
Towards Explainable Segmentation of Complex Boundaries in Lung Nodule Detection

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Abstract

Many deep learning models are computationally expensive while capturing complex edges in tasks such as lung nodule segmentation from 2D CT scans. Also, the lack of explainability hinders their adoption for clinical use. To address these challenges, this work proposes a Sobel-enhanced edge-aware powered U-Net architecture capable of emphasising the edges of nodules in lung computed tomography images. The model is trained and evaluated on the benchmark LIDC-IDRI dataset. To provide interpretability, four post hoc explainers were employed: Grad-CAM, Score-CAM, Layer-CAM, and Counterfactual explainability. The proposed model achieved competitive performance across several metrics, including accuracy, dice score, intersection over Union, sensitivity, and specificity, when compared with three baseline models—U-Net, ResUnet++, and U-Net++. Although it has slightly more parameters (3.4 million) than the U-Net (3.3 million), its ability to identify complex edges of lung nodules makes it stand out. Moreover, the four explainers effectively generated heatmaps that highlight the detected edges. The proposed model delivers competitive segmentation performance with improved edge detection and explainability, highlighting its potential for clinical deployment.

1 Introduction

Lung cancer is the second most common cancer worldwide, with more than 230,000 new cases annually (10). It is one of the major causes of cancer deaths worldwide, making early detection of lung nodules very important. Lung nodules are small growths in the lungs that can be harmless or cancerous. Computed Tomography (CT) scans can spot these nodules, but accurate segmentation—measuring their size, shape, and position—is key. This helps doctors tell if a nodule is benign or malignant and plan the right treatment, especially for cancer cases where staging and therapy choice depend on precise segmentation (1). Several AI developments have been done to precisely segment nodules from CT scan images. Bian et al. (4) proposed a dynamic multiscale weight optimisation network for getting spatial features inside CT scan images. Zhang et al.(19) introduced a multitask learning where a U-Net-based segmentation and a ResNet for classification. To improve the segmentation, feedback is performed on the classification result. Santone et al. (14) proposed a real time YOLO based model for segmentation. This model could capture small nodules properly. Hajim et al.

(3) developed SEDARU-Net, a Squeeze-Excitation Dilated Attention-based Residual U-Net with intensity normalisation and YOLOv3 preprocessing, to improve lung nodule segmentation across diverse types and sizes, achieving high accuracy on the LUNA16 dataset. Agnes et al. (1) proposed a modified swinUnet where a Canny edge detector is used to highlight edges. However, the edge detector is used in the input image and aggregated with the final feature maps from swinUnet. So, the impact of the module is not very significant. Hou et al. (8) also used an attention mechanism to give importance to nodule edges, but the model is computationally expensive.

Although advancements have been made, several limitations remain: significant computational overhead, insufficient attention to refining nodule edges, and a lack of focus on segmentation model explainability.

To address these issues, a modified U-Net–based, edge-aware, Sobel-integrated model is proposed. This model demonstrated competitive performance compared to three baseline models and other state-of-the-art architectures. Furthermore, four XAI techniques were applied to enhance the trustworthiness of the model.

2 Method

This research begins with data acquisition, followed by preprocessing and data splitting, then proceeds with model training and testing using various evaluation metrics, and finally examines model transparency through several XAI techniques.

