

HyperCT: Low-Rank Hypernet for Unified Chest CT Analysis

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Abstract

Non-contrast chest CTs offer a rich opportunity for both conventional pulmonary and opportunistic extra-pulmonary screening. While Multi-Task Learning (MTL) can unify these diverse tasks, standard hard-parameter sharing approaches are often suboptimal for modeling distinct pathologies. We propose **HyperCT**, a framework that dynamically adapts a Vision Transformer backbone via a Hypernetwork. To ensure computational efficiency, we integrate Low-Rank Adaptation (LoRA), allowing the model to regress task-specific low-rank weight updates rather than full parameters. Validated on a large-scale dataset of radiological and cardiological tasks, HyperCT outperforms various strong baselines, offering a unified, parameter-efficient solution for holistic patient assessment. Our code will be made publicly available.

Keywords: Chest CT, Hypernetwork, Low-Rank Adaptation, Multi-task Learning

1. Introduction

Non-contrast chest computed tomography (CT) is a fundamental modality of modern radiology, serving as the standard for pulmonary screening due to its high spatial resolution and rapid acquisition. This has led to the creation of vast archives of chest CT data. While these scans are primarily used for **conventional screening** tasks such as detecting pulmonary nodules or emphysema (Hamamci et al., 2024; Anouk Stein et al., 2018), they capture a rich anatomical context, including the heart, great vessels, and upper abdominal organs. This has given rise to an emerging paradigm of **opportunistic screening** (Pickhardt et al., 2023), where a single CT exam is repurposed to screen for a wide range of extra-pulmonary conditions, from cardiovascular diseases (Foraker et al., 2025) to osteoporosis and sarcopenia (Li et al., 2025). This represents a powerful shift toward holistic patient assessment, aiming to extract maximum clinical value from existing data.

Despite the potential for comprehensive health profiling, current chest CT screening approaches remain isolated, typically designed for either entirely for conventional tasks or opportunistic target (Hamamci et al., 2024; Huang et al., 2025). In order to fully exploit chest CT as a comprehensive screening tool, we seek to utilize Multi-task learning (MTL), where a single model jointly learns from both conventional and opportunistic labels. However, standard MTL pipelines still struggle to effectively mitigate task interference, which can result in performance degradation on certain tasks (Kendall et al., 2018; Navon et al., 2022; Lin et al., 2021). The core motivation of this paper is that the central challenge in opportunistic screening is not merely to balance conflicting tasks, but to design a model that can explicitly learn and leverage the synergistic relationships between diverse clinical domains and improve overall diagnostic performance.

Accordingly, we propose **HyperCT**, a novel framework that achieves unified screening by dynamically generating task-specific parameters. Our approach uses a Hypernetwork (Ha et al., 2016) that takes a task’s identity as input and outputs the weights needed to adapt a base model for a specific target. This mechanism enables flexible task-adaptive parameter sharing, moving beyond the rigid backbones of standard MTL. To make this approach computationally feasible for high-capacity architectures like Vision Transformers (ViT) (Dosovitskiy, 2020), we integrate Low-Rank Adaptation (LoRA) (Hu et al., 2022) into the hypernetwork design. Instead of generating full-rank weight matrices, our method regresses low-rank updates, dramatically reducing the complexity of the hypernetwork while preserving the expressive power needed for a diverse set of screening tasks.

We demonstrate the effectiveness of our proposed HyperCT framework on a large-scale curated dataset comprising both conventional and opportunistic screening tasks derived from non-contrast chest CTs. Our results show that the model outperforms standard MTL baselines while achieving comparable performance to dedicated single-task models. This eliminates the need to train separate models for each task while maintaining constant parameter count, highlighting its potential as a unified solution for comprehensive chest CT screening. Our contributions can be summarized as follows:

- We propose a new Hypernetwork-based framework for MTL that effectively unifies conventional and opportunistic screening from non-contrast chest CTs.
- We integrate LoRA into the hypernetwork design, enabling efficient generation of task-specific weights for high capacity architectures like ViTs.
- We curate a comprehensive dataset encompassing both conventional and opportunistic screening tasks and demonstrate that our HyperCT framework outperforms MTL baselines while matching single-task model performance.

2. Related Works

Chest CT screening. The clinical utility of non-contrast chest CT was established by the National Lung Screening Trial (NLST) (Team, 2011), which demonstrated a significant mortality benefit in lung cancer screening. This study catalyzed the application of deep learning to automate radiological interpretation, initially focusing on pulmonary nodules (Setio et al., 2017) and expanding to diffuse chronic diseases like emphysema (Humphries et al., 2020; Li

et al., 2023). Recently, the field has recognized the rich, extra-pulmonary information available in these scans, leading to the paradigm of opportunistic screening for conditions such as esophageal cancer (Yao et al., 2022) and cardiovascular risk (Raikhelkar et al., 2025). However, these two powerful screening paradigms have evolved largely in parallel. Current models are typically developed in isolation, focusing either on a suite of conventional findings or a single opportunistic target. A unified framework capable of performing both simultaneously remains a critical, unaddressed gap.

Multi-task learning. Multi-task learning (MTL) aims to improve performance by jointly learning multiple related tasks (Caruana, 1997). **Optimization-based** approaches focus on balancing task learning through loss weighting—such as Uncertainty Weighting (UW) (Kendall et al., 2018), Random Loss Weighting (RLW) (Lin et al., 2021), and MGDA (Sener and Koltun, 2018), or gradient manipulation strategies like GradNorm (Chen et al., 2018) and Nash-MTL (Navon et al., 2022). These techniques assume tasks are competing and aim to mitigate negative interference, which is a perspective misaligned with medical screening where findings are often synergistic and comorbid. **Architecture-based** approaches, including hard/soft parameter sharing (Misra et al., 2016; Ruder et al., 2019), mixture-of-experts (Chen et al., 2023), and neural architecture search (Guo et al., 2020), offer alternatives but often rely on heuristic designs tailored for CNNs, making adaptation to modern Vision Transformers non-trivial.

Hypernetworks. Hypernetworks (Ha et al., 2016) are a class of neural architectures designed to generate the weights of a “base” model. Recently, this approach has gained traction in Multi-Task Learning (MTL) through the use of task-conditioned hypernetworks. Mahabadi et al. (Mahabadi et al., 2021) demonstrated that hypernetworks can facilitate knowledge sharing across tasks while generating task-specific adapter layers, achieving state-of-the-art results in NLP benchmarks. Similarly, Navon et al. (Navon et al., 2020) utilized hypernetworks to approximate the Pareto front, effectively addressing gradient conflicts in diverse multi-objective settings ranging from fairness constraints to image segmentation. The primary bottleneck for scaling hypernetworks is that their output size is tied to the target model’s parameter count. This often makes the hypernetwork itself too large, limiting its application to small architectures or simple adapters and creating a major challenge for adapting large models like Vision Transformers (ViTs).

3. Method

An overview of our proposed method is presented in Figure 1. The architectural framework includes a pre-trained backbone f_θ parameterized by $\theta = \{\mathbf{W}_1, \mathbf{W}_2, \dots, \mathbf{W}_M\}$, in which M denotes the number of total modules within the base model, and a Hypernetwork h_ϕ parameterized by ϕ , which generates task-specific parameters for the base model. We denote the learnable task embeddings as $E = \{\mathbf{e}^1, \mathbf{e}^2, \dots, \mathbf{e}^K\}$, where each $\mathbf{e}^k \in \mathbb{R}^{d_e}$ corresponds to a specific task representation which is processed by hypernet h_ϕ to generate task-conditioned parameters. Given an input CT scan $x \in \mathbb{R}^{H \times W \times Z}$ and a desired task k , where Z represents the number of slices, and H and W denotes the spatial dimensions, our goal is to leverage those generated task-specific parameters to predict a binary label $\hat{y}^k \in \{0, 1\}$.

