
Lesion in-and-out painting for medical image augmentation

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Abstract

1 Deep learning(DL) in the medical imaging field suffers from lack of usable data
2 compared to natural image because of the private and sensitive nature of medical
3 data. Also it is a highly imbalanced data because for almost any disease, medical
4 imaging has more patients not having it rather than having it. To address these
5 problems, synthetic data generation is considered to be a promising solution. In
6 this study, we present Lesion In-aNd-Out Painting (LINOP) to generate synthetic
7 medical images for data augmentation. Generative model based on Mask Aware
8 Transformer (MAT) architecture was used to synthesize lesions onto normal im-
9 age (inpainting) and synthesis outside of lesion area (outpainting). We train and
10 validate a lesion inpainting pipeline on mammography dataset and a lesion outpaint-
11 ing pipeline on chest X-ray dataset. For mammography, proposed augmentation
12 showed up to 30.3% improvements on mass localization in terms of mAP@50, and
13 for CXR, up to 10.3% improvements on disease classification in terms of AUROC.

14 1 Introduction

15 In the middle of the remarkable success of deep learning, there has always been a big, well-defined
16 dataset. For instance, ImageNet[1] plays an important role for developing and validating new deep
17 learning algorithms in computer vision. It is also true for the medical imaging field. The release of
18 multiple, large, publicly available Chest X-ray (CXR) datasets has encouraged research interest and
19 boosted the number of publications [2]. This has increased the dialogue among radiologists and data
20 scientists, which serves to guide and move the field forward [3].

21 However, in most cases, the medical imaging field suffers from lack of usable data compared to natural
22 image because of the private and sensitive nature of medical data. Also it is a highly imbalanced
23 data because for almost any disease, medical imaging has more patients not having it rather than
24 having it. To address these problems in medical data, synthetic data generated from DL models such
25 as generative adversarial networks (GAN) is considered to be a promising solution. But generating
26 images showing certain types of disease is challenging and difficult to ensure that the imaging feature
27 of certain disease has been correctly generated.

28 In this study, we present Lesion In-aNd-Out Painting (LINOP) to generate synthetic medical images
29 for data augmentation. Using the inpainting method, it is possible to accurately generate a lesion
30 of the desired size in the desired location. Also, using the outpainting method, the imaging feature
31 of the disease can be clearly preserved. These aspects of inpainting and outpainting approach can
32 improve the reliability and controllability of the generated image compared to the generating entire
33 images. MAT[4] architecture based generative model was used to synthesize lesions onto normal
34 image (inpainting) and synthesis outside of lesion area (outpainting).

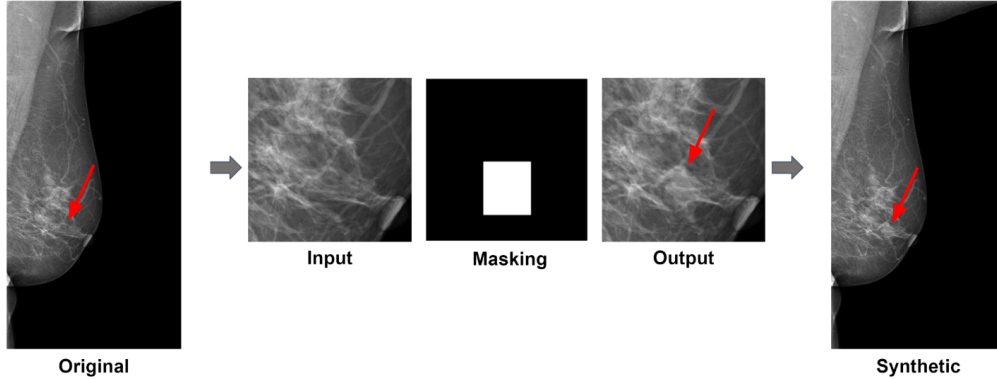


Figure 1: Example of a lesion inpainting on mammography image. The red arrow indicates the synthetic mass.

35 We train and validate a lesion inpainting pipeline on mammography dataset and a lesion outpainting
 36 pipeline on CXR dataset. For mammography, proposed inpainting augmentation showed up to
 37 30.3% improvements on mass localization in terms of mAP@50, and for CXR, proposed outpainting
 38 augmentation showed improvement on 4 class disease classification both on accuracy and AUROC,
 39 up to 11.2% and 10.3% increases respectively. The example of synthetic data generation process is
 40 depicted in Figure 1

41 2 Methods

42 2.1 Dataset

43 **VinDr-Mammo** VinDr-Mammo[5] is a large-scale full-field digital mammography dataset of
 44 5,000 four-view exams, which are double read by experienced mammographers to provide cancer
 45 assessment and breast density following the Breast Imaging Report and Data System (BI-RADS).
 46 Breast abnormalities that require further examination are also marked by bounding box. In this study,
 47 we used "Mass" only images to train the lesion inpainting model, and "No finding" images to generate
 48 inpainting results for data augmentation.