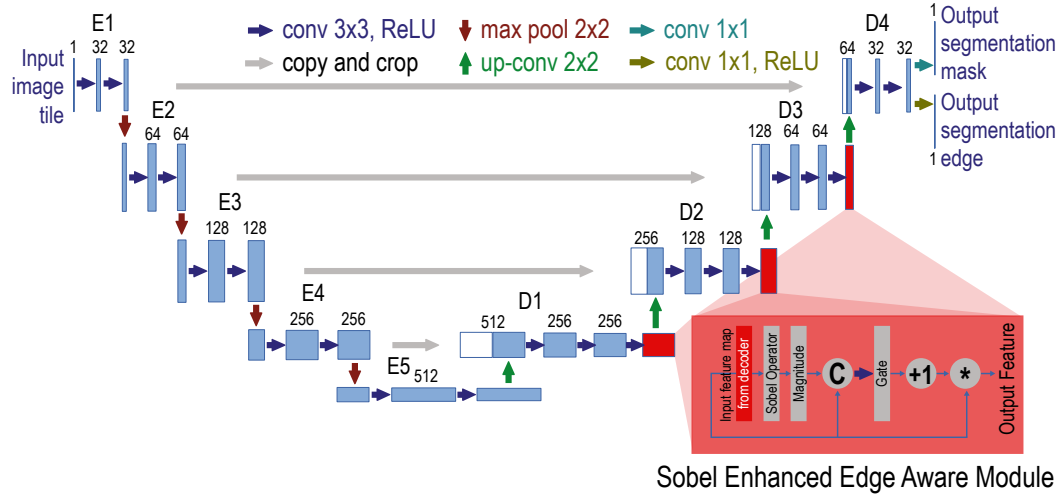


Figure 1: Modified U-Net with encoder (E1–E5), bottleneck (E5), and decoder (D1–D5). Each decoder output passes through an edge-aware block using Sobel (S), magnitude, concatenation (C), and gating, producing upsampled features for the final mask and edge prediction.

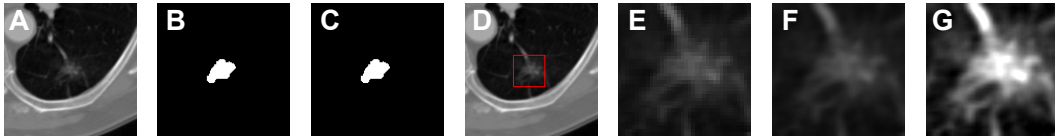


Figure 2: The Preprocessing pipeline: (a) Original grayscale, (b) Mask, (c) Binarised, (d) Nodule-centred square crop, (e) Cropped, (f) Resized 256×256, (g) Percentile clipping 2–98%.

The LIDC-IDRI dataset was used. The 2D slices with masks annotated by four radiologists were provided, and the dataset was collected from Kaggle, which contains some empty masks. After excluding empty masks, one valid image–mask pair was randomly selected per case, yielding 15,548 nodules from 875 patients. Each slice was converted to grayscale, masks were binarised, and lesion-centred crops with margins were resized to 256×256 (bilinear for images, nearest-neighbour for masks). Intensities were percentile-clipped to [0,1] for normalization. The dataset was split into five

folds for cross-validation, with each fold containing about 175 patients, ensuring fair and unbiased evaluation. Figure 2 gives each preprocessing output of the dataset.

2.1 Proposed Model Architecture

Figure 1 shows the proposed model architecture and edge aware module . The proposed model is an **edge-aware U-Net** that consists of three main parts: an encoder, a bottleneck, and a decoder augmented with Sobel Edge Attention (SEA) modules.

The encoder extracts hierarchical features from the input image while progressively reducing the spatial resolution. At each stage, the feature maps are downsampled using max-pooling and refined by a DoubleConv block (two successive Conv–BN–ReLU operations), i.e., $E_{\ell+1} = \phi(\text{BN}(W_{\ell,2} * \phi(\text{BN}(W_{\ell,1} * \text{Pool}(E_{\ell}))))$, where E_{ℓ} is the feature map at stage ℓ , Pool denotes 2×2 max pooling, BN is batch normalization, $*$ is convolution, and ϕ is the ReLU activation.

At the lowest resolution, the bottleneck captures global semantic context as $B = \phi(\text{BN}(W_{b,2} * \phi(\text{BN}(W_{b,1} * E_L))))$, where E_L is the last encoder feature.

The decoder restores spatial detail by progressively upsampling features, concatenating them with corresponding encoder skip connections, and applying DoubleConv blocks, i.e., $\hat{D}_k = \text{Up}(D_{k+1})$, $U_k = [\hat{D}_k, E_k]$, $F_k = \phi(\text{BN}(W_{k,2} * \phi(\text{BN}(W_{k,1} * U_k))))$.

Each decoder stage is followed by an SEA module, which emphasizes boundary information. For a feature map F , Sobel filters S_x, S_y (7) are applied channel-wise to compute gradient magnitude $M^c = \sqrt{(F^c * S_x)^2 + (F^c * S_y)^2}$, and a learned gate $G = \sigma(W_g * [F, M])$ is predicted to boost edge regions, producing $D = F \odot (1 + G)$.

Finally, the last decoder output D_4 is fed into two heads: a 1×1 convolution for segmentation logits $\hat{Y}$, and an auxiliary edge head for edge logits $\hat{E}$.