Hypernetwork-based Weight Generation: Unlike static multi-task learning, where a set of back-bone parameters θ is shared across tasks, we employ the Hypernetwork h_ϕ to

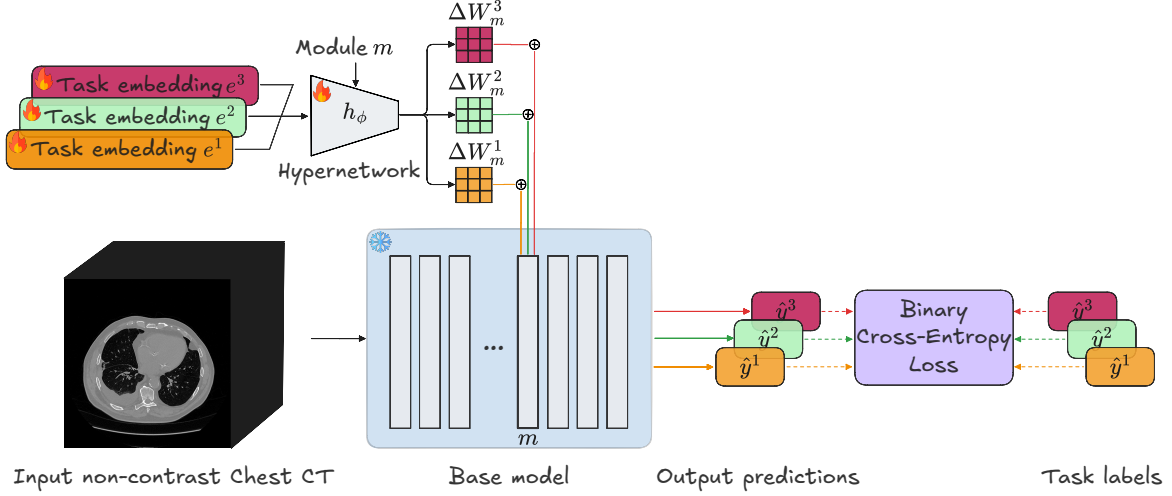


Figure 1: Overview of HyperCT. Given a set of learnable task embeddings, e.g., $\{e^1, e^2, e^3\}$, a hypernet h produces task-specific weight adjustments $\Delta \mathbf{W}^1, \Delta \mathbf{W}^2, \Delta \mathbf{W}^3$, which modulate the weights of the base model. The base model, produces task-specific predictions $\{\hat{y}^1, \hat{y}^2, \hat{y}^3\}$. These outputs are compared with ground-truth task labels $\{y^1, y^2, y^3\}$ via Binary Cross-Entropy Loss.

dynamically regress the parameter of the base model f_θ conditioned on the task representation e^k . Our objective is to generate a task-specific parameter set θ^k for each task k as the following:

$$\theta^k = h_\phi(e^k), \quad \hat{y}^k = f_{\theta^k}(\mathbf{x}), \quad \mathcal{L} = \frac{1}{K} \sum_{k=1}^K \text{BCE}(\hat{y}^k, y^k) \quad (1)$$

where \mathcal{L} is the Binary Cross-Entropy (BCE) loss between a task-specific model prediction \hat{y}^k and the ground truth y^k . This formulation allows the model to adaptively distribute the capacity based on the specific screening task encoded in e^k .

Instead of outputting all the base model weights together, in our implementation, the hypernetwork outputs the weights of each module, using a module indicator as an additional input. The module indicator is a learned vector-valued function ϕ_{pos} of the module index. The hypernetwork h_ϕ generates weights for the target modules by iterating through M target modules, using the task encoding vector e^k and module indicator $\phi_{\text{pos}}(m)$.

Low-Rank Adaptation with Hypernetworks: A practical implementation of the above framework requires careful consideration of the parameter efficiency of h_ϕ . Directly regressing high-dimensional weight matrices \mathbf{W}_m^k can lead to an explosion in the number of parameters within h_ϕ , especially for recent ViT based architectures with large hidden dimensions. However, previous approaches naively consider only a few low-dimensional target modules can result in a significant loss of information (Navon et al., 2020), as the hypernetwork may not capture the full complexity of the task-specific weight distributions.

To mitigate this, we integrate Low-Rank Adaptation (LoRA) (Hu et al., 2022) as h_ϕ target modules. LoRA implements model adaptation via a low-dimensional intrinsic subspace.

By decomposing the task-specific weight update into two low-rank matrices generated by the hypernetwork, we significantly constrain h_ϕ 's output complexity while preserving the generalization ability of the overall pre-trained model. We perform a detailed analysis of the parameter efficiency in Appendix. Sec. E.

Specifically, for each target module weight $\mathbf{W}_m \in \mathbb{R}^{d_{in} \times d_{out}}$ with input dimension d_{in} and output dimension d_{out} , we decompose it into a sum of a frozen pre-trained weight $\mathbf{W}_m^{\text{base}}$ and a low-rank update $\Delta \mathbf{W}_m^k$ generated by the hypernetwork. The overall forward pass and parameter generation are formulated as follows:

$$\begin{aligned} \mathbf{B}_m^k &= h_\phi^B(\mathbf{e}^k, \phi_{\text{pos}}(m)) \quad \mathbf{A}_m^k = h_\phi^A(\mathbf{e}^k, \phi_{\text{pos}}(m)) \\ \Delta \mathbf{W}_m^k &= \mathbf{B}_m^k \mathbf{A}_m^k \quad \forall m \in \{1, \dots, M\}, \\ \theta^k &= \left\{ \mathbf{W}_m^{\text{base}} + \frac{\alpha}{r} \Delta \mathbf{W}_m^k \right\}_{m=1}^M \end{aligned}$$

where $\Delta \mathbf{W}_m^k$ is a low-rank matrix formed by two matrices $\mathbf{B}_m^k \in \mathbb{R}^{d_{in} \times r}$ and $\mathbf{A}_m^k \in \mathbb{R}^{r \times d_{out}}$ (with rank $r \ll \min(d_{in}, d_{out})$), each output by the hypernetwork h_ϕ . This update weight is scaled by $\frac{\alpha}{r}$, where α is a predefined constant.

4. Experiments

4.1. Datasets curation

Dataset Statistics. We curated a large-scale dataset comprising 36,286 non-contrast chest CT scans collected from two major medical centers, Columbia University (CU) Medical Center and Weill Cornell Medical Center (WCM). The dataset is stratified into retrospective and prospective cohorts to rigorously evaluate the generalizability of HyperCT across different clinical settings and time periods. The primary retrospective cohort consists of 34,058 scans acquired between 2011 and 2022. To assess cross-institutional robustness, we trained our models exclusively on the data from CU. Specifically, the 25,948 retrospective CU scans were partitioned into 18,213/2,561/5,174 training/validation/testing samples using a 70/10/20 split, with strict patient-level separation to prevent data leakage. The 8,110 retrospective scans from WCM were reserved strictly as an external test set. Additionally, we collected a prospective cohort of 2,228 scans acquired from 2023 to 2024 to serve as a temporal validation set, containing 1,411/817 exams from CU and WCM respectively.

Task Definition and Labeling. We defined a comprehensive set of $K = 25$ binary classification targets to evaluate on both conventional (18) and opportunistic (7) screening tasks. For the conventional tasks, we employed Llama3.1 (Grattafiori et al., 2024) to parse free-text radiology reports and extract binary pathology labels (Prompt shown in Appendix. Sec. G). For the opportunistic tasks, we matched CT scans to corresponding echocardiography exams using patient identifiers and the closest acquisition dates. We then defined binary ground truth labels for 7 clinically relevant measurements based on established thresholds determined in consultation with expert clinicians (Thresholds are shown in Appendix. Sec. F). The detail label statistics is shown in Appendix Sec. B. It is important to note that radiology report were not collected for the prospective cohort, and therefore the prospective evaluation focuses exclusively on the cardiology tasks.

4.2. Implementation Details

We implement our framework using Pytorch (Paszke et al., 2019). For data processing, each chest CT volume is resized to $H = W = 144$ and $Z = 165$ respectively. For the base model f_θ , we adopt DINOv3 (Siméoni et al., 2025) as the pretrained frozen backbone architecture. We select ViT-base (Dosovitskiy, 2020) variant with 12 transformer layers, $D = 768$ hidden dimension. The hypernetwork h_ϕ is designed as a 3-layer MLP with hidden dimension $d_h = 64$ and ϕ_{pos} is an Embedding layer with $d_p = 64$. The task embeddings \mathbf{e}^k are learnable vectors of dimension 512, initialized randomly. We set the LoRA rank $r = 16$ and scaling factor $\alpha = 16$ for all target modules to match the total trainable parameter size of baselines. We follow previous approaches and compress three consecutive slices as one 2D input to the base model (Gu et al., 2025; Lee et al., 2025).

During training, we use AdamW optimizer (Loshchilov and Hutter, 2017) with an initial learning rate of $1e^{-5}$ and weight decay of 0. We train the model for 20 epochs with a batch size of 8 on 1 NVIDIA A100 GPUs. The learning rate is decayed by a factor of 0.1 every 15 epochs. For each batch, we randomly sample one available task for each sample and compute BCE loss for the corresponding task prediction. During inference, we evaluate all available tasks for each sample and compute the Area Under Curve (AUC) for each task. Best model is selected by validation AUC.

For the MTL baseline implementation, we use the same base model and training hyperparameters for a fair comparison. We use LibMTL (Lin and Zhang, 2023), a publicly-available library, to implement various MTL baselines including Equal Weighting (EW), Uncertainty Weighting (UW) (Kendall et al., 2018), Random Loss Weighting (RLW) (Lin et al., 2021), Dynamic Weight Averaging (DWA) (Liu et al., 2019), and Multi-gradient Descent Algorithm (MGDA) (Sener and Koltun, 2018). Note we did not include recent gradient-based methods such as PCGrad (Yu et al., 2020) and Nash-MTL (Navon et al., 2022). These approaches require multiple gradient computations per training iteration, which introduces prohibitive computational overhead and infeasible for training on our large-scale datasets. Additionally, we compare with a single-task learning baselines (STL) that separately finetune the base model for each task.

