

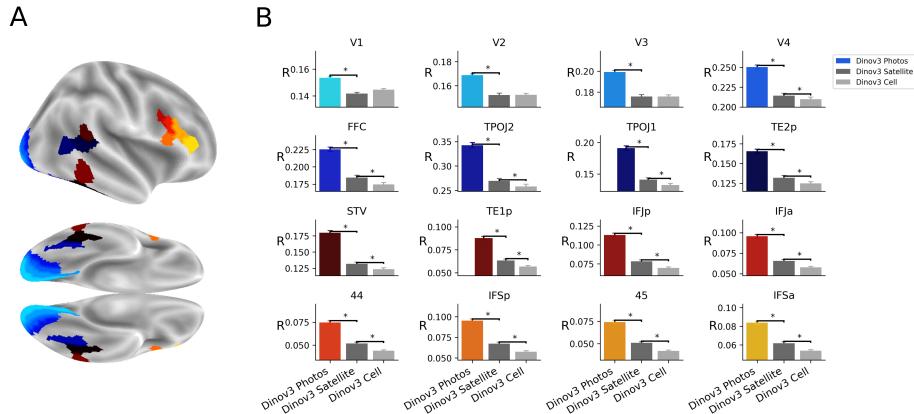


Figure S11: **Impact of image type for multiple ROIs.** For inter-model comparisons, significance to $p < 1e^{-3}$ are represented by asterisks *. **A.** Brain ROIs. **B.** Encoding scores for each ROI at the end of training.

1080 **C ETHICS STATEMENT**
10811082 Among the three datasets this study leverages, only the human-centric dataset is constituted from
1083 images from the web and imageNet; each of these images went through platform-level content
1084 moderation to prevent any harmful contents (Siméoni et al., 2025).1085 The present paper uses two datasets regarding research with human subjects, both these datasets have
1086 already been published, are open-source and cited in the paper. These open-source recordings were
1087 collected after participants' informed consent and were validated by the corresponding Institutional
1088 Review Boards.1089 **D LLM USE**
10901091 An LLM was used in preparing this manuscript, exclusively for proofreading purposes: typos, gram-
1092 mar, and in a few instances to search for improved sentence formulations.
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