2.1.1 Loss Function

The architecture is trained with a multi-task loss that supervises both the segmentation and edge predictions. The segmentation branch is optimized with a combination of weighted binary cross-entropy and Dice loss (6), $\mathcal{L}_{\text{seg}} = \text{BCE}(\sigma(\hat{Y}), y) + 0.5 \times (1 - \frac{2 \sum (p \cdot y)}{\sum p + \sum y + \epsilon})$, where $p = \sigma(\hat{Y})$ are predicted probabilities and y is the ground-truth mask. The auxiliary edge branch is supervised with binary cross-entropy against boundary labels y_{edge} , i.e., $\mathcal{L}_{\text{edge}} = \text{BCE}(\sigma(\hat{E}), y_{\text{edge}})$.

The total objective combines both segmentation and edge terms as

$$\mathcal{L}_{\text{total}} = \mathcal{L}_{\text{seg}} + \lambda_{\text{edge}} \mathcal{L}_{\text{edge}}, \quad (1)$$

where λ_{edge} controls the contribution of the edge loss. The effect of varying λ_{edge} is analyzed through an ablation study, as shown in Table 3.

so that the decoder is guided to predict accurate nodule regions while the edge branch and SEA modules are explicitly supervised to sharpen boundary localization.

2.2 Experimental Settings, Evaluation Metrics and Explainability

Training used a batch size of 8, for 60 epochs with patience 10, optimized with AdamW (lr 1e-3, weight decay 1e-5, betas 0.9/0.999, eps 1e-8). The model had 32 base channels and ran on an NVIDIA RTX 3090 GPU. The models' results are evaluated by six metrics: Dice score (DSC), Intersection over union (IoU), Accuracy, Sensitivity, Specificity and Harmonic Mean (12). Four XAI techniques: Grad-CAM (15), Score-CAM (17), Layer-CAM and Counterfactual-XAI (11) are used to highlight regions that were used for edge prediction. The source code is available at: <https://github.com/brai-acslab/edge-aware-unet>.

3 Results and Discussion

Table 1 compares our model with three baselines. It outperforms others in all metrics except specificity and IoU. While accuracy matches UNet++ (0.90), our model has a much lower standard deviation (0.005 vs. 0.24), indicating stronger generalizability. Table 2 compares the computational efficiency of different models. The proposed model achieves a balanced trade-off between speed and

Table 1: Comparison of segmentation performance across models (Mean $\pm$ Std).

Model	DSC	IoU	Accuracy	Sensitivity	Specificity	Harmonic Mean
U-Net	0.81 $\pm$ 0.33	0.78 $\pm$ 0.31	0.83 $\pm$ 0.39	0.79 $\pm$ 0.35	0.92 $\pm$ 0.22	0.85 $\pm$ 0.26
ResUNet++	0.86 $\pm$ 0.41	0.75 $\pm$ 0.51	0.83 $\pm$ 0.31	0.72 $\pm$ 0.37	0.95 $\pm$ 0.29	0.82 $\pm$ 0.33
U-Net++	0.88 $\pm$ 0.27	0.79 $\pm$ 0.31	0.90 $\pm$ 0.24	0.87 $\pm$ 0.27	0.94 $\pm$ 0.21	0.90 $\pm$ 0.24
Proposed	0.90 $\pm$ 0.005	0.74 $\pm$ 0.006	0.90 $\pm$ 0.005	0.92 $\pm$ 0.017	0.89 $\pm$ 0.014	0.90 $\pm$ 0.015

Table 2: Comparison of model complexity (batch size = 1) on an RTX 3090 for image size of 256×256 .

Model	Params (M)	GFLOPs	Latency(ms / image)
UNet	3.35	15.59	2.18
UNet++	6.21	66.82	5.02
ResUNet++	4.17	27.13	3.87
Proposed	3.40	17.29	3.41

complexity—requiring only 3.4 M parameters and 17.3 GFLOPs, with an inference time of 3.41 ms per image. This makes it nearly as lightweight as U-Net but substantially faster and more efficient than U-Net++ and ResUNet++.

Table 3: Ablation study of the loss function for a single fold by changing the coefficient λ_{edge} of the edge loss in Eq. 1.