4.3. Retrospective Evaluation

Table 1 benchmarks HyperCT against six multi-task learning strategies, including gradient-balancing algorithms like MGDA and GLS in retrospective data. Across 25 tasks, HyperCT consistently achieves the highest performance, with an overall average AUC of 78.1% (CU) and 76.5% (WCM), surpassing the competitive MGDA baseline. We note that STL baselines show strong performance in retrospective data, but do not generalize as well in prospective evaluation (see below) and are significantly resource intensive (with each STL model containing roughly the same number of learnable models as the full HyperCT).

4.4. Prospective Evaluation

To validate real-world utility, we evaluated our model on prospective cohorts from both CU and WCM (Table 2). HyperCT demonstrates strong generalization, achieving the highest average AUCs of 77.8% (CU) and 78.6% (WCM). Interestingly, while Single-Task Learning (STL) models perform comparably well on the retrospective study, they are consistently

Table 1: Comprehensive comparison of AUC scores (%) on retrospective study. Best results among MTL methods are **bolded**, second best are underlined.

		CU Test								WCM Test							
Task		STL	EW	UW	RLW	DWA	GLS	MGDA	HyperCT	STL	EW	UW	RLW	DWA	GLS	MGDA	HyperCT
Conventional	Overall Average	79.3	74.3	74.4	74.0	74.3	71.6	76.0	78.1	77.6	72.9	72.9	72.8	72.9	69.5	74.9	76.5
	Med. Mat.	88.2	83.6	83.2	81.8	83.6	76.4	85.9	85.8	89.3	85.5	85.2	84.4	85.5	78.9	87.6	87.3
	Art. Calc.	82.0	79.5	79.4	79.0	79.5	76.8	80.5	81.9	75.3	73.9	73.9	73.2	73.9	71.2	74.4	76.0
	Cardiomeg.	86.9	84.1	84.1	83.4	84.1	81.5	85.3	87.0	87.1	85.0	85.0	84.3	85.0	82.8	86.0	87.0
	Peri. Eff.	70.2	68.0	68.0	67.5	68.0	63.9	69.4	68.5	73.3	67.4	67.4	67.3	67.4	62.6	69.9	71.1
	Cor. Art. Calc.	90.1	83.8	83.8	83.3	83.8	81.6	84.8	88.2	84.6	78.7	78.6	77.8	78.6	76.1	79.3	82.3
	Hiatal Hernia	70.8	59.6	60.1	58.5	59.6	59.2	61.3	67.6	70.6	56.7	57.3	55.6	56.7	56.0	60.5	68.8
	Lymphadenop.	72.6	65.4	65.1	65.1	65.4	62.4	68.3	67.1	74.5	67.0	66.8	67.0	67.0	64.3	70.1	69.4
	Emphysema	82.8	76.6	76.8	74.3	76.6	73.6	77.6	79.1	79.4	73.4	73.6	72.1	73.4	70.4	74.6	74.9
	Atelectasis	80.3	74.8	74.6	74.0	74.8	72.1	76.7	77.7	80.5	76.3	76.2	76.1	76.4	74.0	78.0	78.2
	Lung Nodule	68.1	68.8	68.6	68.5	68.8	66.3	70.0	70.0	62.3	65.0	64.8	64.8	65.0	62.3	65.6	64.4
	Lung Opacity	78.8	75.6	75.4	74.7	75.6	73.3	78.2	78.2	77.5	75.1	74.9	74.4	75.1	72.5	77.4	78.0
	Pulm. Fibrosis	85.9	84.2	84.3	83.5	84.2	83.4	84.7	85.2	81.8	80.3	80.3	79.8	80.2	79.6	81.0	80.6
	Pleural Eff.	96.1	94.4	94.5	94.1	94.4	94.2	94.5	95.6	96.7	94.6	94.7	94.3	94.6	94.5	94.7	95.9
	Mosaic Attn.	70.2	61.2	61.6	60.4	61.3	56.8	65.7	71.6	67.7	60.3	60.7	59.5	60.4	57.3	64.4	68.1
	Peribronchial	66.9	62.7	62.5	62.1	62.7	59.5	64.9	66.3	65.5	63.7	63.4	62.8	63.7	60.3	66.3	66.5
	Consolidation	87.9	83.2	83.1	82.3	83.2	80.3	85.0	86.3	83.9	78.9	78.9	78.0	78.9	75.7	80.5	82.0
	Bronchiectasis	81.7	78.6	78.7	78.5	78.6	77.1	79.8	80.6	78.2	74.6	74.8	74.2	74.6	73.1	75.8	76.8
Septal Thick.	76.0	74.9	74.9	73.9	74.9	72.4	76.0	75.8	78.0	77.8	77.7	77.5	77.8	74.1	79.1	79.3	
Group Avg.		79.8	75.5	75.5	74.7	75.5	72.8	77.1	78.5	78.1	74.1	74.1	73.5	74.1	71.4	75.8	77.0
Opportunistic	Red. RV	79.9	74.1	74.2	73.3	74.1	70.3	75.3	77.5	80.1	74.8	74.8	74.4	74.8	71.4	76.4	77.9
	Red. LV	80.0	70.7	70.8	70.9	70.7	67.3	73.2	77.0	77.9	70.5	70.5	70.5	70.5	66.2	72.8	74.6
	Pulm. HTN	71.2	71.6	71.4	70.7	71.6	68.5	72.9	72.7	71.6	70.1	69.8	70.0	70.1	67.6	71.4	72.0
	Atrial Enlg.	83.9	75.8	75.9	75.8	75.8	69.8	78.2	83.0	82.3	74.1	74.2	74.3	74.1	68.6	76.6	79.9
	Vent. Enlg.	83.8	68.6	69.2	69.9	68.6	62.7	72.0	80.4	75.0	61.0	61.4	61.6	61.0	58.5	64.5	73.1
	LA Pressure	75.6	74.2	74.0	73.3	74.2	70.6	76.0	77.1	75.6	73.7	73.5	73.3	73.7	70.6	75.8	77.1
	RA Pressure	72.1	63.8	64.6	64.1	63.8	59.0	69.1	71.4	71.0	64.0	64.4	64.8	64.0	58.3	69.0	72.4
Group Avg.		78.1	71.3	71.4	71.1	71.3	66.9	73.8	77.0	76.2	69.7	69.8	69.8	69.7	65.9	72.4	75.3

surpassed by HyperCT in this prospective setting. This suggests that multi-task frameworks learn more robust representations that better withstand the distributional shifts common in real-world deployment, a quality at which HyperCT’s dynamic architecture excels.

Table 2: Comprehensive comparison of AUC scores (%) on prospective study. Best results among MTL methods are **bolded**, and second-best results are underlined.

		CU Prospective								WCM Prospective							
Task		STL	EW	UW	RLW	DWA	GLS	MGDA	HyperCT	STL	EW	UW	RLW	DWA	GLS	MGDA	HyperCT
Overall Average		75.4	69.7	70.9	71.6	70.9	66.8	74.4	77.8	75.2	73.0	72.9	73.2	73.0	68.1	76.1	78.6
Opportunistic	Red. RV	77.0	74.8	73.8	73.6	73.9	68.7	75.1	77.2	80.6	79.7	79.5	78.5	79.7	76.2	79.9	79.2
	Red. LV	74.1	70.5	71.1	70.8	71.1	65.4	74.1	76.6	72.5	70.0	69.7	69.5	70.0	66.0	73.2	77.2
	Pulm. HTN	71.7	70.1	70.9	71.8	71.1	69.9	72.7	73.6	71.0	72.9	72.5	73.2	73.0	68.7	75.7	75.5
	Atrial Enlg.	80.2	74.1	72.0	72.3	72.0	68.6	74.3	80.0	83.5	77.1	77.1	77.7	77.1	69.8	80.2	80.8
	Vent. Enlg.	78.3	61.0	71.5	73.3	71.2	65.7	77.0	86.6	67.0	69.5	69.4	71.0	69.5	63.8	73.7	81.8
	LA Pressure	76.8	73.7	75.7	75.8	75.9	73.4	76.8	78.5	77.7	76.2	76.0	75.9	76.2	72.3	77.9	79.1
	RA Pressure	70.0	64.0	61.5	63.7	61.0	56.2	70.6	72.3	74.2	65.4	65.8	66.4	65.4	59.7	72.4	76.7

5. Ablation Study

Module selection. Table 3 presents an ablation study comparing the AUC scores of three LoRA module variants—Attn Only, MLP only, and HyperCT—across 18 conventional medical imaging tasks on the CU and WCM retrospective study. The results demonstrate that the HyperCT architecture (85.0M parameters) consistently delivers the superior performance, achieving the highest average AUC scores of 78.5% for the CU group and 77.0% for the WCM group. While the lighter Attn Only (35.9M) and MLP only (49.3M) vari-

Table 3: Comparison of AUC scores (%) for LoRA module variants on retrospective study. Best results are **bolded**, and second best are underlined. Full table is in Appendix Sec. A