49 **VinDr-CXR** VinDr-CXR[6] is an open large-scale dataset of chest X-rays with radiologist's
 50 annotations. The published dataset consists of 18,000 postero-anterior view chest x-ray scans that
 51 come with both the localization of critical findings and the classification of common thoracic diseases.
 52 These images were annotated by a group of 17 radiologists with at least 8 years of experience for
 53 the presence of 22 critical findings and each finding is localized with a bounding box. The dataset is
 54 divided into the training set of 15,000 scans and the test set of 3,000 scans. In this study, we used
 55 10,478 of "No finding" only images from training set to train the outpainting model, and 4,522 not
 56 "No finding" images to generate outpainting results for data augmentation.

57 2.2 Mask Aware Transformer (MAT)

58 To perform realistic-looking inpainting and outpainting, we used a DL-model based on MAT[4]
 59 architecture. It consists of a convolutional head designed for tokenization, a transformer body that
 60 extracts information through multi-head contextual attention and window shifting, and a Conv-U-Net
 61 used for reconstruction. The shifted window enables cross-window connections to conduct non-local
 62 interactions and the multi-head contextual attention module employs the feature from the partial valid
 63 tokens. In the original work, non-saturating adversarial loss was adopted to enhance the quality and
 64 diversity of the texture synthesis. The non-saturating adversarial loss is formulated as,

$$L_G = -\mathbb{E}_{\hat{x}} [\log (D(\hat{x}))],$$

$$L_D = -\mathbb{E}_x [\log (D(x))] - \mathbb{E}_x [\log (1 - D(\hat{x}))],$$

65 where x and \hat{x} are the real and generated outputs. In addition, the generator was optimized by
 66 employing a perceptual loss. The perceptual loss is expressed as

$$L_p = \sum_t s_i \|\phi_i(\hat{x}) - \phi_i(x)\|,$$

67 where $\phi_i(\cdot)$ is the layer activation of pre-trained VGG-19[7] network, with scaling coefficients s_i .

68 3 Results

69 The MAT-based LINOP model was trained with VinDr-Mammo and VinDr-CXR dataset separately
 70 for 1,000 kimgs on 4 NVIDIA V100 GPUs and choosed the checkpoint that shows the best FID score.
 71 The best FID score for VinDr-Mammo and VinDr-CXR was 6.76 at 840 kimgs and 3.83 at 960 kimgs,
 72 respectively.

73 3.1 Synthetic data generation for mass detection

74 We generated synthetic mass onto a normal mammography image using the proposed inpainting
 75 pipeline. Normal mammography images were fed into the LINOP model trained with VinDr-Mammo
 76 with masking images. The size and location of the masking area determines the size and location of
 77 the mass to be generated. The examples with various mask sizes are shown in Figure 2.

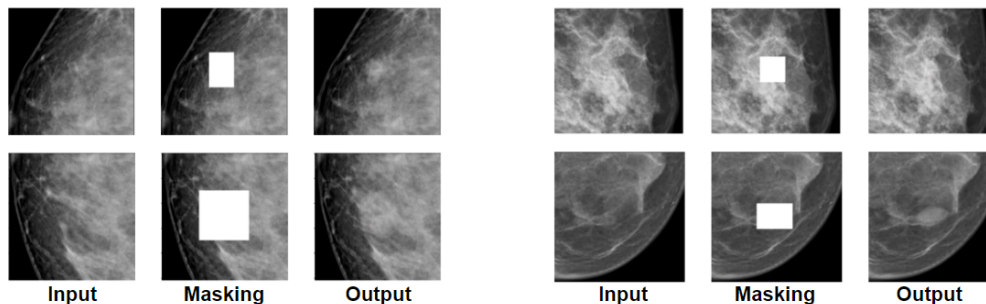


Figure 2: Examples of mass inpainting results with various mask sizes.

78 To evaluate the effectiveness of inpainting augmentation, mass localization of mammography was
 79 performed on images crresponding to normal and mass cases. Cascade R-CNN was trined for object
 80 detection, and original VinDr-Mammo data was randomly split it to 80% training, 10% validation and
 81 10% test set, and the 976 inpainting data was used as training data. Table 1 shows the experimental
 82 results of original only baseline and proposed inpainting augmentation for different portions of data
 83 used. Proposed augmentation showed improvement on mAP@50, up to 30.3% increases.