λ	Accuracy	Dice	IoU	Sensitivity	Specificity	Harmonic Mean
0.25	0.8894	0.8384	0.7218	0.9507	0.8629	0.9045
0.50	0.9034	0.8508	0.7403	0.9123	0.8995	0.9059
0.75	0.8859	0.8361	0.7184	0.9639	0.8522	0.9058
1.00	0.8989	0.8485	0.7368	0.9375	0.8822	0.9094

Table 3 presents the ablation study on the edge-loss weighting coefficient λ_{edge} . The results show that setting $\lambda = 0.5$ yields the best overall balance across all metrics, achieving the highest Accuracy, Dice, IoU, and Specificity. Lower or higher values of λ either overemphasize edge information or reduce its influence, slightly degrading segmentation quality. Thus, $\lambda = 0.5$ was selected as the optimal configuration for the proposed model.

Table 4: Comparison of segmentation performance across different SOTA.

Method	DSC	IoU	Accuracy	Sensitivity	Specificity
Agnes et al (2)	—	—	—	0.726	—
Kido et al. (9)	—	—	—	0.738	—
Usman et al. (16)	—	—	—	—	—
SAR-UNet (18)	0.8846	0.8971	0.8760	0.8745	0.8810
Attention-UNet (13)	0.9190	0.9179	0.9071	0.9063	0.9190
Swin-UNet (5)	0.8674	0.8697	0.8518	0.8501	0.8670
Proposed	0.90	0.74	0.90	0.92	0.89

Table 4 presents the performance comparison with other state-of-the-art architectures. Our model outperforms all others across all metrics, except for Attention U-Net (13), which is only about 1% higher. However, Attention U-Net requires substantially more computational resources, whereas our model is a simple modified U-Net, demonstrating superior computational efficiency.

3.1 Intrepretability

Figure 3 illustrates the predicted edges, segmentation masks, and heatmaps generated by four XAI techniques. Grad-CAM clearly highlights the nodule boundaries, with Score-CAM and Layer-CAM showing similar emphasis on edge regions. Counterfactual-XAI, despite slight perturbations in the input, produced stable edge predictions, underscoring the model’s transparency and robustness.

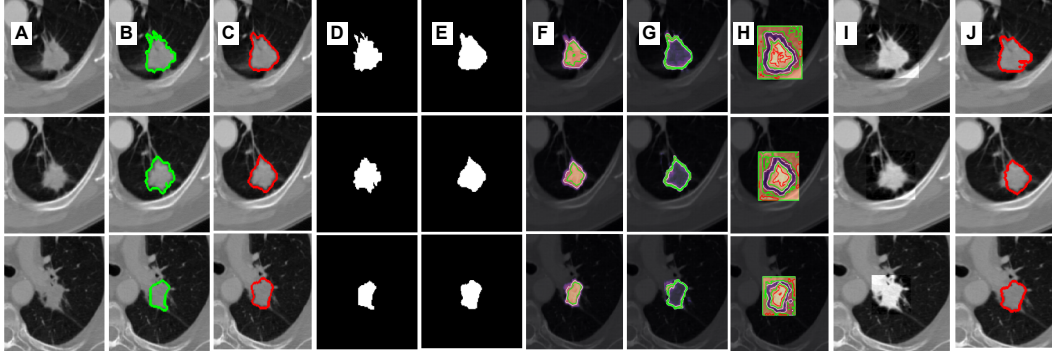


Figure 3: Heatmap generation of all XAI techniques: (a) Raw image, (b) GT edges, (c) Predicted edges, (d) GT mask, (e) Predicted mask, (f) Grad-CAM, (g) Layer-CAM, (h) Score-CAM, (i) Counterfactual image, (j) Counterfactual predicted edges.

4 Limitations and Future Work

Although this work is effective and explainable, there are several limitations: the dataset was already 2D-sliced. The actual 3D images can give more insight. Moreover, there are other metrics which were not used for the evaluation. Based on the explanations from XAI techniques, the model is not retrained to improve performance. Traditional Unet is simple; adding an edge-aware module to other powerful segmentation models, like transformers, can be more effective. Moreover, future work will focus on incorporating zero-shot and fine-tuned predictions using large foundation models to enhance generalization and diagnostic robustness .

5 Conclusion

The presented research demonstrates that the proposed model can accurately predict both segmentation masks and nodule edges from CT scans. Despite its simplicity, the model outperforms several state-of-the-art architectures. With only 3.4 M parameters, significantly fewer than other U-Net variants, it is computationally efficient and suitable for clinical deployment. Moreover, the XAI techniques showed that the model is robust and can provide clinicians with greater confidence in its predictions.

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