	Method	Params	Med. Mat.	Art. Calc.	Cardiomeg.	Peri. Eff.	Cor. Art. Calc.	Hiatal Hernia	Lymphadenop.	Emphysema	Atelectasis	Lung Nodule	Lung Opacity	Pulm. Fibrosis	Pleural Eff.	Mosaic Attn.	Peribronchial	Consolidation	Bronchiectasis	Septal Thick.	Avg
CU	Attn Only	35.9M	<u>85.3</u>	<u>81.8</u>	86.7	68.8	88.3	<u>67.1</u>	67.4	77.7	<u>77.0</u>	70.4	77.4	84.2	<u>95.3</u>	70.3	<u>65.6</u>	85.1	<u>80.1</u>	<u>75.4</u>	<u>77.9</u>
	MLP only	49.3M	85.0	81.6	87.1	67.0	87.9	66.7	66.9	<u>78.0</u>	76.9	69.8	<u>77.7</u>	<u>85.0</u>	95.2	70.0	65.5	<u>85.4</u>	80.6	75.1	77.8
	HyperCT	85.0M	85.8	81.9	<u>87.0</u>	<u>68.5</u>	<u>88.2</u>	67.6	<u>67.1</u>	79.1	77.7	<u>70.0</u>	78.2	85.2	95.6	71.6	66.3	86.3	80.6	75.8	78.5
WCM	Attn Only	35.9M	<u>87.1</u>	76.0	86.4	71.2	<u>82.1</u>	<u>67.0</u>	<u>69.4</u>	73.5	78.4	64.8	76.9	80.7	<u>95.6</u>	65.7	<u>65.3</u>	<u>80.7</u>	76.5	<u>79.0</u>	<u>76.5</u>
	MLP only	49.3M	86.8	<u>75.7</u>	87.2	70.2	82.0	65.4	69.5	<u>73.9</u>	77.2	<u>64.4</u>	<u>77.2</u>	81.3	<u>95.6</u>	<u>66.3</u>	65.1	80.4	<u>76.6</u>	78.8	76.3
	HyperCT	85.0M	87.3	76.0	<u>87.0</u>	<u>71.1</u>	82.3	68.8	<u>69.4</u>	74.9	<u>78.2</u>	<u>64.4</u>	78.0	80.6	95.9	68.1	66.5	82.0	76.8	79.3	77.0

ants perform comparably to one another with slightly lower averages, HyperCT secures the top results (bolded) in the vast majority of individual pathologies, such as Emphysema, Consolidation, and Septal Thickening, across both datasets.

 Table 4: Ablation of LoRA Rank (r) dimensions on retrospective study (Conventional labels). Best results are **bolded**, and second-best results are underlined. Full table is in Appendix. Sec. D

	Rank	Med. Mat.	Art. Calc.	Cardiomeg.	Peri. Eff.	Cor. Art. Calc.	Hiatal Hernia	Lymphadenop.	Emphysema	Atelectasis	Lung Nodule	Lung Opacity	Pulm. Fibrosis	Pleural Eff.	Mosaic Attn.	Peribronchial	Consolidation	Bronchiectasis	Septal Thick.	Avg
CU	$r = 1$	76.0	80.2	85.4	66.1	84.8	65.8	65.8	73.9	74.5	69.8	75.7	82.3	94.5	66.6	64.0	81.1	78.9	74.2	75.2
	$r = 2$	83.6	80.7	85.6	66.8	86.2	<u>66.6</u>	67.5	75.5	76.6	69.8	77.1	84.3	94.9	69.6	65.0	83.3	79.9	75.3	76.7
	$r = 4$	84.8	81.1	86.7	68.5	87.1	65.4	<u>67.4</u>	76.8	76.6	<u>70.2</u>	77.4	84.1	95.2	<u>70.5</u>	<u>65.6</u>	84.9	<u>80.3</u>	75.1	77.4
	$r = 8$	<u>85.6</u>	<u>81.5</u>	<u>86.9</u>	<u>68.4</u>	<u>87.7</u>	66.0	67.3	<u>77.0</u>	<u>76.9</u>	70.4	<u>77.6</u>	<u>84.5</u>	<u>95.3</u>	70.3	65.5	<u>85.2</u>	<u>80.3</u>	<u>75.4</u>	<u>77.7</u>
	$r = 16$	85.8	81.9	87.0	68.5	88.2	67.6	67.1	79.1	77.7	70.0	78.2	85.2	95.6	71.6	66.3	86.3	80.6	75.8	78.5
WCM	$r = 1$	76.6	74.5	84.8	69.1	79.1	62.8	68.2	70.1	75.7	63.9	74.6	80.3	94.6	62.2	63.5	76.3	75.0	77.8	73.5
	$r = 2$	85.8	75.4	85.4	69.0	80.8	63.8	<u>69.4</u>	71.4	77.0	64.0	75.9	81.5	95.1	64.3	63.7	78.5	<u>76.3</u>	78.3	74.8
	$r = 4$	86.7	75.6	<u>86.6</u>	71.2	81.4	63.9	69.5	<u>73.9</u>	77.2	64.3	76.7	80.7	95.5	<u>66.7</u>	64.9	80.2	76.2	78.5	75.8
	$r = 8$	<u>86.9</u>	<u>75.8</u>	86.4	70.9	<u>82.0</u>	<u>64.6</u>	69.3	72.6	<u>77.4</u>	64.5	<u>77.1</u>	<u>81.1</u>	<u>95.7</u>	65.5	<u>65.0</u>	<u>80.5</u>	75.5	<u>78.8</u>	<u>75.9</u>
	$r = 16$	87.3	76.0	87.0	<u>71.1</u>	82.3	68.8	<u>69.4</u>	74.9	78.2	<u>64.4</u>	78.0	80.6	95.9	68.1	66.5	82.0	76.8	79.3	77.0

LoRA rank. Table 4 presents the ablation study on the impact of the LoRA rank dimension (r) across 18 conventional tasks on the retrospective study. We observe a consistent trend where increasing the rank from $r = 1$ to $r = 16$ yields performance gains across both institutions. Specifically, the configuration with $r = 16$ achieves the highest average AUC scores of 78.5% for Columbia (CU) and 77.0% for Cornell (WCM), securing the best results in the majority of individual tasks. This indicates that while Low-Rank Adaptation is designed for parameter efficiency, a sufficient rank dimension is essential to provide the necessary model capacity for effectively adapting the frozen backbone features to a diverse range of cardiopulmonary pathologies.

Backbone selection. Table 5 evaluates the impact of backbone selection by benchmarking the 3D-pretrained CTViT (Hamamci et al., 2023) against the 2D-pretrained DINOv3 foundation model on conventional radiological tasks. The results unequivocally favor the 2D backbone, with DINOv3 establishing a new baseline by outperforming CTViT across every individual task in both the CU and WCM test sets. This shows the importance of

backbone selection for base model. With DINOv3 extensively pretrained on large-scale 2D natural images, it appears to capture more generalizable features that transfer effectively to medical imaging tasks, even when applied to 3D volumetric data through slice-wise processing. This finding underscores the potential of leveraging large-scale 2D pretraining for enhancing performance in 3D medical imaging applications.

Table 5: Comparison of 3D (CTViT) and 2D (DINOv3) backbones on retrospective study (Conventional labels). Best results are **bolded**. Full table is in Appendix. C

	Method	Med. Mat.	Art. Calc.	Cardiomeg.	Peri. Eff.	Cor. Art. Calc.	Hiatal Hernia	Lymphadenop.	Emphysema	Atelectasis	Lung Nodule	Lung Opacity	Pulm. Fibrosis	Pleural Eff.	Mosaic Attn.	Peribronchial	Consolidation	Bronchiectasis	Septal Thicken.	Avg
CU	CTViT	66.7	68.3	79.4	67.0	71.7	65.8	65.5	71.3	71.5	69.0	71.8	76.8	91.0	67.5	61.6	77.9	74.4	68.6	71.1
	DINOv3	85.8	81.9	87.0	68.5	88.2	67.6	67.1	79.1	77.7	70.0	78.2	85.2	95.6	71.6	66.3	86.3	80.6	75.8	78.5
WCM	CTViT	65.8	64.3	79.1	69.1	67.9	65.3	67.5	64.4	72.3	62.8	69.9	69.9	89.9	63.4	59.4	72.0	67.1	70.3	68.3
	DINOv3	87.3	76.0	87.0	71.1	82.3	68.8	69.4	74.9	78.2	64.4	78.0	80.6	95.9	68.1	66.5	82.0	76.8	79.3	77.0