Table 1: Mass localization performance of original only and proposed inpainting augmentation.

Dataset	mAP@50
Baseline	0.228
+ 50% of inpainting augmentation	0.2814
+ 100% of inpainting augmentation	0.297

84 3.2 Synthetic data generation for disease classification

85 We also generated synthetic abnormal chest x-ray images using the proposed outpainting pipeline.
 86 Chest X-rays with abnormal findings were fed into the LINOP model trained with VinDr-CXR with
 87 masking images. For outpainting, the masking area is where the abnormal finding is, so the generated
 88 image also contains the information of abnormal findings from original images while changing the
 89 other areas which have no information of abnormal findings. The example of this outpainting process
 90 is shown in Figure 3.

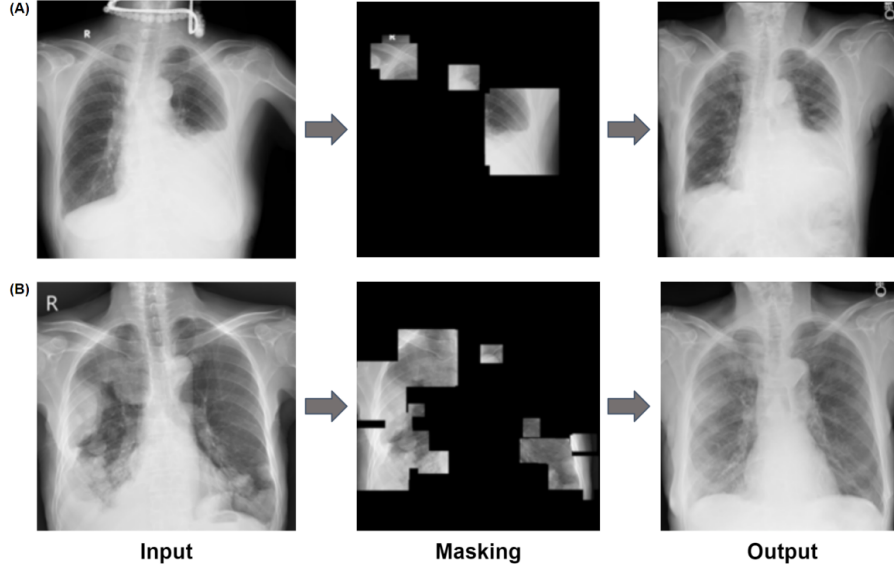


Figure 3: Examples of the proposed outpainting pipeline on chest X-ray image. (A) shows outpainting process of pleural effusion case and (B) shows outpainting process of pneumonia case.

91 To evaluate the effectiveness of outpainting augmentation, 4 class classification of CXR was performed
 92 on images corresponding to normal, pleural effusion, pneumothorax and pneumonia among the total
 93 data. Densenet121 was trained for classification and original VinDr-CXR data was randomly split
 94 it to 80% training, 10% validation and 10% test set, and the outpainting data was used as training
 95 data. Table 2 shows the experimental results of original only baseline and proposed outpainting
 96 augmentation for different portions of data used, from 100% to 12.5%. For all portions, proposed
 97 augmentation showed improvement both on accuracy and AUROC, up to 11.2% and 10.3% increases
 98 respectively.

Table 2: Classification performance of original only and proposed augmentation for different portions of dataset used.

Portion of dataset used:		100%	50%	25%	12.5%
Baseline	Accuracy	0.8113	0.7506	0.723	0.661
	AUROC	0.933	0.8845	0.8387	0.8023
Outpainting augmentation	Accuracy	0.8571	0.8349	0.7912	0.7102
	AUROC	0.9638	0.9528	0.9255	0.8619

99 4 Conclusion

100 In this study, We present the LINOP model, lesion inpainting and outpainting model for medical
 101 image data augmentation. We generated lesion inpainting results using mammography data with
 102 mass and outpainting results with CXR data with various abnormal findings. Using the proposed
 103 method, it is possible to accurately generate a lesion of the desired size in the desired location or keep
 104 the imaging feature of the disease. This approach can improve the reliability and controllability of
 105 the generated image compared to the generating entire images, and is expected to further improve
 106 the quality of synthetic data for data augmentation. Further studies on more modalities of medical
 107 images and lesions, as well as studies verifying the data augmentation effect of generated images,
 108 should be conducted.

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