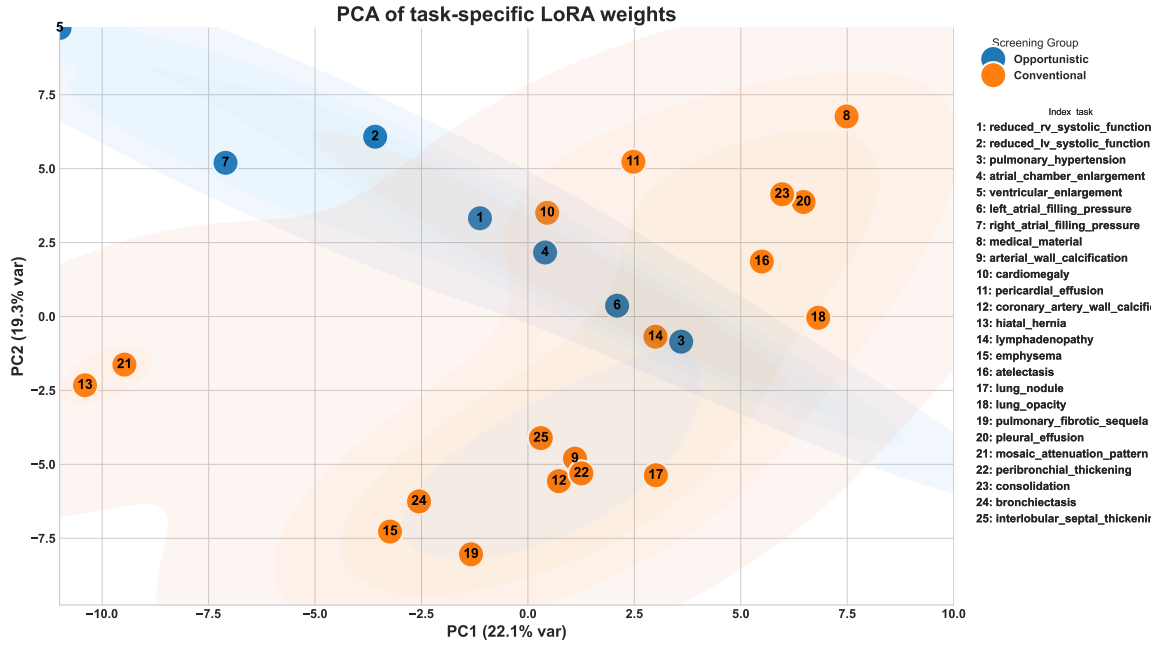


Figure 2: Principle Component Analysis (PCA) of task-specific LoRA. Blue is opportunistic labels and orange is conventional labels. Number is the index of labels.

Task visualization. Fig. 2 visualizes the Principal Component Analysis (PCA) of the task-specific LoRA weights generated by the hypernetwork. A distinct semantic separation is evident between the **Opportunistic** (blue) and **Conventional** (orange) screening groups; the opportunistic tasks—primarily relating to cardiac function and hemodynamics—cluster in a specific region separate from the broader distribution of conventional radiological findings. Note that index 10 (Cardiomegaly) and 14 (lymphadenopathy) are overlap

with the blue manifold because they are associated with cardiovascular health. This clustering suggests that the hypernetwork effectively captures the underlying domain shifts between these task categories, automatically learning to allocate different parameter subspaces to address the distinct feature extraction requirements of physiological estimation versus anatomical detection.

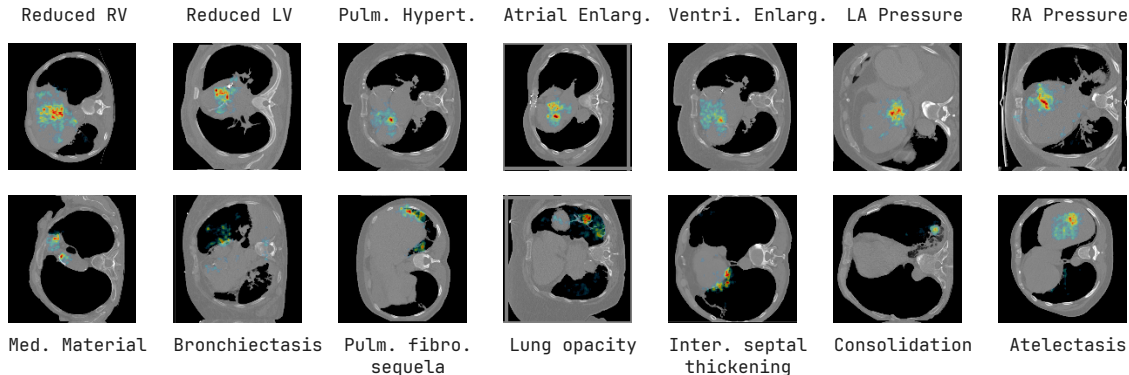


Figure 3: Saliency maps generated using Grad-CAM for different tasks. First row is opportunistic screening tasks and second row is part of the conventional screening tasks.

Saliency map. Fig. 3 illustrates the model’s visual attention through Grad-CAM-generated saliency maps for a range of diagnostic tasks, which are divided into opportunistic cardiovascular screenings (top row) and conventional pulmonary screenings (bottom row). For opportunistic tasks, the saliency maps consistently and accurately localize the attention regions within the cardiac silhouette. Similarly, for conventional pulmonary findings, the model correctly focuses its attention on the relevant areas within the lung parenchyma and pleura. This strong alignment between the model’s focus and the expected anatomical locations for each specific pathology enhancing the interpretability and trustworthiness of its predictions.

6. Conclusion

In this work, we introduced HyperCT, a novel framework using a LoRA-integrated hypernetwork to unify conventional and opportunistic chest CT screening. Our model demonstrated superior generalization on prospective, multi-institutional data, outperforming both strong MTL baselines and matching with specialized Single-Task Learning models. Analyses of the generated LoRA weights and saliency maps confirmed that our dynamic approach learns a meaningful, task-adaptive parameter space. HyperCT offers a parameter-efficient and unified solution for holistic patient assessment, paving the way for maximizing the clinical value of routine medical imaging.

References

- MD Anouk Stein, Carol Wu, Chris Carr, George Shih, Jamie Dulkowski, kalpathy, Leon Chen, Luciano Prevedello, MD Marc Kohli, Mark McDonald, Peter, Phil Culliton, Safwan Halabi MD, and Tian Xia. Rsn pneumonia detection challenge. <https://kaggle.com/competitions/rsna-pneumonia-detection-challenge>, 2018. Kaggle.
- Rich Caruana. Multitask learning. *Machine learning*, 28(1):41–75, 1997.
- Zhao Chen, Vijay Badrinarayanan, Chen-Yu Lee, and Andrew Rabinovich. Gradnorm: Gradient normalization for adaptive loss balancing in deep multitask networks. In *International conference on machine learning*, pages 794–803. PMLR, 2018.
- Zitian Chen, Yikang Shen, Mingyu Ding, Zhenfang Chen, Hengshuang Zhao, Erik G Learned-Miller, and Chuang Gan. Mod-squad: Designing mixtures of experts as modular multi-task learners. In *Proceedings of the IEEE/CVF Conference on Computer Vision and Pattern Recognition*, pages 11828–11837, 2023.
- Alexey Dosovitskiy. An image is worth 16x16 words: Transformers for image recognition at scale. *arXiv preprint arXiv:2010.11929*, 2020.
- Randi Foraker, Laurence Sperling, Lisa Bratzke, Matthew Budoff, Michelle Leppert, Alexander C Razavi, Fatima Rodriguez, Michael D Shapiro, Seamus Whelton, Nathan D Wong, et al. Opportunistic detection of coronary artery calcium on noncardiac chest computed tomography: An emerging tool for cardiovascular disease prevention: A scientific statement from the american heart association. *Circulation*, 152(19):e391–e401, 2025.
- Aaron Grattafiori, Abhimanyu Dubey, Abhinav Jauhri, Abhinav Pandey, Abhishek Kadian, Ahmad Al-Dahle, Aiesha Letman, Akhil Mathur, Alan Schelten, Alex Vaughan, et al. The llama 3 herd of models. *arXiv preprint arXiv:2407.21783*, 2024.
- Hanxue Gu, Yaqian Chen, Nicholas Konz, Qihang Li, and Maciej A Mazurowski. Are vision foundation models ready for out-of-the-box medical image registration? In *Deep Breast Workshop on AI and Imaging for Diagnostic and Treatment Challenges in Breast Care*, pages 101–112. Springer, 2025.
- Pengsheng Guo, Chen-Yu Lee, and Daniel Ulbricht. Learning to branch for multi-task learning. In *International conference on machine learning*, pages 3854–3863. PMLR, 2020.
- David Ha, Andrew Dai, and Quoc V Le. Hypernetworks. *arXiv preprint arXiv:1609.09106*, 2016.
- Ibrahim Ethem Hamamci, Sezgin Er, Anjany Sekuboyina, Enis Simsar, Alperen Tezcan, Ayse Gulnihan Simsek, Sevval Nil Esirgun, Furkan Almas, Irem Dogan, Muhammed Furkan Dasdelen, et al. Generatect: Text-conditional generation of 3d chest ct volumes. *arXiv preprint arXiv:2305.16037*, 2023.

- Ibrahim Ethem Hamamci, Sezgin Er, Chenyu Wang, Furkan Almas, Ayse Gulnihan Simsek, Seval Nil Esirgun, Irem Dogan, Omer Faruk Durugol, Benjamin Hou, Suprosanna Shit, et al. Developing generalist foundation models from a multimodal dataset for 3d computed tomography. *arXiv preprint arXiv:2403.17834*, 2024.
- Edward J Hu, Yelong Shen, Phillip Wallis, Zeyuan Allen-Zhu, Yuanzhi Li, Shean Wang, Lu Wang, Weizhu Chen, et al. Lora: Low-rank adaptation of large language models. *ICLR*, 1(2):3, 2022.
- Jiaxing Huang, Heng Guo, Le Lu, Fan Yang, Minfeng Xu, Ge Yang, and Wei Luo. Opportunistic osteoporosis diagnosis via texture-preserving self-supervision, mixture of experts and multi-task integration. In *International Conference on Medical Image Computing and Computer-Assisted Intervention*, pages 428–438. Springer, 2025.
- Stephen M Humphries, Aleena M Notary, Juan Pablo Centeno, Matthew J Strand, James D Crapo, Edwin K Silverman, David A Lynch, and Genetic Epidemiology of COPD (COPDGene) Investigators. Deep learning enables automatic classification of emphysema pattern at ct. *Radiology*, 294(2):434–444, 2020.
- Alex Kendall, Yarin Gal, and Roberto Cipolla. Multi-task learning using uncertainty to weigh losses for scene geometry and semantics. In *Proceedings of the IEEE conference on computer vision and pattern recognition*, pages 7482–7491, 2018.
- Jeong Hoon Lee, Cynthia Xinran Li, Hassan Jahanandish, Indrani Bhattacharya, Sulaiman Vesal, Lichun Zhang, Shengtian Sang, Moon Hyung Choi, Simon John Christoph Soerensen, Steve Ran Zhou, et al. Prostate-specific foundation models for enhanced detection of clinically significant cancer. *arXiv preprint arXiv:2502.00366*, 2025.
- Thomas Z Li, Ho Hin Lee, Kaiwen Xu, Riqiang Gao, Benoit M Dawant, Fabien Maldonado, Kim L Sandler, and Bennett A Landman. Quantifying emphysema in lung screening computed tomography with robust automated lobe segmentation. *Journal of Medical Imaging*, 10(4):044002–044002, 2023.
- Yali Li, Suwei Liu, Yan Zhang, Mengze Zhang, Chenyu Jiang, Ming Ni, Dan Jin, Zhen Qian, Jiangxuan Wang, Xuemin Pan, et al. Deep learning-enhanced opportunistic osteoporosis screening in ultralow-voltage (80 kv) chest ct: A preliminary study. *Academic Radiology*, 2025.
- Baijiong Lin and Yu Zhang. LibMTL: A Python library for multi-task learning. *Journal of Machine Learning Research*, 24(209):1–7, 2023.
- Baijiong Lin, Feiyang Ye, Yu Zhang, and Ivor W Tsang. Reasonable effectiveness of random weighting: A litmus test for multi-task learning. *arXiv preprint arXiv:2111.10603*, 2021.
- Shikun Liu, Edward Johns, and Andrew J Davison. End-to-end multi-task learning with attention. In *Proceedings of the IEEE/CVF conference on computer vision and pattern recognition*, pages 1871–1880, 2019.
- Ilya Loshchilov and Frank Hutter. Decoupled weight decay regularization. *arXiv preprint arXiv:1711.05101*, 2017.

- Rabeeh Karimi Mahabadi, Sebastian Ruder, Mostafa Dehghani, and James Henderson. Parameter-efficient multi-task fine-tuning for transformers via shared hypernetworks. *arXiv preprint arXiv:2106.04489*, 2021.
- Ishan Misra, Abhinav Shrivastava, Abhinav Gupta, and Martial Hebert. Cross-stitch networks for multi-task learning. In *Proceedings of the IEEE conference on computer vision and pattern recognition*, pages 3994–4003, 2016.
- Aviv Navon, Aviv Shamsian, Gal Chechik, and Ethan Fetaya. Learning the pareto front with hypernetworks. *arXiv preprint arXiv:2010.04104*, 2020.
- Aviv Navon, Aviv Shamsian, Idan Achituve, Haggai Maron, Kenji Kawaguchi, Gal Chechik, and Ethan Fetaya. Multi-task learning as a bargaining game. *arXiv preprint arXiv:2202.01017*, 2022.
- Adam Paszke, Sam Gross, Francisco Massa, Adam Lerer, James Bradbury, Gregory Chanan, Trevor Killeen, Zeming Lin, Natalia Gimelshein, Luca Antiga, et al. Pytorch: An imperative style, high-performance deep learning library. *Advances in neural information processing systems*, 32, 2019.
- Perry J Pickhardt, Ronald M Summers, John W Garrett, Arun Krishnaraj, Sheela Agarwal, Keith J Dreyer, and Gregory N Nicola. Opportunistic screening: radiology scientific expert panel. *Radiology*, 307(5):e222044, 2023.
- Jayant Raikhelkar, Zilong Bai, Ashley Beecy, Fengbei Liu, Nusrat Nizam, Varsha Kishore, Chris Kelsey, Jeffrey Ruhl, Naomi Tesfuzigta, Erica Lancet, et al. An artificial intelligence model to detect abnormal ejection fraction from non-contrast chest computed tomography: The ct-lvef study. 2025.
- Sebastian Ruder, Joachim Bingel, Isabelle Augenstein, and Anders Søgaard. Latent multi-task architecture learning. In *Proceedings of the AAAI conference on artificial intelligence*, volume 33, pages 4822–4829, 2019.
- Ozan Sener and Vladlen Koltun. Multi-task learning as multi-objective optimization. *Advances in neural information processing systems*, 31, 2018.
- Arnaud Arindra Adiyoso Setio, Alberto Traverso, Thomas De Bel, Moira SN Berens, Cas Van Den Bogaard, Piergiorgio Cerello, Hao Chen, Qi Dou, Maria Evelina Fantacci, Bram Geurts, et al. Validation, comparison, and combination of algorithms for automatic detection of pulmonary nodules in computed tomography images: the luna16 challenge. *Medical image analysis*, 42:1–13, 2017.
- Oriane Siméoni, Huy V Vo, Maximilian Seitzer, Federico Baldassarre, Maxime Oquab, Cijo Jose, Vasil Khalidov, Marc Szafraniec, Seungeun Yi, Michaël Ramamonjisoa, et al. Dinov3. *arXiv preprint arXiv:2508.10104*, 2025.
- National Lung Screening Trial Research Team. Reduced lung-cancer mortality with low-dose computed tomographic screening. *New England Journal of Medicine*, 365(5):395–409, 2011.

- Jiawen Yao, Xianghua Ye, Yingda Xia, Jian Zhou, Yu Shi, Ke Yan, Fang Wang, Lili Lin, Haogang Yu, Xian-Sheng Hua, et al. Effective opportunistic esophageal cancer screening using noncontrast ct imaging. In *International Conference on Medical Image Computing and Computer-Assisted Intervention*, pages 344–354. Springer, 2022.
- Tianhe Yu, Saurabh Kumar, Abhishek Gupta, Sergey Levine, Karol Hausman, and Chelsea Finn. Gradient surgery for multi-task learning. *Advances in neural information processing systems*, 33:5824–5836, 2020.

Appendix A. Full Table for Ablation LoRA Module

Table 6: Ablation Study: Comparison of AUC scores (%) for LoRA Module variants on Retrospective study. Best results are bolded.

Task		CU Test			WCM Test		
		Attn Only	MLP only	HyperCT	Attn Only	MLP only	HyperCT
<i>Overall Average</i>		77.8	77.7	78.1	76.1	76.1	76.5
Conventional	Medical Material	85.3	85.0	85.8	87.1	86.8	87.3
	Arterial Wall Calcification	81.8	81.6	81.9	76.0	75.7	76.0
	Cardiomegaly	86.7	87.1	87.0	86.4	87.2	87.0
	Pericardial Effusion	68.8	67.0	68.5	71.2	70.2	71.1
	Coronary Artery Wall Calc.	88.3	87.9	88.2	82.1	82.0	82.3
	Hiatal Hernia	67.1	66.7	67.6	67.0	65.4	68.8
	Lymphadenopathy	67.4	66.9	67.1	69.4	69.5	69.4
	Emphysema	77.7	78.0	79.1	73.5	73.9	74.9
	Atelectasis	77.0	76.9	77.7	78.4	77.2	78.2
	Lung Nodule	70.4	69.8	70.0	64.8	64.4	64.4
	Lung Opacity	77.4	77.7	78.2	76.9	77.2	78.0
	Pulmonary Fibrotic Sequela	84.2	85.0	85.2	80.7	81.3	80.6
	Pleural Effusion	95.3	95.2	95.6	95.6	95.6	95.9
	Mosaic Attenuation Pattern	70.3	70.0	71.6	65.7	66.3	68.1
	Peribronchial Thickening	65.6	65.5	66.3	65.3	65.1	66.5
	Consolidation	85.1	85.4	86.3	80.7	80.4	82.0
	Bronchiectasis	80.1	80.6	80.6	76.5	76.6	76.8
	Interlobular Septal Thick.	75.4	75.1	75.8	79.0	78.8	79.3
<i>Group Avg.</i>		77.9	77.8	78.5	76.5	76.3	77.0
Opportunistic	Reduced RV Systolic Function	77.1	77.1	77.5	77.5	78.0	77.9
	Reduced LV Systolic Function	77.2	77.1	77.0	74.8	74.7	74.6
	Pulmonary Hypertension	72.9	72.6	72.7	71.9	72.2	72.0
	Atrial Chamber Enlargement	82.6	82.0	83.0	79.6	80.1	79.9
	Ventricular Enlargement	80.5	81.2	80.4	73.2	73.6	73.1
	Left Atrial Filling Pressure	77.0	77.1	77.1	77.0	77.1	77.1
	Right Atrial Filling Pressure	73.4	73.6	71.4	73.0	73.2	72.4
	<i>Group Avg.</i>	77.2	77.2	77.0	75.3	75.6	75.3

Table 7: Ablation Study: Comparison of AUC scores (%) for LoRA Module variants on Prospective Datasets. Best results are bolded.

Task		CU Prospective			WCM Prospective		
		Attn Only	MLP only	HyperCT	Attn Only	MLP only	HyperCT
<i>Overall Average</i>		77.7	77.5	77.8	78.9	79.6	78.6
Opportunistic	Reduced RV Systolic Function	76.6	76.6	77.2	78.7	80.5	79.2
	Reduced LV Systolic Function	76.9	76.8	76.6	79.0	80.7	77.2
	Pulmonary Hypertension	71.7	73.4	73.6	75.0	76.2	75.5
	Atrial Chamber Enlargement	80.1	79.5	80.0	81.6	82.1	80.8
	Ventricular Enlargement	85.8	86.2	86.6	81.7	83.3	81.8
	Left Atrial Filling Pressure	78.3	77.8	78.5	79.4	79.8	79.1
	Right Atrial Filling Pressure	74.5	72.5	72.3	76.8	74.7	76.7

Appendix B. Valid label fraction

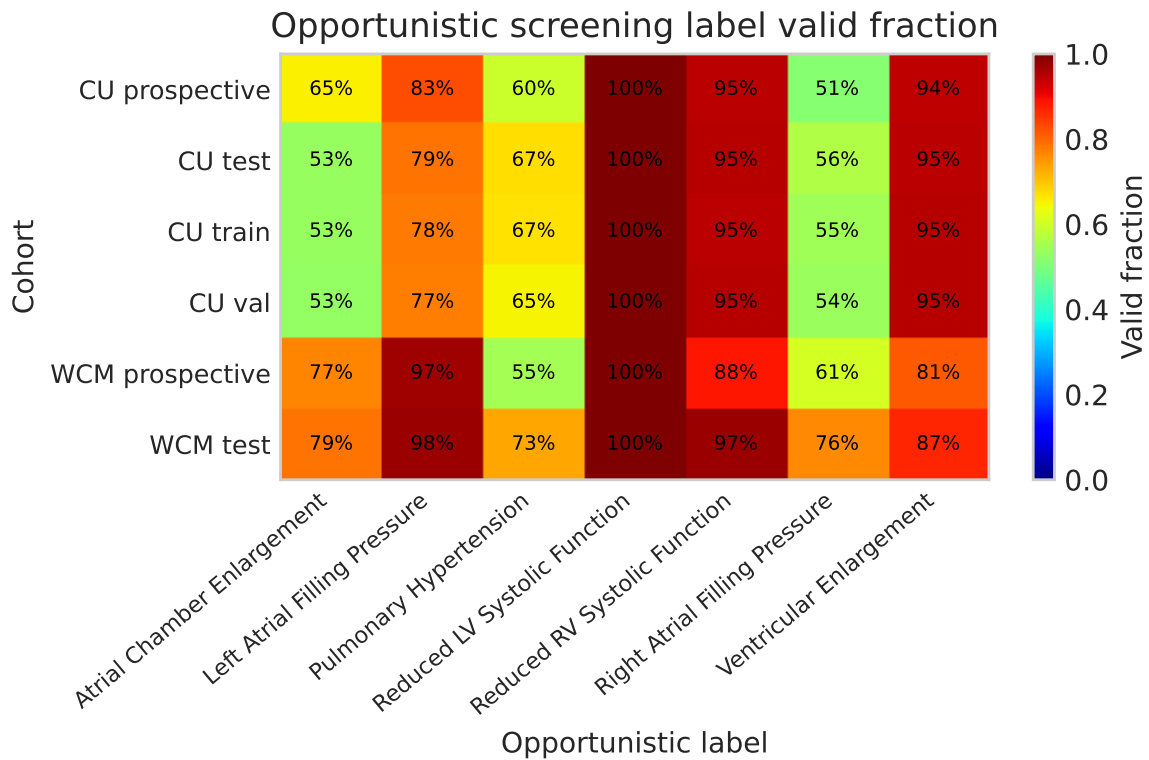


Figure 4: Sample valid fraction heatmaps for opportunistic screening labels

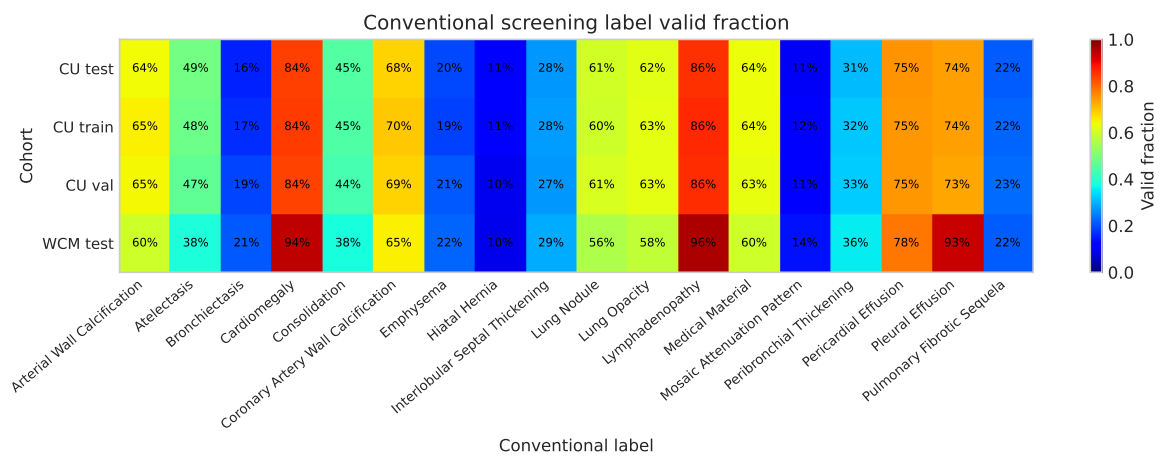


Figure 5: Sample valid fraction heatmaps for conventional screening labels

Appendix C. Ablation: Backbone selection

Table 8: Comparison of 3D (CTViT) and 2D (DINOv3) backbones on Opportunistic Tasks across all datasets. Best results are bolded.

	Method	Reduced RV	Reduced LV	Pulmonary Hypertension	Atrial Enlargement	Ventricular Enlargement	LA Pressure	RA Pressure	Avg
CU (Retro)	CTViT-Encoder	72.4	70.6	69.2	75.9	73.4	71.5	70.0	71.9
	DINOv3	77.5	77.0	72.7	83.0	80.4	77.1	71.4	77.0
WCM (Retro)	CTViT-Encoder	72.5	66.3	70.0	72.1	66.9	71.4	70.0	69.9
	DINOv3	77.9	74.6	72.0	79.9	73.1	77.1	72.4	75.3
CU (Prosp)	CTViT-Encoder	70.8	68.6	69.7	75.6	79.2	74.8	68.1	72.4
	DINOv3	77.2	76.6	73.6	80.0	86.6	78.5	72.3	77.8
WCM (Prosp)	CTViT-Encoder	74.0	70.7	73.8	73.0	74.5	73.7	74.3	73.4
	DINOv3	79.2	77.2	75.5	80.8	81.8	79.1	76.7	78.6

Appendix D. Ablation: rank selection

Table 9: Ablation of LoRA Rank (r) dimensions on Opportunistic Tasks (Retrospective vs. Prospective Test Sets). Best results are bolded per institution.

		Retrospective								Prospective							
	Rank	Red. RV Sys.	Red. LV Sys.	Pulm. HTN	Atrial Enl.	Vent. Enl.	LA Pressure	RA Pressure	Avg	Red. RV Sys.	Red. LV Sys.	Pulm. HTN	Atrial Enl.	Vent. Enl.	LA Pressure	RA Pressure	Avg
CU	$r = 1$	75.4	75.4	72.0	81.3	67.9	75.6	71.8	74.2	75.2	73.8	70.9	77.4	71.2	76.1	68.6	73.3
	$r = 2$	76.2	75.6	71.9	81.1	77.2	75.2	72.4	75.6	75.4	74.7	71.9	78.0	79.0	76.1	73.6	75.5
	$r = 4$	76.7	76.8	72.4	82.2	80.7	76.6	72.9	76.9	76.1	76.6	71.8	79.2	85.6	77.3	73.3	77.1
	$r = 8$	76.6	77.1	72.4	82.6	80.3	76.9	73.7	77.1	76.2	76.3	72.1	79.0	85.8	77.5	73.6	77.2
WCM	$r = 1$	76.0	72.4	70.9	78.5	64.6	76.0	71.0	72.8	78.4	77.6	73.2	79.9	75.0	77.8	73.2	76.4
	$r = 2$	77.4	72.9	71.0	78.5	68.8	75.4	71.5	73.6	79.0	79.8	75.0	80.0	79.9	78.1	73.5	77.9
	$r = 4$	78.0	74.5	72.1	79.5	72.2	76.5	73.2	75.1	78.2	79.7	75.4	81.6	81.9	79.2	76.2	78.9
	$r = 8$	77.4	74.6	71.9	79.5	73.0	76.6	73.4	75.2	78.8	79.5	75.5	80.9	82.5	79.5	76.0	79.0

Appendix E. Theoretical Analysis of Parameter Efficiency

To analysis the parameter efficiency of introducing LoRA, we analyze the complexity of the hypernetwork with respect to the width of a ViT. Let the ViT base model consists of layers with a hidden embedding dimension of D . A standard weight matrix \mathbf{W}_m (e.g. either multi-head attention or Feed Forward Netowrk (FFN)) typically has dimensions $\mathbf{W}_m \in \mathbb{R}^{D \times D}$. Let d_h be the dimension of the hypernetwork hidden layer.

1) *Naive Full-Rank Generation (Quadratic Complexity)*: In a direct regression scheme, the final projection layer of h_ϕ must output a flattened weight matrix of size D^2 . The number of parameter denoted as P_{full} is given by:

$$P_{\text{full}} = d_h \cdot D^2 = \mathcal{O}(D^2) \quad (2)$$

This shows that full-rank requires quadratic complexity with respect to the ViT hidden dimension D .

2) *Low-Rank Adaptation Generation (Linear Complexity)*: By adopting LoRA, h_ϕ bypasses the generatioin of full matrix \mathbf{W}_m . Instead, it generates two low-rank matrices \mathbf{A}_m and \mathbf{B}_m with dimensions $\mathbf{A}_m \in \mathbb{R}^{r \times D}$ and $\mathbf{B}_m \in \mathbb{R}^{D \times r}$. The number of parameters P_{LoRA} in this case is:

$$P_{\text{LoRA}} = d_h \times D \times 2r = \mathcal{O}(D) \quad (3)$$

since r is fixed and $r \ll D$. The complexity is now linear with respect to D . This analysis demonstrates that integrating LoRA into the hypernetwork architecture reduces the parameter complexity from quadratic to linear with respect to the ViT hidden dimension D . This significant reduction enables the practical deployment of hypernetwork-based multi-task learning in large-scale medical imaging applications.

Appendix F. Opportunistic screening label curation

Table 10: Clinical Definitions for Cardiovascular Condition Curation

Condition	Clinical Criteria for Presence
Left Atrial Filling Pressure (Elevated)	Considered present if any of the following echocardiographic findings are true: <ul style="list-style-type: none"> • Mitral inflow E/A ratio ≥ 2 • OR Indexed Left Atrial Volume (LAVI) $> 34 \text{ mL/m}^2$ • OR Peak Tricuspid Regurgitation (TR) velocity $> 2.8 \text{ m/s}$
Right Atrial Filling Pressure (Elevated)	Peak Tricuspid Regurgitation (TR) velocity $> 3.4 \text{ m/s}$
Reduced Right Ventricular (RV) Systolic Function	Qualitative assessment of RV systolic function is anything other than 'normal' (e.g., 'mildly', 'moderately', or 'severely' reduced).
Reduced Left Ventricular (LV) Systolic Function	Left Ventricular Ejection Fraction (LVEF) $< 50\%$
Pulmonary Hypertension	Estimated Pulmonary Artery Systolic Pressure (PASP) $> 35 \text{ mmHg}$
Atrial Chamber Enlargement	Indexed Left Atrial Volume (LAVI) $> 34 \text{ mL/m}^2$
Ventricular Enlargement	Considered present if the Left Ventricular internal dimension in diastole (LVIDd) meets either of the following gender-specific criteria: <ul style="list-style-type: none"> • For female patients: LVIDd $> 5.3 \text{ cm}$ • OR for male patients: LVIDd $> 5.9 \text{ cm}$

Appendix G. Conventional screening label prompt

System Prompt: Radiology Expert Assistant

"" You are a highly experienced radiology expert assistant. Your task is to analyze a CT chest radiology report and determine, for each of the 18 abnormalities listed below, whether it is:

- Present (label 1): The report explicitly describes or clearly implies the abnormality.
- Absent (label 0): The report explicitly states that the abnormality is not present.
- Not mentioned (label -1): There is no reference to the abnormality anywhere in the report.

Return your answer as a single JSON object that contains all 18 keys exactly as shown, with each value set to 1, 0, or -1.

Abnormalities and Their Definitions:

1. "Medical material" Definition: Any foreign medical objects or devices (e.g., central venous catheters, surgical clips, pacemakers, stents, fixation hardware). Example Clues: "central venous catheter present" or "surgical clips" indicate presence.
2. "Arterial wall calcification" Definition: Calcification along the walls of arteries, suggesting atherosclerotic changes. Example Clues: Phrases like "atherosclerotic calcification" in arterial structures.
3. "Cardiomegaly" Definition: Enlargement of the heart silhouette. Example Clues: "heart is enlarged" (present) or "borderline enlarged heart" (present) or "normal heart size" (absent).
4. "Pericardial effusion" Definition: Fluid accumulation within the pericardial sac. Example Clues: "pericardial effusion" or "small pericardial effusion" (present).
5. "Coronary artery wall calcification" Definition: Calcifications within the walls of the coronary arteries. Example Clues: "calcification of the coronary vessels."
6. "Hiatal hernia" Definition: Protrusion of a portion of the stomach through the diaphragm into the chest cavity. Example Clues: Any mention of "hiatal hernia."
7. "Lymphadenopathy" Definition: Enlargement of lymph nodes (mediastinal, hilar, or axillary). Example Clues: "enlarged lymph nodes," "reactive adenopathy."
8. "Emphysema" Definition: Destruction of lung tissue leading to abnormally enlarged airspaces. Example Clues: "emphysematous lung changes," "bullous emphysema."
9. "Atelectasis" Definition: Collapse or incomplete expansion of lung tissue. Example Clues: "atelectasis" or "opacity likely representing atelectasis."
10. "Lung nodule" Definition: A small, round lesion within the lung parenchyma. Example Clues: Descriptions of "lung nodule" or specific measurements of nodules.

11. "Lung opacity" Definition: Areas of increased lung density (e.g., ground-glass opacities, consolidations, patchy opacities). Example Clues: "ground-glass opacity," "consolidation," "patchy opacities."

12. "Pulmonary fibrotic sequela" Definition: Evidence of fibrotic scarring in the lungs, such as reticulations or honeycombing. Example Clues: "fibrotic lung disease," "honeycombing," "UIP pattern."

13. "Pleural effusion" Definition: Accumulation of fluid within the pleural space. Example Clues: "pleural effusion" (specify if small, moderate, or loculated).

14. "Mosaic attenuation pattern" Definition: Patchy areas of differing lung attenuation that can indicate small airway disease. Example Clues: "mosaic attenuation" or "air trapping."

15. "Peribronchial thickening" Definition: Thickening of the tissues surrounding the bronchi, often reflecting inflammation. Example Clues: "peribronchial wall thickening."

16. "Consolidation" Definition: Solidification of lung tissue due to alveolar filling (by fluid, pus, blood, or cells). Example Clues: "consolidation" clearly stated or "no consolidation" when absent.

17. "Bronchiectasis" Definition: Permanent dilation of the bronchial airways. Example Clues: "bronchiectasis" (e.g., "traction bronchiectasis" or "varicoid bronchiectasis").

18. "Interlobular septal thickening" Definition: Thickening of the septa between lung lobules. Example Clues: Phrases like "septal thickening" or "interlobular septal thickening."

Instructions for Analysis: - For each abnormality: - If the report explicitly describes or implies the abnormality, assign a value of 1. - If the report explicitly states that the abnormality is absent, assign a value of 0. - If the abnormality is not mentioned at all, assign a value of -1. - Use all details in the FINDINGS and IMPRESSION sections to guide your labeling. - Ensure the output JSON object contains all 18 keys exactly as listed.

Now, analyze the provided CT chest report and output a JSON object with the 18 abnormality keys set to 1, 0, or -1 accordingly. ""